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1 **Form function relationships underlie rapid dietary changes in a lizard.**

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15

16 **Abstract**

17 Macroevolutionary changes such as variation in habitat use or diet are often associated with
18 convergent, adaptive changes in morphology. However, it is still unclear how small-scale
19 morphological variation at the population level can drive shifts in ecology as observed at a
20 macroevolutionary scale. Here, we address this question by investigating how variation in cranial form
21 and feeding mechanics relate to rapid changes in diet in an insular lizard (*Podarcis siculus*) after
22 experimental introduction into a new environment. We first quantified differences in the skull shape
23 and jaw muscle architecture between the source and introduced population using 3D geometric
24 morphometrics and dissections. Next, we tested the impact of the observed variation in morphology
25 on the mechanical performance of the masticatory system using computer-based biomechanical
26 simulation techniques. Our results show that small differences in shape, combined with variation in
27 muscle architecture, can result in significant differences in performance allowing access to novel
28 trophic resources. The confrontation of these data with the already described macroevolutionary
29 relationships between cranial form and function in these insular lizards provides insights into how
30 selection can, over relatively short time scales, drive major changes in ecology through its impact on
31 mechanical performance.

32 **Keywords:** Adaptation, diet, bite force, lizard, finite element models, multibody dynamics

33 Introduction

34 Macroevolutionary changes such as changes in habitat use or diet are often associated with
35 convergent, adaptive changes in morphology. Previous studies have suggested that for
36 macroevolutionary changes to occur, directional selection driven by consistent changes in the
37 environment is needed. Consequently, [Carroll and colleagues \(2007\)](#) suggested that “macroevolution
38 may thus be nothing more than an aggregate of many small events”. Despite the initial assertion that
39 macroevolutionary patterns cannot be predicted from processes at the population level ([Eldredge
40 and Cracraft, 1980](#)), subsequent authors have demonstrated that patterns of variation among taxa
41 can be predicted using population genetics theory ([Arnold et al., 2001](#)). Moreover, in some cases,
42 variation in morphology can be rapid and may drive the subsequent evolutionary trajectory of a
43 population ([Herrel et al., 2008](#)). Indeed, variation in fitness-relevant traits has the potential to rapidly
44 drive a population across a valley of low fitness to a new adaptive peak ([Arnold, 1983; Schluter, 2000;
45 Arnold et al., 2001; Svensson and Calsbeek, 2012](#)), thus potentially driving rapid and seemingly
46 punctuated changes in morphology ([Gingerich, 1983; Eldredge, 1985](#)). Yet, for small-scale
47 population-level variation to facilitate or drive rapid shifts in ecology and potentially allow organisms
48 to reach these new adaptive peaks, this variation in morphology needs to have a significant impact
49 on function. As the link between morphology and function is often non-linear ([Koehl, 1996](#)), even
50 small differences in form may potentially give rise to significant differences in function. For example,
51 since the force output of a musculoskeletal system scales to the second power of linear dimensions,
52 small changes in head dimensions can generate significant differences in bite force ([Herrel and
53 O’Reilly, 2006](#)), which might in turn allow species to access novel resources ([Aguirre et al., 2003;
54 Herrel et al., 2004, 2006, 2008](#)).

55 Herbivory is an attractive ecological strategy that, at least in mammals, has resulted in fast species
56 diversification ([Price et al., 2012](#)) with over 38% of all mammals being considered herbivores
57 ([Atwood et al., 2020](#)). In contrast to mammals, squamate herbivores are rare with merely 2% of all
58 species being considered herbivores ([Cooper and Vitt 2002](#)). Among lizards this value may be as high
59 as 5% ([Meiri, 2018](#)), but herbivory remains an uncommon dietary niche. Among the reasons that
60 have been suggested to have prevented lizards from becoming herbivorous are their small body size
61 ([Szarski, 1962; Ostrom, 1963; Pough, 1973](#)), unspecialized dentition ([Hotton, 1955](#)), and lack of
62 complex food processing ([King, 1996](#)). However, it has since been demonstrated that even small
63 lizards can be herbivorous ([Espinoza et al., 2004](#)) and that complex cusped teeth have evolved
64 associated with an herbivorous diet ([Lafuma et al., 2021](#)). Moreover, herbivorous lizards typically
65 have higher bite forces than insectivorous species ([Herrel et al., 2004; Herrel, 2007](#)) which may allow
66 them to crop leaves from a larger plant. The herbivorous niche in lizards thus appears to be an
67 adaptive peak that is rather difficult to attain and needs to be accompanied by a suite of distinct
68 anatomical and functional specializations.

