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# 43 Abstract

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Microscopy is a fundamental approach for plant cell and developmental biology as well as an essential tool for mechanistic studies in plant research. However, setting up a new microscopy-based experiment can be challenging, especially for beginner users, when implementing new imaging workflows or when working in an imaging facility where staff may not have extensive experience with plant samples. The basic principles of optics. chemistry, imaging and data handling are shared amongst all cell types. However, unique challenges are faced when imaging plant specimens due to their waxy cuticles, strong/broad spectrum autofluorescence, recalcitrant cell walls and air spaces that impede fixation or live imaging, impacting sample preparation and image guality. As expert plant microscopists, we share our collective experience on best practices to improve the quality of published microscopy results and promote transparency, reproducibility and data reuse for meta-analyses. We offer plant-specific advice and examples for microscope users at all stages of fluorescence microscopy workflows, from experimental design through sample preparation, image acquisition, processing, and analyses, to image display and methods reporting in manuscripts. We also present standards for methods reporting that will be valuable to all users and offer tools to improve reproducibility and data sharing. 

#### 74 Introduction

75

76 Imaging experiments can provide invaluable mechanistic and quantifiable insights into 77 biological processes, and they have become essential for modern plant biology studies. Light microscopy is arguably the most widely used imaging approach in plants (Berg and 78 79 Beachy 2008; Colin et al. 2022; Gilroy 1997; Ovečka et al. 2018). While other imaging approaches such as electron microscopy (Engel et al. 2015; Otegui and Pennington 2019; 80 Wickramanayake and Czymmek 2023; Wightman 2022; Wilson and Bacic 2012), X-ray 81 microscopy (Duncan et al. 2022; Piovesan et al. 2021), atomic force microscopy (Kirby et 82 83 al. 1996), mass spectrometry imaging (Zou, Tang, and Li 2024), and high-throughput phenotyping (Fahlgren, Gehan, and Baxter 2015) have been applied for plant research, 84 85 light microscopy dominates the literature in plant biology as an accessible, convenient, efficient and powerful approach to address important scientific questions in plant 86 research. Fluorescence microscopy, in particular, can be used to localize fluorescently 87 tagged proteins of interest in cells or tissues. The localization of cellular components. 88 89 such as nucleic acids (Tirichine et al. 2009), polysaccharides (Piccinini, Nirina Ramamoniy, and Ursache 2024), lipids (Chu et al. 2022), hormones (Balcerowicz, Shetty, 90 91 and Jones 2021; Herud-Sikimić et al. 2021), ions or other metabolites (Monshausen, Messerli, and Gilroy 2008) within cells or tissues are readily possible. In addition, 92 93 fluorescent probes can be used to track developmental processes and cellular growth, 94 compare wild type versus mutant or genetically engineered plants and/or compare control 95 versus plants treated with external agents. Samples can be viewed live or fixed during 96 microscopy experiments, depending on the biological question at hand. Often, 97 components of interest (organelles, proteins, metabolites, etc.) will be tagged with 98 fluorescent molecules such as fluorescent protein fusions in live or fixed cells (Berg and Beachy 2008; Haseloff 1999; Wu et al. 2013) including the convenient use of transient 99 100 expression in tobacco leaves or protoplasts, localized via immunolabeling of fixed cells 101 (Baskin et al. 1992; Lee and Knox 2014; Shimamura 2015), or identified using fluorescent 102 stains (Hepler and Gunning 1998; Shaw and Ehrhardt 2013; Yu et al. 2008), all of which 103 are widely used in plant biology. More sophisticated imaging approaches, such as 104 Fluorescence Recovery after Photobleaching (FRAP) (Scheuring et al. 2024), Förster

105 Resonance Energy Transfer (FRET) (Krebs et al. 2012), Fluorescence Correlation 106 Spectroscopy (FCS) (Clark et al. 2016), Fluorescence Lifetime Imaging Microscopy 107 (FLIM) (Noble et al. 2017), Bimolecular Fluorescence Complementation (BiFC) (Waadt 108 and Kudla 2008), multiphoton microscopy (Kurihara et al. 2015; Mizuta 2021), variable 109 angle Total Internal Reflection Fluorescence Microscopy (TIRFM) (Wan et al. 2011) and 110 expansion microscopy (ExM) (Cox et al. 2025; Kao and Nodine 2021) can be used to 111 understand molecular interactions and their dynamics, but these techniques are outside 112 the scope of this review, which is intended as a primer for novice and intermediate 113 fluorescence microscope users.

114 Imaging experiments and analyses must be rigorously designed, and results must be judiciously interpreted and carefully communicated to ensure that the underlying data 115 116 generated support the authors' claims. Indeed, there are numerous considerations and 117 pitfalls that must be accounted for to achieve reliable, reproducible and meaningful results when using fluorescence imaging. Best practices in fluorescence imaging have been 118 119 emphasized in several excellent overviews elsewhere (Lichtman and Conchello 2005; 120 Montero Llopis et al. 2021; North 2006), and while many of the same guiding principles 121 apply to plants, these use cases are typically focused on biomedical imaging using cell 122 culture or animal tissue examples. Here, we provide practical guidelines focused on the 123 fundamentals of fluorescence imaging and solutions for specific and unique challenges 124 that plant biologists often face. These guidelines are aimed at beginning or intermediate 125 microscopists but also offer standards that even advanced users could find useful. Like 126 any scientific pursuit, excellence in imaging is an iterative process that is always grounded 127 in the biological question being asked. We walk users through the steps of fluorescence 128 imaging experiments from initial experimental setup, experimental design, sample 129 preparation, image acquisition, through to data processing and analysis, image display 130 and finally, methods reporting in manuscripts using plant-specific examples (Fig. 1). 131 Importantly, before undertaking a large-scale imaging experiment we suggest a smaller 132 pilot project with an expert mentor following the proposed imaging workflow (Fig. 1). 133 Establishing a "design, test, learn, and iterate" mindset, creates a rapid feedback loop to 134 address any unanticipated challenges and make to any refinements, accordingly. Our 135 collective experience as instructors and microscopists has led us to emphasize the

common insights, misconceptions and pitfalls that newer users may experience.
Ultimately, the goal of this manuscript is to help shorten the learning curve, improve
experimental quality, foster reproducibility, and support success when fluorescence
microscopy is applied to plant research.

140

#### 141 **1. Instrument & Fluorescence Probe Selection**

142 Two of the most important upfront decisions when starting a plant imaging 143 experiment are what probes to use and what type of microscope is best suited to answer 144 the biological question. These two decisions are intrinsically linked. Ideally, one must 145 consider the strengths and weaknesses of a particular imaging platform including 146 assessment of the experimental requirements for lateral (x-y) and axial (z) resolution, 147 acquisition speed, sensitivity (high signal collection efficiency), and spectral (wavelength) separation, in a concept referred to as "Dimensions of Imaging" (Fig. 2). While this chart 148 149 represents common imaging modalities and their representative strengths/limitations, a majority of biological questions can be answered on any of these platforms, albeit with 150 151 some technology-related constraints (reviewed by (Davidson 2024; Ovečka et al. 2018)). 152 Practically speaking, many conventional widefield epi-fluorescence and/or confocal 153 microscopes are suitable for many routine experiments.

154

## 155 *1.1 Choosing an Imaging Platform*

156 Widefield microscopes, which simultaneously illuminate the whole sample with a 157 light source and collect emitted light, are likely to be the most accessible, flexible, affordable and easy-to-use option for plant scientists (Fig. 3). Although widefield epi-158 159 fluorescence microscopy is generally only suitable for thinner samples, deconvolution 160 algorithms can partially restore resolution, contrast and signal using corrections derived 161 from expected (theoretical) or measured (empirical) microscope performance (McNally et 162 al. 1999; Swedlow 2007; Wernersson et al. 2024). The convenience and benefit of 163 widefield microscopes should not be underestimated for many projects, especially for 164 efficiently screening and documenting large sample sets, detecting weak signals (with 165 high-end systems), and/or working with thin or thinly-sectioned materials. For example,

the out-of-focus blur observed using widefield microscopy of a thick plant leaf (Fig. 3A)
can be partially resolved using deconvolution .

168 Laser scanning confocal microscopy (LSCM; also called point scanning confocal 169 microscopy) is another primary workhorse for plant imaging experiments. LSCM excites 170 fluorescent molecules using a laser focused to a point that is raster-scanned across the 171 sample, and a pinhole aperture is used to reject out-of-focus emission light creating thin, 172 high contrast "optical sections" (Fig. 3B & C). When 2D optical sectioning is combined 173 with motorized focus control, z-stacks can be generated and reconstructed into 3D 174 perspectives (Fig. 3: compare Widefield 3D, Confocal 3D & Super-Resolution 3D). A 175 drawback of LSCM is speed (Fig. 2), since it takes time to raster the laser point-by-point 176 across the sample. However, technology such as detector element arrays (e.g., Zeiss 177 Airyscan) can further improve scan speed and resolution of LSCM (Fig. 3G) (Kana, 178 Sediva, and Prasil 2023; Scipioni et al. 2018).

179 When higher imaging speeds are required for cell dynamics studies (e.g., calcium 180 imaging, cytoskeleton dynamics, vesicle trafficking, or fast 3D collection (Oreopoulos, 181 Berman, and Browne 2014; Ueda et al. 2010; Verbančič, Huang, and McFarlane 2021) spinning disk confocal microscopy (Fig. 3E & F) with multiple pinhole optics is often the 182 183 tool of choice. Spinning disk confocal microscopy can capture data at imaging rates of 184 ~100+ frames/second. Practically speaking, imaging rates will be much slower for many 185 experiments. Fast imaging on spinning disk systems reduce photobleaching, relative to 186 LSCM systems. Like LSCM, spinning disc systems can effectively be combined with the 187 benefits of deconvolution (compare Fig. 3E & F).

