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Dose-response and normal tissue complication probabilities after proton therapy for choroidal melanomas

Dose response after proton therapy for choroidal melanoma

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No conflicting relationship exists for any author.

This article contains additional online-only material. The following should appear online-only:

Supplementary material (Appendix A-C).

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1 **Abstract**

2 ***Purpose***

3 Normal tissue complication probability (NTCP) models could aid the understanding of dose-
4 dependence of radiation-induced toxicities after eye-preserving radiotherapy of choroidal
5 melanomas. We performed NTCP-modelling and established dose-response relationships for visual
6 acuity deterioration and common late complications after treatments with proton therapy (PT).

7
8 ***Design***

9 Retrospective study from single large referral centre.

10

11 ***Subjects***

12 We considered patients diagnosed with choroidal melanoma and primarily treated with hypo-
13 fractionated PT (52 Gy physical dose in 4 fractions). 1020 patients had complete visual acuity
14 deterioration information, 991 patients had complete information on late complications.

15

16 ***Methods***

17 Treatment details and dose-volume histograms (DVHs) for relevant anatomical structures and
18 patient and tumour characteristics were available from a dedicated ocular database. Lasso variable
19 selection was used to identify variables with the strongest impact on each endpoint, followed by
20 multivariable Cox regressions and logistic regressions to analyse the relationship between dose,
21 clinical characteristics and clinical outcomes. Dose-response relationships were estimated, adjusting
22 for relevant clinical variables.

23

24 ***Main Outcome Measures***

25 Dose-response relationship for visual acuity deterioration and late complications

26

27 **Results**

28 Dose metrics for several structures (i.e. optic disc, macula, retina, globe, lens, ciliary body)
29 correlated with clinical outcome. The near-maximum dose to the macula (macula $D_{2\%}$) showed the
30 strongest correlation with visual acuity deterioration. Retina $D_{20\%}$ was the only variable with clear
31 impact on the risk of developing maculopathy; optic disc $D_{20\%}$ had the largest impact on optic
32 neuropathy; cornea $D_{20\%}$ had the largest impact on neovascular glaucoma; ciliary body $D_{20\%}$ had the
33 largest impact on ocular hypertension; the volume of the ciliary body receiving 26 Gy (ciliary body
34 V_{26Gy}) was the only variable associated with the risk of cataract; and retina V_{52Gy} was associated
35 with the risk of retinal detachment. Optic disc-tumour distance was the only variable associated
36 with dry eye syndrome in the absence of DVH for the lachrymal gland.

37

38 **Conclusions**

39 Visual acuity deterioration and specific late complications demonstrated dependence on dose
40 delivered to normal structures in the eye after PT for choroidal melanoma. Visual acuity
41 deterioration depended on dose to a range of structures, while more specific complications were
42 primarily related to dose metrics for specific structures.

43 **Introduction**

44 Eye-preserving proton therapy is commonly used to treat choroidal melanomas [1]. The ultimate
45 objective of the treatment is to destroy the malignancy without producing complications on adjacent
46 healthy tissues, thereby preserving long term function. Nonetheless, some structures may be
47 exposed to large doses during treatment, and radiation-induced visual deterioration and toxicities
48 are common side-effects [2]. Normal tissue complication probability (NTCP) models for most
49 complications have not yet been established for hypo-fractionated proton therapy and the relevance
50 of damage to the various ocular structures has not been fully examined. To rectify this, we
51 examined data from a large cohort of patients treated at a dedicated proton therapy facility, with
52 long follow-up. We conducted dose-response modelling to examine the relationships between dose
53 delivered to healthy tissue and the occurrence of visual acuity deterioration and various radiation-
54 induced toxicities.

55

56 **Materials and methods**

57 *Patients*

58 This retrospective study included patients treated for choroidal melanomas between 1991 and 2015
59 at a dedicated proton centre. Patients and tumour characteristics as well as treatment details were
60 prospectively registered in an ocular database.

