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## RESEARCH NOTE

# Mitral regurgitation quantification by cardiac magnetic resonance imaging (MRI) remains reproducible between software solutions [version 1; peer review: 1 approved with reservations]

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## Abstract

**Background:** The reproducibility of mitral regurgitation (MR) quantification by cardiovascular magnetic resonance (CMR) imaging using different software solutions remains unclear. This research aimed to investigate the reproducibility of MR quantification between two software solutions: MASS (version 2019 EXP, LUMC, Netherlands) and CAAS (version 5.2, Pie Medical Imaging).

**Methods:** CMR data of 35 patients with MR (12 primary MR, 13 mitral valve repair/replacement, and ten secondary MR) was used. Four methods of MR volume quantification were studied, including two 4D-flow CMR methods ( $MR_{MVAV}$  and  $MR_{Jet}$ ) and two non-4D-flow techniques ( $MR_{Standard}$  and  $MR_{LVRV}$ ). We conducted within-software and inter-software correlation and agreement analyses.

**Results:** All methods demonstrated significant correlation between the two software solutions:  $MR_{Standard}$  ( $r=0.92$ ,  $p<0.001$ ),  $MR_{LVRV}$  ( $r=0.95$ ,  $p<0.001$ ),  $MR_{Jet}$  ( $r=0.86$ ,  $p<0.001$ ), and  $MR_{MVAV}$  ( $r=0.91$ ,

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1. Antonio Luna , HT Médica, Jaén, Spain

2. Nay Aung , HT Médica, Jaén, Spain

$p < 0.001$ ). Between CAAS and MASS,  $MR_{\text{Jet}}$  and  $MR_{\text{MVAV}}$ , compared to each of the four methods, were the only methods not to be associated with significant bias.

**Conclusions:** We conclude that 4D-flow CMR methods demonstrate equivalent reproducibility to non-4D-flow methods but greater levels of agreement between software solutions.

### Keywords

Magnetic resonance imaging; Mitral valve insufficiency; Reproducibility of results.

Any reports and responses or comments on the article can be found at the end of the article.

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## Introduction

Mitral regurgitation (MR) is one of the most common types of valvular heart disease and is one of the most frequent indications for valve surgery<sup>1</sup>. Even though echocardiography remains the first-line investigation for MR assessment<sup>2</sup>, recent evidence suggests that cardiovascular magnetic resonance (CMR) quantitative assessment of MR is more precise and has a better prognostic association<sup>3</sup>. One of the key strengths of CMR quantification of MR is that it allows many different ways to quantify MR<sup>4</sup>. These include direct and indirect methods using standard techniques and emerging four-dimensional (4D) flow methods<sup>5</sup>.

Our recent work demonstrated that 4D-flow methods of MR quantification may offer superior precision for reproducibility compared to standard methods<sup>5</sup>. In practice, a combination of standard and 4D-flow methods of MR quantification can be used to build confidence in reporting CMR images and clinical decision-making. Our previous work involved the use of a research software solution from Leiden lab (MASS). MASS is not currently a commercial software package for clinical use and is limited to research applications only. Moreover, there is a paucity of evidence evaluating the reproducibility of MR volume quantification between different software solutions across the breadth of methods<sup>6</sup>. Demonstrating reproducibility between different software solutions is vital as clinical outcome research within CMR imaging is multiplatform and multicentre. It is essential that the data generated from analysis is accurate, precise, and reproducible, regardless of which software platform is used.

The primary objective of this research was to investigate the reproducibility and agreement in MR volume quantification between two software solutions (CAAS, version 5.2, Pie Medical Imaging) using subjects from previously published cohorts spanning the spectrum of MR disease states<sup>5</sup>. Using CAAS, we also conducted within-software agreement analysis between different methods of MR volume quantification. Third, we present interobserver reproducibility analysis within CAAS across the four methods of MR volume quantification.