Super-resolution microscopy (Hickey et al. 2021; Sydor et al. 2015) is appropriate 188 189 when resolution is paramount to visualize features 2-10X below the diffraction limit (~250 190 nanometers with green light) such as with sub-organellar studies (e.g., localization of 191 nuclear structures and pores (Schubert 2017), plasmodesmata (Bell et al. 2013; 192 Czymmek, Duncan, and Berg 2023) and others as reviewed in (Komis et al. 2015; Ovečka 193 et al. 2022)). A few common super-resolution techniques include single molecule 194 localization microscopy (SMLM) approaches, such as photoactivated localization 195 microscopy (PALM) and stochastic optical reconstruction microscopy (STORM), 196 structured illumination microscopy (SIM) and Stimulated Emission Depletion (STED)

microscopy. With these more advanced techniques (Leung and Chou 2011), we strongly
encourage consultation with an expert to assess feasibility and benefits/limitations for
individual research goals.

200 Another factor to consider is whether the best microscope to use is upright (the 201 objective lens above the sample) or inverted (the objective lens below the sample) or 202 vertical (the objective lens and sample both horizontal). In general, upright and inverted 203 configurations are readily amenable to traditional slide mounted specimens, although 204 dipping lenses (that can directly contact the specimen medium) are primarily used with 205 upright configurations (see 2.1 Tips for Working with Live Samples). Inverted microscopes 206 can work well with certain live experiments where extra space or access above the 207 objective lens is required, such as for a heating stage, manipulators or multi-well plates.

208 System performance is a function of the entire system's light path, including characteristics of all optical elements (filters, mirrors, objective lens, etc.) and the detector 209 210 (a camera array versus point detector photo-multiplier tube (PMT)). For example, 211 considering just the detector, high sensitivity scientific Complementary Metal-Oxide-212 Semiconductor (sCMOS) cameras can detect up to 95% of photons that reach it (referred 213 to as its quantum efficiency (QE)) compared to ~45% for Gallium arsenide phosphide 214 (GaAsP) photocathode (GaAsP-PMT) or 20% for traditional PMTs and these differences 215 in sensitivities are also wavelength dependent (Montero Llopis et al. 2021). Ultimately, if 216 weaker signals are anticipated, a more sensitive configuration may be critical.

217

#### 218 1.2 Selecting Fluorescent Probes

219 Once the imaging approach is selected, it is important to determine what light 220 sources/wavelengths and filters are available and to match these with the appropriate 221 fluorescent probe. Here, widefield epi-fluorescence microscopy typically has some 222 flexibility by using low cost and broad-spectrum white light (e.g., mercury or xenon arc 223 lamps, metal halide lamps) or light emitting diodes (LEDs) as light sources (Aswani, 224 Jinadasa, and Brown 2012). Most epi-fluorescence systems use filter cubes (containing 225 filters and a dichroic mirror (specialized optical elements that differentially reflect/transmit 226 light) to separate the excitation/emission light path (Supplementary Fig. 1) matched to 227 the corresponding wavelengths appropriate for imaging the selected fluorescence

228 probe(s). While the majority of systems will have common filtersets for Blue (e.g., UV 229 dyes, DAPI, Calcofluor White), Green (e.g., GFP, FITC, AlexaFluor 488) and Red (e.g., 230 RFP, mCherry, Rhodamine, Texas Red, AlexaFluor 546, Propidium Iodide) fluorophores, 231 other fluorophores (e.g., CFP, YFP) or longer wavelength fluorophores (e.g., chlorophyll 232 A/B autofluorescence, Cy5 and AlexaFluor 660, or near-infrared probes) may require 233 additional appropriate filters. Furthermore, filtersets can be long pass (having a wide 234 emission range, e.g., 500 nm and all wavelengths above) or band pass (having a narrow 235 emission range, e.g., 500 nm - 550 nm), and this distinction can have important 236 implications for the experiment. For example, when working with leaf tissue, chlorophyll 237 autofluorescence (650nm - 700nm) will often contribute undesirable signal (bleed-through 238 or crosstalk) to the emission spectra of most lower wavelength fluorophores in the absence of band pass filters. Likewise, multiple fluorophore imaging almost always 239 240 requires band pass filters to separate different fluorophores.

Many laser-based imaging systems, such as LSCM or spinning disk microscopes 241 242 have discrete high-powered laser lines (e.g., 405 nm, 488 nm, 514 nm, 561 nm and 640 243 nm) or broader spectrum and/or tunable excitation ranges (e.g., white light or multi-photon 244 lasers). Dichroic mirrors, filters, prisms, and/or diffraction gratings separate the excitation 245 and emission pathways (Fig. 4) in laser-based systems. Notably, prisms and diffraction 246 gratings in the emission pathway can be combined with sliders that are user definable, 247 which allows flexible wavelength ranges and spectral imaging of fluorophore emission 248 signals. Spectral imaging, in which a series of images collected at continuous discrete 249 wavelength bands (e.g. 10 nm windows) along a defined spectrum (e.g., 400-600 nm) 250 can be used to generate emission fingerprints and processed via linear unmixing to 251 separate closely overlapping fluorophores. This capability is especially useful to help 252 remove (unmix) various forms of plant autofluorescence that may contaminate target 253 signals and/or to separate closely overlapping fluorophores (Conéjéro et al. 2014; 254 Hardham 2012) to allow more fluorescent probes to be used in an experiment 255 (Zimmermann et al. 2014). See 3.2 Controls on strategies to ensure that crosstalk does 256 not impact multi-color experiments.

Ultimately, the microscope's excitation and emission configuration and the fluorescent probes need to be carefully matched. However, there is some forgiveness

259 with filtersets and fluorophore choice, allowing sufficient excitation and emission signals 260 to be collected even if not perfectly matched (e.g., a GFP filterset can be used to image 261 YFP in many cases). Nevertheless, when fluorophore choice is flexible in experimental 262 design and/or target molecule(s) are of low abundance and optimized conditions are 263 critical, it is prudent to determine system light sources and excitation/emission 264 configuration and to refer to excellent publicly available tools for optimizing probe choices 265 with system configuration (Fig. 4). See FPbase.org (Lambert 2019) for fluorescent 266 proteins, (SpectraViewer 2024) for common organic dyes, and (Colin et al. 2022; 267 Malabadi, Teixeira Da Silva, and Nataraja 2008; Stewart 2001) for plant-specific 268 genetically encoded probes.

269 When constructing genetically encoded fluorescent protein fusions, there are 270 important considerations beyond fluorophore selection, including promoter selection and 271 fluorescent protein fusion orientation. For example, the choice of promoter, fluorescent 272 protein, and fusion orientation can all have profound effects on the behavior of actin 273 binding fluorescent probes for visualizing the plant cytoskeleton (Dyachok et al. 2014; 274 Wang, Yoo, and Blancaflor 2008). Additionally, consider using a monomeric version when working with fluorescent protein fusions i. Multimerization of fluorescent proteins is very 275 276 common and while it can improve brightness, it can cause aggregation, affecting the 277 localization pattern and/or function of target proteins (Campbell et al. 2002; Segami et 278 al. 2014).

Ideally new fluorescent protein fusions are tested for functionality by the ability of the
fusion protein to complement knockout mutant phenotypes before conducting imaging
experiments.

282 Simply matching a fluorophore and system configuration is not always sufficient. 283 The properties of a fluorophore also can play a role in imaging success, such as its 284 pH/environmental sensitivity, size, photostability (resistance to bleaching) (Colin et al. 285 2022; Duwé and Dedecker 2019; Shaner et al. 2013; Tanz et al. 2013; Voss, Larrieu, 286 and Wells 2013) and its overall brightness. Brighter probes allow for more gentle 287 imaging (lower excitation power), improved signal-to-noise and faster acquisition times, 288 which are all particularly important for live-cell imaging. The relative brightness of a 289 probe can be calculated as the extinction coefficient (EC - likelihood of a fluorophore

290 absorbing excitation light) multiplied by the guantum yield (QY - the fraction of absorbed 291 photons that result in fluorescence emission) divided by 1000 (McNamara 2024). For 292 example, Enhanced GFP (EGFP) (EC = 55,900, QY = 0.6) has a relative brightness of 293 33.54 while mNeonGreen (EC = 116,000, QY = 0.8) has a relative brightness of 92.8 294 and is nearly 3X brighter. Although not all fluorophores are equal, many probes can be 295 used interchangeably without issues. When flexibility is possible (e.g., starting 296 experimental design from scratch) and/or the biological question demands specific 297 conditions (low expression levels, high-speed imaging of dynamic events, multi-298 fluorophore imaging, autofluorescence challenges, etc.), optimizing probe choice for the 299 biological question and the imaging system will increase the chances of a successful 300 outcome and allow far greater versatility in imaging approaches across the dimensions 301 of fluorescence imaging (Fig. 2).

302

# 303 2. Sample Preparation and Mounting

304

A critical step of successful plant imaging is sample preparation. There are at least four very important questions that should be part of that decision-making process: 1) Will the sample be live or fixed? 2) What microscope/objective lens is required to achieve the imaging goals? 3) How will the sample be mounted to ensure adequate optical quality? and 4) What controls are required to ensure that image features are not a result of optical, fixation, or other preparation-induced artifacts?