61 Post-treatment visits, with tumour assessment by an onco-ophthalmologist and liver ultrasound,
62 were performed every sixth months the first two years and annually subsequently. Patients were
63 followed until at least 5 years after treatment if possible. At each visit, the Snellen' scale was used
64 to evaluate the best corrected visual acuity, and fundus photography and/or fluorescein angiography
65 were used to examine the fundus. Furthermore, tumour thickness and diameter were measured at
66 each visit using ultrasound. Complications were recorded prospectively at each clinical visit.

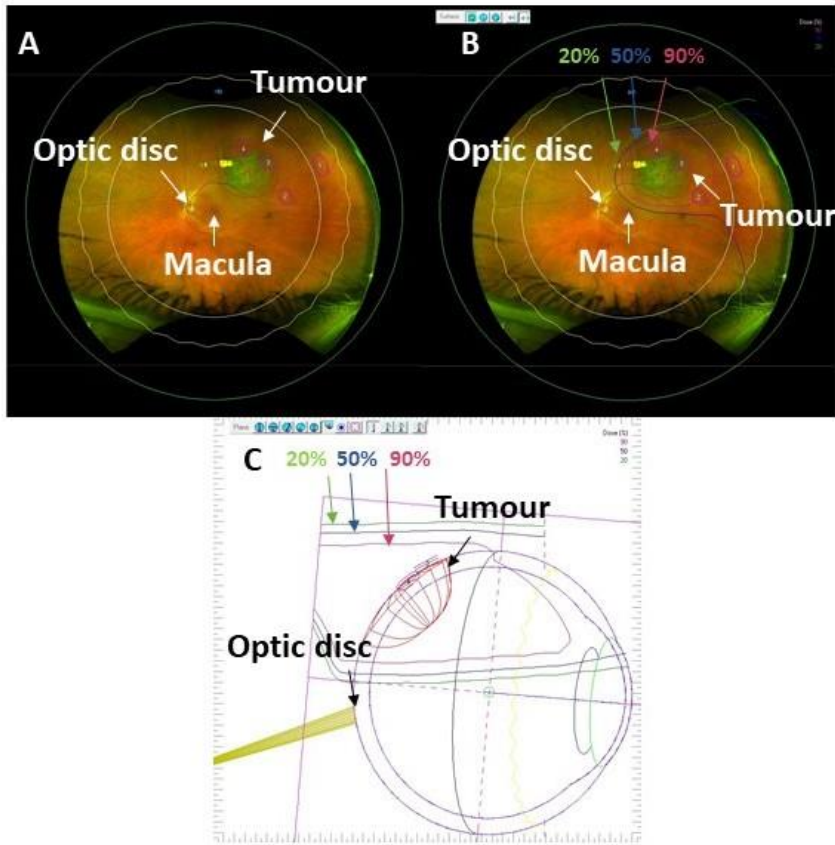
67 Information on recurrence, secondary enucleation, and side-effects were collected [3]. For the
68 purpose of this study, patient and tumour characteristics as well as treatment and outcome data were
69 retrospectively extracted from the database; with patients with missing information on general
70 characteristics and/or outcomes excluded. The study was retrospective and received a waiver of
71 informed consent approved by the Ethics Committee of the French Society of Ophthalmology (IRB
72 00008855 Société Française d’Ophthalmologie IRB#1) and the research adhered to the tenets of the
73 Declaration of Helsinki.

