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24 79% sensitivity and 61% specificity. The estimated area under the curve for volume
25 loss was 0.80 (95%CI 0.71-0.89, p<0.001).

26 **Conclusions.** This is the first study to propose rates of high wear progression in
27 adolescents. Limited sensitivity and specificity confirms that quantitative analysis is
28 an adjunct tool to be used alongside history taking and clinical judgement.

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30 **Clinical Significance.** The rapid advancement of digital technologies may result in
31 improved diagnosis in erosive tooth wear (ETW). Intra-orals scans and registration
32 software are a promising adjunct for monitoring ETW progression in clinical practice.

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36 **Key words** Tooth erosion, Tooth wear, Epidemiology, Progression, Diagnostic
37 imaging.

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54 **1. Introduction**

55 Erosive tooth wear (ETW), known as the chemical-mechanical process of
56 tooth wear caused by the presence of non-bacterial acids in the oral cavity [1], has
57 been described as common with around 30% of adults [2]. Severe cases of ETW
58 represent 2-3% of the population [2]; however, the prevalence is increasing globally
59 and this is particularly true for younger age groups [3]. The increase in consumption
60 of acidic/erosive food products, as is seen in many modern diets [4], may be
61 associated with this higher prevalence [2, 5-7]. Further frequent consumption may
62 increase the rate of ETW and could compromise the dentition function at younger
63 ages.

64 There is limited evidence on the rate of physiological ETW progression.
65 Lambrechts et al. 1989 identified a normal rate of tooth wear progression, as
66 measured by overall reduction in crown height, of 29 μm a year in molars and 15 μm
67 in premolars in healthy young adults [8]. Rodriguez et al. 2012 reported an average
68 of 15 μm per tooth to be a normal rate of wear over 6 months but noted that this was
69 also below the detection limit of the measurement system [9]. O'Toole et al. 2018
70 observed in a randomised controlled clinical trial that altered dietary habits in a high-
71 risk group of tooth wear patients decreased the volume loss on the central aspect of
72 their central incisors to a rate of 0.00 mm^3 over 6 months compared to 0.07 mm^3 lost
73 in those who maintained a high level of dietary acid intake [10]. These studies have
74 used profilometric measurements of casts and the use of engineering or custom-
75 built proprietary software to align and analyse change, all of which are difficult to
76 apply in primary care. Intra-oral scanners have been suggested as a promising

77 instrument that could potentially be used for the clinical diagnosis and monitoring of
78 ETW [11]. Recently, two studies have used intra-oral scans (IOS) to assess ETW
79 and the use of such records improved significantly the detection of ETW [12, 13].
80 However, intraoral scanners can also be used to digitise casts and perform 3D
81 analysis on them. The possibility to superimpose IOS, instead of laboratory based
82 profilometers, has the potential to overcome many diagnostic issues in primary care.
83 However, this technology needs to be validated and rates of tooth wear progression
84 associated with pathological tooth wear need to be determined. The aims of this
85 study were to investigate whether wear quantification on IOS of study casts could
86 differentiate between scans which showed visual progression compared to those
87 that did not. The null hypothesis was that there would be no difference in the volume
88 loss detected on sites with visible wear progression compared to those without.

89

90 **2. Materials and methods**

91 Previously collected data from pre- and post-orthodontic treatment casts belonging
92 to 120 adolescents (age range 11-13 years at pre-treatment cast) with an interval
93 median time of 29 months (± 3.4) between the pre-and post-treatment model were
94 used for selection proposal (Ethical committee reference number: BC2016/0615 &
95 2016/0616). Orthodontic patients were chosen as a convenient sample as long-term
96 storage of orthodontic models and records facilitated a convenient longitudinal data
97 set. Treatment casts at baseline and follow-up were digitised using a confocal intra-
98 oral scanner TRIOS™ (3Shape, Copenhagen, Denmark) according to the
99 manufacturer's scanning instructions.

100 The occlusal surfaces of the first molars were visually assessed and scored using
101 the BEWE index [13]. Any surface showing an increase in BEWE score was
102 categorised into the progression group whereas surfaces with the same BEWE score
103 over the 2-year period was categorised into the non-progression group. All visual
104 assessment was performed by a single operator (FM).

105 Volumetric analysis for power calculation was performed on a pilot sample of 10
106 surface pairs with visible wear progression and 10 surface pairs without wear
107 progression. An effect size of 0.88 was observed between groups. Assuming $\alpha =$
108 0.05 and at 95% power, a minimum of 29 cases were needed to be included per
109 group to observe differences between groups.