311

# 312 2.1 Tips for Working with Live Samples

313 Imaging living samples is usually convenient and fast (preparation steps are 314 generally less involved) and since samples are not fixed, fixation artifacts can be avoided 315 and dynamic events can be recorded. However, living samples are typically removed from 316 their experimental growth conditions/environment and/or excised before mounting, which 317 can cause substantial changes to the sample, including wounding responses and cell 318 death. Indeed, some dyes tend to stain tissue more guickly at or adjacent to damaged or 319 cut regions, leading to the temptation to image these sites (Truernit and Haseloff 2008). 320 Users should avoid imaging areas of cell damage or death (unless scoring viability), since 321 these images will not be biologically relevant and will not reflect the reality of healthy, 322 living cells (see 3.4 below). When working with aerial tissues, such as leaves, stems, or 323 flowers, bubbles of air may be trapped between the epidermis and coverslip due to the 324 hydrophobic waxy cuticle. These are relatively straightforward to identify as transmitted 325 light images readily reveal the air bubble edge and the sample itself tends to have higher 326 contrast in those areas. Avoid imaging within these regions as light scattering will severely 327 impact optical guality and affect gualitative and guantitative results. Surface air bubbles 328 can be reduced by adding surfactants such as 0.01% Silwet or Tween-20 (Huynh et al. 329 2022; Zhao et al. 2017) in aqueous sample mounting media. Intracellular air spaces can 330 be infiltrated using gentle vacuum/syringe pressure to replace the air spaces in the 331 spongy mesophyll with an aqueous medium to improve dye staining and optical continuity 332 (**Supplementary Fig. 2**). When working with tissues that lack a waxy cuticle, particular 333 care must be taken during sample preparation and mounting to avoid drying the tissue

334 (Ovečka et al. 2018; Prunet, Jack, and Meyerowitz 2016; Sawchuk et al. 2007; Silveira et 335 al. 2022; Zhu et al. 2020). For deep or long-term imaging, non-toxic and non-cell 336 permeable media with low surface tension and excellent optical and gas-exchange properties may be useful, such as Perfluorodecalin (a component of artificial blood) and 337 338 its derivatives (Littlejohn et al. 2010, 2014). Long-term imaging under the coverslip may 339 lead to the compression of observed samples, which can influence the organization of 340 structures such as the microtubule cytoskeleton, which is mechanoresponsive (Hamant 341 et al. 2008; Jacques, Verbelen, and Vissenberg 2013). These effects can be partially 342 mitigated by using adequate spacers between mounting slides and coverslips that 343 prevent mechanical compression of the tissue and by reducing water evaporation during 344 imaging. For many developmental studies, a more specialized lightsheet (Ovečka et al. 345 2018) or upright microscope configuration with dipping lenses are often the best choice, 346 if available (Silveira et al. 2022; Zhu et al. 2020). When using dipping lenses, samples 347 are often mounted on agar medium in small Petri dishes or other plastic containers. The 348 presence of air bubbles on the surface of the sample and sample movement can pose 349 problems when imaging with dipping objectives, requiring additional preventive measures 350 to avoid artifacts such as localized signal loss and geometric distortions of the sample 351 (Prunet et al. 2016; Sawchuk et al. 2007).

352

## 353 2.2 Tips for Working with Fixed Samples

354 For fixed samples, a broad range of affinity probes are available, such as stains, 355 antibodies, or *in situ* hybridization to detect nucleic acids. Additionally, with appropriate 356 fixation protocols, fluorescent protein signals can be retained (Kurihara et al. 2015; Nybo 357 2012). Samples can be fixed, typically in aldehydes, and imaged intact as a whole mount 358 (Kurihara et al. 2015; Truernit et al. 2008) or prepared for sectioning via hand sections, 359 vibratome (Leroux 2020), cryostat (Knapp et al. 2012; Tirichine et al. 2009) or microtomy 360 (Baskin et al. 1992; Marion et al. 2017). Which sectioning approach is most appropriate 361 will depend on tissue type and size, desired section thickness, probe accessibility needs, 362 and the capabilities of the selected imaging platform. Generally, hand sections will be 363 thicker (millimeter scale) and more variable, vibratome and cryostats can reliably produce 364 sections (tens of microns), while microtomy of resin embedded specimen can yield 365 sections ranging from tens of nanometers to a few microns. To identify an appropriate 366 sectioning strategy, we suggest identifying a publication with similar probe types and 367 imaging goals and/or contacting a domain expert. Antibodies and other larger probes can 368 be used to label sections, or with special treatment to disrupt or remove plant cell walls, 369 such as enzyme or chemical permeabilization, or freeze shattering methods (Celler et al. 370 2016; Shimamura 2015) these large probes can be applied to whole-mount samples. 371 Notably, the fixation strategy and buffers themselves can induce artifacts (Yoshida, Maity, 372 and Chong 2023). When working with fixed specimen, autofluorescence can be a by-373 product of aldehyde fixation, especially glutaraldehyde. Use of 0.1% sodium borohydride 374 (Clancy and Cauller 1998) can help reduce aldehyde induced autofluorescence, and 375 addition of glycine to block unreacted aldehydes (Piña et al. 2022). In some instances, 376 samples can be cleared (Hériché et al. 2022; Kurihara et al. 2015; Sakamoto et al. 2022) 377 and/or mounting media with/without antifade components can be applied to improve the 378 optical homogeneity throughout the sample for high quality, deeper imaging (Bassel and 379 Smith 2016). Photobleaching results in chemical modification of a fluorophore 380 (Mahmoudian et al. 2011) causing the irreversible loss of fluorescence. Antifade agents 381 are chemical compounds that serve as oxygen free radical scavengers, which can reduce 382 photobleaching. However, not all anti-fade agents are created equal, and many do not work effectively or universally for all probes and are toxic for living cells (Ono et al. 2001).
For further reading to help select an appropriate mounting media, we recommend an
excellent primer describing various mounting media components and comparing their
performance (Collins 2006).

387

#### 388 2.3 The Objective Lens, Immersion Medium, Coverslip, & Mounting Medium

For high-resolution imaging of live or fixed samples, the sample mounting medium (the media in which the sample is suspended in between the slide and the coverslip) should be considered as an extension of the objective lens. The mounting medium should be an optically- and sample-suitable solution (water, buffer, etc.) that considers both the sample and the objective lens.

394 Many objective lenses are labeled to use a specific immersion media (the media between the objective and the slide coverslip; e.g., air, water, oil) to achieve their 395 396 designed performance specifications. With the exception of air lenses, a small droplet of 397 immersion media is placed between the front lens element of the objective and the sample 398 coverslip, ensuring optical continuity (no coverslip is used with a dipping lens - see 2.1 399 *Tips for Working with Live Samples*). For more detailed background reading, we highly 400 recommend an excellent overview of the important characteristics and concepts of 401 immersion media (Abramowitz and Davidson 2015).

402 Importantly, the NA of an objective lens has a dependency on the refractive index 403 (RI) of the immersion medium (Keller 1990; Staudt and Hell 2008) and the more closely 404 matched and uniform the RI of the objective immersion medium is to the sample and its 405 mounting medium, the better the image quality (compare Fig. 5A and B, air vs water 406 infiltration). In simple terms, the objective lens numerical aperture (NA) essentially relates 407 to the cone of light that is collected by the lens and represents its light gathering and x-y-408 z resolving power. For reference, common objective immersion media are as follows; air 409 (RI = 1), water (RI = 1.33), glycerol (RI = 1.47), silicone (RI = 1.4) or oil (RI = 1.51). For 410 example, this is illustrated by imaging a uniform 3% agarose gel (RI ~1.33, like many 411 biological tissues) infiltrated with 1µg/ml of fluorescein isothiocyanate (FITC) 412 demonstrating the effect of the objective lens on signal intensity from the coverslip to ~300 413 um deep (Supplementary Fig.3). In this homogeneous sample, there is a notable

414 decrease in signal when using the 20X air lens (NA 0.7) and excellent uniformity with the 415 40X water lens (NA 1.2). Although there is substantial signal attenuation with the highest 416 NA 100X lens (NA 1.4), the 100X lens outperforms these other lenses in resolution when 417 imaging very near the coverslip (**Supplementary Fig. 4**). This example demonstrates the 418 tradeoff between high resolution imaging with a low depth of imaging (e.g. with the high 419 NA, 100X oil objective) and low-resolution imaging with a greater depth of imaging (e.g. 420 with lower NA, 40x water objective). Additionally, even in this relatively uniform sample (Supplementary Fig. 3) and in more complex plant samples (Fig. 5), image quality and 421 422 resolution are degraded due to spherical aberrations (Diel, Lichtman, and Richardson 423 2020: Goodwin 2007) that increase in severity at increasing distances from the coverslip 424 due to RI mismatch. This means the image guality, resolution and signal intensity can degrade rapidly away from the coverslip, compounded by many light-scattering plant 425 426 structures. Even slide-to-slide variations in mounting medium thickness covering the 427 sample can make a measurable difference in fluorescence signals and image quality. 428 Nevertheless, in some instances, it is worthwhile to verify specific experimental 429 requirements and compare images acquired with different objective lenses, for example, 430 a higher NA 100X lens versus a 40X oil objective (Supplementary Fig. 4).

431 Using the proper coverslip is another important component of the optical path, 432 since it will be placed between the sample and the objective lens. The coverslip is 433 therefore included as part of lens design and impacts how light is focused on and 434 collected from the sample. Deviations in coverslip thickness from the manufacturer's 435 specification (typically No 1.5 for high NA lenses) can have a pronounced impact on 436 image quality and data quantification, causing decreased resolution and contrast (Fellers, 437 Thomas J.; Davidson 2024). Even when using the proper coverslip, care must be taken 438 that it is perpendicular to the objective, as tilted coverslips covering thick or uneven 439 samples increase the apparent thickness of the coverslip and introduce asymmetrical 440 aberrations and signal degradation.

