

This is a repository copy of Inertia Properties of a Prosthetic Knee Mechanism.

White Rose Research Online URL for this paper: http://eprints.whiterose.ac.uk/102321/

Version: Accepted Version

Proceedings Paper:

Awad, MI, Dehghani-Sanij, AA, Moser, D et al. (1 more author) (2015) Inertia Properties of a Prosthetic Knee Mechanism. In: Dixon, C and Tuyls, K, (eds.) Towards Autonomous Robotic Systems: Proceedings. 16th Annual Conference, TAROS 2015, 08-10 Sep 2015, Liverpool, UK. Lecture Notes in Computer Science (9287). Springer, Cham, Switzerland, pp. 38-43. ISBN 978-3-319-22415-2

https://doi.org/10.1007/978-3-319-22416-9_5

© 2015 Springer International Publishing. This is an author produced version of a paper published in Lecture Notes in Computer Science. The final publication is available at Springer via https://doi.org/10.1007/978-3-319-22416-9_5. Uploaded in accordance with the publisher's self-archiving policy.

Reuse

Unless indicated otherwise, fulltext items are protected by copyright with all rights reserved. The copyright exception in section 29 of the Copyright, Designs and Patents Act 1988 allows the making of a single copy solely for the purpose of non-commercial research or private study within the limits of fair dealing. The publisher or other rights-holder may allow further reproduction and re-use of this version - refer to the White Rose Research Online record for this item. Where records identify the publisher as the copyright holder, users can verify any specific terms of use on the publisher's website.

Takedown

If you consider content in White Rose Research Online to be in breach of UK law, please notify us by emailing eprints@whiterose.ac.uk including the URL of the record and the reason for the withdrawal request.



eprints@whiterose.ac.uk https://eprints.whiterose.ac.uk/

Inertia Properties of a Prosthetic Knee Mechanism

Mohammed I. Awad and Abbas A. Dehghani-Sanij

Institute of Design, Robotics and Optimization (iDRO), University of Leeds, LS2 9JT, U.K m.i.awad@leeds.ac.uk; a.a.dehghani-sanij@leeds.ac.uk

David Moser and Saeed Zahedi

Chas A Blatchford & Sons Ltd, Lister Road, Basingstoke, Hants, RG22 4AH, UK David.Moser@blatchford.co.uk; Saeed.Zahedi@blatchford.co.uk

Abstract. The prosthetic knee mechanism should be able to assist the amputees during activities of daily living and improve their quality of life. The inertia asymmetry between intact and the prosthetic sides is one of the reasons for amputee gait asymmetry. This paper shows how to calculate the overall inertia properties during the design process.

1 Introduction

Every year, thousands of lower limb amputations are carried out around the world due to complications of diabetes, circulatory and vascular disease, trauma, or cancer in limb segments [1]. The loss in mobility following amputation results in a degradation of the quality of life of the amputees as it affects many aspects of their personal and professional lives. Lower limb prostheses are used to replace the lost limbs and assist amputees in restoring their missing mobility functions. The current commercial stateof-the-art prostheses can be divided into three main categories: purely mechanical, microprocessor damping control and powered prostheses.

Purely mechanical prostheses depend only on mechanical components and require significant mental and voluntary control effort during walking. Microprocessor-damping-controlled prostheses are developed with the objective of approximating the human gait functions. These prostheses are equipped with integrated sensors to supply information to a microprocessor which is used to control the prosthesis in real-time. The main task of this type of prosthetic is to support the body weight in the stance phase and provide dynamic control during the swing phase. This group of prostheses was introduced during the 1990s with the release of the Intelligent Knee (Nabtesco), the Intelligent Prosthesis (IP) (Chas. A. Blatchford & Sons), and the C-Leg (Otto Bock). These prostheses are still passive and cannot contribute any net positive power to the gait which limits the amputee ability. Actively powered prostheses, such as the Victhom knee [2-4], commercially known as the Power Knee (Ossur) are fully actuated. This group of prostheses can be powered using either DC motors [5-7], or pneumatic actuators [8] to provide positive power to the prosthetic limb.

adfa, p. 1, 2011. © Springer-Verlag Berlin Heidelberg 2011 Despite the current technological advances in prosthetics, lower limb amputees still suffer from noticeable gait asymmetry [9-11] and high metabolic energy costs [12] in comparison to healthy subjects. This gait asymmetry pattern occurs due to the inertia asymmetry between the intact and the prosthetic leg [13] and other factors. The prosthesis inertia plays an important role in the gait dynamics especially during the swing phase as in passive dynamic walkers. In order to improve the prostheses performance and design efficient lower limb prostheses, the inertia properties of lower limb prosthesis should be altered without increasing the prosthetic weight to allow more energetic amputee locomotion. This paper focuses on developing a prosthetic knee actuation mechanism and studying the inertia parameters in the mechanism.