69 A notable exception to the general idea that herbivory is difficult to achieve in lizards is the
70 previously documented rapid evolution of a largely herbivorous diet in a population of Italian wall
71 lizards (*P. sicula*) roughly three decades after its introduction onto a small islet in the Adriatic ([Nevo
72 et al. 1972; Herrel et al., 2008](#)). Indeed, lizards that were introduced onto the islet of Pod Mrčaru
73 from the neighboring islet of Pod Kopište switched to a diet composed of up to 60% of plants in
74 summer and show physiological adaptations, as well as differences in their microbiome, allowing
75 them to more efficiently extract energy from a plant-based diet ([Herrel et al., 2008; Wehrle et al.,](#)

76 [2020; Lemieux-Labonté et al., 2022](#)). Moreover, in the 36 years since the introduction of these lizards
77 on Pod Mrčaru, they developed larger heads, muscles, and bite forces and changed the shape of their
78 cranium and mandible ([Herrel et al., 2008; Taverne et al., 2021](#)). As the two islets are similar in size
79 and show similar vegetation types and high lizard densities ([Herrel et al., 2008](#)) the ecological drivers
80 of the observed changes in diet remain unclear. Moreover, despite the documented changes in head
81 shape and muscle architecture it remains unclear how these lizards were able to gain a great enough
82 functional advantage to allow them to occupy a new adaptive peak in the fitness landscape (i.e., a
83 plant-based diet). Here, we use dissections, geometric morphometrics, and mechanical engineering
84 tools, including multibody dynamics analysis (MDA) and finite element modeling (FEM), to better
85 understand the functional advantages provided by the rather subtle changes in skull shape and
86 muscle architecture previously documented in these two populations ([Taverne et al., 2021](#)). We
87 demonstrate how an intricate co-evolution of skull and mandible shape with muscle architecture can
88 allow for a more efficient mechanical transfer of forces from the muscles to the jaws, and a more
89 resistant skull configuration when biting. These results provide insights into how subtle phenotypic
90 variation may give rise to fitness-relevant changes in function allowing the rapid transition towards
91 new adaptive peaks and the occupation of novel trophic niches in lizards.

92 **Material and methods**

93 *Quantification and comparison of head shape and muscular anatomy*

94 Thirteen male specimens from Pod Kopište and 14 male specimens from Pod Mrčaru were captured
95 by hand or by noose at the end of the summer of 2013. Their body size (SVL: snout-vent length) and
96 head size was measured with a Mitotoyo digital caliper (± 0.01 mm) and their bite force was measured
97 using a custom-designed bite force set-up ([Herrel et al., 1999b](#)). They were sacrificed by an
98 intramuscular injection of pentobarbital under a permit of the Croatian Ministry of the Environment.
99 Specimens were preserved in a 10% aqueous formaldehyde solution for 48h, rinsed and stored in a
100 70% aqueous ethanol solution.

101 The heads of these 27 specimens were scanned at the University of Poitiers on an Easytom micro-CT
102 (at a voxel size of $24.90 \mu\text{m}$ with the following parameters: X-ray voltage, 90 kV; X-ray intensity, $70 \mu\text{A}$;
103 exposure time, 2000 ms; number of projections, 2500). Scans were imported into Avizo 9.0 (Thermo
104 Fisher Scientific) to segment the mandible and skull which were exported as PLY files. A set of
105 landmarks and semi-landmarks on curves were used to quantify the skull and mandible shape (see
106 [Taverne et al., 2021; Figure S1, Table S1](#)). Semi-landmarks on curves were slid while minimizing the
107 bending energy and all landmarks were aligned by a Procrustes superimposition with the function
108 “gpagen” (“geomorph” package). The function “prcomp” from the *stats* package was used to run a
109 Principal Component Analysis (PCA) on the Procrustes coordinates. A MANOVA on the principal
110 components (PC) cumulatively explaining at least 85% of the variance was run to test for shape
111 differences between populations. The theoretical shapes corresponding to the extremes of the PCs
112 that distinguish populations were visualized using the functions “tps3d” and “shade3d” (“Morpho”
113 package).