441

442 **3. Experimental Design, Image Acquisition and Instrument Settings** 

443

444 3.1 Experimental Bias

445 When designing any experiment, steps should be taken to minimize bias. 446 Experimental biases can affect experimental outcomes and compromise reproducibility. 447 potentially leading to skewed data acquisition, analyses, and conclusions (Lee et al. 2024; 448 Munafò et al. 2017). Biases during image acquisition emerge from two main sources: 1) 449 sample bias, i.e., when specific sections, regions, technical and/or biological replicates 450 are selected for imaging and 2) human/unconscious bias, i.e., visual perception is biased 451 toward the detection of certain features in a non-quantitative way, and thus cannot provide 452 reliable information (Brown 2017; Jonkman 2020; Jost and Waters 2019). Bias can be 453 managed with good experimental design, which may include technical and biological 454 replicates, use of appropriate controls, blinded/randomized samples, automated 455 acquisition, and increased sample size using tiling and/or z-stack acquisition modes. 456 Before acquisition, it is important to set up ways to track raw data, acquisition settings, 457 image processing steps and other parameters that will be required for analysis (Lee and 458 Kitaoka 2018). Steps to limit biases, sample size, number of replicates and any sample 459 processing before imaging should be reported accurately when preparing images for 460 publication.

461

#### 462 *3.2 Controls*

463 Controls are required for the proper interpretation of any scientific data (Baker 464 1984; Lipsitch, Tchetgen Tchetgen, and Cohen 2010; Torday and Baluška 2019), and 465 microscopy is no exception. While controls will be specific for each experiment, common 466 themes emerge. As in any biological experiment, biotic, abiotic and/or chemical 467 treatments need to be compared to mock treatment (i.e., vehicle only) and mutants need 468 to be compared to wild-type control samples. However, imaging experiments also require 469 additional controls. For example, the expression level of genetically encoded reporters 470 (e.g., GFP-fusion proteins) can have a profound effect on their observed subcellular 471 localizations (Lisenbee, Karnik, and Trelease 2003). Fusion proteins should be tested for 472 functionality by their ability to complement corresponding mutant phenotypes and it is 473 best practice to confirm the molecular weight of the fluorescent protein-fusion protein via 474 western blotting to ensure that the fluorophore is not cleaved from the protein of interest 475 (Moore and Murphy 2009). When using affinity probes such as antibodies for

476 immunolocalization (Baskin et al. 1992; Guerin 2023a, 2023b; Shimamura 2015), 477 important negative controls include the use of non-immune serum, pre-immune serum 478 (when available) and samples treated without a primary antibody, but otherwise 479 underwent all of the same processing steps as immunolabelled samples. For nucleic acid 480 localization via *in situ* hybridization, a scrambled probe is an essential negative control 481 (Jiang 2019; Prieto, Moore, and Shaw 2007). Staining protocols should always compare 482 stained samples to unstained controls to evaluate background signal and 483 autofluorescence. Establishing an imaging pipeline with appropriate positive and negative 484 controls is essential to obtain reliable, meaningful and reproducible data, both to enhance 485 interpretation and assist in troubleshooting experimental anomalies.

486

#### 487 *3.3 Autofluorescence and Imaging Multiple Fluorophores*

Experimental conditions should also be established considering background 488 489 autofluorescence and bleed- through. Plants produce many autofluorescent compounds 490 - both generalized and environmentally induced and species/tissue specific. 491 Autofluorescent compounds are often found in the cell wall, plastids or vacuole but may 492 also be cytosolic. Common autofluorescent compounds in plant samples include cell wall 493 lignin in the blue range (400-440 nm), chlorophyll in the red/far-red range (600-800 nm), 494 and cell wall (grasses) or phloem (conifer) ferulic acid/ferulate in the blue range. 495 (Donaldson 2020). Stressed or dying cells often produce secondary metabolites that 496 autofluoresce in the cytosol or vacuole. We refer readers to a detailed list and associated 497 spectra (Donaldson 2020). Autofluorescence will often appear in multiple channels, so 498 checking for fluorescent signals across multiple channels will help identify if a signal is 499 "real" and also identify the best wavelength range for the probe. To further discriminate 500 between autofluorescence and "true" signals, appropriate controls should be used. For 501 example, non-transgenic plants, when using genetically encoded fluorescent reporters 502 (e.g., GFP) or unstained plants, when using dyes or immunofluorescence, should be 503 imaged using identical acquisition settings. The mere presence of autofluorescence does 504 not in itself prevent useful imaging results if proper controls are used; for example, strong 505 fluorescence from the selected probe(s) can often overcome weak or tissue/organelle 506 specific autofluorescence. (Clancy and Cauller 1998)(Piña et al. 2022). If the autofluorescence emission is at a wavelength that is not collected for other fluorophores
in the experiment but provides useful cell structure markers (e.g., cell walls , vacuoles,
chlorophyll etc.) it can provide useful context in imaging studies.

510 When using multiple fluorophores, an important control is to check for and apply 511 strategies to minimize/eliminate bleed-through into other channels (Fig. 4) which can also 512 result in misassignment of emission signals, and particularly false "co-localization". For 513 example, many commonly used dyes, such as propidium iodide and FM4-64, have broad 514 excitation and emission spectra that can be detected across multiple channels. Therefore, 515 a useful approach is to image a specimen across multiple channels to determine if there 516 is any channel bleed-through and then apply strategic selection of excitation wavelengths, 517 sequential imaging and emission filters to limit any crosstalk. (Fig. 4C-F). The sequential 518 excitation and emission strategy (one fluorophore being exited and imaged at a time) 519 along with judicious emission filter settings, is very effective to reduce/eliminate crosstalk 520 of compatible multi-color fluorophore combinations (Fig. 4C-F); however, sequential 521 imaging will be slower compared to a simultaneous approach.

522 When planning to conduct fluorescent intensity measurements, best practice is to 523 image a second fluorophore that should not change under experimental conditions. For 524 example, nuclear-localized fluorescent proteins have been used as internal standards to 525 conduct ratiometric measurements of fluorescent intensity of secreted GFP (Samalova, 526 Fricker, and Moore 2006) and during bimolecular fluorescence complementation (BiFC) 527 experiments (Grefen and Blatt 2012). Autofluorescence can also be useful in this context. 528

## 529 3.4 Controls for Live-Cell Imaging

530 Live cell imaging experiments need to be carefully monitored to avoid imaging 531 dying or dead cells. Best practice includes imaging samples for the shortest possible time; 532 however, with careful sample preparation and appropriate controls, images can be 533 collected over days or even weeks (Czymmek et al. 2004, 2007; Le Gloanec et al. 2024; 534 Gómez-Felipe et al. 2024; Hervieux et al. 2016; Schneider et al. 2022). Environmental 535 conditions should be monitored and controlled, including sample temperature and light 536 conditions, since these can affect cellular dynamics and organization (Fujita et al. 2013; 537 Lindeboom et al. 2013; Wang et al. 2020). Tissue dehydration can also adversely affect

538 imaging, especially for tissues without a waxy cuticle, such as roots. Although the signs 539 of decreasing cell health can vary, some indicators of "dead cell imaging" include 540 decreased or cessation of cytoplasmic streaming and Brownian motion (wiggling) of 541 subcellular components (Chow, Mohammad, and McFarlane 2025); fragmentation of the 542 plasma membrane, vacuole, ER network, and cytoskeletal networks; increased 543 autofluorescence; or cessation of cellular growth. Vital stains can be used to determine 544 whether cells remain alive during established imaging conditions; for example, although 545 propidium iodide is a common counterstain for plant cell wall outlines, and it will stain the cytoplasm and nuclei when the plasma membrane (cell viability) has been compromised 546 (Hoffmann, Mohammad, and McFarlane 2024). Fluorescein diacetate (FDA) or SYTOX<sup>™</sup> 547 dyes (Truernit et al. 2008) are other cell viability stains that can be effectively used in 548 549 plants (Jones et al. 2016). Finally, when imaging cells and/or organs, especially for long 550 imaging experiments, it is prudent to ensure imaging experiments do not alter sample 551 biology. Best practice is to monitor a control specimen that is not subjected to the 552 microscopy experiments to determine if there are differences in the size, shape and 553 developmental stage compared to the imaged specimen.

554

## 555 *3.5 Instrument Settings*

556 Acquisition settings must be consistent when performing quantitative image 557 comparisons. For example, if fluorescence intensity is being compared, the same 558 microscope and acquisition settings (e.g., detector settings (offset/gain), pixel or frame 559 exposure time, averaging, image size, filters, excitation power, objective lens) must be 560 used to image control and test samples. Indeed, many commercial systems conveniently 561 have a "reuse" (or equivalent) function to allow users to reload hardware/software settings 562 from previously acquired data. Although convenient, not all settings may automatically be 563 reapplied so the stored image metadata should be carefully compared with "reuse" 564 settings for all imaging sessions.

565 There are dozens of instrument settings, many often not readily apparent, that can 566 influence measurements for quantitative fluorescence microscopy such as system 567 alignment or laser/light source stability (Pawley 2000). For system hardware, periodic 568 system alignment, regular cleaning and other tests using standard slides by the

responsible core facility or system manager should be performed for quality control assessment of the imaging system. Recently, a kit for evaluating system performance has become available by loan from Bioimaging North America to assess and ensure reproducibility (BINA 2024; Gaudreault 2022; Nelson 2022).