## Methods

### Study population

The subjects included within this study have been reported on in other published works<sup>5</sup>. In brief, the data relates to a UK multicentre prospective study involving 35 subjects with MR diagnosed on echocardiography. Recruited from outpatient cardiology clinics at two centres with dedicated mitral valve services (Sheffield and Leeds) between January 2015 – December 2020, 12 subjects had primary MR, ten subjects had secondary MR, and 13 subjects had mitral valve replacement (MVR). Patients with significant valvular stenosis and cardiac shunts were not considered eligible.

### Ethics

This study was approved by the National Research Ethics Committee in the UK (17/LO/0283 and 12/YH/0169).

Informed written consent was obtained from all subjects before participation.

### CMR protocol

At Sheffield, CMR was performed on a 3.0 Tesla Phillips Healthcare system (Achieva TX) equipped with a 28-channel coil and Philips dStream digital broadband MR architecture technology. In Leeds, CMR was performed on a 1.5 Tesla Philips Healthcare system (Ingenia).

The CMR protocol included baseline surveys, cines (vertical long-axis, horizontal long-axis, short-axis contiguous left ventricle volume stack, 3-chamber, and aortic root) and 4D-flow acquisition. Cine images were acquired during end-expiratory breath-holds with a balanced steady-state free precession, single-slice breath-hold sequence. Procedures relating to 4D-flow pre-processing were delivered in accordance with established standards of practice<sup>7</sup>.

### Image analysis

Image analysis was completed within two CMR software solutions: MASS software (version 2019 EXP, LUMC, Netherlands) and CAAS MR Solutions (version 5.2). The image analysis and MR quantification methods for the MASS platform are published elsewhere<sup>5</sup>. In CAAS, both aliasing correction and phase offset correction were applied.

In total, four quantification methods for MR were computed within the CAAS platform, aligning with the methods used within MASS (Figure 1). One assessor completed the analysis of all 35 subjects within CAAS, blinded to the data generated from MASS.

#### 1. $MR_{\text{Standard}}$ (LVSV - AoPC)

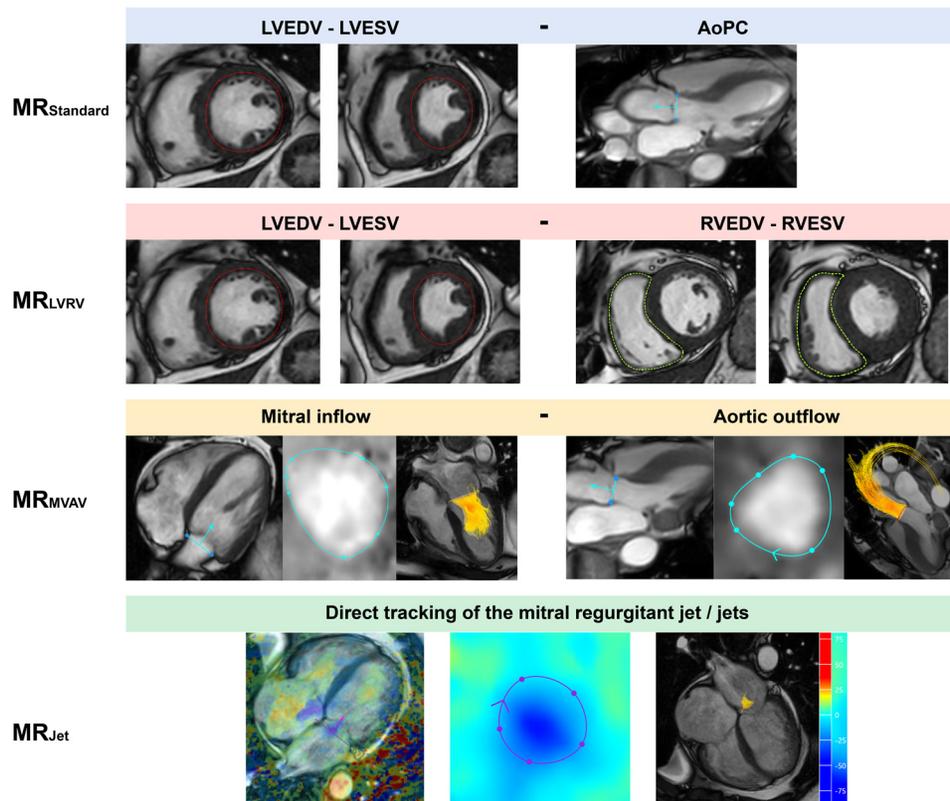
Left ventricular stroke volume (LVSV) was determined through endocardial segmentation of the short-axis cine stack. Aortic stroke volume was obtained using a static reformatted aortic phase-contrast (AoPC) plane through the sino-tubular junction.

