

This is a repository copy of *Probabilistic biomechanical finite element simulations:whole-model classical hypothesis testing based on upcrossing geometry*.

White Rose Research Online URL for this paper:

<https://eprints.whiterose.ac.uk/105935/>

Version: Accepted Version

Article:

Pataky, Todd, Koskei, Michihiko and Cox, Philip Graham orcid.org/0000-0001-9782-2358
(2016) Probabilistic biomechanical finite element simulations:whole-model classical hypothesis testing based on upcrossing geometry. PeerJ. e96. ISSN 2167-8359

<https://doi.org/10.7717/peerj-cs.96>

Reuse

This article is distributed under the terms of the Creative Commons Attribution (CC BY) licence. This licence allows you to distribute, remix, tweak, and build upon the work, even commercially, as long as you credit the authors for the original work. More information and the full terms of the licence here:

<https://creativecommons.org/licenses/>

Takedown

If you consider content in White Rose Research Online to be in breach of UK law, please notify us by emailing eprints@whiterose.ac.uk including the URL of the record and the reason for the withdrawal request.

1 Probabilistic biomechanical finite element 2 simulations: whole-model classical 3 hypothesis testing based on upcrossing 4 geometry

5 Todd C. Pataky¹, Michihiko Koseki², and Philip G. Cox^{3,4}

6 ¹Institute for Fiber Engineering, Shinshu University, Ueda, Japan

7 ²Department of Bioengineering, Shinshu University, Ueda, Japan

8 ³Centre for Anatomical and Human Sciences, Hull York Medical School, University of
9 York, UK

10 ⁴Department of Archaeology, University of York, UK

11 ABSTRACT

12 Statistical analyses of biomechanical finite element (FE) simulations are frequently conducted on scalar
13 metrics extracted from anatomically homologous regions, like maximum von Mises stresses from demar-
14 cated bone areas. Advantages of this approach are numerical tabulability and statistical simplicity,
15 but disadvantages include region demarcation subjectivity, spatial resolution reduction, and results inter-
16 pretation complexity when attempting to mentally map tabulated results to original anatomy. This study
17 proposes a method which abandons the two aforementioned advantages to overcome these three limita-
18 tions. The method is inspired by parametric random field theory (RFT), but instead uses a non-parametric
19 analogue to RFT which permits flexible model-wide statistical analyses through non-parametrically
20 constructed probability densities regarding volumetric upcrossing geometry. We illustrate method funda-
21 mentals using basic 1D and 2D models, then use a public model of hip cartilage compression to highlight
22 how the concepts can extend to practical biomechanical modeling. The ultimate whole-volume results
23 are easy to interpret, and for constant model geometry the method is simple to implement. Moreover,
24 our analyses demonstrate that the method can yield biomechanical insights which are difficult to infer
25 from single simulations or tabulated multi-simulation results. Generalizability to non-constant geometry
26 including subject-specific anatomy is discussed.

27 Keywords: Biomechanics, Finite element analysis, Computational statistics, Probabilistic simulation,
28 Random field theory

29 1 INTRODUCTION

30 In numerical finite element (FE) simulations of biomechanical continua model inputs like material
31 properties and load magnitude are often imprecisely known. This uncertainty arises from a variety of
32 sources including: measurement inaccuracy, *in vivo* measurement inaccessibility, and natural between-
33 subject material, anatomical and loading variability (Cheung et al., 2005; Ross et al., 2005; Cox et al.,
34 2011, 2015; Fitton et al., 2012b). Despite this uncertainty, an investigator must choose specific parameter
35 values because numerical simulation requires it. Parameters are typically derived from published data,
36 empirical estimation, or mechanical intuition (Kupczik et al., 2007; Cox et al., 2012, 2013; Rayfield,
37 2011; Cuff et al., 2015).

38 It is also possible to perform multiple FE simulations using a spectrum of feasible model input values
39 to generate a distribution of model outputs (Dar et al., 2002; Babuska and Silva, 2014). More simply,
40 probabilistic model inputs yield probabilistic outputs, and continuum mechanics' inherent nonlinearities
41 ensure that these input and output probabilities are nonlinearly related. Probing output distributions
42 statistically therefore generally requires numerical simulation. Such analyses can require substantial
43 computational resources: probabilistic FE outputs have been shown to converge to stable numerical values
44 only for on-the-order of 1000 to 100,000 simulation iterations depending on model complexity (Dopico-

45 González et al., 2009). The advent of personal computing power has mitigated problems associated with
 46 this computational demand and has led to a sharp increase in probabilistic FE simulation in a variety of
 47 engineering fields (Stefanou, 2009) including biomechanics (Easley et al., 2007; Laz et al., 2007; Lin
 48 et al., 2007; Radcliffe and Taylor, 2007; Fitzpatrick et al., 2012).

49 Producing a probabilistic input-output mapping is conceptually simple: iteratively change input
 50 parameters according to a particular distribution and assemble output parameters for each iteration to
 51 yield an output distribution. The simplest method is Monte Carlo simulation which randomly generates
 52 input parameters based on given mean and standard deviation values (Dar et al., 2002). More complex
 53 methods like Markov Chain Monte Carlo can accelerate probabilistic output distribution convergence
 54 (Boyaval, 2012).

55 Once probabilistic inputs / outputs are generated they may be probed using a variety of statistical
 56 methods. A common technique is to extract scalars like maximum von Mises stress from anatomically
 57 demarcated regions of interest (Radcliffe and Taylor, 2007). Other techniques include Taguchi global
 58 model comparisons (Taguchi, 1987; Dar et al., 2002; Lin et al., 2007) to fuzzy set modeling (Babuska and
 59 Silva, 2014) and probability density construction for specific model parameters (Easley et al., 2007; Laz
 60 et al., 2007; McFarland and Mahadevan, 2008; Dopico-González et al., 2009).

61 The purpose of this paper is to propose an alternative method which conducts classical hypothesis
 62 testing at the whole-model level using continuum upcrossing geometry. An ‘upcrossing’ is a portion of
 63 the continuum that survives a threshold (Fig.1) like an island above the water’s surface or a mountain
 64 top above clouds. Each upcrossing possess a number of geometrical features including maximum height,
 65 extent and integral, where integrals, for examples, are areas, volumes and hyper-volumes for 1D, 2D
 66 and 3D continua, respectively. Parametric solutions to upcrossing geometry probabilities exist for n -
 67 dimensional Gaussian continua in the random field theory (RFT) literature (Adler and Taylor, 2007), and
 68 non-parametric approximations have been shown to be equally effective (Nichols and Holmes, 2002). The
 69 method we propose follows the latter, non-parametric permutation approach because it is ideally suited to
 70 the iterative simulation which characterizes probabilistic FE analysis.

71 The method is inspired by hypothesis testing approaches in nonlinear modeling (Legay and Viswanatha,
 72 2009) and in particular a label-based continuum permutation approach (Nichols and Holmes, 2002). It first
 73 assembles a large number of element- or node-based test statistic volumes through iterative simulation,
 74 then conducts inference using non-parametrically estimated upcrossing probabilities. These upcrossing
 75 distributions form a general framework for conducting classical, continuum-level hypothesis testing on
 76 FE models in arbitrarily complex experiments.

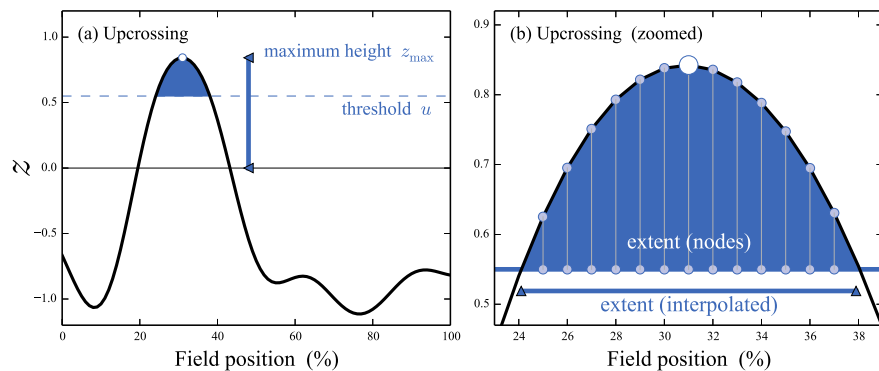


Figure 1. Example upcrossing in a 1D continuum. A thresholded continuum contains zero or more upcrossings, each with particular geometric characteristics including: maximum height, extent, integral, etc., each of which is associated with a different probability. The maximum height characteristic — across all upcrossings — can be used to conduct classical hypothesis testing as described in §2.