573

## 574 3.6 Background and Dynamic Range

575 Background signals are common in many imaging experiments and will vary by 576 detector type. For example, widefield and spinning disk microscopes have cameras 577 (rather than point detectors like PMTs, or comparable, which are common on LSCMs) 578 and it is common to have gray rather than black (pixels with a zero-intensity value) 579 backgrounds. There may be a temptation to adjust contrast (gain) and brightness (offset) 580 settings, especially on LSCMs, to reduce/exclude background or unwanted signals, 581 increase contrast or to emphasize a feature of interest. Image acquisition conditions 582 should be adjusted to avoid excessive under- or over-saturated pixels (blue or red, 583 respectively in (Fig. 6C-E) to prevent "clipping" or truncation of the data, which can hinder 584 reliable interpretation, cause loss of features and compromise the ability to quantitatively 585 analyze the image. During acquisition, this can be done by adjusting exposure/pixel dwell 586 time, exposure time and or camera/detector contrast and brightness (gain and offset) 587 settings. These same settings should be used to image all samples in a given experiment 588 (i.e., wild type and mutant, or control and treatment). When first setting-up experimental 589 conditions, we recommend leveraging the "range indicator" option available on many 590 imaging systems that will apply a single color to represent black (e.g., blue assigned to 0 591 intensity pixels in an 8-bit image) and saturated/white pixels (e.g., red assigned to 255 592 intensity pixels in an 8-bit image), while all pixel intensities in between these extremes 593 remain greyscale (Fig. 6C-E). Alternatively, a histogram of the image can be generated, 594 representing the pixel intensity distribution of the entire image (Fig. 6C'-E'), for 595 experimental set-up or post processing to reveal "clipping". For quantitative settings 596 across images, it is important that images reflect the truth in a comparable manner, rather 597 than offering an artistic or aesthetically pleasing image. For fluorescence quantification, 598 images should only be acquired using consistent settings without over- and under-599 saturated pixels, as these pixels can skew the results. An exception to this rule is the

acquisition of channels used to determine cell outlines for 2D/3D segmentation because
many image analysis software packages can better detect cell outlines when the signal
is strong (Wang et al. 2025).

603

#### 604 3.7 Photobleaching

605 Even if settings are identical and the imaging system stable, other hardware 606 dependent settings, such as the laser/light power at the sample can adversely impact 607 results. Notably, photophysical effects such as photobleaching can cause an irreversible 608 loss of fluorescence due to a chemical modification of the fluorophore in the presence of 609 light and free radical oxygen (Mahmoudian et al. 2011). These issues are especially 610 problematic when collecting z-stacks or time-lapse experiments (compare Fig. 7A & B 611 with Fig. 7C & D). While improved fluorophore design and free radical scavengers (antifade agents; see also 2.2) help mitigate photobleaching, light/laser power and 612 613 exposure/dwell time settings can also be adjusted to limit photobleaching depending on 614 microscope platform. A quick check to assess photobleaching is to measure the intensity 615 of the sample over time; non-linear intensity-changes over time indicate that significant 616 photobleaching is occurring (**Fig. 7E**). Photobleaching can be reduced by lowering the 617 laser power (in this example from 0.8% to 0.08%) and plotting intensity over time until 618 average intensity remains constant over the expected imaging duration (Fig. 7E) and/or 619 by decreasing image collection time, either by decreasing exposure time on camera-620 based systems, or by increasing scan speed in LSCM systems. Additionally, cropping an 621 image (scanning a smaller bounding area), while maintaining the same pixel resolution 622 with point scanning microscopes is an effective way to limit bleaching of larger tissue 623 areas and increase scan rate. However, zooming to reduce scan area can potentially 624 increase photobleaching and has a squared relationship to the zoom factor. For example, 625 zooming from 1 to 2 concentrates the same amount of excitation light into one-fourth of 626 the area, zooming from 1 to 3 into one-nineth, etc. While lower excitation light and/or 627 faster image collection will decrease signal-to-noise (image quality), keep in mind that 628 noise is inherently present in all images and when the goal is to capture and measure a 629 dynamic process or large volume, maintaining the integrity of the data should outweigh 630 simply having an aesthetically pleasing dataset.

631

## 632 3.8 Objective versus Pixel Resolution

633 The resolution of a given objective lens is fixed and determined by its NA and the 634 wavelength(s) of light being used, known as Rayleigh Resolution Limit (Pawley 2006). 635 The theoretical Rayleigh lateral resolution for an objective lens for fluorescence is 636 calculated: 0.61( $\lambda$ )/NA, and for axial resolution (optical section thickness): 1.67( $\lambda$ )/(NA)<sup>2</sup> (Jonkman et al. 2003, 2020), where  $\lambda$  = wavelength of the fluorophore. Thus, for a GFP 637 638 fluorophore (530 nm peak emission) and 40X 1.1 NA lens, the Rayleigh resolution is 639 calculated to be 294 nm, and optical section thickness of 731 nm. However, depending 640 on the number of final pixels in an image, often the full resolving power of the objective 641 lens is not captured, and may not always be needed. If the full-resolution of the objective 642 is required for an experiment, Nyquist sampling must be met, namely, there must be 643 sufficient spacing of pixels in a 2D and/or 3D image to oversample the smallest resolvable 644 structure by two to four-fold (Pawley 2006). For example, a selected 2D field-of-view 645 imaged with 2048x2048 pixels (pixel size 57 nm) meets the Nyquist sampling for the 40X 646 1.1 NA lens (Fig. 6A), while using 128x128 pixels (pixel size 918 nm) (Fig. 6B) falls far 647 below and subtle features may be lost in an under-sampled image. However, if the goal 648 is simply to count the number of cells or measure cell perimeters, the smaller image size 649 is perfectly adequate, has a smaller file size and is ~250 times faster to collect. 650 Undersampling also can be accomplished by increasing the scan speed by using a 651 smaller frame size on a LSCM system, or by "binning" an EM-CCD (i.e. grouping a square 652 of 2x2 adjacent pixels together into one larger pixel). Importantly, binning can also help 653 with detection of weak signals. It is worth keeping in mind that most journals require 300 654 dots per inch (dpi) pixel resolution for figures. Thus, a 512 x 512 pixel image will be ~1.7 655 x1.7 inches at 300 dpiresolution and this may be inadequate to display the desired feature 656 without acquiring at greater pixel resolutions or interpolation (Fig 6A & B).

657

## 658 4. Image Processing & Analysis

659

660 Image processing and analysis are expansive topics and advanced image 661 processing or analyses are beyond the scope of this primer. Processing and analysis can

662 occur in a variety of software programs, including software that is used for acquisition 663 (such as Nikon Elements, Leica LAS-X, Olympus FluoView, or ZEISS Zen), open source 664 software such as ImageJ, specifically the Fiji distribution (Schindelin et al. 2012), or 665 specialized software such as Imaris, Huygens (Day et al. 2017), CellProfiler (Stirling et al. 666 2021) or MorphoGraphX (Barbier de Reuille et al. 2015; Strauss et al. 2022). Here, we 667 focus on the basics that every plant microscopist needs to address. We will briefly discuss 668 common fundamentals, but refer readers to several excellent general reviews that cover 669 topics such as optimizing image acquisition settings, enhancing image quality, and 670 performing basic measurements for data analysis (Bassel and Smith 2016; Hickey et al. 671 2021; Hobson et al. 2022; Russ 2006; Waters 2009).

672

#### 673 4.1 Documenting Processing Steps

674 Image processing steps include anything that changes an image from its original 675 form. These may include seemingly mundane changes such as adjustments to intensity 676 (e.g., brightness/contrast), background subtraction or thresholding, smoothing or 677 sharpening filters, applying lookup tables (false color of images), cropping, rotating, merging channels, changing bit-depth or resolution, creating z-projections or 3D 678 679 reconstructions and image compression, to name a few. It can also include more 680 advanced processing, deconvolution, segmentation, or use of artificial intelligence with 681 machine- or deep-learning approaches. Importantly, all of these image processing 682 adjustments can alter the pixel values of images, which can dramatically affect any 683 subsequent quantitative image analyses (Halazonetis 2005; Russ 2006). Understanding 684 how detectors (Spring 2001) and processing steps can impact quantitative data will help 685 microscopists make good decisions about processing and analysis (Pawley 2006). For 686 example, when exporting images to work with other software, many confocal microscopes 687 acquire images with dynamic ranges of 8-bit (256 pixel gray levels), 12-bit (4,096 pixel 688 gray levels), or 16-bits (65,536 pixel gray levels), while RGB color images are typically at 689 least 24-bit (8-bits/channel, 16,777,216 colors). When given the choice, 16-bit images (or 690 system maximum) are preferred, as images can be down-scaled to 8-bit for display 691 purposes, but it can't be reverted to 16-bit without loss of information. Likewise, when 692 capturing and/or saving screenshots, color images are typically 8-bit RGB (only 256 total

693 colors) and screenshots do not match the raw data pixel intensity values. Thus, 694 conversion from 16- to 8-bit necessarily rescales the image. Also note that all detectors 695 (point or camera-based) are simply collecting photons which are converted into a digital 696 signal where the relative number of photons collected represents the intensity of the 697 sample at a given position. RGB cameras use a color filter array and point detectors, such 698 as PMTs, leverage user defined emission filters for each fluorescent channel. In either 699 instance a Look Up Table (LUT), black and white or color is typically assigned to reflect 700 the intensity range (Spring 2001). Quantification of pixel intensities must always be done 701 on the original, full bit-depth images, and when converting to 8-bit for display, users should 702 be aware of the image scaling impact. For example, Figure 6C & D shows an example 703 of a single image acquired at one setting but displayed at different intensity scales. 704 Digitally rotating images usually involves interpolating pixel information, which will also 705 change pixel values. Assembling figures in PowerPoint or other presentation software, 706 while convenient for presentations, has the risk of intentional or inadvertent changes in 707 aspect ratio and image data compression, depending on settings. Likewise, converting 708 images to different types (e.g., from TIFF to JPEG) to save disk space or for portability 709 with other software results in lossy image compression which will impact the quantitative 710 and qualitative information in images (Fig. 8) and should only be used for presentations, 711 websites or communications where file-size is limiting. An acceptable option, if space is 712 a concern, is lossless compression formats of TIFF for multi-channel or z-stacks, or PNG 713 files for single images. Overall, when comparing fluorescence intensity between samples, 714 best practices include applying the same preparation steps to all samples, using the same 715 acquisition settings to gather all data, and applying the same processing steps (avoiding 716 irreversible file compression-based loss) to each image before data analysis.

