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1 **Risk factors for revision of polished taper-slip cemented stems for postoperative**  
2 **periprosthetic femoral fracture after primary total hip replacement: A registry based**  
3 **cohort study from the National Joint Registry for England, Wales, Northern Ireland**  
4 **and the Isle of Man**

5

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25 *Abstract*

26 *Background*

27 Total hip replacement (THR) with a cemented polished taper-slip (PTS) femoral stem has  
28 excellent long-term results but are associated with a higher post-operative periprosthetic  
29 femoral fracture (PFF) risk compared to composite beam stems. This study aims to identify  
30 risk factors associated with PFF revision following THR with PTS stems.

31

32 *Methods*

33 299 019 primary THRs using PTS stems from the National Joint Registry (UK) were  
34 included in a retrospective cohort study with a median follow up of 5.2 (IQR, 3.1-8.2) years.  
35 Adjusted hazard ratio (HR) of PFF revision was estimated for each variable using  
36 multivariable Cox survival regression analysis.

37

38 *Results*

39 1055 of 299 019 THRs were revised for PFF at a median time of 3.1 (IQR, 1.0-6.1) years.  
40 Mean age (SD) was 72 years (9.7), 64.3% (192 365 of 299 019) participants were female and  
41 82.6% (247,126 of 299 019) were ASA grade one or two. Variables associated with increased  
42 HR (HR, 95% Confidence interval) of PFF were: increasing age (1.02, 1.01 to 1.03, per year),  
43 intraoperative fracture (2.57, 1.42 to 4.66), ovaloid (1.96, 1.22 to 3.16) and round cross  
44 sectional shapes (9.58, 2.29 to 40.12), increasing stem offset (1.07, 1.05 to 1.09 per  
45 millimetre), increasing head size (HR 1.04, 1.01 to 1.06 per millimetre), THR performed  
46 from 2012 to 2016 (1.45, 1.18 to 1.78), cobalt chrome stem material (6.7, 3.0 to 15.4) and  
47 cobalt chrome stems with low viscosity cement (22.88, 9.90 to 52.85). Variables associated  
48 with a decreased risk of PFF revision were: female gender (0.52, 0.45 to 0.59), increasing

49 stem length (0.97, 0.96 to 0.98 per millimetre) and a ceramic on polyethylene bearing (0.55,  
50 95% 0.36 to 0.85).

51

52 *Conclusion*

53 Increased risk of PFF revision was associated with PTS stems which are short, high offset,  
54 used with large femoral heads, made of cobalt chrome or have ovaloid or round cross  
55 sectional shapes. Large increases in PFF risk were associated with cobalt chrome stems used  
56 with low viscosity cement. Further study is required to confirm causation.

57

58 *Level of evidence*

59 Level III: Retrospective cohort study

60

61 *Introduction*

62 The risk of postoperative periprosthetic femoral fracture (PFF) following primary total hip  
63 replacement (THR) is estimated at 3.5% and this is expected to rise in the future<sup>1,2</sup>. Most  
64 patients require complex surgery which is costly and associated with substantial morbidity  
65 and mortality<sup>3,4</sup>. Prevention is likely to be a more effective strategy than treatment, thus  
66 identification of modifiable risk factors which can guide surgical decision-making is crucial.  
67 Surgical technique and implant choice are the most easily modifiable risk factors for PFF.  
68 Cemented stems are considered to reduce the risk of PFF compared with cementless stems<sup>1,5-</sup>  
69 <sup>9</sup>. Use of modern polished taper-slip (PTS) or ‘force-closed’ stems have overtaken more  
70 traditional composite beam (CB) or ‘shape-closed’ stems<sup>10</sup>. PTS stems have excellent  
71 survivorship beyond 20 years<sup>11-13</sup>, but a higher incidence of PFF compared to CB stems<sup>5,8,14-</sup>  
72 <sup>16</sup>. PTS stem geometry and lack of cement-implant bonding may cause the femoral  
73 component to split the bone upon traumatic loading<sup>17,18</sup>.  
74 Large differences in risk of PFF revision exist between PTS stem designs, but the aetiology  
75 remains unclear<sup>14</sup>. Biomechanical studies have shown a reduction in torque required for PFF  
76 in PTS stems which are shorter or smaller<sup>19,20</sup>. PTS stems are used in conjunction with a  
77 range of cements with different mechanical properties which may affect the strength of the  
78 femoral construct<sup>21,22</sup>. Accumulation of wear particles and osteolysis may also increase the  
79 risk of fracture<sup>23,24</sup>. Implant design features which may predict PFF revision could be  
80 identified using large registry datasets<sup>25</sup>. This may develop hypotheses to reduce PFF risk  
81 which can be subsequently tested.  
82 The aim of this study is to determine factors which are associated with revision surgery for  
83 PFF following primary THR using PTS stems using UK National Joint registry (NJR) data.