2 Kinematics Analysis of The Proposed Prosthetic Knee Mechanism

In this section, the analysis of the proposed prosthetic knee based on closed kinematics chain mechanism, shown in **Fig. 1**a, is presented. According to the geometry of the closed loop configuration in **Fig. 1**a, the screw length is calculated by applying Cosine rule in $\triangle ABC$ as shown in the following equation:

$$L_{screw} = \sqrt{L_1^2 + x^2 - 2L_1 x \cos\beta} \tag{1}$$

It is clear that the knee's torque (\mathbf{T}_k) and speed $(\dot{\boldsymbol{\theta}}_k)$ relative to the motor's torque (\mathbf{T}_m) and speed $(\dot{\boldsymbol{\theta}}_m)$ are functions of the mechanism transmission ratio (\mathbf{r}) , the ball screw pitch (\mathbf{p}) and the overall efficiency of the mechanism $(\boldsymbol{\eta}_o)$ as shown in Equations (2) and (3). These relations show that the knee's torque (\mathbf{T}_k) will increase when the transmission arm (\mathbf{r}) increases, and the knee's speed $(\dot{\boldsymbol{\theta}}_k)$ will increase when the transmission arm (\mathbf{r}) decreases.

$$T_k = F_{screw} \cdot r = \frac{2\pi\eta_0 r}{p} \cdot T_m \tag{2}$$

$$\dot{\boldsymbol{\theta}}_{k} = \frac{p}{2\pi r} \cdot \dot{\boldsymbol{\theta}}_{m} \tag{3}$$

The transmission arm (**r**) of the torque arm can be calculated based on the mechanism geometry. By applying the sine rule in ΔABC , the transmission arm (**r**) is calculated as:

$$r = \frac{xL_1}{\sqrt{L_1^2 + x^2 - 2xL_1 \cos\beta}} \sin\beta \tag{4}$$

Where:

r: the transmission ratio (torque arm length) of the mechanism, x: the length between joints A and C in Fig. 1a, L_1 : the length between joints A and B in Fig. 1a, β : the angle of $\angle CAB$ in Fig. 1a.

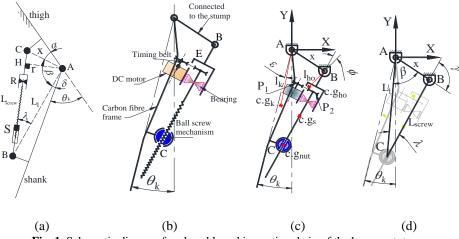


Fig. 1. Schematic diagram for closed loop kinematics chain of the knee prototype.

Based on these selected parameters and the physical constrains of the mechanical components, the prosthetic knee design shown in **Fig. 1**b was proposed to produce the maximum torque and speed profiles. This prosthetic knee mechanism consists of seven main links (**n**) as shown in **Fig. 1**b. These links are, respectively, the fixed link (**AB**) that is attached to the amputee's socket as shown in **Fig. 1**c, the carbon fibre frame for the knee, the ball screw (**CD**), the ball screw nut (**C**), the ball screw housing (**BD**), the motor shaft and the timing belt (**E**). Furthermore, there are three types of joints used in the mechanism for kinematics and physical constraints: five lower pairs revolute joints (**A**, **B**, **C**, **D**, **E**), one screw joint, and two wrapping pair joints (higher pairs) between the belt and the pulleys. These joints create constraints that restrict the mechanism mobility to one degree of freedom (DoF).

3 Sources of Inertia and Impedance Torques in The Mechanism

The mechanism components have passive elements to mechanically dissipate the energy such as friction and damping while the inertias and the potential energy of the knee weight are used as energy storage elements. Equation (5) specifies the equivalent dynamics characteristics of the prosthetic knee prototype relative to joint A, which are shown in **Fig. 1**a and b.

$$J_{eq \to A} \ddot{\theta}_k + D_{eq \to A} \dot{\theta}_k + T_{f_{eq \to A}} = T_k + T_w + T_R \tag{5}$$

Where:

 $T_w = m_{k_{eff}}gl_k \sin(\theta_k - \varepsilon), J_{eq \to A}$: equivalent reflected inertia referred to knee revolute joint A, $\ddot{\theta}_k$: angular acceleration of the knee at joint A (rad/sec²), $D_{eq \to A}$: equivalent reflected damping coefficient referred to revolute joint A (Nm/(rad/sec)), $\dot{\theta}_k$: angular velocity of the knee at joint A (rad/sec), $T_{f_{eq \to A}}$: equivalent reflected friction torque referred to joint A (Nm), T_k : active knee torque generated by the motor at joint A (Nm), T_w : equivalent torque produce by the prosthetic weight (Nm), T_R : external resistance torque applied on the prosthetic knee (Nm), $m_{k_{eff}}$: effective prosthetic weight (kg), l_k : the distance between the joint A and the prosthetic centre of gravity (m), θ_k : prosthetic knee angle (rad), ε : static equilibrium angle of the prosthesis.