Analysis routines can also range from simple to sophisticated and can be highly customized for specific applications. In general, image analyses involve extracting quantitative information from images, such as object size, object intensity, or the relationship between objects (e.g., ratiometric imaging (Ast et al. 2017; Samalova et al. 2006), colocalization (Lathe et al. 2024), or kymographs (Verbančič et al. 2021; Zhou et al. 2020). Since analyses rely on quantifying pixel/region intensity and/or coordinate values from images, and processing steps will change these values, it is best practice to

conduct analyses on minimally processed or unprocessed images. It is also essential for
users to report the software used (including version number) for image analyses, and all
details of any segmentation and analysis steps applied (including parameters/settings in
any algorithms applied), and how regions of interest were selected for analysis.

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- 729

#### 4.2 Image Analysis in Biological Context

730 Plants have several unique features that should be specifically considered during 731 image analyses. These include autofluorescence, rapid cytosolic streaming, and large 732 central vacuoles. As discussed in 3.3, appropriate controls should be used to assess 733 whether autofluorescence is contributing to the image and to minimize these 734 contributions, especially for any quantitative analyses. For any live-cell imaging 735 experiments, microscopists should consider whether rapid cytosolic streaming might be 736 a confounding factor, since cellular contents can move at speeds up to  $4.2 \,\mu m \, s^{-1}$ 737 (Nebenführ et al. 1999) which may be faster than the interval between images. In z-738 stacks, cytoplasmic streaming can alter the shape of objects, creating an elongated object 739 (Nebenfuhr et al 1999;). In colocalization experiments, cytosolic streaming can decrease 740 the degree of colocalization (Ebert et al. 2018). The large central vacuoles in many plant 741 cell types, including protoplasts and *N. benthamiana* leaf epidermal cells, will push 742 cytoplasmic contents to the edge of the cell, which can cause cytoplasm, ER, tonoplast 743 membrane or plasma membrane signals to be mistaken for each other (Fig. 9). Such mistakes can be avoided by colocalization of known markers with the construct of interest. 744 745 Markers that positively identify many subcellular compartments with different fluorophores 746 are available from stock centers (e.g., the Arabidopsis Biological Resource Center 747 (ABRC) or Eurasian Arabidopsis Stock Centre (uNASC)) for a nominal fee as constructs for transient co-transformation (Nelson, Cai, and Nebenführ 2007) or as stable 748 749 Arabidopsis lines for crossing (Geldner et al. 2009). Alternatively, FM4-64 and PI 750 counterstaining can differentiate between the plasma membrane and the cell wall, 751 respectively, with some exceptions depending on tissue type and image modalities 752 (Galvan-Ampudia et al. 2020). In either case, generating a line scan by drawing a line 753 perpendicular to the plasma membrane and plotting fluorescent intensity of the marker 754 compared to the probe of interest over the length of the line will illustrate whether the

intensity peak of the signal of interest matches the intensity peak of the marker line or
 counterstain (Fig. 9D-F, inserts). Z-stacks can also help to differentiate between different
 compartments, since ER-localized proteins will show characteristic web-like architecture
 in the cortical cytoplasm and peri-nuclear signal (Fig. 9A-C).

759

## 760 4.3 Image Manipulation, Image Integrity and Use of Artificial Intelligence

761 As discussed (see 3.1), human bias can be a large contributing factor in collecting 762 and interpreting data. For microscopists this is further compounded in the digital era by 763 the relative ease with which images can be adjusted, converted or otherwise modified in 764 numerous places along a workflow. Indeed, it was reported that ~2% of accepted papers 765 have either inappropriate modifications and/or manipulation, which can result in 766 misrepresentation of the data (Cromey 2010; Martin and Blatt 2013) or insufficient 767 reporting details (Margués, Pengo, and Sanders 2020) Often in our experience, improper 768 data handling can be unintentional and/or caused by lack of training. Furthermore, 769 considering the power, potential and rapid adoption of artificial intelligence (AI), a growing 770 number of scientific hardware and software solutions (including generative AI) can 771 automate finding, collecting, processing, segmenting, visualizing and analyzing data 772 (Wang et al. 2023). However, the same rules for data analysis and reporting apply when 773 using AI. Namely, any approach that modifies or processes data, AI or other, must be 774 accounted for, users should understand the consequences of these analyses and all 775 processing steps must be reported with sufficient detail to ensure reproducibility. 776 Furthermore, since AI models and training data are evolving rapidly, simply using the 777 same tool does not assure reproducible analyses, especially when using proprietary or 778 otherwise opaque image processing algorithms, and results may vary unless the same 779 version is used and/or a fixed model and training data are used for processing and all 780 analyses.

781

## 782 *4.4 Image Annotation and Presentation*

The specifications of figure assembly are typically provided by each journal, but microscopists must make many decisions about how to display and communicate data. Researchers have created community-driven checklists to improve the quality and

786 reporting of microscopy images in publications (Schmied et al. 2024). These resources offer practical guidance on image preparation, including formatting, color choices, and 787 788 data sharing, as well as best practices for describing image analysis workflows. Basic 789 image annotations should always include scale bars, plus time stamps, if applicable. If 790 multiple images are to be compiled and compared (e.g. wild type vs mutant) matched 791 magnification and a common scale is best. Insets or additional panels, either showing a 792 tissue overview or a zoomed-in view may help orient the reader or highlight elements of 793 interest at increased detail. Similarly, if a z-projection is being performed and images are 794 being compared, the same method (e.g., maximum intensity projection) must be used, 795 and the number of planes projected should be reported and ideally the same amongst 796 samples. When displaying a single channel and/or transmitted light, side-by-side 797 grayscale images are best, as we have done herein (Figs. 6 & 9). When displaying multi-798 channel or multi-color images, application of a cyan, yellow, magenta, green and/or 799 grayscale color-schemes are the most accessible to readers and avoid using a 800 combination of colors that are indistinguishable for color blind people (Jambor et al. 2021); 801 we have provided several different examples of suitable color combinations throughout 802 this manuscript (Figs. 3, 5 & 6).

803

## 804 5. Reporting

805

## 806 5.1 FAIR Principles and Public Repositories

807 Comprehensive reporting is essential for accurate research communication, 808 reproducibility. and data accessibility/reusability. Findability. Accessibility. 809 Interoperability, and Reusability (FAIR) guiding principles outline best practices for data 810 management (Wilkinson et al. 2016). Unfortunately, microscopy methods and micrograph 811 analyses are often vaguely or incompletely described in publications (Heddleston et al. 812 2021; Margues et al. 2018; Montero Llopis et al. 2021). The responsibility to improve 813 reporting lies with authors, reviewers, editors and ultimately with scientific journals. 814 However, we recognize that the complexities of these considerations may be daunting for 815 novice microsocpe users or non-expert reviewers. As a companion, and not replacement 816 for written materials and methods, we provide a straightforward reporting spreadsheet

817 template (Supplementary Table 1) that can be used as a convenient approach to 818 manage details about the samples and imaging setup for each figure. Excellent 819 alternatives are also available to meet diverse lab needs (Heddleston et al. 2021). Ideally, 820 all corresponding original raw data underlying images in the vendor's native format and 821 methods are deposited in an open and public data repository, such as Zenodo (Sicilia, 822 García-Barriocanal, and Sánchez-Alonso 2017) or Open Science Framework (OSF) 823 (Foster and Deardorff 2017). Depending on file size and data type, other publicly funded 824 repositories such as BioImage Archive (Hartley et al. 2022) or Electron Microscopy Public 825 Image Archive (EMPIAR) (Iudin et al. 2016, 2023) may be appropriate. Sharing data via 826 repositories also permits data reuse or meta-analyses by the community. An 827 unambiguous organizational schema for image classification that includes sample type (plant, tissue, and cell type), fluorophore/stain, instrument and image acquisition 828 829 parameters, and any processing steps can facilitate data reuse. While this framework for 830 representing fluorescence imaging data does not currently exist in a mature form and 831 data size is still an issue, other databases, such as the Protein Data Bank (Burley et al. 832 2019), may offer useful lessons for establishing community driven data frameworks, 833 similar to the macromolecular Crystallographic Information Framework (mmCIF), the data 834 standard for structural biology (Westbrook et al. 2022). For now, accurate recording and 835 reporting of all imaging experiment steps promotes reproducibility and can support 836 troubleshooting when experimental outcomes vary or are unexpected. Importantly, good 837 reporting goes hand-in-hand with thoughtful experimental design and recording from the 838 very beginning of the process, thus we recommend consulting the reporting spreadsheet 839 template (Supplementary Table 1) (or a similar alternative) prior to starting each 840 experiment and while conducting experiments.

841

# 842 5.2 Sample Treatment and Microscope Settings

As discussed above, many factors can dramatically influence microscopy data and these must all be reported. For example, the specific fluorophore used or manufacturer and catalog number of any antibodies or dyes must be reported since their spectral and binding properties can vary greatly. Likewise, for fixed samples, a detailed protocol will include manufacturer and catalog numbers for all reagents plus concentration and timing

848 for key steps, such as fixation, washes with buffers and incubation with antibodies. For 849 live cell imaging, environmental conditions during the experiment can have a strong effect 850 on plant cells and the biological phenomenon being studied, including ambient 851 temperature and light conditions, and/or how live tissues were oriented relative to the 852 gravity vector (von Wangenheim et al. 2017) (Supplementary Fig. 5), so these should 853 also be reported. Similarly, microscope characteristics and settings such as imaging 854 modalities, objective properties, excitation and emission optics, and image collection 855 parameters must be reported (Supplementary Table 1).