#### 2. $MR_{\text{LVRV}}$ (LVSV - RVSV)

Right ventricular stroke volume (RVSV) was determined by segmentation of the RV in the short-axis cine stack. This method was not used in the ten patients with secondary MR, given the regular presence of concurrent MR and tricuspid regurgitation.

#### 3. $MR_{\text{MVAV}}$ (4D-flow mitral forward flow - 4D-flow aortic forward flow)

Using retrospective mitral valve and aortic valve tracking within the four-chamber cine and three-chamber cine, respectively, a phase-contrast, valvular formatted plane was generated. Using the formatted valvular plane, we segmented the forward



**Figure 1. Visual description of the four cardiovascular magnetic resonance imaging mitral regurgitation volume quantification methods investigated within this study.** AoPC - aortic phase contrast; LVEDV - left ventricular end diastolic volume; LVESV - left ventricular end systolic volume; RVEDV - right ventricular end diastolic volume; RVESV - right ventricular end systolic volume.

flow whilst taking into account the through-plane motion of the valve plane.

#### 4. $MR_{Jet}$ (4D-flow direct jet assessment)

Jets of MR were directly quantified from the 4D-flow dataset. The jet(s) were first identified in multiple long-axis chamber views. Where available, the four-chamber view was used to draw a reformatted plane perpendicular to the regurgitant jet within the left atrium for each phase it was present. If multiple, jet volumes were summated to provide a total MR volume.

#### Interobserver reproducibility

Interobserver tests were performed by two investigators (CGC, PG) blinded to the results of each other. A random mix of ten subjects was studied, where each investigator estimated MR volume using the four methods previously described. Each observer had at least two years of CMR experience.

#### Statistical analysis

All statistical analysis were completed using SPSS version 25, though Microsoft Excel could also be used. All continuous parameters are reported as mean  $\pm$  standard deviation (SD).

Statistical parameters to assess inter-software and within-software MR quantification method correlation were calculated using Pearson correlation coefficient. Agreement between methods of MR quantification within-software (CAAS) and between software's (CAAS versus MASS) was calculated using Bland-Altman statistics where the mean difference between two methods was reported as the relative risk of bias (measured in ml). For all analyses,  $p < 0.05$  was deemed to be statistically significant. Defined *a priori*, bias between methods of greater than 5 ml was felt to be clinically significant, as determined through consensus amongst study investigators.

#### Results

All 35 subjects underwent CMR imaging, and at the time of investigation, were in sinus rhythm. Demographic and clinical data for the 35 subjects are presented in Table 1. As quantified using CAAS, the average MR volume (across all four methods) for subjects with primary MR was 30.5 ml, 16.4 ml for subjects with secondary MR, and 3.2 ml in those with a replaced/repai

#### Inter-software correlation and agreement

Quantification of MR in CAAS correlated strongly with the values from MASS for all four methods of assessment (Table 2).  $MR_{LVRV}$  was the most strongly correlated method between