114 Five additional male specimens per population were included to quantify variation in jaw muscle
115 architecture (resulting in a total 18 specimens from Pod Kopište and 19 specimens from Pod Mrčaru).
116 Each muscle bundle was extracted by dissecting the left side of the head. Muscle bundles were blotted
117 dry and weighed with a digital balance (Mettler AE100; ± 0.1 mg). The connective tissue surrounding

118 the muscles was digested by submerging the muscles in a 30% aqueous nitric acid solution for 24h.
119 Next, the nitric acid was removed, and a 50% glycerol solution was added to arrest the muscle
120 digestion. Muscle fibers were drawn under a binocular scope (Leica) with *camera lucida* (see [Taverne
121 et al. 2021](#)) and measured using Image J (Rasband 1997). Muscle volume was calculated as the ratio
122 between muscle mass and muscle density (1.06 g.cm^{-3} ; see [Mendez & Keys 1960](#)). The physiological
123 cross-sectional area (PCSA) of each muscle bundle was subsequently calculated by dividing muscle
124 volume by the mean fiber length and was subsequently corrected for pennation angle. The muscles
125 were grouped into four functional groups: the external adductors, the pseudotemporalis group, the
126 adductor posterior, and the pterygoid group ([Table S2](#)). The jaw depressors and the constrictor dorsalis
127 muscles were not considered since they are not involved in jaw closing.

128 Differences in the muscular architecture (muscle volume, PCSA, fiber length) between populations
129 were tested by means of a multivariate analysis of covariance (MANCOVA) with the island as factor
130 and SVL as co-variable, using the function “mancova” from the package “jmv”. Subsequent univariate
131 ANOVAs were used to test which muscle groups were responsible for the observed differences.

132 *Multibody dynamics model design*

133 The skull and the mandible of two males of similar size, one from the island of Pod Kopište (PK), one
134 from Pod Mrčaru (PM), were segmented using Avizo 9.0 (Thermo Fisher Scientific). The 3D models of
135 the cranium and jaw of each specimen were used to build two MDA models. The location of the origin
136 and insertion of each jaw muscle was assessed based on dissections and each muscle was virtually
137 divided into several distinct muscle bundles according to the size of the muscle. The number of bundles
138 used was based on the muscle volume and area of insertion ([Table 1](#)). The coordinates of the sites of
139 origin and insertion of each muscle bundle were determined using Avizo 9.0 (Thermo Fisher Scientific).
140 The mandible was converted into a parasolid format allowing to compute the inertial properties based
141 on a bone density of 1.5 g.cm^{-3} ([Sellers & Crompton, 2004](#)). The skull surface, the mandible parasolid,
142 and the muscle bundle coordinates were imported into MSC ADAMS multibody dynamic simulation
143 software (Santa Ana, CA, USA). The muscle bundles were modelled as contractile springs. Where
144 necessary, muscle bundles were wrapped around the bone to increase the accuracy of modelling
145 ([Gröning et al., 2013; Fig. 1](#)). Muscle PCSAs were corrected by both the pennation angle and the typical
146 10% loss in muscle volume due to tissue preservation ([Kikuchi & Kuraoka, 2014](#)). The maximum force
147 of each muscle ([Table 1](#)) was calculated by multiplying the PCSA by an intrinsic muscle stress of 40
148 N/cm^2 ([Gröning et al., 2013](#)). The MDA models simulated opening and closing of the jaw assuming
149 maximal activation of the bundles when the system was at equilibrium. A food particle was created
150 and aligned perpendicularly to the toothrow of the upper jaw to generate a reaction force due to jaw
151 closing (simulated bite force). To ensure consistency in the output bite force generated by the MDA
152 models, the location of the contact between the food particle and the teeth was prescribed to match
153 the location of the contact between the teeth and the plates of the force transducer used to measure
154 *in vivo* bite force in the field ([Taverne et al., 2020](#)). To run further simulations, the location of the item
155 was then standardized at the middle of the maxillary toothrow, as observations revealed that lizards
156 typically crush prey at that location ([Taverne et al., 2022](#)). The stiffness of the food particle was
157 intentionally set beyond the hardness of prey typically consumed by the lizards to ensure that the gape
158 angle did not change during a biting simulation and to obtain the maximal bite force.