110 The IOS scan of each occlusal molar surface was aligned and measured individually
111 in WearCompare (www.leedsdigitaldentistry.com/WearCompare) using a previously
112 validated selective surface alignment protocol [14, 15]. Initially a global alignment
113 between the two scans at separate time points was performed to bring the two scans
114 into closer approximation. A more refined iterative closest point alignment was then
115 performed aligning only on areas which were less likely to have experienced wear
116 progression (the buccal and lingual surfaces of the molars). Alignment quality was
117 assessed by analysing the percentage of data points within these reference areas
118 as being within 25 microns of each other. Figure 1 illustrates the protocol used to
119 superimpose the sample and quantify the ETW. Volume change (in mm^3) was the
120 primary measurement outcome. Volume change per mm^2 , the maximum point loss
121 (μm) and the mean profile loss (μm) were also recorded as secondary measurement
122 outcomes.

123 Scan pairs were excluded from analysis if the baseline or sequential scan was
124 missing, incomplete data on the IOS, blebs/errors on the cast, restorations involving
125 $\geq 50\%$ of the surface, or if there were any alterations which would affect the reference
126 alignment protocol of the scan (e.g. orthodontics, partial eruption). The final data set
127 to be analysed were first molar surfaces which did not have visual progression and
128 first molar surfaces with visual progression. More than one molar per participant was
129 included in some cases.

130 A single investigator was trained in the use of the software and performed all
131 alignments and measurements. To assess intra-operator reproducibility (ICC), a
132 single pair of scans, not used in the study protocol were aligned 15 times and the
133 volume loss between the scans recorded. The mean volume loss noted was 5.39
134 (0.34 SD) and the ICC between readings was excellent at 0.99 (CI: 0.96-1.00;
135 $p < 0.001$)[16].

136 The final sample of 42 surface pairs without wear progression and 54 surface pairs
137 with wear progression were then aligned, analysed and measurements recorded
138 Volume change (mm^3), volume change/ mm^2 (mm), maximum point loss and mean
139 profile loss.

140 Data were analysed using SPSS version 25 (SPSS Inc., Armonk, NY). To assess
141 the sensitivity and specificity of software performance at identifying the visual
142 progression, receiver operating characteristic (ROC) curves were drafted and the
143 area under the curve was estimated. The distribution of the data was assessed
144 visually using boxplots and histograms. Data were not normally distributed and are
145 therefore presented using medians and interquartile ranges (IQR). A Mann-Whitney

146 U test with Bonferroni correction was used to analyse differences between groups
147 (progression and no progression), with a significance level set at $p < 0.001$.

148

149 **3. Results**

150 *3.1 Demographics*

151 The average time between scans was 29.5 months (3.5 SD; range 24-35 months)
152 within 32 adolescents (Table 1: age range at baseline 12-13, 20 females, 12 males).
153 There were no statistical differences in the age, gender or mean period scans from
154 the progression and no progression group.

155 *3.2 Quantitative Analysis*

156 The median volume loss (mm^3) on occlusal surfaces of the progression group was -
157 2.19 mm^3 (IQR $-3.65, -0.91$) and non-progression was -0.37 mm^3 (IQR $-1.02, 0.16$),
158 ($p < 0.001$). When volume loss was standardised per mm^2 , the volume loss was -
159 0.025 mm^2 (IQR $-0.048, -0.012$) for the progression group and -0.005 mm^2 (IQR-
160 $0.13, 0.002$) for the non-progression group ($p < 0.001$). The full quantitative analysis
161 results showing volume loss, standardised volume loss per mm^2 , maximum point
162 loss and mean profile loss are reported in Table 2 according to the progression and
163 no progression group. Overall the volume loss (in mm^2 and mm^3) differed
164 significantly between groups, whereas the maximum point loss and mean profile loss
165 did not.

166 *3.3 ROC analysis*

167 The ROC curves in Figure 2 and Table 3 demonstrate the diagnostic ability for each
168 measurement metric. Analysing volume loss measurements on IOS scans resulted
169 in an estimated area under the curve of 0.80 (95%CI 0.70-0.89, $p < 0.001$) and similar

170 to the volume loss per mm² of 0.79 (95% CI 0.69-0.88, p<0.001). The ROC curve of
171 0.64 for mean profile loss (95% CI: 0.53-0.75, p=0.018), indicates a poor diagnostic
172 capability. The area under the curve for maximum point loss was 0.61 (95% CI: 0.50-
173 0.72, p=0.053), which also indicates a poor diagnostic capability. Table 3
174 demonstrates the sensitivity and specificity of the discrimination threshold. A cut off
175 point of -1.22 mm³ was associated with a sensitivity of 79% and a specificity of 61%
176 of predicting visible ETW progression over 2 years.