74

75 ***Treatment and planning***

76 Protons with energy of 65 MeV were produced by a fixed-frequency cyclotron. The construction
77 and the physics of the aperture and beam have previously been described [4–6]. EyePlan (version
78 3.06) was used as treatment planning system (TPS). Experienced dosimetrists created each plan in
79 close cooperation with radiation oncologists, choosing the modulator, the collimator shape and
80 angles for eye orientation. Each tumour received a physical tumour dose of 52 Gy in 4 fractions of
81 13 Gy, delivered on 4 consecutive days [3]. This planning and treatment have previously been
82 described in detail [7]. Figure 1 illustrates the main steps of the treatment planning. Dose-volume
83 histograms for each of the relevant anatomical structures were extracted from the TPS. Physical
84 doses were used for all analyses and no correction from fraction size effects was thus employed.
85 Dose volume histograms (DVHs) or dose surface histograms (DSHs) were extracted for each
86 normal tissue structure. A range of dose metrics were calculated to represent the entire DVH/DSH
87 while still limiting the number of variables in the analysis and avoiding excessive collinearity
88 between variables. These included the volume or the surface treated to a specific (discretised) dose
89 level x (V_x/S_x), or the dose delivered to a specific volume or surface y (D_y) (V/S_{52Gy} , V/S_{42Gy} ,
90 V/S_{26Gy} , V/S_{10Gy} , V/S_{5Gy} , $D_{98\%}$, $D_{50\%}$, $D_{20\%}$ and $D_{2\%}$). We prioritised metrics representing the

91 'extremes' of the dose distribution as well 'mid-range' of the DVHs. Details on the treatments and
92 planning are described further in Appendix A.



93
94 **Figure 1:** The steps in 3D image-guided treatment planning using EyePlan. A) Tumour contouring
95 in the exact location on pre-treatment fundus photography. B) Three levels of isodoses. Dose levels
96 90% (purple), 50% (dark blue), and 20% (green) are used for illustrative purposes. C) 3D
97 illustration of the treatment plan, the tumour, optic disc, and the isodose levels.

98
99

100 ***Definition of toxicity and complications***

101 ***Visual acuity deterioration***

102 Visual acuity was measured using the Snellen scale. For analysis purposes it was converted into the
103 logarithm of Minimum Angle of Resolution (logMAR) scale [8,9]; this has been used throughout
104 the analyses. Longitudinal measures were not available for visual acuity, and the analysis was thus
105 entirely based on the measure from last follow-up. We defined visual acuity deterioration of ≥ 0.3
106 logMAR compared to the baseline measure.

107

108 ***Posterior complications***

109 **Maculopathy:** Radiation-induced maculopathy was diagnosed based on visual acuity deterioration
110 and the presence of micro-aneurysms, ischemia and/or oedema in the entire macular region,
111 assessed by ophthalmoscopy or preferably visualized from fundus photography and optical
112 coherence tomography (OCT).

113

114 **Optic neuropathy:** Ophthalmoscopy was used to diagnose the condition. An oedematous and/or
115 atrophic optic disc in combination with a considerable decrease in visual acuity were the most
116 common observations in the diagnosis of radiation-induced optic neuropathy (RION). Additionally,
117 an undelimited and pale disc was used in the diagnosis.

118

119 **Ocular hypertension:** Ocular hypertension was defined as intraocular pressure (IOP) higher than 21
120 mmHg at multiple measurements without signs of visual field defects or cupping of the disc.

121

122 Neovascular glaucoma: In cases of elevated IOP and neovascularization, examined either in the
123 angle using gonioscopy or in retina using ophthalmoscopy, combined with visual field loss or optic
124 nerve head cupping, the diagnose neovascular glaucoma was given.

125
126 Retinal detachment: Presence of retinal detachment was determined by ophthalmoscopy and
127 reported without time-to-event.

128
129 Vasculopathy: Radiation-induced vasculopathy was found as micro-occlusions and intraretinal
130 microvascular abnormalities adjacent to ischemic areas as seen from ophthalmoscopy.

131
132 *Anterior complications*

133 Cataract: Lens opacity resulting in gradual deterioration of the visual acuity. It was diagnosed by
134 slit lamp examination or ophthalmoscopy.

135
136 Dry eye: Reduced production of lacrimal fluid occurring after irradiation of the lacrimal gland and
137 resulting in itching, redness and general discomfort in the eye. These symptoms formed the basis
138 for the diagnosis while measurements from Schirmer's test were used to confirm diagnosis.