159 *Finite element model design*

160 Two finite-element meshes consisting of about 1.5 million tetrahedral elements (Pk: 1,527,268
161 elements; PM: 1,321,278 elements) were generated in Avizo and imported into ANSYS (ANSYS, Inc.,
162 Canonsburg, PA, USA) for finite element analysis. Bone was assumed to have isotropic homogenous
163 material properties with a Young's modulus of 17 GPa and a Poisson's ratio of 0.3 (Cowin, 2001;
164 Rayfield, 2005). The meshes were constrained at the ventral base of the quadrates (the right side in all
165 three directions, the left in A-P and D-V only) and at two symmetrical bite points in the D-V direction
166 (Fig. 1). The coordinates of these locations were directly exported from ADAMS, with the three-
167 dimensionally resolved forces exported from the MDA solutions then directly applied onto the skull
168 model. The quadrato-jugal and the epipterygoid-parietal ligaments were modelled as tension-only
169 links with a stiffness of 250 N/mm² and a cross-sectional area of 1mm² (Fig. S2). Sensitivity tests were
170 carried out using the Pod Kopište model biting at a 20° gape to quantify the impact of the presence /
171 absence and variation in stiffness of the ligaments (50, 250, and 500 N/mm²) on the stress distribution
172 (Figs. S3, S4). The stress values associated with each element of the mesh were exported into an
173 element table for postprocessing.

174 *Simulations*

175 Four different MDA and FEA models were built: two “natural” models in which the specimens were
176 modelled with their own musculature (PK_PK and PM_PM); and two “theoretical” models in which
177 muscle PCSAs were swapped (i.e., PK_PM: the morphology of Pod Kopište with the musculature of Pod
178 Mrčaru, and PM_PK the morphology of Pod Mrčaru with the musculature of Pod Kopište). These
179 models allowed us to test the impact of changes in cranial morphology and muscle anatomy on the
180 calculated bite force by comparing the results of the simulations. The calculated bite force in each of
181 the four models was calculated for 10 different gape angles, from 0° (closed jaw) to 45° (maximum
182 gape typically attained at the onset of fast closing, Taverne et al., 2022), thereby effectively varying
183 the size of the prey item. For each MDA model, the conversion rate of the total muscle force into bite
184 force was calculated at every gape tested by dividing bite force by the total muscle force and was used
185 to assess the efficiency of a muscle to translate intrinsic muscle force into bite force. The total amount
186 of change in bite force between the two natural models was quantified as it provides direct information
187 on how much the mechanical properties of the masticatory system of the two specimens differ. The
188 amount of change in bite force due to the change in muscle anatomy or to the change in cranial
189 morphology alone was also quantified. This allowed us to estimate the relative contribution (in %) of
190 changes in cranial morphological or in muscular anatomy to generate the observed differences in bite
191 force between the specimens. The role of each muscle in bite force generation was assessed by running
192 MDAs with only one muscle activated at a time.

193 The results of the MDA models were then imported into ANSYS, after having been multiplied by five
194 to obtain realistic absolute loads corresponding to *in vivo* bite forces (i.e. the calculated bite forces
195 were five times lower than the *in vivo* forces). For each model, FEAs were performed at three gape
196 values that mimicked three ecologically relevant scenarios: biting a thin object like a leaf (0°), biting a
197 prey of medium size (20°) and biting a large prey item or a conspecific during for example male-male
198 interactions (45°). Values of stress in each skull element were saved. Specifically, we focused on the
199 von Mises' stress (vMS) and recorded the mean stress values for the whole skull and the variation in
200 the stress along the skull. To do so we divided the geometry into 10 segments of equal length (Fig. 1)
201 and averaged the vMS values within each section. We then calculated the ‘advantage’ of the PM
202 morphology relative to the PK morphology as the percentage of increase/decrease of the mean vMS

203 accumulation along the skull. Finally, we estimated the homogeneity of the distribution of stress by
204 calculating the Shannon's entropy (Shannon, 1948) based on the density distribution of vMS values. A
205 higher entropy reflects a low redundancy and a high disparity in the data. Thus, the 'advantage'
206 provided by the PM morphology was estimated as the proportional difference in entropy between the
207 two models.

208 **Results**

209 *Morphological differences*

210 Lizards from the two islets differ in snout-vent length (Pod Kopište: 62.3 ± 3.7 mm for males; 58.2 ± 3.0
211 mm for females; Pod Mrčaru: 68.3 ± 3.2 mm for males; 62.72 ± 2.9 for females), head length (Pod
212 Kopište: 14.9 ± 0.7 mm for males; 13.0 ± 0.6 mm for females; Pod Mrčaru: 16.22 ± 0.8 mm for males;
213 13.8 ± 0.6 for females), and bite force (Pod Kopište: 17.3 ± 4.6 N for males and 9.6 ± 1.9 N for females;
214 Pod Mrčaru: 27.01 ± 3.2 N for males and 14.8 ± 2.7 N for females).