77 2 METHODS

78 All analyses were implemented in FEBio v.2.4.2 and v.2.5.0 (Maas et al., 2012) and Python 2.7
 79 (van Rossum, 2014). All partial differential equations underlying the models’ numerical solutions are

80 described in the FEBio Theory Manual (Maas et al., 2015). Model files and analysis scripts are available
 81 in this project's GitHub repository (github.com/0todd0000/probFEApy).

82 2.1 Models

83 2.1.1 Model A: Simple anisotropic bone compression

84 A single column of hexahedral elements (Fig.2a) with anisotropic stiffness (Fig.2b) was used to repre-
 85 sent bone with local material inconsistencies. This simplistic model was used primarily to efficiently
 86 demonstrate the key concepts underlying the proposed methodology. Nodal displacements were fully
 87 constrained at one end, and a total compressive force of 8000 N was applied to the other end along the
 88 longitudinal axis. The bone material was linearly elastic with a Poisson's ratio of 0.3.

89 Local anisotropy in Young's modulus (Fig.2b) was created using Gaussian pulses centered at 70%
 90 along the bone length with amplitudes and breadths of approximately 10% and 20%, respectively. The
 91 actual amplitudes and breadths of the stiffness increase were varied randomly to simulate an experiment
 92 involving $N=8$ randomly sampled subjects in which the bone's anisotropic stiffness profile was measured
 93 separately for each subject. Additionally, a small random signal was separately applied to each of the eight
 94 cases to ensure that variance was greater than zero, and thus that test statistic values were computable at
 95 all points in the continuum.

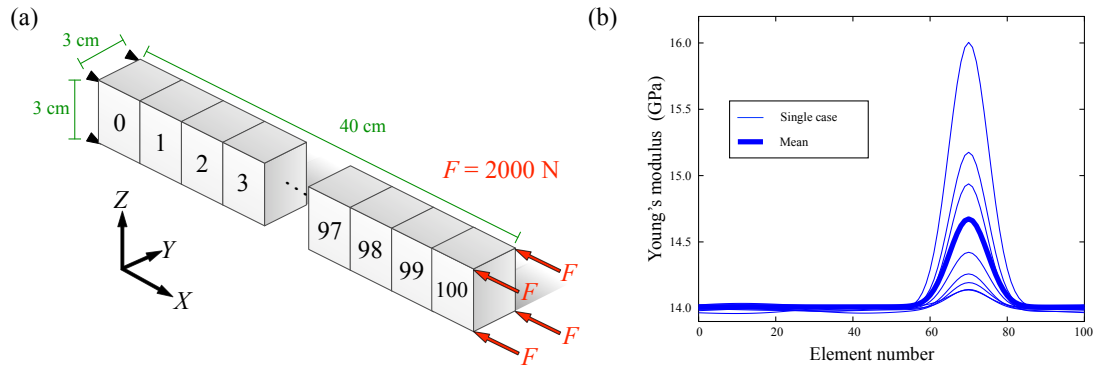


Figure 2. Model A. (a) Stack of cuboids representing a simplified bone. (b) Elemental Young's moduli representing local stiffness increase in $N=8$ cases.

96 2.1.2 Model B: Soft tissue indentation

97 A rigid hexahedral block was compressed against soft tissue to a depth of 1 cm height as depicted in
 98 Fig.3. Nodal displacements on the soft tissue's bottom surface were fully constrained. The soft tissue was
 99 modeled as hyperelastic with the following Moony-Rivlin strain energy function (Maas et al., 2015) :

$$W = a(I - 3) + \frac{k}{2}(\ln J)^2 \quad (1)$$

100 Here a is the hyperelastic parameter, k is the elasticity volume modulus, I is the deformation tensor's
 101 first deviatoric invariant, and J is the deformation Jacobian. The parameter a was set to 100 and eight k
 102 values (800, 817, 834, 851, 869, 886, 903, 920) were compared to a datum case of $k=820$.

103 Additionally, three different indenter face types were compared. The first indenter face was perfectly
 104 flat, and the other two were uneven but smooth as depicted in Fig.4. The uneven surfaces were generated
 105 by adding spatially smoothed Gaussian noise to the indenter face's z coordinates (i.e. the compression
 106 direction), then scaling to a maximum value of approximately 2.5 mm, or 1.7% the indenter's height.

107 2.1.3 Model C: Hip cartilage compression

108 A separately-published model of hip cartilage compression (Maas et al., 2015) (Fig.5) was selected to
 109 demonstrate how the concepts from the simple models A and B above may extend to realistic biomedical
 110 applications. This model is available in the FEBio test suite (febio.org; model name: "hip_n10rb"),
 111 and the scripts we used to manipulate this model are available in this paper's GitHub repository (github.com/0todd0000/probFEApy).
 112

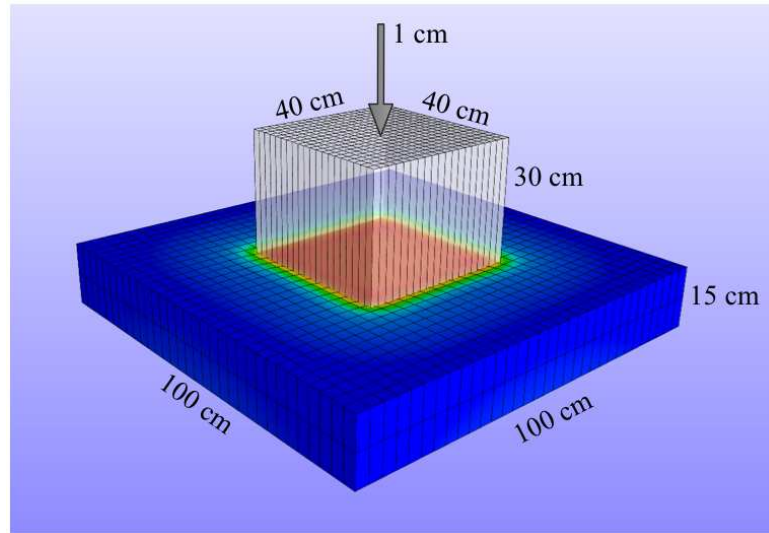


Figure 3. Model B: rigid block indentation on a hyperelastic material.

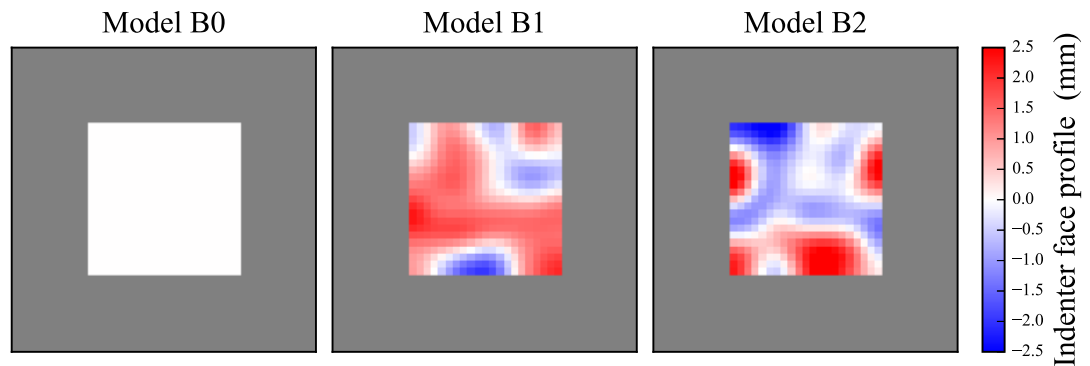


Figure 4. Model B indenter faces. The grey area depicts the compressed soft tissue.

113 The bones were rigid and the cartilage was modeled using the hyperelastic Mooney-Rivlin model
 114 above (Eqn.1) with a constant a value of 6.817. Ten different values of k were simulated for each of two
 115 hypothetical groups (Table 1) to mimick a two-sample experiment involving *in vivo* or *in vitro* material
 116 property measurements. The pelvis and acetabular cartilage were fixed and the femur was kinematically
 117 driven 1 mm in the upward direction.

Table 1. Model C material parameters; see Eqn.1. SD = standard deviation.