**Table 1. Study participant demographics and clinical data.**

	Primary MR	Secondary MR	MVR	p-value
<b>Number of subjects</b>	12	10	13	-
<b>Age (years)</b>	67 ± 11	68 ± 11	62 ± 11	0.97
<b>Male, n (%)</b>	6 (50.0)	6 (60.0)	13 (100.0)	0.03
<b>Height (cm)</b>	167 ± 8	167 ± 9	177 ± 6	0.04
<b>Weight (Kg)</b>	75 ± 11	77 ± 11	93 ± 19	0.01
<b>Diabetes mellitus (n)</b>	1	2	1	0.87
<b>Smoker (n)</b>	7	7	5	0.98
<b>Atrial fibrillation (n)</b>	3	2	0	0.26
<b>Ischaemic heart disease (n)</b>	0	0	9	-
<b>NYHA class</b>	2.4 ± 0.9	1.3 ± 0.6	1.7 ± 0.7	0.01

MR-magnetic resonance; MRV-mitral valve replacement; NYHA-New York Heart Association.

**Table 2. Correlation and agreement analysis between CAAS and MASS mitral regurgitation quantification methods.**

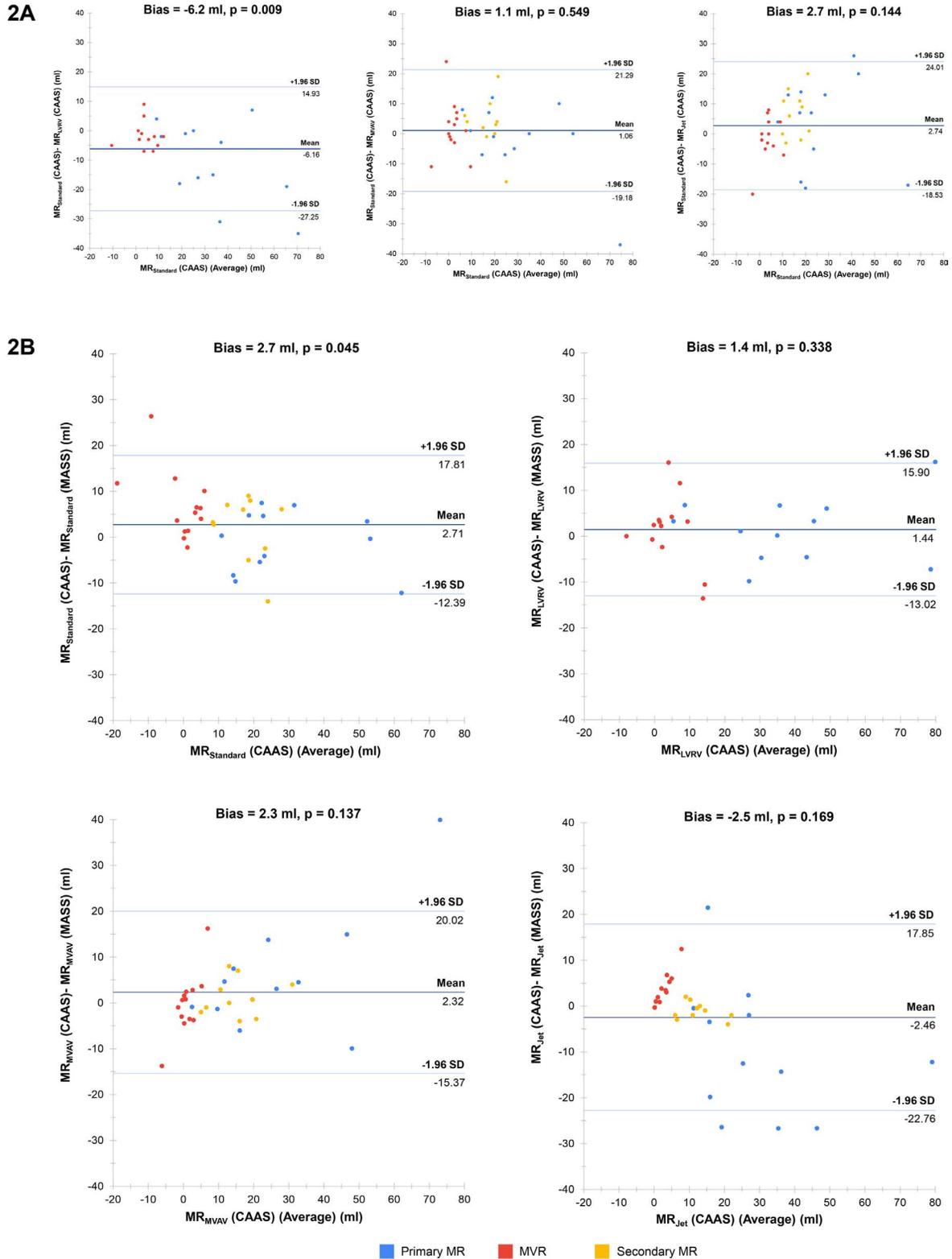
Correlation analysis using the Pearson correlation coefficient (denoted *Correlation*) and agreement analysis using Bland-Altman statistics (denoted *Bias*). The table provides within-vendor analysis (i.e., correlation and agreement between each method within CAAS software solutions) and inter-vendor analysis (correlation and agreement for each method between CAAS and MASS software solution). For agreement analysis, bias refers to the mean difference between two methods of MR volume quantification (measured in ml) and is deemed statistically significant if the corresponding p-value (denoted P) is < 0.05. For negative bias values, this indicates that the method used in CAAS (uppermost panel) to quantify MR is systematically lower than the method in either CAAS (for within-vendor analysis) or MASS (for inter-vendor analysis). For correlation analysis, a p-value < 0.05 is deemed statistically significant. MR=magnetic resonance.