215 The MANOVA including the first nine axes of the PCA carried out on skull shape (cumulative variance:
216 85.2%) revealed an effect of island (Wilks' lambda = 0.22; $F_{1,25} = 6.861$; $P < 0.001$), especially on PC3
217 (variance = 9.3%; $F_{1,25} = 26.48$; $P < 0.001$) and PC6 (variance = 3.3%; $F_{1,25} = 4.83$; $P = 0.037$). The
218 theoretical shape deformation along PC3 showed that the population of PM had a slightly shorter
219 snout and a more curved quadrate (Figure S5). The MANOVA including the first 9 axes of the PCA
220 carried out on mandible shape (cumulative variance: 85.0%) also revealed an effect of island (Wilks'
221 lambda = 0.40; $F_{1,25} = 2.86$; $P = 0.029$), especially along PC1 (variance = 24.4%; $F_{1,25} = 7.50$; $P = 0.011$).
222 The theoretical shape deformation along PC1 showed that the mandible of the PM population was
223 overall more ventrally curved (Figure S5). The coronoid was medially and caudally thicker, the lateral
224 crest, which serves as the insertion site of external adductors was wider, the retroarticular process
225 shorter, and the joint surface area larger.

226 The MANCOVA carried out on the muscle variables detected significant differences between islands
227 (Table 2). All variables (muscle mass, fiber length, and PCSA) were greater in specimens from Pod
228 Mrčaru. When accounting for body size, specimens from Pod Mrčaru had heavier external adductors
229 and pterygoid muscles, shorter fibers in the AMP, and a greater PCSA of the external adductors and
230 the AMP (Table 3).

231 *Mechanical basis of variation in bite force*

232 The MDAs showed that models with the musculature of the PM specimen always resulted in higher
233 bite forces, and that models with the shape of PM individuals resulted in higher bite forces irrespective
234 of variation in muscle architecture (Fig. 2, Table 4). This held irrespective of the gape tested, and was
235 even exacerbated with an increase in gape. Simulated bite force reached two peaks in the four models,
236 at closed gapes (0° or 5° in PK_PM) and wide gapes (45°) and was minimal at a gape of around 30° /
237 35° . Knowing that the total bite force of the PK and the PM individuals modeled in the present study
238 was 19.1 N and 25.0 N respectively, the simulations showed that the conversion rate of the PM
239 morphology is always higher than in the PK morphology (Fig. 2). The total amount of change in
240 simulated bite force between the two natural models varied between 30.5% (0°) and 37.5% (40°). On
241 average, the relative contribution from the change in skull shape to total variation in bite force

242 increased with gape and varied between 2.41% (5°) and 12.49% (45°), the remainder being explained
243 by variation in muscle architecture (Fig. 3).

244 In all models, the external adductors contributed the most to bite force (on average approximately
245 50%), then the pseudotemporalis (35%), and the pterygoids (15%) (Fig. S6, Fig. S7, Table S3). The
246 relative contribution of the muscles varied with gape; the contribution of the external adductors
247 decreased with gape, while that of the pterygoid increased. The pseudotemporalis group had the
248 highest conversion rate of muscle force into bite force (approximately 30% on average), followed by
249 the external adductors (22%) and the pterygoids (12%) (Figure S7). The conversion rate of the
250 adductors decreased with gape in all models, while the conversion rate of the pterygoids increased,
251 and that of the pseudotemporalis decreased from gape 0° to 30° and increased from 30° to 45°.
252 Compared to the morphology of PK, the PM morphology was associated with higher conversion rates
253 of the adductors for all gapes, of the pseudotemporalis for gapes wider than 10°, and for the pterygoids
254 for gapes wider than 30°.

255 *Structural performance of the skull*

256 The comparison of the two natural models showed that, on average, the von Mises stress magnitude
257 (vMS) in the cranium of PM_PM model was higher than in that in the PK_PK model (from 6% to 17%)
258 (see Fig. 4). Although PM_PM showed lower vMS magnitudes (except for the two most posterior
259 sections of the skull) at a 0° gape, more stress was detected at 20° and 45°. Interestingly, the amount
260 of vMS observed significantly increased with gape in PM_PM, whereas this was not the case in PK_PK.
261 Specifically, the increase in vMS in the PM_PM natural model affected the whole skull (Fig. 4). An
262 increase of 2% to 6% was also observed in the overall entropy in the PM_PM model (Table 5).