139
140 *Data analysis*

141 For each endpoint, we pre-specified relevant normal tissues (and their corresponding dose metrics)
142 and clinical factors for analysis; resulting in more than 50 potential variables per endpoint. Pre-
143 specification was performed by a consultant ophthalmologist and a radiation oncologist, both with
144 several years of experience in ocular oncology. See details in the analysis plan in Appendix B.

145

146 Due to the large number of potential variables, Lasso (least absolute shrinkage and selection
147 operator) regression analysis was used to perform variable selection among the numerous and
148 correlated variables [10,11]. The variables with the strongest correlation with each outcome were
149 estimated from the regularized method by shrinkage and elimination of variable coefficients. The
150 optimal shrinkage parameter (λ) was determined from 100-fold cross-validation. We used the first
151 standard error of λ to obtain the smallest number of predictors, and thus the simplest model with an
152 acceptable error [12]. We carried out the multivariable regression analyses with the variables
153 selected from the Lasso.

154

155 For visual acuity deterioration, we carried out two analyses; one where we included the entire cohort
156 irrespective of pre-treatment visual acuity (group 1, analysis 1); and one in which we examined the
157 visual acuity deterioration for patients with a pre-treatment visual acuity ≤ 0.5 logMAR (but
158 keeping all other analysis details unchanged) (group 1, analysis 2). The risk of visual acuity
159 deterioration was analysed using logistic regression (but including follow-up time as separate
160 variable).

161

162 Specific late complications were analysed using Cox's proportional hazards regression [13]. Time
163 was measured from start of radiotherapy to whichever happened first: event, death or loss of follow-
164 up (with patients censored for the two latter). For retinal detachment, time-to-event was missing in
165 the follow-up data, and logistic regression rather than Cox regression was performed (see previous
166 paragraph). Preventive treatments were not made for any of the ocular complications. Treatment
167 was initiated after the complications occurred. As such, the time-to-event was not affected.

168

169 Model performance was assessed by Hosmer-Lemeshow for goodness-of-fit of the logistic
170 regression analyses, while concordance index and Brier score were used to evaluate the Cox
171 regression models. Schoenfeld residuals demonstrated no time dependence for any of the variables
172 included, and the proportional hazard assumption was thus assumed not to be violated.

173

174 Dose-response for each complication was visualized by plotting the predicted risk of
175 complication/toxicity (at a fixed time point (5 years) for Cox regression) as a function of dose, with
176 all other model variables kept constant. Additionally, the impact of clinical factors, such as tumour
177 height or optic disc-tumour distance, on the risk of toxicity was demonstrated by varying these
178 using relevant clinical values.

179

180 The median potential follow-up time was assessed using the inverse Kaplan-Meier estimate [14].

181 All analyses were performed in RStudio (Version 0.99.467). The full, annotated model fits are
182 available as R files at Electronic Research Data Archive (ERDA) [15].