856

#### 857 5.3 Image Analysis and Statistics

858 Image analysis details must also be reported since software for image processing 859 is constantly evolving. In general, the program/software must be reported (manufacturer 860 and/or citation to publication, including version number), as well as any details of the 861 algorithms applied to the images and the parameters/settings used for application of 862 these algorithms. Some examples include details of brightness & contrast adjustments. 863 background subtraction, denoising, deconvolution, thresholding, and segmentation 864 (Aaron and Chew 2021). Sufficient detail for reproducibility should be provided for any 865 quantification, such as which tissues and cell types were used for quantification, how 866 features were selected for measurements, and how the sample size was calculated. P-867 values are often dramatically overestimated in microscopy experiments (also called "p-868 hacking") by measuring multiple events/objects from a single biological organism or cell 869 but counting each of these events/objects as independent biological replicates (Lord et 870 al. 2020). For example, if 10 plastids were measured from one control plant and 10 871 plastids were measured from one inhibitor-treated plant, then n = 1 for each condition, 872 since differences in the plastids could simply be due to natural variation between the 873 plants, location in the plant or due to the inhibitor treatment (Lord et al. 2020). Many 874 commonly used statistical tests, including the t-test, are sensitive to sample size and data 875 distribution, so oversampling each biological replicate and therefore artificially inflating 876 sample size can dramatically skew conclusions from statistical analyses and data that do 877 not fit a normal distribution may need to be compared via alternative statistical tests. Best 878 practices include clearly defining sample size in methods and figure legends, defining

sample size as the number of independent biological replicates, testing data for
assumptions of common statistical tests (e.g., normality, equal variance), using
appropriate statistical analyses, and plotting data in a transparent fashion (e.g., using a
plot type that displays all data points along with summary statistics).

883

## 884 5.4 Figure/Results Presentation

885 While each journal will have individual requirements for figure preparation, several 886 steps are universal when preparing microscopy figures for publication. Figure and movie 887 legends must include essential information for interpretation, such as scale bars, time 888 stamps, and calibration bars for any non-linear lookup tables (false-coloring of images). 889 Figure legends should also contain clear information about the cell type and 890 developmental stage observed, as well as an indication of whether images are single 891 frame or a projection (e.g. a maximum intensity projection of a z-stack or sum projection 892 of a time series). When direct comparisons are being made between wild type and mutant, 893 or treatment and control, control and experimental images should be displayed in the 894 same fashion.

While the complete list of factors that must be reported for any microscopy 895 896 experiment can seem overwhelming, appropriate methods reporting facilitates research 897 communication, experimental reproducibility, and data accessibility. Therefore, we urge 898 authors and reviewers to make use of the reporting spreadsheet template provided here 899 (Supplementary Table 1) and suggest that scientists collect this information as they 900 conduct their experiments to ensure that microscopy methods are appropriately reported 901 in any resulting publication. While reporting can be complex, regularly updating 902 conventional or electronic lab notebooks through the entire process simplifies data 903 analysis, data interpretation and manuscript preparation (Buckholt and Rulfs 2022).

904

## 905 Conclusion

906

Many factors are involved in obtaining robust and meaningful results when applying fluorescence imaging across diverse scientific questions in plant research. While not exhaustive, the goal of this primer was to bring attention to and provide a guide

910 through some of the most common challenges that arise in plant fluorescent imaging 911 experiments from experimental design to publication. Many common pitfalls in plant 912 imaging can be simply remedied through awareness and training. Ultimately, imaging 913 data can be obtained in many different ways but depending on the experimental goal and 914 how data were acquired, there can be limitations on meaningful interpretation and 915 guantitative results due to lack of adequate documentation and reporting. More 916 importantly, in an effort toward transparency and following FAIR principles we urge the 917 plant science community to accelerate improvements in quality control, efficiency, 918 reproducibility, data availability, and biological insights by adopting these best practices 919 in plant fluorescence imaging.

920

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#### 940 Supplemental Data

941					
942	All original raw microscope image data (Figs. 3, 5, 6, 7, 8, 9, Supplementary Figs. 3, 4 &				
943	5) will be made available as a public repository at Zenodo upon publication				
944	(10.5281/zenodo.14895059).				
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1656 Figure 1: Key steps to imaging experiment workflow. 1) Consider Fluorescence Probe and Instrument Selection which are often interdependent and based on 1657 1658 resource availability. 2) Select appropriate Sample Preparation & Mounting conditions. 3) Image Acquisition includes appropriate experimental design (e.g., 1659 controls) and instrument settings to obtain meaningful qualitative and/or 1660 quantitative results. Multiple imaging modalities and platforms may be useful to 1661 answer different aspects of a scientific question and the experiment setup may 1662 need to be refined depending on preliminary results. 4) Image Processing (if 1663 1664 necessary) with documentation may be performed to facilitate visualization and/or quantification of target features, while 5) Image Analysis will translate image data 1665 1666 into measurable quantitative comparisons of results. 6) Reporting includes 1667 disclosure of any essential parameters to document these steps for reproducibility,

1668	peer review and reader interpretation. Note that this workflow is meant to provide
1669	a useful and logical framework but sometimes workflow order may not necessarily
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Figure 2



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1702 Figure 2: Dimensions of fluorescent imaging (and trade-offs). Selection of the 1703 optimal imaging platform depends on experimental goals. Super-resolution microscopy followed by point scanning confocal microscopy (aka LSCM) provide 1704 1705 the greatest lateral (x-y) resolution, while spinning disk and widefield microscopy 1706 have the best speed for capturing dynamic events. Other criteria of note are the 1707 high signal collection efficiency (sensitivity) of spinning disk and the best z-1708 resolution and wavelength separation with LSCM systems. Wavelength separation 1709 is best with spectral detection (more common in point scanning confocal 1710 microscopes) versus filter-based systems typically used in widefield and spinning 1711 disk systems. All platforms can be used for many plant imaging experiments, but some will perform better than others for certain tasks where resolution, dynamics, 1712 1713 and/or spectral separation are critical. Note that this is a generalized chart and the 1714 exact proportional difference in each dimension is dependent upon the microscope 1715 setup and specific technique employed. 1716

## Figure 3



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1719 Figure 3. Plant leaf and root imaging comparing common fluorescence imaging modes. 1720 (A-D) A comparison of image contrast and detail with cytoplasmic expression of untagged 1721 CFP (cyan) and chlorophyll autofluorescence (magenta) in N. benthamiana leaf 1722 mesophyll cells. (A) 3D Widefield microscopy (z-stack maximum intensity projection) 1723 exhibited the lowest contrast while a single 2D optical section (B) and 3D confocal z-stack 1724 maximum intensity projection (C) showed increased contrast and cellular detail, while (D) 1725 3D super-resolution (z-stack maximum intensity projection) provided the greatest cellular detail (resolution). (E-G) A. thaliana root division zone cell imaging of membrane stain, 1726 FM4-64 (magenta) and Syntaxin of Plants 61 CFP-SYP61 (green) comparing signal-to-1727 1728 noise, contrast and cellular detail from 3i spinning disk without (E) and with (F) 1729 deconvolution to ZEISS LSM980 Airyscan imaging (G); full details of the microscope 1730 hardware, software, and imaging setup for this and all other figures are supplied in 1731 Supplementary Table 1. Scale bars  $A-D = 10 \mu m$ ,  $E-G = 5 \mu m$ .

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#### Figure 4



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Figure 4: Fundamentals of excitation (dashed lines, unfilled curves) and emission 1739 1740 spectra (solid lines, filled curves) and their relationship to microscope excitation (single vertical lines) and emission filters (thick vertical bars). (A) The fluorescence emission 1741 1742 maximum from EGFP (white arrow) when excited with 488 nm laser (vertical cyan line) 1743 and collected with 525/50 (500-550 nm) bandpass emission filter (transparent green thick vertical bar). (B) With suboptimal 458 nm excitation of EGFP (compare white 1744 1745 versus black arrow), there is an ~40% decrease in peak emission intensity compared to 1746 488 nm laser excitation when using the same emission filter as (A). (C) When 1747 performing multicolor experiments, fluorophore selection (including potential 1748 autofluorescence) and imaging setup/strategy must be carefully considered to avoid 1749 detection of emission signal overlap due to crosstalk. Note emission spectra overlap portions (white asterisks) of the EGFP (green filled), mCherry (orange filled) and Alexa 1750 1751 Fluor 660 (red filled) signals. (D) Imaging of one dye at a time with EGFP (488 nm excitation, 525/50 bandpass emission filter) still excites and collects mCherry (orange 1752 1753 arrow) and Alexa Fluor 660 (red arrow) signals, but this sequential imaging limits crosstalk into the EGFP image. (E) Likewise, sequential imaging of mCherry (561 nm 1754 1755 excitation, 610/60 bandpass emission filter) prevents excitation shorter wavelength

fluorophores (i.e., EGFP) and reduces Alexa Fluor 660 (red arrow) crosstalk in the mCherry image. (F) Finally, sequential imaging of Alexa Fluor 660 (640 nm excitation, 700/50 bandpass emission filter) prevents any lower wavelength fluorophore crosstalk into the image. Spectra created using ThermoScientific Fluorescence SpectraViewer (SpectraViewer 2024). 