263 The PM morphology enabled the mean vMS to decrease by 15% compared to a PK skull model with
264 the PM musculature. The advantage provided by the PM morphology, estimated in percentage of loss
265 in vMS, increased at low gape and was more pronounced in the anterior part of the skull than the
266 posterior part (see Fig. 5). Indeed, the advantage of a PM morphology was 13% to 41% in the snout,
267 9% to 20% in the region of the jugal, and became null or slightly negative in the two most posterior
268 regions (where stress magnitude increased). Specifically, the unloading allowed by the PM skull
269 morphology concerned the maxilla, the vomer, the frontal, the anterior part of the pterygoid, the
270 epipterygoid, the parietal, and the quadrate. On the contrary, the areas that showed higher stress
271 magnitudes included the wings of the prootic and the posterior tip of the pterygoid. Although less
272 obvious when reaching a 45° gape, this pattern of stress distribution was similar at all gapes (Fig. 5).
273 On average, the vMS magnitude increased (from 19% at 0° to 27% at 45°) when a PM musculature
274 rather than a PK musculature was applied to a given morphology. In all cases, the overall level of
275 entropy increased when a PM musculature rather than a PK musculature was applied on a given
276 morphology (from 6% at 0° to 7% at 45°). The PM morphology provided only a small advantage in
277 reducing overall entropy (differences < 5%; Table 5).

278 **Discussion**

279 A significant difference in cranial anatomy and muscle architecture exists between the individuals from
280 Pod Kopište and Pod Mrčaru. The latter showing stronger jaw adductors associated with their larger
281 size and omnivorous diet. Lizards from Pod Mrčaru are bigger than those from Pod Kopište, but the
282 variation in muscle cross-sectional area is not only due to differences in size. This is in line with the

283 results of a previous study comparing multiple populations of *Podarcis* lizards (Taverne et al. 2021).
284 Our results suggest that other factors may impact the differences in muscle architecture. For example,
285 lizards from Pod Mrčaru have stronger pterygoid muscles which have a low moment arm at low gape
286 (Herrel et al. 1999 a,b). As plant consumption typically involves biting at low gape, this suggests that
287 diet might not underpin the differences in the cross-sectional area of pterygoid muscles observed
288 between lizards from the two populations. We rather suggest that biting in the context of intraspecific
289 interactions may better explain this difference. The density of lizards on Pod Mrčaru is roughly five
290 times higher than on Pod Kopište (Herrel et al., 2008; Vervust et al., 2009), increasing the probability
291 of encounters and aggressive interactions. Biting congeners involves biting at large gape which may
292 drive the observed differences in the pterygoid muscle (Donihue et al., 2016). Populations also differed
293 in cranial and mandibular shape. Our results show that lizards on Pod Mrčaru have a mandible that is
294 more ventrally curved, with a wider lateral insertion area for adductor muscles, and a more robust
295 coronoid. The results for skull morphology are less clear and mainly show differences in the curvature
296 of the quadrate and a shorter snout in animals from Pod Mrčaru. The fact that the morphological
297 differences in the cranium are less clear is likely a consequence of the multiple functions that the
298 cranium fulfills (e.g., protection of the central nervous system and of the sensory organs), and the
299 associated constraints and trade-offs. Non-adaptive processes including founder effects or genetic
300 drift after introduction may also have driven the phenotypic differences between the two populations
301 observed here (Kolbe et al. 2012).

302 Our modeling results demonstrate that differences in bite force between the two morphotypes are
303 principally driven by the difference in the total muscle PCSA (Table 2). The *in-silico* estimates of bite
304 force generated by the MDA simulations suggested that the lizards from Pod Mrčaru bite harder than
305 those of Pod Kopište. Yet, subtle differences in cranium and mandible shape also contributed to the
306 observed variation in bite force between the two populations. The comparison of the natural and
307 hybrid models showed that the morphology of Pod Mrčaru enables greater bite forces to be generated
308 in all cases. Moreover, the correlation between bite force and gape parallels the observed relation
309 between conversion rate and gape (Fig. 2). Hence, variation in bite force at different gape angles
310 depends on the proportion of muscle force converted into bite force, which in turn is impacted by head
311 shape. This is further supported by the relative contribution of musculature and morphology to the
312 differences in bite force. Consequently, the relatively subtle shape changes in the mandible and
313 cranium between these two recently diverged populations are responsible for a considerable part of
314 the variation in bite force. This is achieved by modulating the lever-arms associated with the muscle
315 bundles that depend on the variation in skull and mandible geometry as well as differences in muscle
316 size and cross-sectional area.