		CAAS															
		MR <sub>Standard</sub>				MR <sub>LVRV</sub>				MR <sub>MVAV</sub>				MR <sub>Jet</sub>			
		Correlation		Bias		Correlation		Bias		Correlation		Bias		Correlation		Bias	
		R	P	Bias	P	R	P	Bias	P	R	P	Bias	P	R	P	Bias	P
CAAS	MR <sub>Standard</sub>	-	-	-	-	0.91	<0.001	6.2	0.009	0.85	<0.001	-1.1	0.549	0.73	<0.001	-2.7	0.144
	MR <sub>LVRV</sub>	0.91	<0.001	-6.2	0.009	-	-	-	-	0.83	<0.001	-5.2	0.02	0.76	<0.001	-7.2	0.007
	MR <sub>MVAV</sub>	0.85	<0.001	1.1	0.549	0.83	<0.001	5.2	0.02	-	-	-	-	0.83	<0.001	-1.7	0.385
	MR <sub>Jet</sub>	0.73	<0.001	2.7	0.144	0.76	<0.001	7.2	0.007	0.83	<0.001	1.7	0.385	-	-	-	-
MASS	MR <sub>Standard</sub>	0.92	<0.001	2.7	0.045	0.89	<0.001	9.1	<0.001	0.86	<0.001	1.7	0.353	0.76	<0.001	0.0	0.988
	MR <sub>LVRV</sub>	0.88	<0.001	-4.7	0.064	0.95	<0.001	1.4	0.338	0.85	<0.001	-5.0	0.071	0.78	<0.001	5.8	0.073
	MR <sub>MVAV</sub>	0.90	<0.001	3.4	0.006	0.93	<0.001	9.2	<0.001	0.91	<0.001	2.3	0.137	0.75	<0.001	0.6	0.705
	MR <sub>Jet</sub>	0.78	<0.001	0.3	0.892	0.81	<0.001	4.3	0.158	0.86	<0.001	-2.1	0.362	0.86	<0.001	2.5	0.169

software solutions (R 0.95, p < 0.001), followed by MR<sub>Standard</sub> (r = 0.92, p < 0.001) and MR<sub>MVAV</sub> (r = 0.91, p < 0.001). MR<sub>Jet</sub> (r = 0.86, p < 0.001) was the least strongly correlated method.