Figure 5



Figure 5. Comparison of objective lens and sample infiltration medium for live-cell imaging of *N. benthamiana* leaf epidermal and mesophyll cells. Single xz axis images of a tobacco leaf showed dramatically reduced image guality using a lower magnification/numerical aperture (A) 20X Air (NA 0.7) compared with a (B) 40X W (NA 1.1) objective lens. Scale Bar = 5 µm. Due to differences in spherical aberration, leaves that were mounted in water but not infiltrated to remove air spaces (C) 40X W (Air) exhibited reduced intensity and image quality, especially in deeper parts of the tissue, compared to water infiltrated leaves (D) 40X W (Water) or with best match of refractive index when using (E) Perfluorodecalin infiltrated leaves (40X W (Perfluorodecalin). Cell cytoplasm (cyan or green), Chlorophyll autofluorescence (magenta). Refractive Index of air = 1, water = 1.33, perfluorodecalin = 1.313. Scale bars =  $10 \mu m$ .

Figure 6



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**Figure 6.** Pixel resolution and dynamic range on a test sample. (A) An image of an acridine orange stained Convallaria stem section acquired at an image pixel number (2048x2048) and size (57 nm) that met Nyquist sampling requirements and achieved the best possible resolution for a 40X Water (NA 1.1) objective lens. (B) A comparison of the same location as (A) with reduced image pixel number (128x128) and size (918 nm) that did not meet Nyquist sampling but was acquired ~250 times faster. (B) would be sufficient to identify nuclei and measure cell area or shape, but not fine detail of the image (compare

1811	insets for magnified detail with/without Nyquist sampling conditions). Scale bars = 20 $\mu$ m.
1812	Inset scale bars = 5 $\mu$ m. (C) The dynamic range of an 8-bit image can be assessed by
1813	viewing its corresponding histogram (C') and the dynamic range optimized for viewing
1814	and display by selecting min/max (D and D'). It is essential to avoid (E) "clipping" the data
1815	(loss of information) by overexposure as evidenced with a range indicator to show any
1816	saturated pixels (red in E) or by reviewing the image histogram (E') which showed
1817	stacking of pixels at the extremes (magenta arrow). The Zeiss ZEN specific range
1818	indicator was applied in images C - E to show under (blue) and over saturated (red)
1819	pixels. Note: range indicator colors will vary depending on software/ vendor used. Scale
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Figure 7. Effects of laser power on photobleaching. 100 frame time-lapse series of an acridine orange stained Convallaria stem section acquired over 185 seconds, at (A) FRAME 1 B) final FRAME 100 at 0.8% Laser Power (488 nm) showed lower signal intensity in FRAME 100 compared to FRAME 1 due to photobleaching. Decreasing the laser power by 10-fold (0.08% Laser Power) showed comparable signal intensity in Frame 1 (C) versus FRAME 100 (D). (E) Plotting the intensity over time in a region of the cell wall (yellow box) in this sample showed that while the 0.08% Laser Power (blue line) was noisier, it displayed minimal photobleaching compared to 0.8% Laser Power (orange line) where the signal decreased about 30% in this ~185 second time-lapse. Scale bar = 20 μm.

Figure 8



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**Figure 8.** Image formats and lossless (TIFF) versus lossy (JPEG) compression. (A) A 1865 1024x1024 pixel image of an acridine orange stained Convallaria stem section saved as 1866 TIFF compared to JPEG compression (B). (C) Increasing the image brightness of the 1867 TIFF image (A) showed fine texture in vacuoles and no detail loss. (D) Increasing the 1868 image brightness of the JPEG image (B) revealed numerous artifacts and edge effects 1869 from the altered/compressed pixels making this data impossible to reliably quantify. Scale 1870 bar = 20  $\mu$ m.

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#### Figure 9



1876 Figure 9. Distinguishing different membranes in plant cells. (A-C) Mid-plane view 1877 and insert of cortical view of *N. benthamiana* leaf epidermal cells transiently transformed with plasma membrane (PM) marker, PIP2A-mCherry (pm-RK; @Nelson et al 2007@))(A); 1878 cytosolic marker, untagged GFP (B), and the synthetic mCherry-tagged endoplasmic 1879 reticulum (ER) marker er-RB (Nelson et al 2007) (C). The main panels show a cell around 1880 1881 its mid-point, while the insets show a region of the same cell but close to its cortex. The 1882 dotted lines mark the areas shown in inserts. Arrowheads indicate transvacuolar strands. 1883 (D-F) Border regions between N. benthamiana leaf epidermal cells transiently co-1884 expressing markers for PM (pm-RK, magenta) plus cytosol (untagged GFP, green) (D), ER (er-RB, magenta) plus cytosol (untagged GFP, green) (E), and plasma membrane 1885 (pm-RK, magenta) plus ER (er-GB,green) (F). Chlorophyll autofluorescence is yellow. 1886 1887 Inserts show line scan analyses for the white lines drawn in the main panels. The X-axis 1888 of the graph corresponds to the position along the line (the total line length is  $4.2 \mu m$ , 3.5μm, and 4.9 μm in D, E, and F, respectively), while the Y-axis shows the fluorescent 1889 1890 intensity for both channels at each point along the line. Note the differences in the relative

1891	position of the peaks from the two channels. All images were subjected to deconvolution
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## **Supplementary Figure 1**

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1926 **Supplementary Figure 1.** A simplified upright fluorescence microscopy light path. The 1927 light source is directed through a dichroic filter cube which contains an excitation filter, a 1928 dichroic mirror, and an emission filter. The excitation filter is used to select the excitation 1929 wavelength and the dichroic mirror reflects the light through to the objective lens, which acts as a condenser, focusing the light into the specimen. Fluorescence emission signals 1930 1931 will be generated at longer wavelengths which pass back through the objective lens and then are transmitted through the dichroic mirror and emission filter. The emission filter is 1932 1933 used to define what wavelengths match the target signal (e.g., GFP) and the signal is 1934 collected by the detector (e.g. camera, photomultiplier tube or other).

# **Supplementary Figure 2**



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**Supplementary Figure 2.** Low-cost method of sample preparation of leaf tissue. (A) 6 mm biopsy punch, 10 ml syringe and parafilm strips. (B). C) Using proper PPE, use a 6 mm biopsy punch and rubber stopper behind the leaf to remove leaf disks (D). (E) Add or draw up water, buffer or buffer with stain into the syringe to desired level, remove the plunger (F), add leaf disks, replace plunger and while orienting the syringe with tip upward (H), carefully push out any trapped air. Note the leaf disk has a light coloration due to air within the mesophyll. While pressing at the syringe tip with an index finger to close off the

aperture, gently pull the syringe plunger to create a vacuum and note air bubbles coalescing on the leaf surface (I), release the index finger and the surrounding solution will enter the leaf, replacing the air spaces (J). Repeat the cycles a few times until the entire leaf darkens (K). (L) Using double-sided adhesive spaces, (M) mount onto a standard glass slide. (O) Add a small drop of water/buffer solution to the center of the well, (P) place the leaf disk onto the drop in desired orientation (e.g., adaxial/or abaxial facing up). To minimize air trapped between the coverslip and leaf surface, (Q) place a small drop of solution on a 22X30mm coverslip, quickly invert, (R) align and (S) place the coverslip onto the adhesive chamber and gently press along edges to seal. (T) Inspect to ensure minimal air bubbles between the tissue and the coverslip. Small bubbles adjacent to the leaf disk are acceptable if not interfering with leaf surface imaging. 

# **Supplementary Figure 3**



**Supplementary Figure 3.** Quantitative imaging of thick samples can be impacted by objective lens choice. This objective comparison showed XZ axis images that extended from the coverslip (top) to ~300 µm z-depth (bottom) of a FITC infiltrated agar slab with similar optical properties to living tissue. Each hash mark represents 50 µm. Signal Intensity using a low magnification/numerical aperture 10X Air (NA 0.3) or intermediate magnification/numerical aperture water immersion 40X Water (NA 1.1) was greater and more uniform with increased depth than the 20X Air (NA 0.70) or 100X Oil (NA 1.4) largely due to spherical aberration. However, the 100X NA 1.4 lens outperforms these other lenses in resolution when imaging very near the coverslip

## **Supplementary Figure 4**



Supplementary Figure 4. 40X and 100X oil objective lens comparison of A. thaliana root division zone epidermal cells using spinning disk confocal microscopy. (A) Overview and (B) digital zoom image of *A. thaliana* root imaging of membrane stain, FM4-64 (magenta) and Syntaxin of Plants SYP61 CFP-SYP61 (cyan) collected with a 40x NA 1.3 oil immersion objective. (C) Under the same acquisition settings as (A) but using a 100X NA 1.49 oil immersion objective, a notable loss in signal strength (compare A & C) but rescaling of the histogram (D) showed an increase in contrast and cellular detail (resolution) of CFP-SYP61 vesicles. (A) Scale bar = 20  $\mu$ m, (B-D) Scale bar = 10  $\mu$ m.
## **Supplementary Figure 5**



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Supplementary Fig 5: Dynamics of gravi-dependent amyloplast sedimentation in 2009 2010 Arabidopsis primary roots. (A) Overview of a vertically mounted Zeiss LSM800 2011 confocal microscope compared to a horizontal stage microscope (B) used to image the 2012 Arabidopsis transgenic marker line (Pt-YK) expressing YFP tagged plastids 2013 counterstained with propidium iodide (magenta) for analysis of gravity-dependent statolith 2014 sedimentation. . (C) Dense starch filled amyloplasts (green) sediment towards the 2015 physical bottom of gravity sensing columella cells in Arabidopsis primary roots. (D) In 2016 gravistimulated roots, the sedimentation of these amyloplasts (indicated by white 2017 arrowheads) towards the new physical bottom of these cells can be clearly visualized 2018 when imaged with a vertical confocal microscope. (E) However, the dynamics of 2019 amyloplast sedimentation are lost when images are captured with a conventional 2020 horizontal microscope. Scale bar =  $20 \mu m$ .

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