317 The comparison of the natural models PK_PK and PM_PM highlighted differences in structural
318 performance between the phenotypes of the two populations and revealed that the phenotype of Pod
319 Mrčaru accumulates more stress. Given that the PM model includes a greater total muscle PCSA, this
320 is expected. Moreover, our models confirm that applying greater forces on a given morphology
321 increases the level of VM stress over the skull. But the magnitude of differences in stress due to
322 musculature is greater (19% to 27%) than that observed between the natural models (from 6% to 17%)
323 suggesting that morphology itself might help dissipate stress. Indeed, the PM morphology conferred a
324 clear advantage in dissipating stress compared to the PK morphology (Fig. 5). Similarly, the comparison
325 of the natural models revealed that the phenotype of the Pod Mrčaru individuals had a greater level
326 of overall entropy compared to that of Pod Kopište (from 2% at 0° to 6% at 45°). Again, this is mainly

327 due to an increase in the total muscle force with the application of a PM musculature to a given
328 morphology leading to an overall increase in entropy (from 6% at 0° to 7% at 45°). Interestingly, our
329 results suggest that an increase in the total muscle force is accompanied with an increased disparity in
330 the distribution of the stress over the skull, yet the phenotype of Pod Mrčaru maintained a more
331 homogenous stress distribution.

332 Unexpectedly, the PM morphology was more advantageous than the PK morphology in producing bite
333 force at wide gapes (as revealed by the MDA simulations), whereas it is more advantageous in
334 dissipating stress at lower gapes (as revealed by the FEA simulations). Although this might first seem
335 contradictory, we propose that these two results are not incompatible. We rather think that selection
336 primarily acts upon the performance of the musculoskeletal system (i.e., bite force) within the limits
337 imposed by the intrinsic capacity of the system to dissipate the associated stress and strain. Therefore,
338 the MDA results suggest that the evolution of skull morphology towards a Pod Mrčaru phenotype
339 enabled an optimization of bite force at wide gapes. This is likely driven by intraspecific competition,
340 enhanced by a five-fold increase in population density on Pod Mrčaru (Herrel et al. 2008, Vervust et al.
341 2009). The consumption of hard and fibrous material like plant matter requires repeated and frequent
342 biting (Herrel, Verstappen & De Vree, 1999) to reduce the item into smaller and more easily digestible
343 bite-size pieces (Bjorndal et al. 1990; Bjorndal & Bolten, 1992). The structural advantage provided by
344 the PM morphology at low gapes might be important in this context. Indeed, the repeated loading
345 occurring at low gapes experienced by the skull while feeding on plants is likely to be particularly
346 constraining and might represent an important selective agent driving variation in skull shape. A
347 scenario in which head shape in insular *Podarcis* lizards is initially driven by intraspecific competition,
348 and maintained by functional demands associated with resource use, would be in line with the results
349 of Donihue and collaborators (2016) concerning intraspecific variation in morphology and performance
350 in another *Podarcis* species.

351 Previous comparative studies on the colonization of *Podarcis melisellensis* and *Podarcis siculus* in the
352 Adriatic archipelago and their morphological evolution in relation to variation in ecological contexts
353 (Taverne et al. 2020, 2021) suggested that relationships between form and function were similar at
354 different levels of integration, whether between isolated populations or between species, and even
355 when accounting for phylogenetic relationships. Specifically, convergent evolution of muscle
356 architecture and head morphology were found in similar ecological contexts. Here, we demonstrate
357 that these form-function relationships can evolve on ecological time scales and be associated with an
358 optimization of the mechanical output of the masticatory system. Consequently, subtle morphological
359 variation may accumulate over time and give rise to macroevolutionary patterns.