177 **4. Discussion**

178 Volumetric tissue loss observed using intra-oral scans over the two-year period was
179 statistically different between progression and non-progression groups based on the
180 visual assessment. A detected wear of $\leq -1.22\text{mm}^3$ on the occlusal surfaces of first
181 molars was observed to have a sensitivity of 79% and a specificity of 61% of
182 diagnosis of visible wear progression. Volume loss also indicated that quantitative
183 tooth wear progression using intraoral scanners is a feasible aid for diagnosing
184 increased rates of ETW progression over this time period.

185 Molar surfaces with visual wear progression were observed to have an average loss
186 of -2.19mm^3 over the two-year period compared to -0.37mm^3 of loss for those without
187 visual wear progression. Although wear does not always progress at a constant rate,
188 this would correspond to -0.55mm^3 in the high progression group and -0.09mm^3 in
189 the low progression group over a 6-month period. Pintado et al., 1997 observed a
190 volume loss of 0.047mm^3 over two years on molar occlusal surfaces, again on
191 healthy adults [17]. Tantbirojn et al. 2012 observed volumetric loss of -0.18mm^3 in
192 adults with GERD (n=12) compared to a volumetric loss of -0.06mm^3 in control
193 patients (n=6) over 6 months [18]. However, the same author analysed and

194 averaged wear over the whole mouth. The mean profile loss in our low progression
195 group was 63 μm and 75 μm in the high progression group over 2 years. Lambrechts
196 et al. 1989 estimated an annual rate of 29 μm on molars on low progression groups
197 [8]. More recently Rodriguez et al. 2012 observed an average wear rate of 15 μm over
198 6 months [9]. This study and others did not observe statistical differences between
199 a high progression group and a low progression group when calculating average
200 profile loss [9, 17, 19]. Unfortunately, direct comparison between other studies is
201 difficult due to different methods of analysis over different time periods [18]. The
202 majority of alignment techniques have focused on a best fit or least mean squares
203 registration which can underestimate the wear [15]. It is, however, interesting to see
204 that the wear quantified in the control groups were relatively similar.

205

206 It is also difficult to compare studies due to the differences in the measurement
207 metrics. For profile loss, large differences are averaged out over the entire surface
208 and can pose problems when detecting localised wear. A moderate AUC value was
209 observed using this measurement metric. No differences were observed between
210 groups in this study when the maximum point loss data was used. A poor, non-
211 significant AUC value was also observed. As the maximum point loss relies upon a
212 single data point, measurements are susceptible to outliers or process errors. Based
213 upon this data, the use of the maximum point loss with IOS data on casts cannot be
214 recommended. Volumetric wear analysis reported the highest AUC value. Other
215 groups using volumetric analysis were also able to observe differences between
216 groups [10, 18]. The difficulty with using volumetric analysis is that the size of the

217 surface is not standardised. A larger surface will show a higher wear value than a
218 smaller surface even if the proportional reduction is the same. Two volumetric
219 measurements are reported in this study. One reports the total volumetric loss over
220 the whole surface and this has advantages in that it gives an overall volume and
221 localised wear defects do not get averaged out over the surface. The disadvantage
222 is that it is not standardised. A standardised volume loss per squared mm of
223 analysed surface is also presented. Although this increases comparability across
224 surfaces it is a less tangible measurement metric when used for patient education.
225 Both measurement metrics offer good predictive values.

226

227 There were limitations in this study. Single tooth analysis is time consuming and it
228 was not within the scope of this study to perform analysis on each surface of the
229 dentition. The occlusal surface of the lower first molar is a known index surface when
230 assessing ETW [20]. There are also several published and validated protocols
231 assessing the occlusal surfaces of the molar teeth [14]. Wear rates reported may or
232 may not be generalizable to other surfaces and this will need to be an area for further
233 research. The comparison of visible wear progression as the gold standard is
234 fundamentally flawed as non-localised wear could have occurred over the entire
235 surface which was not detected by the human eye. Secondly, there were high
236 standard deviations (SD) and positive values in the data representing tissue “gain”.
237 Although these are consistent with previous observations reported in the literature
238 [9, 17, 21] and could be a simple reflection of true biologic variations of the tooth
239 surfaces, they are possibly an error in the data capture and analysis process.
240 Erroneous positive values are a known error when using a free-form 3D scan