Group	Mooney-Rivlin k values	Mean (SD)
1	[1200, 1230, 1260, 1290, 1320, 1350, 1380, 1410, 1440, 1470]	1335 (90.8)
2	[1380, 1410, 1440, 1470, 1500, 1530, 1560, 1590, 1620, 1650]	1515 (90.8)

118 2.2 Analysis

119 We used a non-parametric permutation method from the Neuroimaging literature (Nichols and Holmes, 2002)
 120 to conduct classical hypothesis testing at the whole-model level. The technique employs observation per-
 121 mutation to generate non-parametric approximations to probabilities from (parametric) multi-dimensional

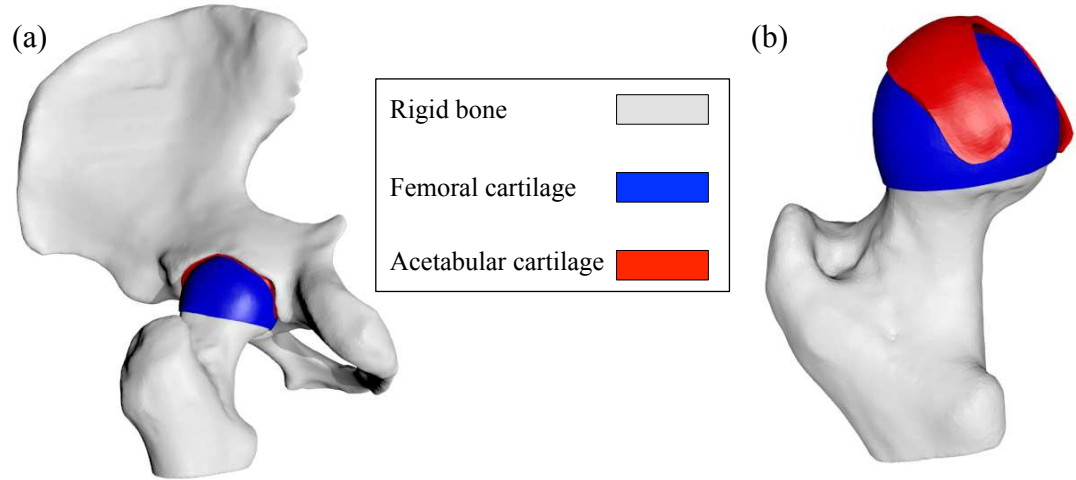


Figure 5. Model C; “hip_n10rb” from the FEBio test suite containing femoral and acetabular cartilage compressed via rigid bone displacement. (a) Full model. (b) Pelvis removed to expose the cartilage surface geometries.

122 Random Field Theory (Adler and Taylor, 2007). The method is described below and is depicted in Fig.6.
 123 All permutations described below were applied to pre-simulated FEA results.

124 2.2.1 Model A

125 The datum Young’s modulus ($E=14$ GPa) was subtracted from the eight 1D Young’s modulus continua
 126 (Fig.2b), and the resulting difference continua were sign-permuted (Fig.6a) to generate a number of
 127 artificial data samples. For each sample the t continuum was computed according to the typical one-
 128 sample t statistic definition:

$$t(\mathbf{q}) = \frac{\bar{y}(\mathbf{q}) - \mu(\mathbf{q})}{s(\mathbf{q})/\sqrt{N}} \quad (2)$$

129 where \bar{y} is the sample mean, μ is the datum, s is the sample standard deviation, N is sample size and \mathbf{q}
 130 is continuum position. Repeating for all permutation samples produced a distribution of 1D t continua
 131 (Fig.6b), whose maxima formed a ‘primary’ probability density function (PDF) (Fig.6c). This primary
 132 PDF represents the expected maximum difference (from the datum case of $E = 14$ GPa) that smooth,
 133 purely random continua would be expected to produce if there were truly no effect.

134 We conducted classical hypothesis testing at $\alpha=0.05$ using the primary PDF’s 95th percentile (t^*)
 135 as the criterion for null hypothesis rejection; if the t continuum associated with original, non-permuted
 136 data (Fig.6a) exceeded t^* the null hypothesis was rejected. In this example the original t continuum
 137 failed to traverse t^* (Fig.6e) so the null hypothesis was not rejected. Based on the primary PDF the exact
 138 probability value was: $p = 0.101$ in the depicted example.

139 We repeated this procedure for the effective strain and von Mises stress distributions associated with
 140 the eight Young’s modulus continua. In cases where the original t continuum exceeded the t^* threshold,
 141 probabilities associated with the upcrossing(s) (Fig.1) were computed with a ‘secondary’ PDF (Fig.6d)
 142 which embodied the probability of observing upcrossings with particular volume (i.e. supra-threshold
 143 integral). Note that (i) $(1-\alpha)\%$ of the values in the secondary PDF are zero by definition, (ii) an upcrossing
 144 which infinitesimally exceeds t^* has an integral of zero and a p value of α , and (iii) the minimum
 145 upcrossings p value is $1/n$, where n is the total number of permutations. All integrals were computed
 146 using trapezoidal approximation.

147 2.2.2 Model A, Part 2

148 We conducted a secondary analysis of Model A to examine how additional probabilistic variables
 149 increase computational demand. For this analysis we considered load direction (θ) to be uncertain,

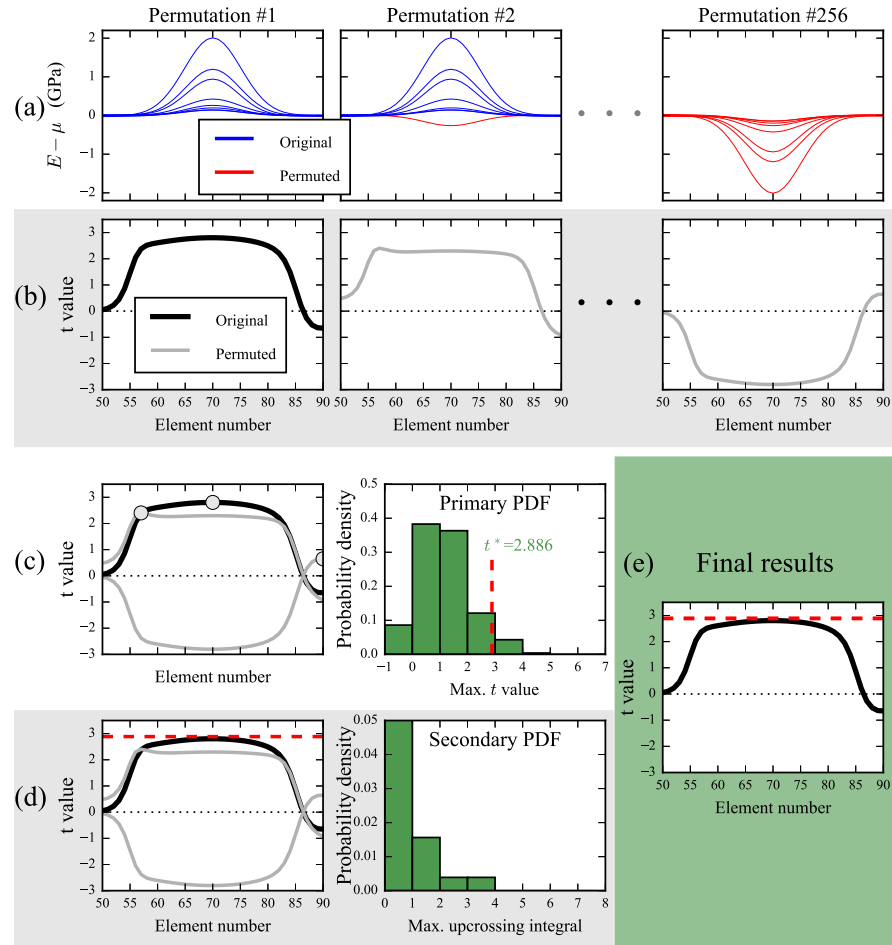


Figure 6. Depiction of non-parametric, permutation-based continuum-level hypothesis testing. This example uses five of the Young’s modulus continua from Fig.2b and compares the mean continuum to the datum: $\mu=14$ GPa. (a) Original continua were sign-permuted by iteratively multiplying subsets by -1 . (b) For each permutation a t continuum was computed using Eqn.2 . (c) The maximum t values from all permutations were assembled to form a primary probability density function (PDF) from which a critical test statistic (t^*) was calculated. (d) Thresholding all permuted test statistic continua at t^* produced upcrossings (Fig.1) whose integral formed a secondary PDF from which upcrossing-specific p values are computable. (e) Since the original test statistic continuum failed to traverse t^* the null hypothesis was not rejected at $\alpha=0.05$ for this example.

150 with a mean of zero and a standard deviation of 3 deg (forces with $\theta=0$ deg are depicted in Fig.2a,
 151 and these forces were rotated about the depicted Y axis). For typical simulation of random variables
 152 hundreds or thousands of simulations are usually needed to achieve probability distribution convergence
 153 (Dopico-González et al., 2009) , but we aimed to show that computational increases may be minimal for
 154 the proposed hypothesis testing framework.