360 *Future directions*

361 Further efforts might help make the finite element models even more realistic and circumvent some
362 of the current limitations. First, the simulations revealed an unrealistic accumulation of vMS at the
363 very back of the skull (Figs. 4, 5) at the most lateral region of the neurocranium (paraoccipital process
364 of the exoccipital). In the present study, the joint between the lateral process of the exoccipital and
365 the quadrate was modeled as connected and fixed, hence possibly explaining why abnormal stress
366 concentrations are located in this area instead of being more homogeneously distributed. It would be
367 useful to model a ligamentous connection between these bones allowing a better stress dissipation.
368 Second, bone tissue was modeled as an isotropic material here, although it is known to be anisotropic

369 (Moazen et al. 2015). A precise quantification of the bony material properties throughout the skull
370 (Young's modulus) should be undertaken using a nano-indentation approach. A third way to gain
371 accuracy would be to model the sutures and the osteoderms, since they have been suggested to impact
372 how loads are distributed and dissipated (Moazen et al. 2008; Costantini et al. 2010; Jones et al. 2017).

373 *Conclusions*

374 Our results show significant differences in skull form and function in individuals of two populations of
375 *P. siculus*. Following the introduction into a novel environment, the population on Pod Mrčaru rapidly
376 evolved a largely herbivorous diet. Our analyses of shape and function provide a mechanistic
377 underpinning of the link between relatively subtle differences in morphology and the observed
378 changes in ecology. Our results demonstrate that relationships between form and function may drive
379 variation in fitness-relevant performance traits resulting in changes in trophic ecology over a relatively
380 short time scale.

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388 **Author contributions**

389 MT, MJF and AH designed the study. MT, HD, RB, DL, ZT, ACF and AH generated the raw data. MT, PW
390 and MJF built the models. MT analyzed the data and ran the models. All authors were involved in the
391 interpretation of the results, the writing, and the revision of the manuscript.

392 **Data Accessibility**

393 doi:10.5061/dryad.866t1g1vk

394 sharing link: https://datadryad.org/stash/share/uy5-FARWE09mXDedc1SGivCLqz8aqQU6fK16_Ak9L_Y

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514

515 **Figure legends**

516 **Figure 1:** MDA model design illustrating the muscle bundles used of each muscle and their wrapping.
517 A: left lateral view of the skull, B: dorsal view, C: caudal view, D: ventral view. The jaw opener is
518 represented in yellow, the external adductors in shades of blue, the pseudotemporalis in red and
519 orange and the pterygoids in green. E: segments of the skull used to investigate the variation in stress
520 accumulation over the structure (here represented by a ventral view) in subsequent FEA. Note that
521 the bite points and the joints are indicated by white stars and white circles, respectively.

522 **Figure 2:** A: relationship between bite force (in Newtons), estimated by the MDA for the four models,
523 and the gape (in degrees). B: relationship between the conversion rate of the total muscle force into
524 bite force (in percentage) and the gape (in degrees) for all models. The two natural models (PK_PK:
525 including the morphology and the musculature of Pod Kopište, PM_PM: including the morphology
526 and the musculature of Pod Mrčaru) are represented by full lines, whereas the two hybrid models
527 (PK_PM: including the morphology of Pod Kopište and the musculature of Pod Mrčaru, PM_PK:
528 including the morphology of Pod Mrčaru and the musculature of Pod Kopište) are represented by
529 dashed lines.

530 **Figure 3:** Contribution (in percent) of the differences in musculature (in light gray) and skull shape (in
531 dark gray) in explaining the total difference in calculated bite force between individuals from the two
532 islands (Pod Kopište and Pod Mrčaru). The contributions were estimated for every gape tested (in
533 degrees) by comparing the change in calculated bite force induced by the change in musculature or
534 morphology alone (theoretical models) with the change in calculated bite force between the two
535 natural models.

536 **Figure 4:** von Mises stress distribution in the two natural models (Brown lines: PK_PK, green lines:
537 PM_PM) for the three gapes tested (full lines: 0°, dashed lines: 20°, dotted lines: 45°). Stresses are
538 plotted relative to the virtual skull section number (i.e. position along the antero-posterior axis for
539 which results were averaged; see methods). The left lateral, ventral, caudal and dorsal views of the
540 skull are represented (from left to right). Warmer colors are associated with higher von Mises stress
541 magnitudes (in MPa).

542 **Figure 5:** Consequences of skull shape change on the von Mises stress distribution. The graph
543 represents the mean advantage (in %) provided by the PM morphology along the skull (full line: 0°,
544 dashed line: 20°, dotted line: 45°). Here the models PK_PM and PM_PM (PK / Pod Kopište and PM /
545 Pod Mrčaru in the figure) were compared for each of the three gapes tested (see Figure S8 for the

546 alternative combination PM_PK vs. PK_PK). Hotter colors are associated with higher von Mises stress
547 magnitudes (in MPa).