Despite being the most strongly correlated method between software solutions, MR<sub>Standard</sub> was the only method to result in

significant bias in agreement between CAAS and MASS MR quantification (bias 2.7 ml, p = 0.045) (Figure 2). The degree of bias for the other methods was 2.3 ml for MR<sub>MVAV</sub> (p = 0.137), 1.4 ml for MR<sub>LVRV</sub> (p = 0.338) and -2.5 ml for MR<sub>Jet</sub> (p = 0.169). Of note, when we performed subgroup analysis of agreement for the MR<sub>Standard</sub> stratified by MR type, it was identified that MR<sub>Standard</sub> when used for MR quantification in



**Figure 2.** (A) Bland-Altman plots for mitral regurgitation within CAAS. Each plot represents a comparison between two methods within CAAS. Bias refers to the mean difference between the methods of mitral regurgitation volume quantification (measured in ml) and is deemed statistically significant (i.e., high risk of systematic bias) if the corresponding p-value is < 0.05. (B) Bland-Altman plots for MR quantification between CAAS and MASS. Each plot represents a comparison between like-for-like methods of mitral regurgitation volume quantification between the two software solutions. MR-magnetic resonance.

subjects with MVR, demonstrated poor levels of agreement (bias 6.7 ml,  $p = 0.007$ ). This contrasts with the agreement in subjects with primary and secondary MR, where  $MR_{Standard}$  was associated with low bias (-1.0 ml,  $p = 0.604$  and 2.1 ml,  $p = 0.392$ , respectively). With specific reference to the 4D-flow methods of MR quantification,  $MR_{MVAV}$  and  $MR_{Jet}$ , there was excellent correlation and low bias between these methods in CAAS and all four methods within MASS.

#### Within-software correlation and agreement

Using CAAS, we compared each method to each other to determine correlation and agreement/bias. All methods were strongly correlated to each other, with  $r$  coefficients ranging from 0.73 to 0.91. Of all method comparisons,  $MR_{Standard}$  and  $MR_{LVRV}$  were the most positively correlated ( $r = 0.91$ ,  $p < 0.001$ ). The least strongly correlated methods were  $MR_{Standard}$  and  $MR_{Jet}$  ( $r = 0.73$ ,  $p < 0.001$ ) and also  $MR_{LVRV}$  and  $MR_{Jet}$  ( $r = 0.76$ ,  $p < 0.001$ ).

Despite being the most strongly correlated,  $MR_{Standard}$  and  $MR_{LVRV}$ , when compared to each other, were associated with significant levels of agreement bias (6.2 ml,  $p = 0.009$ ). Further to this,  $MR_{LVRV}$  had significant bias when compared to both  $MR_{MVAV}$  (5.2 ml,  $p = 0.020$ ) and  $MR_{Jet}$  (7.2,  $p = 0.007$ ). Aside from comparisons with  $MR_{LVRV}$ , the 4D-flow methods of MR quantification were associated with low levels of bias when compared to each other and to  $MR_{Standard}$ .

#### Interobserver reproducibility

Reproducibility in analysis between two independent assessors with CAAS demonstrated excellent agreement across all four methods of MR volume quantification (Table 3). The 4D-flow methods of quantification were the most strongly correlated between observers ( $MR_{Jet}$ ,  $r = 0.99$ ,  $p < 0.001$ ;  $MR_{MVAV}$ ,  $0.98$ ,  $p < 0.001$ ).  $MR_{Standard}$  and  $MR_{LVRV}$  were also strongly correlated (0.96 and 0.94, respectively,  $p < 0.001$ ). Only MR volume quantification using the  $MR_{Jet}$  method between two observers demonstrated significant bias<sup>5</sup>.  $MR_{Standard}$ ,  $MR_{LVRV}$

and  $MR_{MVAV}$  methods of quantification were not significantly biased between two observers.

#### Discussion

We have demonstrated that quantification of mitral regurgitation is consistent between two different software solutions. We have also demonstrated that within the CAAS platform, there are high levels of agreement between all methods of quantification. Between software solutions,  $MR_{Standard}$  was the only method to result in significant bias and was identified to be due to subjects with mitral valve replacement. We speculate this may be due to the challenges in segmenting the short-axis basal slices in subjects with a MVR. Of note, despite the bias associated with the  $MR_{Standard}$  method being determined as statistically significant, the quantity of MR volume of 2.7 ml is not clinically significant.