155 We randomly varied θ for an additional 400 FE simulations, 50 for each of the observations depicted in
 156 Fig.2b. We then qualitatively compared the permutation-generated distribution of t continua after just
 157 16 simulations (one extra FE simulation for each observation) to the distribution obtained after 400 FE
 158 simulations. To quantitatively assess the effects of the number of simulations N on the distributions we
 159 examined the null hypothesis rejection rate for the $N=16$ and $N=400$ cases as a function of the number of
 160 post-simulation permutations.

161 2.2.3 Model B

162 The goal of Model B analysis was to qualitatively assess the effects of imperfect contact geometry (Fig.4)
 163 on both mean FE simulation results and statistical interpretations. Nine simulations were conducted

164 for each of the three indenter faces (Fig.4): one datum ($k=820$) and then the eight other values of k as
165 described above. For each indenter we computed the mean von Mises stress distribution in the compressed
166 soft tissue, then compared this mean to the datum ($k=820$) stress distribution through the one-sample test
167 statistic (Eqn.2) .

168 **2.2.4 Model C**

169 The goal of Model C analysis was to demonstrate how the analysis techniques and results for Model A
170 and Model B extend to realistic, complex models. The null hypothesis of equivalent von Mises stress
171 distributions in each group (Table 1) was tested using a slight modification of the permutation approach
172 described above (Fig.6). The only differences were that (i) the two-sample t statistic was computed instead
173 of the one-sample t statistic, and (ii) group permutations were conducted instead of sign permutations.
174 Group permutations were performed by randomly assigning each of the 20 continuum observations to
175 one of the two groups, with ten observations in each group, then repeating for a total of 10,000 random
176 permutations. Although the total number of possible permutations was $20! / (10! 10!) = 184,756$, we
177 found no qualitative effect of adding more than 10,000 permutations.

178 **3 RESULTS**

179 **3.1 Model A**

180 FE simulations of each of the eight cases depicted in Fig.2b yielded the stress/strain distributions and
181 t statistic distributions depicted in Fig.7. In this example Young's moduli only increased (Fig.7a) and
182 strain only decreased (Fig.7b), but stress exhibited central increases (near element #70) and peripheral
183 decreases (near elements #60 and #80) (Fig.7c), emphasizing the nonlinear relation between model inputs
184 and outputs.

185 Maximum absolute t values differed amongst the field variables (Fig.7d–f), with stress exhibiting the
186 largest maximum absolute t values. The null hypothesis was rejected for von Mises stresses but not for
187 either Young's modulus or effective strain. Additionally, both stress increases and stress decreases were
188 statistically significant (Fig.7f). These results indicate that statistical signal associated with the Young's
189 modulus inputs was amplified in the von Mises stress field, but we note that strain would have been the
190 amplified variable had the the model been displacement-loaded instead of force-loaded. More generally
191 these results show that statistical conclusions pertaining to different model variables can be quite different,
192 and that different continuum regions can respond in opposite ways to probabilistic inputs.

193 Although stiffness increased non-uniformly as a Gaussian pulse (Fig.7a) the test statistic magnitude
194 was effectively uniform across that region (elements 60 – 80; Fig.7d). This suggests that mechanical and
195 statistical magnitudes are not directly related, and thus that statistical conclusions mustn't be limited to
196 areas of large mechanical signal unless one's hypothesis pertains specifically to those areas.

197 **3.2 Model A, Part 2**

198 Adding uncertainty to the load direction increased variability and thus caused absolute t value decreases
199 near element #70 (Fig.8a), but general loading environment changes caused increases to absolute t values
200 in other model areas, especially toward elements #50 and #90. The stress response was somewhat different
201 , with absolute t values increasing near element #70 but decreasing elsewhere (Fig.8c), re-emphasizing
202 the complex relation amongst different field variables' response to probabilistic model features.

203 The t distributions for stress and strain were not qualitatively affected by the number of additional
204 FE simulations; 16 simulations, or one extra simulation per observation (Fig.8a,c) yielded essentially the
205 same results as 400 simulations (Fig.8b,d). The reason is that permutation leverages variability in small
206 samples to produce a large number of artificial samples, and thereby approximates the results of a large
207 number of FE simulations.

208 To quantify t continuum distribution stability as a function of the number of permutations we con-
209 sidered the null hypothesis rejection rate in both cases of 16 and 400 FE simulations (Fig.9). After
210 approximately 200 permutation iterations the null hypothesis rejection rate was effectively identical for
211 both 16 and 400 FE simulations. These results suggest that permutation, which is extremely fast compared
212 to FE simulation, may be able to effectively approximate a large number of FE simulations using the
213 results of only a few FE simulations.

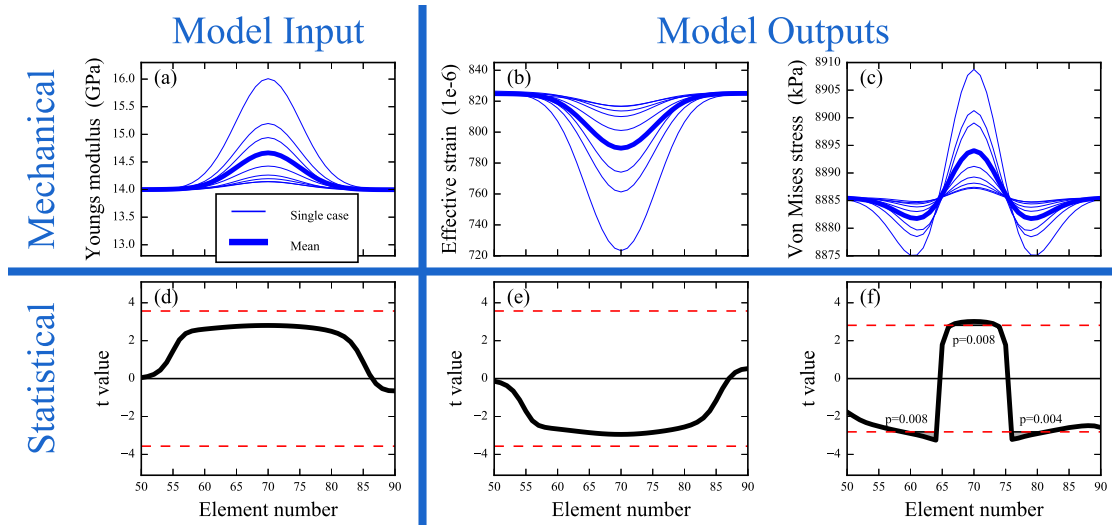


Figure 7. Model A results. (a–c) Young’s modulus input observations and strain/stress continua associated with each observation. (d–f) Hypothesis testing results ($\alpha=0.05$); red dotted lines depict critical thresholds.

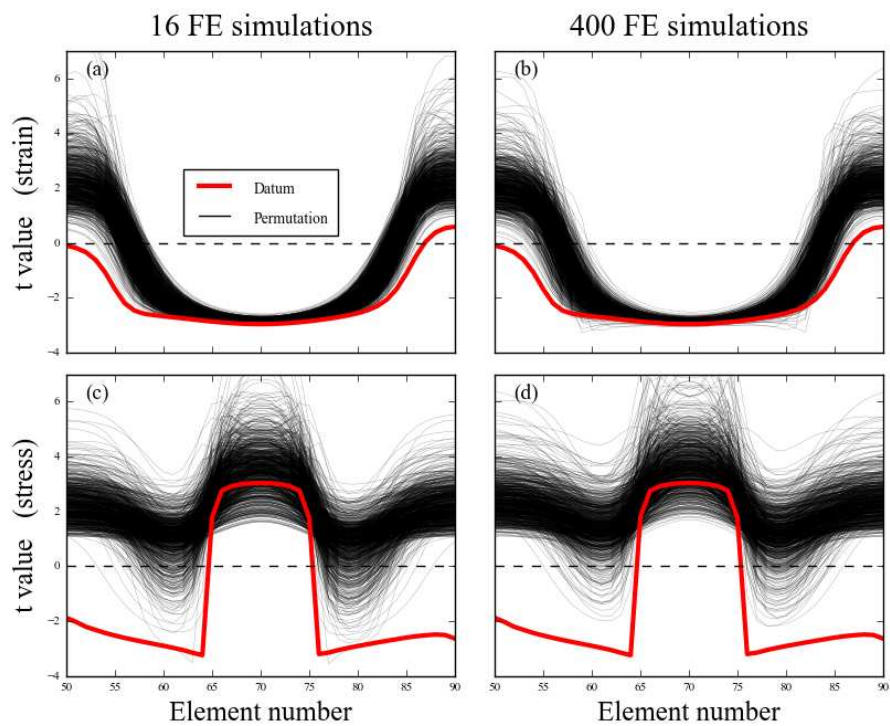


Figure 8. Model A t distributions for strain (upper panels) and stress (lower panels) under a load direction uncertainty with a standard deviation of 3 deg.