183

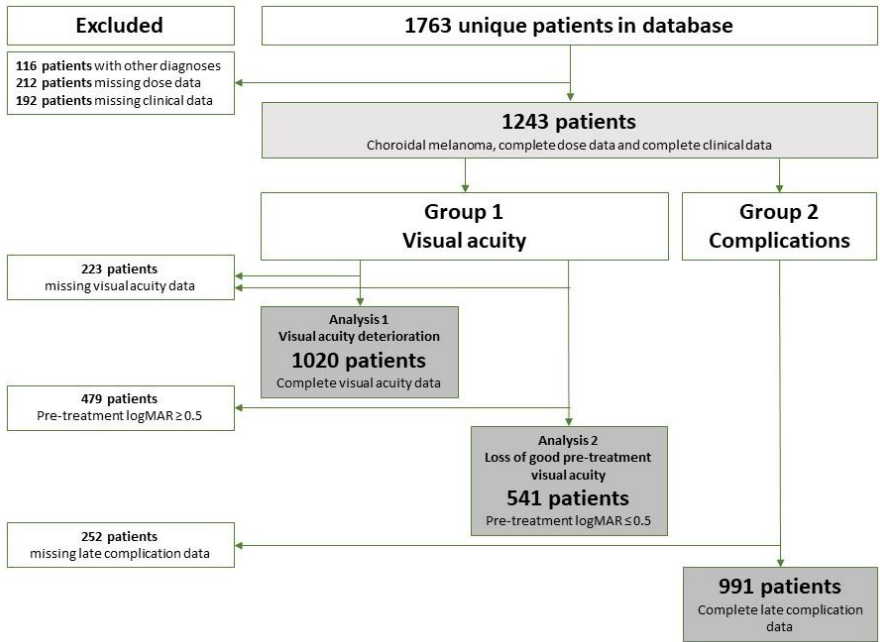
184 **Results**

185 *Patients and descriptive statistics*

186 1020 patients had complete information on clinical characteristics, dose data and visual acuity
187 measures (group 1, analysis 1). 541 patients had pre-treatment visual acuity of ≤ 0.5 logMAR
188 (group 1, analysis 2). 991 patients had complete information on clinical characteristics, dose data
189 and late complications (group 2). Patients could be represented in both groups if they had complete
190 information on all the above variables. See the flowchart in Figure 2 for details on patient data used.

191 The overall median potential follow-up time was 6.1 years (95 % CI 6.0-6.2).

192



193

194 **Figure 2:** Flowchart describing the used patient data. 1020 patients had complete information on
 195 clinical characteristics, dose data and visual acuity measures (group 1, analysis 1). 541 patients had
 196 pre-treatment visual acuity of ≤ 0.5 logMAR (group 1, analysis 2). 991 patients had complete
 197 information on clinical characteristics, dose data and late complications (group 2). Patients could be
 198 represented in both groups if they had complete information on all the above variables.

199

200 Patient, tumour and treatment characteristics for both groups are listed in Table 1.

201

202

203

204

	Group 1 Patients with visual acuity data N=1020	Group 2 Patients with complication data N=991	
Patient and tumour characteristics	Value (median (IQR))	Value (median (IQR))	
Age (years)	66 (56-75)	65 (55-75)	
Gender male/female	476/544	452/539	
Baseline VA (logMAR)	0.4 (0.2-1.0)	-	
Baseline VA logMAR ≤ 0.5 y/n	541/479	-	
Last VA (logMAR)	1.6 (0.4-2.0)	-	
Last VA logMAR ≤ 0.5 y/n	300/720	-	
Follow-up (years)	5.1 (2.8-8.1)	5.1 (2.9-8.0)	
Largest basal dimension (mm)	11.0 (9.0-13.3)	11.0 (9.0-13.3)	
Height (mm)	4.9 (3.2-7.3)	4.9 (3.2-7.3)	
Optic disc-tumour distance (mm)	4.0 (1.2-7.1)	3.7 (1.1-6.8)	
Macula-tumour distance (mm)	3.0 (0.6-6.8)	3.0 (0.3-6.3)	
Complication		Number (%)	5-year probability of freedom from toxicity (95 % CI)
Maculopathy		205 (21 %)	79 % (76-82)
Optic neuropathy		135 (14 %)	85 % (82-97)
Neovascular glaucoma		118 (12 %)	87 % (85-89)
Retinal detachment		357 (36 %)	-

Ocular hypertension		66 (7 %)	92 % (90-94)
Vasculopathy		213 (21 %)	76 % (73-79)
Cataract		310 (31 %)	68 % (65-71)
Dry eye		148 (15 %)	84 % (82-87)

205 **Table 1:** Descriptive statistics and list of incidences for each complication with 5-year risk of
 206 freedom from the complication (based on Kaplan-Meier estimates). The date for retinal detachment
 207 was not available, and the actuarial risk was thus not calculated. VA=visual acuity,
 208 IQR=interquartile range, logMAR= logarithm of Minimum Angle of Resolution.