3.1 Inertia properties of the developed prosthetic knee

The equivalent reflected inertia is the sum of all inertias in the knee mechanism reflected to joint A as follows:

$$J_{eq \to A} = J_{m \to A} + J_{p_1 \to A} + J_{p_2 \to A} + J_{s \to A} + J_{nut \to A} + J_k + J_{ho \to A}$$
(6)

Where:

 $J_{m \to A}$: motor inertia reflected to the revolute joint A (kg.m²), $J_{p_1 \to A}$: inertia of pulley 1 in timing belt arrangement reflected to the revolute joint A (kg.m²), $J_{p_2 \to A}$: inertia of pulley 1 in timing belt arrangement reflected to the revolute joint A (kg.m²), $J_{s \to A}$: ball screw inertia reflected to the revolute joint A (kg.m²), $J_{nut \to A}$: the inertia of the ball screw nut reflected to the revolute joint A (kg.m²), J_{k} : carbon fibre frame reflected to the revolute joint A (kg.m²), $J_{ho \to A}$: ball screw and bearing holder reflected to the revolute joint A (kg.m²).

The effective reflected inertia is determined using the kinetic energy, as the kinetic energy referred to any point must provide the same kinetic energy plus the losses. Hence, equation (7) is used to derive the reflected inertia based on the constant kinetic energy concept.

$$K. E_{m \to A} = \frac{K.E_m}{\eta_{m \to A}} \qquad \rightarrow \qquad \frac{1}{2} J_{m_r \to A} \dot{\theta}_k^2 = \frac{1}{2} J_{m_r} \dot{\theta}_m^2 \left(\frac{1}{\eta_{m \to A}}\right) \tag{7}$$

Where:

 $K.E_{m\to A}$: kinetic energy of the motor's rotor shaft referred to joint **A**, $K.E_m$: kinetic energy of the motor's rotor shaft, $J_{m_r\to A}$: the mass moment of inertia of the motor shaft around the motor shaft referred to **A**, J_{m_r} : the mass moment of inertia of the motor shaft around the rotation axis of the motor shaft, $\eta_{m\to A}$: transmission efficiency from the motor to joint **A**. The conversion ratio of the angular velocity from the knee $(\dot{\theta}_k)$ to the motor $(\dot{\theta}_m)$ is calculated based on equation (3) as the timing belt arrangement between the motor and the ball screw has 1:1 reduction ratio. Hence, the reflected inertia of the motor shaft referred to joint **A** is calculated as follows:

$$J_{m_r \to A} = \frac{J_{m_r}}{\eta_{m \to A}} \left(\frac{2\pi}{p}\right)^2 r^2 \tag{8}$$

The motor shaft not only rotates around the motor shaft axis, but also the motor with the ball screw holder arrangement rotates around joint **B**. Hence, the motor, pulley 1 (P₁), pulley 2 (P₂) and the ball screw have two inertial values which should be reflected to joint **A** as shown in the following equation:

$$J_{m \to A} + J_{p_1 \to A} + J_{p_2 \to A} + J_{s \to A} + J_{ho \to A} = \left[\frac{J_{m_r}}{\eta_{m \to A}} + \frac{J_{p_1 r}}{\eta_{p_1 \to A}} + \frac{J_{p_2 r}}{\eta_{p_2 \to A}} + \frac{J_{s_r}}{\eta_{s \to A}}\right] \left(\frac{2\pi r}{p}\right)^2 + \left[J_{m_B} + J_{p_1 B} + J_{p_2 B} + J_{s_B} + J_{ho_B}\right] \left(\frac{1}{\eta_{B \to A}}\right) \left(\frac{\dot{\gamma}}{\dot{\theta}_k}\right)^2$$
(9)

Where:

 J_{p1_r} : the mass moment of inertia of the pulley 1 around the rotation axis, $\eta_{p1\to A}$: transmission efficiency from the pulley 1 to joint A, J_{p2_r} : the mass moment of inertia of the pulley 2 around the rotation axis, $\eta_{p2\to A}$: transmission efficiency from the pulley 2 to joint A, J_{s_r} : the mass moment of inertia of the ball screw around the rotation axis, $\eta_{s\to A}$: transmission efficiency from the ball screw to joint A, J_{m_B} : the mass moment of inertia of the pulley 1 around the joint B, J_{p1_B} : the mass moment of inertia of the pulley 1 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the pulley 2 around the joint B, J_{p2_B} : the mass moment of inertia of the ball screw around the joint B, $\eta_{B\to A}$: transmission efficiency from joint B to joint A, $\dot{\gamma}$: angular velocity of joint B (rad/sec).