Between methods in CAAS, the degree of correlation between all methods was excellent. The  $MR_{Standard}$  method was not only strongly correlated with the MR volume quantification methods utilising 4D-flow techniques, but there was a low risk of bias between  $MR_{Standard}$  and both  $MR_{MVAV}$  and  $MR_{Jet}$  methods of quantification. We have therefore demonstrated that within CAAS, with reference to the  $MR_{Standard}$  method, agreement is best demonstrated with 4D-flow techniques. We have also shown that between the two software platforms, MR volume quantification using the 4D-flow techniques, is both highly reproducible, and is not associated with significant bias, which was not the case for the non-4D-flow techniques.

A previous multicentre study demonstrated that automated valve tracking on CAAS can provide consistent valvular flow quantification<sup>9</sup>. Our study complements their work and demonstrates interoperability between different CMR methods of MR quantification. This becomes critically important in routine clinical practice for increasing the confidence of reporting MR severity. In addition, in this study, we have demonstrated agreement and consistency in MR quantification between two software solutions. This is important for the clinical translation of all the methods of MR quantification by CMR described in our study.

Our previous work demonstrated that 4D-flow methods of MR quantification, in particular  $MR_{MVAV}$ , is superior to other methods of MR quantification for reproducibility as it enhances precision<sup>5</sup>. As research involving 4D-flow CMR techniques continues to gain interest, there is an evolving need for large multicentre studies with clinical outcomes to provide answers to key clinical questions. It is therefore essential for the research and clinical communities to have confidence that regardless of the software platform used for analysis, the data output is comparable between platforms and can confidently be combined without risk of significant bias.

This study has several limitations. Firstly, patients with MVR and secondary MR only had mild to moderate MR. Secondly, due to lower MR volume in MVR and secondary MR cases,

**Table 3. Interobserver reproducibility analysis.**

	Pearson Correlation		Bland Altman	
	r	p-value	Bias (ml)	P-value
$MR_{Standard}$	0.964	<0.001	0.2	0.938
$MR_{LVRV}$	0.939	<0.001	0.0	1.00
$MR_{MVAV}$	0.980	<0.001	0.5	0.789
$MR_{Jet}$	0.988	<0.001	-6.6	0.125

Correlation analysis using the Pearson correlation coefficient (denoted *Correlation*) and agreement analysis using Bland-Altman statistics (denoted *Bias*) between two observers within the CAAS software solution. MR-magnetic resonance.

the relative bias may appear larger in Bland-Altman analysis. Thirdly, we have only used one commercially available CMR software for comparison. And finally, this study did not evaluate inter-scan variability in MR volume quantification.

## Data availability

### Underlying data

Harvard Dataverse: Mitral regurgitation quantification by cardiac MRI between software solutions. <https://doi.org/10.7910/DVN/I8S00H><sup>8</sup>.

This project contains the following underlying data:

- Data Upload.tab (demographic data; functional data and outputted 4D-flow data from both software solutions; inter-observer data between assessor 1 and 2)

Data are available under the terms of the [Creative Commons Zero “No rights reserved” data waiver](#) (CCO 1.0 Public domain dedication).

Raw CMR images were not uploaded in order to protect the identity of the subjects. Access can be requested by contacting the corresponding author (Ciarang-c@hotmail.com). Access to the raw CMR images will be granted for the purpose of re-analysis relating to the primary aims of this research.

## Consent

Written informed consent for publication of the participants’ data and data resulting from analysis of their cardiac imaging was obtained from the participants.

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# Open Peer Review

Current Peer Review Status: ?