84 *Materials and Methods*

85 *Data sources*

86 The NJR is a population-based dataset which records data for all primary and revision THRs  
87 performed at all hospitals throughout England, Wales Northern Ireland and the Isle of Man  
88 since 2003<sup>26</sup> with missing data estimated at 5.8%<sup>27</sup>. Implant catalogue codes are recorded in  
89 the registry for each implant and were used to link implant design data on all implants (stem,  
90 cement, head, cup or shells and liners etc.).

91 *Participants*

92 Revisions for PFF which occurred within three months of reported intraoperative PFF were  
93 excluded to prevent miss-classification of revision which occurred as a result of  
94 intraoperative PFF rather than a new injury<sup>25</sup>. The formal reporting of intraoperative fractures  
95 was introduced on 01/04/2004 and THRs performed prior to this date were therefore  
96 excluded. This study analysed all primary THRs recorded in the NJR from 01/01/2004 to  
97 30/09/2016 using a polished tapered slip (PTS) cemented femoral stem.

98 *Variables*

99 To reduce the confounding effect of indication, only cases performed for osteoarthritis (OA)  
100 were included. This resulted in 361 091 cases for analysis (step-wise exclusions are displayed  
101 in Figure 1). In the majority of cases, the same cement brand and viscosity was used for the  
102 acetabular and femoral components. These cases, regardless of acetabular implant fixation,  
103 were included in this analysis. Occasionally, different cement brands and viscosities were  
104 used for the acetabular and femoral components and as NJR data does not specify which  
105 cement was used for each component, these cases were excluded. A comparison of excluded  
106 patients to study patients can be seen in Appendix 1.

107 *Patient and surgical modifiers*

108 Patient and surgical variables were patient age (years), year of surgery (2004 to 2007, 2008 to  
109 2011 and 2012 to 2016), gender, American Society of Anaesthesiologists group (1 and 2  
110 versus 3 to 5), side of operation, surgical approach (posterior versus non-posterior), computer  
111 guided surgery, minimally invasive surgery, surgeon grade (consultant versus non-consultant)  
112 and surgeon-reported intraoperative fracture.

### 113 *Implant modifiers*

114 Highly cross-linked polyethylene was defined as polyethylene which had been irradiated  
115 above 50 kGy<sup>28</sup>. Variables included stem material (stainless steel [SS] alloy versus cobalt  
116 chrome [CoCr] alloy, stem length (estimated to allow comparison between stem brands from  
117 medial stem length +10mm or lateral stem length -10mm), diaphyseal cross-sectional shape  
118 (ovaloid, rectangular or round), metaphyseal cross-sectional shape (flat versus vertical ridge),  
119 stem taper (double versus triple tapered), stem offset, head size, bearing combination (metal  
120 on polyethylene [MoP], metal on highly cross-linked polyethylene [MoXLP], ceramic on  
121 polyethylene [CoP], ceramic on highly cross-linked polyethylene [CoXLP] or ceramic on  
122 ceramic [CoC]) and cement viscosity (high, medium or low).