214 3.3 Model B

215 The mean stress distributions associated with the three indenter faces (Fig.10) closely followed indenter
 216 face geometry (Fig.3). Variation in material parameters was associated with stress distribution variability
 217 (Fig.11a). Nevertheless, t values were effectively constant across all elements and all three models
 218 (Fig.11b). This suggests that test statistic continua are more robust to model geometry imperfections than
 219 are stress/strain continua.

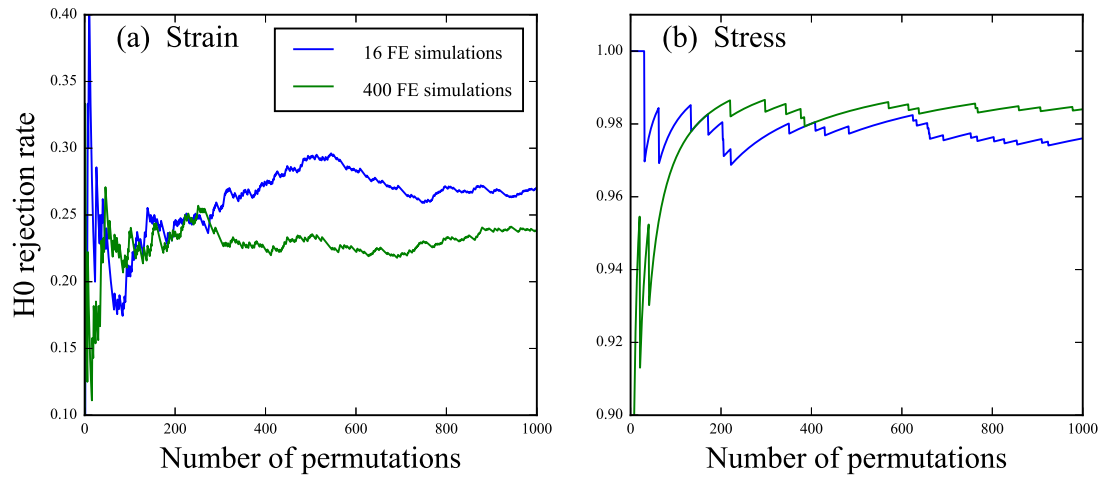


Figure 9. Model A null hypothesis (H_0) rejection rate as a function of the number of permutations for both 16 and 400 FE simulations.

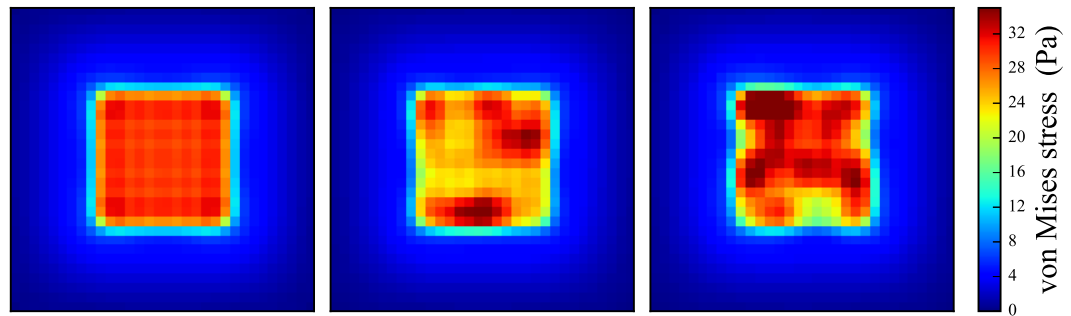


Figure 10. Model B mean stress distributions for the three indenter faces. Note that these patterns closely follow the indenter face geometry depicted in Fig.4.

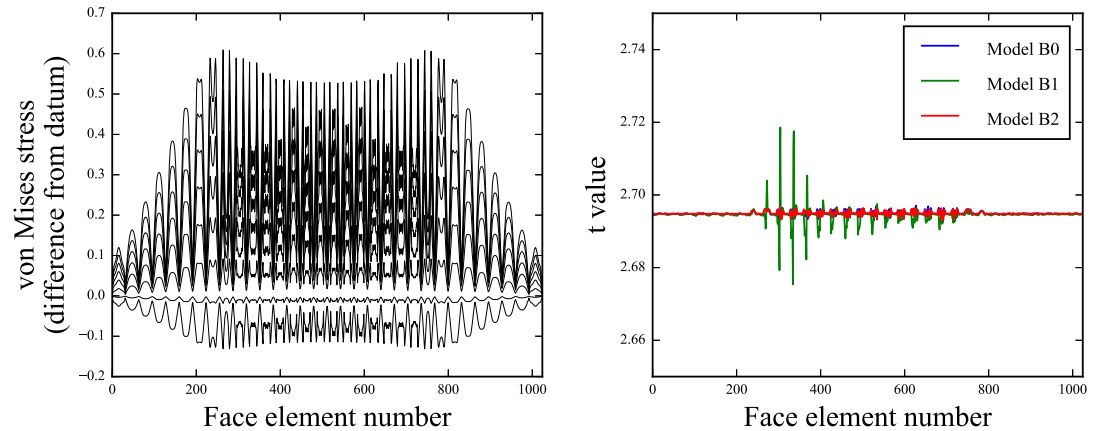


Figure 11. Model B statistical results. (a) Large variation was present amongst the individual continua (only Model B0 results shown). (b) Test statistic continua were effectively constant in all elements and across all three indenters.

220 3.4 Model C

221 A two-sample t test regarding the material parameters (Table 1) yielded $t=5.17$, $p<0.001$ and thus a
 222 rejection of the null hypothesis of equal group means. These probabilistic material parameters produced

223 mean stresses which were generally higher in Group B vs. Group A (Fig.12), where a stress distribution
224 difference plot clarified that inter-group differences were generally confined to areas of large stress
225 (Fig.13). The inter-group statistical differences were much broader, covering essentially the entire femoral
226 cartilage (Fig.14). Moreover, relatively broad regions of the cartilage exhibited significant stress *decreases*,
227 similar to the result observed in the simple bone model (Fig.7f).

228 These results reiterate many of the aforementioned methodological points. In particular, changes in
229 probabilistic model inputs (in this case: material parameter values) can have statistical effects on output
230 fields (in this case: von Mises stresses) which are not easily predicted. Additionally, the visual advantages
231 of full-field analyses are somewhat clearer in this more anatomically correct model; tabulated stresses
232 from different regions of the femoral cartilage would be more difficult to interpret in terms of the original
233 anatomy. Last, mechanical (Fig.13) and statistical (Fig.14) results can be quite different.

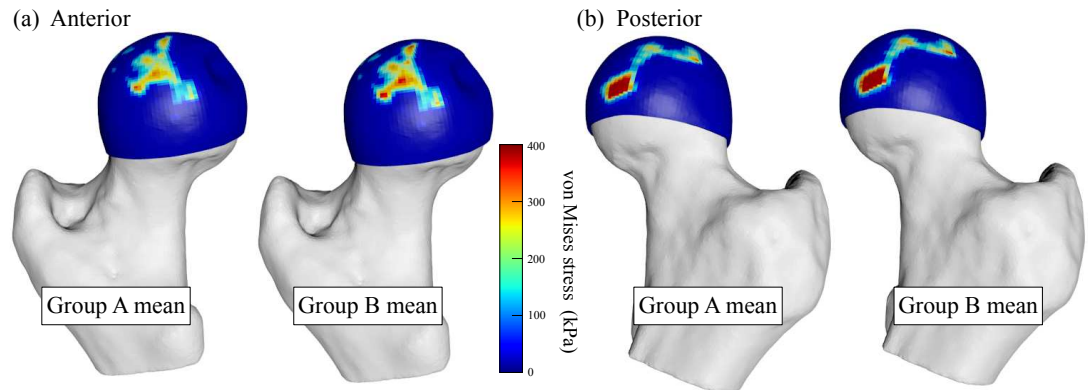


Figure 12. Model C: mean stress distributions.