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## Version 1

Reviewer Report 22 November 2021

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**Antonio Luna**

Department of Imaging, HT Médica, Jaén, Spain

Dear Authors,

Thanks for submitting your research to Wellcome Open Research. You have evaluated the reproducibility of mitral regurgitation using four different methods of CMR from cine and 4D flow acquisitions. For this purpose, you have performed quantifications using a research and commercial software, comparing inter-software and within-software reproducibility, and also interobserver reproducibility. 4D flow methods showed equivalent reproducibility to cine-based ones but with greater levels of agreement. This series adds light to the added value of 4D flow for mitral regurgitation assessment and quantification, supporting similar results using different software platforms. Before indexing, there are some obscure points in the material & methods and results section that should be clarified, as detailed below.

### Material & methods:

- Define the type of coil and elements used in the 1.5T MR.
- Aortic phase contrast sequences are not included as part of the acquisition protocols. I assume that both pulmonary and aortic valve phase contrast sequences were part of it. Please clarify this point.
- Include a table with the parameters of 4D flow acquisitions, aortic phase contrast sequences and short axis cines in both MRI.
- Define the experience of the assessor completing the analysis of all 35 included patients with CAAS software.
- Interobserver reproducibility was performed in a random mix of ten patients. I suppose that excluding cases with secondary MR, as in those you didn't measure **MR<sub>LVRV</sub>**. Please confirm.

### Results:

- You state that all patients were in sinus rhythm at the time of CMR acquisition, but in Table 1, 5 patients are described as having AF.

**Discussion:**

- Add a final paragraph with the main conclusion of your research.

**Is the work clearly and accurately presented and does it cite the current literature?**

Yes

**Is the study design appropriate and is the work technically sound?**

Yes

**Are sufficient details of methods and analysis provided to allow replication by others?**

Yes

**If applicable, is the statistical analysis and its interpretation appropriate?**

Yes

**Are all the source data underlying the results available to ensure full reproducibility?**

Yes

**Are the conclusions drawn adequately supported by the results?**

Yes

**Competing Interests:** No competing interests were disclosed.

**Reviewer Expertise:** Radiologists subspecialist in CMR

**I confirm that I have read this submission and believe that I have an appropriate level of expertise to confirm that it is of an acceptable scientific standard, however I have significant reservations, as outlined above.**

Author Response 29 Dec 2021

**Ciaran Grafton-Clarke**

Dear Dr Antonio Luna,

Thank you for your peer review. We have addressed each of your comments below.

**Comment 1:** Define the type of coil and elements used in the 1.5T MR.

**Response:** We have added this information within the main manuscript.

**Comment 2:** Aortic phase contrast sequences are not included as part of the acquisition protocols. I assume that both pulmonary and aortic valve phase contrast sequences were part of it. Please clarify this point.

**Response:** The aortic phase contrast study was not done. A 4D flow static 2D phase contrast reformatted plane was used instead.

**Comment 3:** Include a table with the parameters of 4D flow acquisitions, aortic phase contrast sequences and short axis cines in both MRI.

**Response:** Thank you for this comment. This has now been added to the supplementary document.

**Comment 4:** Define the experience of the assessor completing the analysis of all 35 included patients with CAAS software.

**Response:** Thank you for this comment. This has been inserted into the manuscript.

**Comment 5:** Interobserver reproducibility was performed in a random mix of ten patients. I suppose that excluding cases with secondary MR, as in those you didn't measure **MR<sub>LVRV</sub>**. Please confirm.

**Response:** Thank you for this comment. This is clarified within the manuscript in the *image analysis* subsection.

**Comment 6:** You state that all patients were in sinus rhythm at the time of CMR acquisition, but in Table 1, 5 patients are described as having AF.

**Response:** Thank you for this comment and we apologise for this inconsistency. This has possibly resulted from the fact that these five patients have had a history of atrial fibrillation, but during the CMR investigation were in sinus rhythm. To avoid confusion, we have removed this comment from the results section.

**Comment 7:** Add a final paragraph with the main conclusion of your research.

**Response:** Thank you for this comment. We have now added this.

Yours faithfully,

**Dr Ciaran Grafton-Clarke** (corresponding author)

Dr Pankaj Garg

**Competing Interests:** No competing interests were disclosed.