### 123 *Outcomes*

124 The primary outcome of registry analysis was implant survival to the end point of PFF  
125 revision.

### 126 *Statistical analysis*

127 Normally distributed continuous variables were expressed as means with standard deviations  
128 (SD) and non-normally distributed continuous variables were expressed as median values  
129 with interquartile range (IQR). Patient time incidence rates (PTIR) were calculated as  
130 revisions occurring per 1000 patient years. Since the dataset in this exploratory analysis was  
131 large and multiple comparisons were performed, statistical significance was set at  $p < 0.01$  to  
132 reduce the risk of inappropriate false positives. Comparisons of continuous variables were

133 performed with Welch's t-tests, and categorical variables were compared with chi-square  
134 tests. Survival was estimated using a Kaplan-Meier method. Cases were censored when the  
135 patient did not undergo revision for PFF and when patients died prior to revision for PFF.  
136 Multivariable Cox regression estimated the adjusted hazard ratio (HR) of revision with 95%  
137 confidence intervals (HR [CI 95%]) for each variable. HR estimates were adjusted for all  
138 other available variables. Assumptions of proportionality were tested numerically and upheld  
139 for all Cox regression models. Regression model discriminatory power was assessed using  
140 the concordance statistic, which is analogous to the area under the receiver operating curve  
141 (useful prognostic model between 0.6 and 0.85)<sup>29</sup>. To control for the effect of stem geometry,  
142 a subgroup analysis of all stems which were manufactured using both CoCr and SS with the  
143 same geometry (CPT, Zimmer Biomet, Warsaw, Indiana and CPCS, Smith and Nephew,  
144 Memphis, Tennessee) were compared as a subgroup using otherwise identical methods as  
145 described above. Analyses were completed using R (v 3.6.1, R, Vienna, Austria).

146

147 Source of Funding

148 None.

149 *Results*

150 1055 PFF revisions in 299 019 cases were recorded in the study group with an overall PTIR  
151 of 0.62 revisions per 1000 years at risk. Mean age (SD) was 72.00 (9.66), 64.3% (192 365 of  
152 299 019) participants were female and 82.6% (247,126 of 299 019) patients were ASA grade  
153 one or two (Table 1). Median follow-up time of non-revised cases was 5.2 (IQR, 3.1-8.2)  
154 years. Minimum follow up of non-revised cases was 1.4 years. Median time to PFF revision  
155 was 3.1 (IQR, 1.0-6.1) years (Figure 2).

156

157

158 *Implant survival to PFF revision*

159 Kaplan-Meier unadjusted 10-year survival until revision for PFF (95% CI) was 99.3% (95%  
160 CI 99.3-99.4, number at risk = 39 173, Figure 3).

161

162 *Predictors of PFF revision*

163 The regression model performed well (concordance statistic 0.76). After adjustment for all  
164 other co-variates, variables associated with an increased risk of PFF revision were increasing  
165 age, reported intraoperative PFF, cobalt chrome stem material, increasing stem offset, ovaloid  
166 and round diaphyseal cross sectional stem shapes, increasing head size and THR performed  
167 between 2012 and 2016 (figure 4 and 5). Variables which were associated with a decreased  
168 risk of PFF revision were female sex, increasing stem length and a CoP bearing couple  
169 (figure 4 and 5).

170 The subgroup contained 49 840 cases (CoCr = 46 525 and SS = 3315). An identical model  
171 was used to estimate the effect of all variables on risk of PFF revision. The model performed  
172 well (concordance statistic 0.76). Median time to PFF was 8.1 (IQR, 4.0-10.0) years for SS  
173 stems and 2.7 (IQR, 0.8-5.0) years for CoCr stems. After adjustment for all other covariates,

174 the HR of PFF revision associated with CoCr versus SS stem material was 6.7 (95% CI 3.0 to  
175 15.4,  $p < 0.001$ ). To investigate the interaction between cement properties and stem material,  
176 modelling was repeated with the complete study cohort using an interaction term to classify  
177 stem material with cement viscosity (figure 6). CoCr stems were associated with a higher risk  
178 of PFF versus SS stems regardless of cement viscosity. The hazard ratio of PFF revision for  
179 CoCr stems compared to SS stems increased when used with low viscosity cement.

180

181 *Discussion*

182 Modifiable risk factors associated with an increase the risk of PFF revision include use of  
183 CoCr stem material, ovaloid and round diaphyseal cross sectional shaped stems, higher stem  
184 offsets, larger head diameter and CoCr stems, particularly when used with low viscosity  
185 cement.