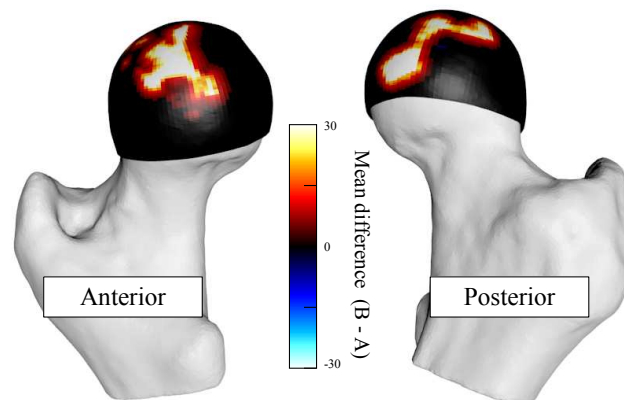


Figure 13. Model C: mean stress difference.

234 4 DISCUSSION

235 This paper demonstrated how a non-parametric permutation technique from Neuroimaging (Nichols and Holmes, 2002)
236 can be used to conduct classical continuum-level hypothesis testing for finite element (FE) models. It's
237 main advantages are:

- 238 1. Easy implementation. As demonstrated in this project's software repository (github.com/0todd0000/probFEapy), non-parametric hypothesis testing for FE models can be implemented
239 using relatively compact scripts.
240

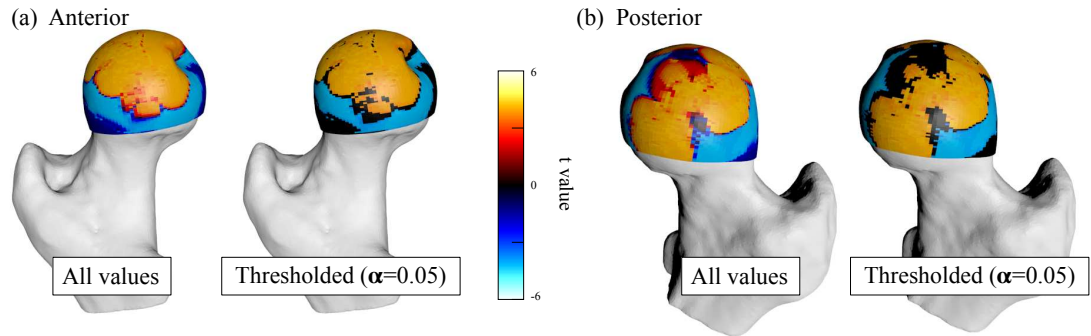


Figure 14. Model C: statistical results.

- 241 2. Computational efficiency. After simulating subject-specific results — which is usually necessary in
 242 arbitrary multi-subject studies — no additional FE simulations are needed; permutation can operate
 243 on pre-simulated small-sample results to approximate large-sample probabilities (Fig.6). Producing
 244 the main Model A results (Fig.7) required a total of only 1.3 s to execute on a desktop PC, including
 245 both FE simulations and permutation-based probability computation.
- 246 3. Non-measured uncertainty capabilities. Adding uncertainty in the form of random model parameters
 247 does not necessarily require large increases in computational demands; results suggest that with
 248 respect to an original dataset with N simulations, it may be possible to robustly accommodate
 249 additional uncertainty with just N additional simulations (Figs.8–9).
- 250 4. Visual richness and tabulation elimination. Continuum-level hypothesis testing results can be
 251 presented in the same geometric context as commonly visualized field variables like stress and
 252 strain (Fig.7b,e and Fig.7c,f), which eliminates the need to separately tabulate statistical results.
- 253 5. Arbitrarily complex experiments. While only one- and two-sample designs were considered here, t
 254 statistic continua generalize to F and all other test statistic continua, so arbitrarily complex designs
 255 ranging from regression to MANCOVA can be easily implemented using permutation.
- 256 6. Robustness to geometric imperfections. Small geometric changes can have qualitatively large
 257 effects on stress/strain continua, but have comparably little-to-no effect on test statistic continua
 258 (Fig.??), implying that continuum-level hypothesis testing may be more robust than commonly
 259 employed procedures which analyze local maxima. This potential danger is highlighted in the
 260 more realistic Model C, whose mean differences (Fig.13) exhibited high focal stresses whereas the
 261 statistical continuum was much more constant across the contact surface (Fig.14).

262 4.1 Mechanical vs. statistical interpretations

263 Mechanical and statistical continua are generally different. For example, for Model A it is clear that
 264 each stiffness increase (Fig.2b) has *mechanical* effects on the strain/stress continuum, but the *statistical*
 265 effects are less clear because there is relatively large uncertainty regarding the true nature of the stiffness
 266 increase in the population that this sample represents. For classical hypothesis testing, mechanical
 267 meaning is irrelevant because all mechanical effects must be considered with respect to their uncertainty.
 268 Further emphasizing the tenuous relation between mechanical and statistical meaning are regions of
 269 small mechanical signals (for Model A: near the periphery of the stiffness increase region) which can be
 270 accompanied by relatively large statistical signals.

271 To objectively conduct classical hypothesis tests on FEA results it is therefore essential to explicitly
 272 identify the hypothesis prior to conducting simulations. If limiting analyses to only areas of large
 273 mechanical signal can be justified in an *a priori* sense, then those, and only those areas should be analyzed
 274 without any theoretical problem. If, however, one's *a priori* hypothesis pertains to general stress / strain
 275 distribution changes, and not specifically to areas of high mechanical signal, it may be necessary to
 276 consider the entire model because maximal mechanical and maximal statistical signals do not necessarily
 277 coincide.

4.2 Comparison with common techniques

In the literature, FE-based classical hypothesis testing is typically conducted via scalar analysis of local extrema (Radcliffe and Taylor, 2007). Applying that approach to the local mechanical change extrema in Model A (Fig.7a-c) yielded the results in Table 2. The null hypothesis (of no mean change with respect to the 14 GPa case) was rejected at $\alpha = 0.05$ for all three mechanical variables: Young's modulus, effective strain and von Mises stress.

While the test statistic magnitudes are the same for both the proposed whole-model approach (Fig.7) and these local extremum analyses, the critical threshold at $\alpha=0.05$ is different because the spatial scope is different. The broader the spatial scope of the hypothesis, the higher the threshold must be to avoid false positives (Friston et al., 2007); in other words, random processes operating in a larger volume have a greater chance of reaching an arbitrary threshold.

The proposed model-wide approach (Fig.7) and the local extremum (scalar) approach have yielded contradictory hypothesis testing conclusions for both Young's modulus and strain distributions, so which approach is correct? The answer is that both are correct, but both cannot be simultaneously correct. The correct solution depends on the *a priori* hypothesis, and in particular the spatial scope of that hypothesis. If the hypothesis pertains to only the local extremum, then the local extremum approach is correct, and whole-model results should be ignored because they are irrelevant to the hypothesis. Similarly, if the hypothesis pertains to the whole model, then the whole model results are correct and local extrema results should be ignored because they are irrelevant to the hypothesis. We would argue that all FE analyses implicitly pertain to the whole model unless otherwise specified, and that focus on specific scalar metrics is appropriate only if justified in an *a priori* manner.

Table 2. Model A results. Analyses of local extrema (at element 70) using a non-parametric permutation-based two-sample *t* test. SD = standard deviation.

Variable	Mean	SD	<i>t</i>	<i>p</i>
Young's modulus (GPa)	14.665	0.670	2.804	0.026
Effective strain (1e-6)	789.6	33.9	-2.946	0.022
von Mises stress (kPa)	8894.0	8.0	3.014	0.020

Historically in biomechanical FEA, low sample sizes (frequently $n = 1$ for each model) permitted nothing more than qualitative comparisons of stress or strain maps, and/or numerical comparison of output parameters at single nodes. Nevertheless conventional FEA can concurrently and ironically suffer from an excess of data when results are tabulated over many regions, often in a non-standardized manner across studies.

With the continued increase of computer power and processing speed, FE models comprising over one million elements are becoming more and more common (Moreno et al., 2008; Bright and Rayfield, 2011a; Cox et al., 2013, 2015; Cuff et al., 2015) (e.g. Moreno et al, 2008; Bright & Rayfield, 2011a; Cox et al, 2013, 2015; Cuff et al, 2015). Yet, typically stress and strain values are only reported and analysed from just a few elements (Porro et al., 2013; Fitton et al., 2012a). Alternatively average or peak stress or strain values can be computed for whole models (Dumont et al., 2011; Cox et al., 2012; Parr et al., 2013; Sharp and Rich, 2016) or selected regions (Wroe et al., 2007a,b; Nakashige et al., 2011). The recent application of geometric morphometrics to FEA results (Cox et al., 2011; Fitton et al., 2012b; O'Higgins and Milne, 2013) has gone some way to providing a method of analysing whole models rather than individual elements, but is limited to the analysis of deformations. The approach outlined here enables, for the first time, the analysis of all stresses or strains in a single hypothesis test.