241 alignment process [15]. The alignment is performed by minimising the mesh distance
242 error between each corresponding data point [21]. This will spread errors evenly over
243 positive and negative deviations until a “best fit” is obtained. If the algorithm decides
244 that the absolute distance between the two datasets is optimally minimized by
245 causing a positive deviation in one area to counteract a large negative deviation in
246 another, it will align the two scans in this way, regardless of the clinical outcome.
247 This is to a large extent overcome by aligning on reference areas less likely to have
248 changed but positive errors will still occur directly impacting on the sensitivity and
249 specificity of the process [15]. Thirdly, IOS on study cast models were used as
250 opposed to direct intraoral scans. Although this offers advantages, such as, being
251 able to ensure an accurate scan there are several disadvantages. In addition to
252 errors in the image processing of an intraoral scan there are also errors in the
253 impression and pouring of a cast which has been estimated to be in the order of 15
254 μm [9]. It is unknown whether the rates of wear on orthodontic patients are different
255 to that of patients who have not undergone orthodontic treatment and this is a
256 limitation of the study. The movement of teeth into positions where the occlusal
257 forces may be unevenly distributed during periods of treatment may exacerbate wear
258 progression rates on those areas. However, as tooth wear is a relatively slow
259 process unless there is an underlying acid involved this may be unlikely to have a
260 significant impact unless previous risk factors were already present. Cunha-Cruz et
261 al., 2010 did not find a direct association between TW and patients wearing
262 orthodontic appliances [22]. Nevertheless, in Belgium 50% of adolescents are being
263 treated or are still under orthodontic treatment [23]. The results of this investigation

264 can be generalized to this group within the limitations of the study. Finally, a good
265 sensitivity but a moderate specificity was observed for intraoral scans as a diagnostic
266 tool. This would ideally be improved through improved technology and a more
267 accurate registration system. However, if enhanced preventive treatment and not
268 restorative treatment, is the outcome of diagnosis, including more false positives in
269 a prevention programme is unlikely to impart harm.

270 Bearing these limitations in mind, this study demonstrates for the first time that there
271 are significantly different increased rates of volume loss in those with visible ETW
272 progression and compared to those with no wear progression. The recommended
273 value for diagnosing a high rate of ETW progression in adolescents, from results
274 observed in this study is -1.22mm^3 over a two-year period. Using this cut-off as the
275 point at which to engage on a preventative programme may delay visible tooth wear
276 progression, although this would have to be confirmed with longitudinal clinical
277 studies, ideally in multiple age groups controlling for risk factors. This also requires
278 further testing with shorter time periods as we know that wear is non-linear [24]. The
279 technique is still developing. The resolution of the IOS is still inferior to that of a
280 laboratory scanner or profilometer. However, this is likely to improve as future
281 technology improves. Scans were also done on casts and direct intraoral
282 measurements may have improved sensitivity of the analysis. Lastly, the alignment
283 process still introduces a large amount of subjectivity and operator error. It is likely
284 that the use of machine learning will help reduce the human error in the future.
285 Further research is required is to establish the true accuracy of IOS for quantifying
286 ETW and in improving the accuracy of the registration technique.

287

288 **Conclusions**

289 Volumetric analysis of dental tissue loss resulted in a good AUC of 0.80 (95%CI
290 0.70-0.89, $p < 0.001$). A cut off point of -1.22 mm^3 was associated with a sensitivity of
291 79% and a specificity of 61% of predicting visible erosive tooth wear progression
292 over 2 years. However, as the standard deviations for measurements are large,
293 quantitative measurement of wear using intraoral scans remains a tool to be used
294 as an adjunct to history taking and clinical judgement.

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300 **Foot Notes Figures**

301

302 **Figure 1.** Graphical description of alignment protocol using WearCompare. (A)
303 Initial alignment of baseline and follow-up scans is provided automatically by the
304 software; (B) Red line is drawn to outline the occlusal surface that aims to be
305 measured, and references areas (in yellow) are chosen to perform a selective
306 surface alignment; (C) Measurement plane perpendicular to the occlusal plane
307 activated; (D) Resulting color distance map of superposition with metrics
308 information included.

309

310 **Figure 2.** ROC curves predicting visible progression against rates of volume loss,
311 mean profile loss and maximum point loss over the study period. The highest Area
312 Under the Curve (AUC) was observed for volume loss progression rates (dark blue
313 line).

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319 **References**

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