186 The overall PFF revision incidence in this study was low and similar to previous findings<sup>8, 14,</sup>  
187 <sup>30</sup>. The unadjusted incidence was comparable to PFF incidence for cementless stems in the  
188 NJR although the patient population in this study is older and possibly at higher risk of PFF  
189 revision<sup>25</sup>.

190 *Patient-related factors*

191 Increasing age was associated with a significantly greater risk of PFF revision and this has  
192 been previously reported as an independent risk factor for PFF<sup>31, 32</sup>. Females were at a  
193 reduced risk of PFF revision which is in agreement with some results for cemented stems<sup>5</sup>  
194 and contradicts the findings of other results for a mixture of stem fixation methods<sup>31, 32</sup>. This  
195 suggests that the influence of age-related changes which reduces bone quality in female  
196 femora is less of a risk factor for PFF when using PTS stems as compared to other femoral  
197 stems. PFF risk may be reduced by the cement acting as a load sharing device which reduces  
198 point loading of the femur<sup>12</sup>. Male patients may be at greater risk because of larger body  
199 mass which may increase forces on the implant, thus increasing the risk of cement mantle  
200 failure and PFF. ASA is a useful surrogate marker of frailty which may infer poorer bone  
201 quality and increased risk of falling<sup>33</sup>. ASA has been identified as a risk factor for PFF in  
202 another study including a majority of cementless stems<sup>32</sup>. In this study, increasing ASA grade  
203 was not associated with an increase in risk of PFF revision, which suggests that PTS stems  
204 may provide some protection in patients with co-morbidities.

205

206 *Surgical factors*

207 Intraoperative fractures were associated with an increased risk of PFF revision, as shown  
208 previously<sup>1</sup>. Intraoperative PFF occur more commonly in elderly patients with osteoporotic  
209 bone who are also at increased risk of postoperative fracture following low-energy trauma<sup>34</sup>,  
210 <sup>35</sup>. THRs performed between most recently were associated with an increased risk of PFF  
211 revision, in keeping with other studies, perhaps due to increasing incidence amongst older  
212 patients<sup>15</sup>. Increasing PFF revisions may also suggest an increase in revision surgery as a  
213 treatment but this is difficult to quantify without data regarding all treatment methods. More  
214 detailed granular data analysis of changes in PFF risk over time are required to understand  
215 why risk may change over time.

216

217 *Implant-related factors*

218 Perhaps most relevant to surgical decision-making is the impact of implant choice on PFF.  
219 CoCr stems were associated with a significantly higher risk of revision (HR 6.7 [95% CI 3.0  
220 to 15.4, p <0.001]) compared to SS stems and this observation is consistent when comparing  
221 stems from the same manufacturer with identical geometry. There was a large difference in  
222 the time to PFF revision between stem materials in the subgroup analysis, which might  
223 suggest that difference between CoCr and SS stems may be in part modified by a process of  
224 wear at the stem-cement interface. Even though CoCr alloys are harder than SS alloys, wear  
225 does occur at the stem-cement interface with CoCr PTS stems through corrosive fretting  
226 wear<sup>36, 37</sup> which may increase the risk of PFF revision. Risk of revision with CoCr stems  
227 increased dramatically when implanted with low viscosity cement. Low viscosity cements are  
228 reported to give poorer bone penetration, reduced tensile strength and inferior implant  
229 fixation compared to higher viscosity cements in vitro<sup>21</sup>. These properties may accelerate an  
230 undefined process of failure at the cement-implant interface leading to PFF revision.

231 Rotational force as a mechanism for PFF around a PTS stem is thought to be a major  
232 contributing factor in Vancouver type B fractures<sup>38, 39</sup>. Shorter PTS stems were associated  
233 with a higher risk for PFF revision which confirms findings in biomechanical models<sup>20</sup>.  
234 Compared to rectangular diaphyseal cross-section shape stems, circular shaped stems are  
235 associated with greater micromotion, inferior rotational stability, thinner cement mantles, and  
236 higher peak stresses within the cement mantle<sup>40, 41</sup>. These factors offer a theoretical basis for  
237 our observation that ovaloid and round stems were associated higher risk of PFF revision.  
238 We found that increasing offset and head size significantly increased the risk of PFF revision.  
239 Increasing femoral offset and head size results in greater torque on the femoral construct and  
240 also increases cement mantle stresses, which may predispose to PFF. Additionally, larger  
241 head sizes are associated with greater volumetric wear of polyethylene acetabular surfaces  
242 and this may result in wear-associated osteolysis<sup>42</sup>. However, our analysis did not show a  
243 consistent protective association of low wear bearing couples and this suggests that overall  
244 differences in PFF revision rates may not be a bearing wear related phenomenon.