Another major benefit of the technique outlined here is its ability to take in consideration input parameters that are only imprecisely known. When modelling biological structures, the material properties of the model, and the magnitude and orientations of the muscle loads cannot always be directly measured. This is an especially acute problem in studies dealing with palaeontological taxa. Previous research has addressed this issue principally by the use of sensitivity analyses which test the sensitivity of a model to changes in one or more unknown parameters (Kupczik et al., 2007; Bright and Rayfield, 2011a; Cox

321 et al., 2011, 2015; Reed et al., 2011; Wood et al., 2016; Toro-Ibacache et al., 2016). The models are
322 identical save for the unknown parameters, which are then varied between extremes representing likely
323 biological limits or the degree of uncertainty. In such studies, the number of different models is usually
324 quite low, with each parameter only being tested at a maximum of five different values. Our method takes
325 this approach to its perhaps logical extreme – the unknown parameter is allowed to vary randomly within
326 defined limits over a large number of iterations (usually on the order of 10,000). These iterations produce
327 a distribution of results that can be statistically compared with other such distributions.

328 A final advantage is that statistical continua may be less sensitive to geometric mesh peculiarities than
329 stress / strain continua. In Fig.10 and Fig.13, for example, it is clear from the oddly shaped regions of
330 stress difference that these effects were likely caused by mesh irregularities and that remeshing would
331 likely smooth out these areas of highly localized stress changes. The test statistic continuum, on the other
332 hand, appeared to be considerably less sensitive to localization effects (Fig.11) and (Fig.14). This may
333 imply that one needn't necessarily develop an ideal mesh, because statistical analysis may be able to
334 mitigate mesh peculiarity-induced stress distribution irregularities.

335 4.3 Limitations

336 The major limitation of the proposed method as it currently stands is that only models of identical geometry
337 can be compared. Thus, while the technique can be readily used to address sensitivity-like questions
338 regarding material properties, boundary conditions and orientations, the method cannot readily address
339 geometry-relevant questions, such as are created by varying mesh density (Bright and Rayfield, 2011b;
340 Toro-Ibacache et al., 2016), or are found in between-taxa analyses (Dumont et al., 2005, 2011; Oldfield
341 et al., 2012; Cox et al., 2012; Wroe et al., 2007a; Sharp, 2015). Nevertheless, through three-dimensional
342 anatomical registration (Friston et al., 2007) and also potentially intra-model spatial interpolation to
343 common continuum positions \mathbf{q} (Eqn.2), it may be possible to apply the technique to arbitrary geometries
344 even in cases of large deformation and/or geometrical disparity (Schnabel et al., 2003).

345 A second limitation is computational feasibility. Although our results suggest that incorporating a
346 single additional uncertain parameter into the model may not greatly increase computational demand,
347 this may not be true for higher dimensional parameter spaces. In particular, given N experimental
348 measurements, our results show that $2N$ simulations are sufficient to achieve probabilistic convergence
349 (Fig.9). However, this result may be limited to cases where the uncertainty is sufficiently small so
350 that it fails to produce large qualitative changes in the underlying stress/strain continua. Moreover, the
351 feasibility for higher-dimensional parameter spaces is unclear. In particular, a sample of N observations is
352 likely unsuitable for an N -dimensional parameter space, or even an $N/2$ -dimensional parameter space.
353 The relation between uncertainty magnitude, number of uncertain parameters, the sample size and the
354 minimum number of FE simulations required to achieve probabilistic convergence is an important topic
355 that we leave for future work.

356 A third potential limitation is that both upcrossing features and the test statistic continuum can be
357 arbitrary. In this paper we restricted analyses to the upcrossing maximum and integral due to the robustness
358 of these metrics with respect to other geometric features (Zhang et al., 2009). Other upcrossing metrics
359 and even arbitrary test statistic continua could be submitted to a non-parametric permutation routine.
360 This is partly advantageous because arbitrary smoothing can be applied to the continuum data, and in
361 particular to continuum variance (Nichols and Holmes, 2002), but it is also partly a disadvantage because
362 it increases the scope of analytical possibilities and thus may require clear justification and/or sensitivity
363 analyses for particular test statistic and upcrossing metric choices.

364 A final limitation is that the both the test statistic and probability continua are directly dependent on
365 the uncertainty one selects via model parameter variance. This affords scientific abuse because it allows
366 one to tweak variance parameters until the probabilistic results support one's preferred interpretation. We
367 therefore recommend that investigators both clearly justify variance choices and treat variance itself as a
368 target of sensitivity analysis.

369 4.4 Summary

370 This paper has proposed a probabilistic finite element simulation method for conducting classical hypoth-
371 esis testing at the continuum level. The technique leverages probability densities regarding geometric
372 features of continuum upcrossings, which can be rapidly and non-parametrically estimated using iterative
373 permutation of pre-simulated stress/strain continua. The method yields test statistic continua which are
374 visually rich, which may eliminate the need for tabulated statistical results, which may reveal unique

375 biomechanical information, and which also may be more robust to mesh and other geometrical model
376 peculiarities than stress/strain continua.

377 REFERENCES

- 378 Adler, R. J. and Taylor, J. E. (2007). *Random Fields and Geometry*. Springer-Verlag.
- 379 Babuska, I. and Silva, R. S. (2014). Dealing with uncertainties in engineering problems using only
380 available data. *Computer Methods in Applied Mechanics and Engineering*, 270(C):57–75.
- 381 Boyaval, S. (2012). A fast Monte-Carlo method with a reduced basis of control variates applied to
382 uncertainty propagation and Bayesian estimation. *Computer Methods in Applied Mechanics and
383 Engineering*, 241-244(C):190–205.
- 384 Bright, J. and Rayfield, E. (2011a). Sensitivity and ex vivo validation of finite element models of the
385 domestic pig cranium. *Journal of Anatomy*, 219:456–471.
- 386 Bright, J. and Rayfield, E. (2011b). The response of cranial biomechanical finite element models to
387 variations in mesh density. *Anatomical Record*, 294:610–620.
- 388 Cheung, J.-M., Zhang, M., Leung, A.-L., and Fan, Y.-B. (2005). Three-dimensional finite element analysis
389 of the foot during standing – a material sensitivity study. *Journal of Biomechanics*, 38:1045–1054.
- 390 Cox, P., Fagan, M., Rayfield, E., and Jeffery, N. (2011). Finite element modelling of squirrel, guinea pig
391 and rat skulls: using geometric morphometrics to assess sensitivity. *Journal of Anatomy*, 219:696–709.
- 392 Cox, P., Kirkham, J., and Herrel, A. (2013). Masticatory biomechanics of the Laotian rock rat, *Laonastes
393 aenigmamus*, and the function of the zygomaticomandibularis muscle. *PeerJ*, 1:e160.
- 394 Cox, P., Rayfield, E., Fagan, M., Herrel, A., Pataky, T., and Jeffery, N. (2012). Functional evolution of the
395 feeding system in rodents. *PLOS ONE*, 7(4):e36299.
- 396 Cox, P., Rinderknecht, A., and Blanco, R. (2015). Predicting bite force and cranial biomechanics in the
397 largest fossil rodent using finite element analysis. *Journal of Anatomy*, 226:215–223.
- 398 Cuff, A., Bright, J., and Rayfield, E. (2015). Validation experiments on finite element models of an ostrich
399 (*Struthio camelus*) cranium. *PeerJ*, 3:e1294.
- 400 Dar, F. H., Meakin, J. R., and Aspden, R. M. (2002). Statistical methods in finite element analysis. *Journal
401 of Biomechanics*, 35:1155–1161.
- 402 Dopico-González, C., New, A. M., and Browne, M. (2009). Probabilistic analysis of an uncemented total
403 hip replacement. *Medical Engineering and Physics*, 31(4):470–476.
- 404 Dumont, E., Davis, J., Grosse, I., and Burrows, A. (2011). Finite element analysis of performance in the
405 skulls of marmosets and tamarins. *Journal of Anatomy*, 218:151–162.
- 406 Dumont, E., Piccirillo, J., and Grosse, I. (2005). Finite-element analysis of biting behaviour and bone
407 stress in the facial skeletons of bats. *Anatomical Record Part A*, 283:319–330.
- 408 Easley, S. K., Pal, S., Tomaszewski, P. R., Petrella, A. J., Rullkoetter, P. J., and Laz, P. J. (2007).
409 Finite element-based probabilistic analysis tool for orthopaedic applications. *Computer Methods and
410 Programs in Biomedicine*, 85(1):32–40.
- 411 Fitton, L., Proa, M., Rowland, C., Toro-Ibacache, V., and O’Higgins, P. (2012a). The impact of simplifi-
412 cations on the performance of a finite element model of a *Macaca fascicularis* cranium. *Anatomical
413 Record*, 298:107–121.
- 414 Fitton, L., Shi, J., Fagan, M., and O’Higgins, P. (2012b). Masticatory loadings and cranial deformation in
415 *Macaca fascicularis*: a finite element analysis sensitivity study. *Journal of Anatomy*, 221:55–68.
- 416 Fitzpatrick, C. K., Baldwin, M. A., Clary, C. W., Wright, A., Laz, P. J., and Rullkoetter, P. J. (2012). Ident-
417 ifying alignment parameters affecting implanted patellofemoral mechanics. *Journal of Orthopaedic
418 Research*, 30(7):1167–1175.
- 419 Friston, K. J., Ashburner, J. T., Kiebel, S. J., Nichols, T. E., and Penny, W. D. (2007). *Statistical Parametric
420 Mapping: The Analysis of Functional Brain Images*. Elsevier, London.
- 421 Kupczik, K., Dobson, C., Fagan, M., Crompton, R., Oxnard, C., and O’Higgins, P. (2007). Assessing
422 mechanical function of the zygomatic region in macaques: validation and sensitivity testing of finite
423 element models. *Journal of Anatomy*, 210:41–53.
- 424 Laz, P. J., Stowe, J. Q., Baldwin, M. A., Petrella, A. J., and Rullkoetter, P. J. (2007). Incorporating
425 uncertainty in mechanical properties for finite element-based evaluation of bone mechanics. *Journal of
426 Biomechanics*, 40(13):2831–2836.
- 427 Legay, A. and Viswanatha, M. (2009). Simulation + Hypothesis Testing for Model Checking of Proba-