Similarly, the reflected mass moment of the ball screw nut is calculated as follows:

$$J_{nut\to A} = \frac{m_{nut}}{\eta_{nut\to A}} r^2 + \frac{J_{nut}}{\eta_{C\to A}} \left(\frac{\dot{\lambda}}{\dot{\theta}_k}\right)^2 \tag{10}$$

Where:

 m_{nut} : the ball screw nut mass in kg, $\eta_{nut \to A}$: transmission efficiency from the pulley the ball screw nut to joint A, J_{nut} : the mass moment of inertia of the ball screw nut around the joint C, $\eta_{C \to A}$: transmission efficiency from the joint C to joint A, $\dot{\lambda}$: angular velocity of joint C.

Further work is required to optimize the distribution of the masses and inertia parameters to provide the prosthetic knee $(J_{eq \rightarrow A})$ with inertia properties similar to the natural limb without increase its weight. Also, these inertia parameters are important during the selection process of the actuator.

4 Conclusions

This paper study the kinematics and the inertia properties of the developed knee mechanism. These parameters are important to optimise and improve the performance of the knee mechanism and then reduce the amputee gait asymmetry. The significant sources of inertia in the proposed knee mechanism are highlighted and studied in this paper.

Acknowledgement

This work is linked to a current research sponsored by EPSRC (EP/K020462/1).

References

- 1. Cristian, A.: Lower Limb Amputation: A Guide to Living a Quality Life. Demos Health (2005)
- 2. Bedard, S.: Control system and method for controlling an actuated prosthesis. United States (2004)
- 3. Bedard, S.: Control device and system for controlling an actuated prosthesis. United States (2006)
- 4. Bédard, S., Roy, P.-o.: Actuated leg prosthesis for above-knee amputees. Victhom Human Bionics Inc. (Saint-Augustin-de-Desmaures, (Quebec), CA), United States (2008)
- Goldfarb, M.: Consideration of Powered Prosthetic Components as They Relate to Microprocessor Knee Systems. JPO: Journal of Prosthetics and Orthotics 25, P65-P75 10.1097/JPO.1090b1013e3182a8953e (2013)
- 6. Goldfarb, M., Lawson, B.E., Shultz, A.H.: Realizing the Promise of Robotic Leg Prostheses. Science Translational Medicine 5, 210ps215 (2013)
- Shultz, A., Lawson, B., Goldfarb, M.: Running with a Powered Knee and Ankle Prosthesis. IEEE Transactions on Neural Systems and Rehabilitation Engineering PP, 1-1 (2014)
- Sup, F.C., Goldfarb, M.: Design of a Pneumatically Actuated Transfermoral Prosthesis. ASME Conference Proceedings 2006, 1419-1428 (2006)
- Jaegers, S., Arendzen, J.H., Dejongh, H.J.: PROSTHETIC GAIT OF UNILATERAL TRANSFEMORAL AMPUTEES - A KINEMATIC STUDY. Archives of Physical Medicine and Rehabilitation 76, 736-743 (1995)
- Seroussi, R.E., Gitter, A., Czerniecki, J.M., Weaver, K.: Mechanical work adaptations of above-knee amputee ambulation. Archives of Physical Medicine and Rehabilitation 77, 1209-1214 (1996)
- 11. Vrieling, A.H., van Keeken, H.G., Schoppen, T., Otten, E., Halbertsma, J.P.K., Hof, L., Postema, K.: Gait initiation in lower limb amputees. Gait & Posture 27, 423-430 (2008)
- Sagawa Jr, Y., Turcot, K., Armand, S., Thevenon, A., Vuillerme, N., Watelain, E.: Biomechanics and physiological parameters during gait in lower-limb amputees: A systematic review. Gait & Posture 33, 511-526 (2011)
- Smith, J.D., Martin, P.E.: Short and longer term changes in amputee walking patterns due to increased prosthesis inertia. JPO: Journal of Prosthetics and Orthotics 23, 114-123 (2011)