#### 245 *Limitations*

246 We accept certain limitations to this study. This observational study benefits from large  
247 numbers from a national registry but is unable to determine causality between risk factors and  
248 risk of revision. Confirmation of causation should be pursued using the breadth of good  
249 clinical research. In order to control for and analyse the effects of cement and implant design  
250 features, we excluded data which was not possible to interpret or was not supplied by  
251 manufacturers. The resulting dataset contains the majority of currently used constructs which  
252 makes the analysis useful for current practice but exclusions may reduce the power and scope  
253 of observations. Despite this, the large numbers in this study increase statistical power and  
254 may have led to results which are statistically significant but do not reach levels of clinical  
255 significance. As such, they should be viewed within the overall clinical context by

256 experienced clinicians. This registry analysis estimated the risk of PFF revision and whilst  
257 this includes most cases of PFF in UK practice<sup>43</sup>, it was likely to be an underestimate of total  
258 PFF incidence which would also include cases undergoing internal fixation or conservative  
259 management<sup>15</sup>. Disparities could exist in management of PFF between hospitals or between  
260 surgeons which may have substantial impact on our findings herein. Further analysis  
261 combining data on all PFFs should be performed to corroborate our findings. We excluded  
262 patients with PFF which occurred within three months of a reported intraoperative PFF to  
263 reduce confounding but a proportion of early PFFs may be due to unrecognised or unreported  
264 intraoperative fracture which propagate during the early postoperative stage<sup>25</sup>. This paper  
265 relies on NJR data which is a rich source of information regarding implant and practice but  
266 there is a lack of patient information which may bias the inference of results and prevent  
267 adjustment for important known and unknown patient confounding factors. Further analysis  
268 should seek to include a wider source of patient data to improve the accuracy of estimates.  
269 We were unable to analyse all the properties of implants which may be useful in predicting  
270 risk of PFF, for example, exact stem geometry, cement porosity and cement mixing  
271 technique. Future work should attempt to classify implants used to include all pertinent  
272 predictors.

### 273 *Conclusion*

274 This is the first study to evaluate detailed implant-related risk factors for revision of cemented  
275 PTS stems for PFF and it confirms that the majority of risk for PFF is attributable to  
276 modifiable factors such as surgical practice and design of PTS stem. Whilst the overall  
277 survival of PTS stems is excellent, revisions for PFF comprise of a large portion of total PFF  
278 revisions and based on our findings, we recommend that surgeons should evaluate the  
279 association between the increased risk of PFF revision and exercise prudence when using  
280 PTS stems which are short, made of cobalt chrome or have ovaloid or round diaphyseal cross

281 sectional shapes. Caution must be applied when using high-offset stems and larger femoral  
282 heads. Elderly patients, males and those who have had an intraoperative fracture must be  
283 appropriately counselled about the increased risk of PFF. Further analysis is warranted and  
284 planned, including looking at variations in surgeon characteristics and surgical techniques as  
285 well as radiographic and biomechanical analysis that may further our understanding of risk  
286 factors associated with PPF.

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416

417 *Figure legends*

418

419 **Figure 1.** Flow chart summarising exclusion parameters. For a comparison of excluded  
420 patients to study patients please see Appendix 1.

421 **Figure 2.** Distribution of revisions for PFF in primary THR using polished tapered stems  
422 over time.

423 **Figure 3.** Kaplan-Meier survival to an endpoint of PFF revision for all study cases.

424 **Figure 4.** Forest plot displaying the effect of categorical predictors on the risk of PFF  
425 revision following THR with cemented PTS stems.

426 **Figure 5.** Effect of continuous predictors on the hazard of PFF revision.

427 **Figure 6.** Forest plot displaying the effect of stem material and cement viscosity on the risk  
428 of PFF revision following THR with cemented PST stems