- 428 bilistic Systems. In *2009 Sixth International Conference on the Quantitative Evaluation of Systems*
429 (*QUEST*), pages 3–3. IEEE.
- 430 Lin, C.-L., Chang, S.-H., Chang, W.-J., and Kuo, Y.-C. (2007). Factorial analysis of variables influencing
431 mechanical characteristics of a single tooth implant placed in the maxilla using finite element analysis
432 and the statistics-based Taguchi method. *Eur J Oral Sci*, 115:408–416.
- 433 Maas, S., Ellis, B., Ateshian, G., and Weiss, J. (2012). FEBio: Finite Elements for Biomechanics. *Journal*
434 *of Biomechanical Engineering*, 134(1):011005–10.
- 435 Maas, S., Rawlins, D., Weiss, J., and Ateshian, G. (2015). FEBio theory manual version 2.4.
- 436 McFarland, J. and Mahadevan, S. (2008). Multivariate significance testing and model calibration under
437 uncertainty. *Computer Methods in Applied Mechanics and Engineering*, 197(29-32):2467–2479.
- 438 Moreno, K., Wroe, S., Clausen, P., McHenry, C., D’Amore, D., and Rayfield, E. J. and Cunningham,
439 E. (2008). Cranial performance in the Komodo dragon (*Varanus komodoensis*) as revealed by high-
440 resolution 3-D finite element analysis. *Journal of Anatomy*, 212:736–746.
- 441 Nakashige, M., Smith, A., and Strait, D. (2011). Biomechanics of the macaque postorbital septum
442 investigated using finite element analysis: implications for anthropoid evolution. *Journal of Anatomy*,
443 218:142–150.
- 444 Nichols, T. and Holmes, A. (2002). Nonparametric Permutation Tests for Functional Neuroimaging: A
445 Primer with Examples. *Human Brain Mapping*, 15(1):1–25.
- 446 O’Higgins, P. and Milne, N. (2013). Applying geometric morphometrics to compare in size and shape
447 arising from finite elements analyses. *Hystrix, the Italian Journal of Mammalogy*, 24:126–132.
- 448 Oldfield, C., McHenry, C., Clausen, P., Chamoli, U., Parr, W., Stynder, D., and Wroe, S. (2012). Finite
449 element analysis of ursid cranial mechanics and the prediction of feeding behaviour in the extinct giant
450 *Agriotherium africanum*. *Journal of Zoology*, 286:163–170.
- 451 Parr, W., Chamoli, U., Jones, A., Walsh, W., and Wroe, S. (2013). Finite element micro-modelling of a
452 human ankle bone reveals the importance of the trabecular network to mechanical performance: New
453 methods for the generation and comparison 3D models. *Journal of Biomechanics*, 46:200–205.
- 454 Porro, L., Metzger, K., Iriarte-Diaz, J., and Ross, C. (2013). In vivo bone strain and finite element
455 modelling of the mandible of *Alligator mississippiensis*. *Journal of Anatomy*, 223:195–227.
- 456 Radcliffe, I. A. J. and Taylor, M. (2007). Investigation into the affect of cementing techniques on load
457 transfer in the resurfaced femoral head: A multi-femur finite element analysis. *Clinical Biomechanics*,
458 22(4):422–430.
- 459 Rayfield, E. (2011). Strain in the ostrich mandible during simulated pecking and validation of specimen-
460 specific finite element models. *Journal of Anatomy*, 218:47–58.
- 461 Reed, D., Porro, L., Iriarte-Diaz, J., Lemberg, J., Holliday, C., Anapol, F., and Ross, C. (2011). The
462 impact of bone and suture material properties on mandibular function in *Alligator mississippiensis*:
463 testing theoretical phenotypes with finite element analysis. *Journal of Anatomy*, 218:59–74.
- 464 Ross, C., Patel, B., Slice, D., Strait, D., Dechow, P., Richmond, B., and Spencer, M. (2005). Modeling
465 masticatory muscle force in finite element analysis: sensitivity analysis using principal coordinates
466 analysis. *Anatomical Record Part A*, 283:288–299.
- 467 Schnabel, J. A., Tanner, C., Castellano-Smith, A. D., Degenhard, A., Leach, M. O., Hose, D. R., Hill,
468 D. L. G., and Hawkes, D. J. (2003). Validation of nonrigid image registration using finite-element
469 methods: application to breast MR images. *IEEE Transactions on Medical Imaging*, 22(2):238–247.
- 470 Sharp, A. (2015). Comparative finite element analysis of the cranial performance of four herbivorous
471 marsupials. *Journal of Morphology*, 276:1230–1243.
- 472 Sharp, A. and Rich, T. (2016). Cranial biomechanics, bite force and function of the endocranial sinuses in
473 *Diprotodon optatum*, the largest known marsupial. *Journal of Anatomy*, in press:doi: 10.1111/joa.12456.
- 474 Stefanou, G. (2009). Comput. methods appl. mech. engrg. *Computer Methods in Applied Mechanics and*
475 *Engineering*, 198(9-12):1031–1051.
- 476 Taguchi, G. (1987). *System of Experimental Design*. UNIPUB Kraus International Publications, New
477 York.
- 478 Toro-Ibacache, V., Fitton, L., Fagan, M., and O’Higgins, P. (2016). Validity and sensitivity of a human
479 cranial finite element model: implications for comparative studies of biting performance. *Journal of*
480 *Anatomy*, 228:70–84.
- 481 van Rossum, G. (2014). The python library reference release 2.7.8.
- 482 Wood, S., Strait, D., Dumont, E., Ross, C., and Grosse, I. (2016). The effects of modelling simplifications

- 483 on craniofacial finite element models: The alveoli (tooth sockets) and periodontal ligaments. *Journal*
484 *of Biomechanics*, 44:1831–1838.
- 485 Wroe, S., Clausen, P., McHenry, C., Moreno, K., and Cunningham, E. (2007a). Computer simulation
486 of feeding behaviour in the thylacine and dingo as a novel test for convergence and niche overlap.
487 *Proceedings of the Royal Society B*, 274:2819–2828.
- 488 Wroe, S., Moreno, K., Clausen, P., McHenry, C., and Curnoe, D. (2007b). High-resolution three-
489 dimensional computer simulation of hominid cranial mechanics. *Anatomical Record*, 290:1248–1255.
- 490 Zhang, H., Nichols, T. E., and Johnson, T. D. (2009). Cluster mass inference via random field theory.
491 *NeuroImage*, 44(1):51–61.