210 **Group 1: Visual acuity**

211 *Analysis 1 - Visual acuity deterioration*

212 For patients irrespective of initial pre-treatment visual acuity, the risk of visual acuity deterioration
 213 correlated with near-maximum macula dose (macula D_{2%}). As did to a smaller extent various other
 214 dose metrics (optic disc D_{2%}, retina D_{20%}, globe V_{10Gy} and globe V_{5Gy}) as well as tumour height,
 215 optic disc-tumour distance and follow-up time. Odds ratios are listed in Table 2. Figure 3A
 216 illustrates the dose-response relationship for macula D_{2%} for all cases, while Figure 3B illustrates
 217 the relationship for three specific tumour heights (3.0, 6.0 and 9.0 mm), respectively.

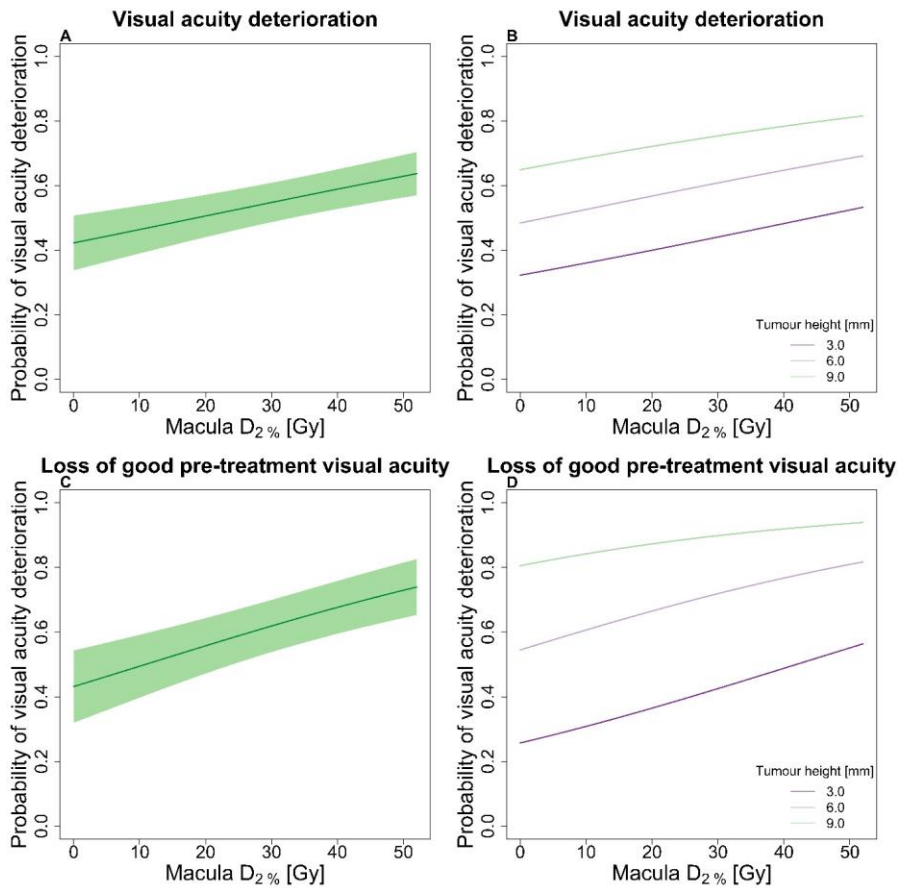
218 *Analysis 2 – Loss of good pre-treatment visual acuity*

219 For patients with good initial pre-treatment visual acuity, the risk of visual acuity loss correlated
 220 with macula D_{2%} and pre-treatment visual acuity. Additionally, the volume of the optic disc
 221 receiving 50% of the prescribed dose (optic disc V_{26Gy}) demonstrated weaker correlation. Besides
 222 dose, tumour height and optic disc-tumour distance were the only clinical variables correlated with
 223 the risk of loss of pre-treatment visual acuity. Odd ratios are listed in Table 2. Figure 3C and Figure
 224 3D illustrate the dose-response relationship for macula D_{2%} and for three specific tumour heights.

225 Note the stronger dose-dependence for macula D_{2%} compared to analysis 1 on all patients
 226 irrespective of initial pre-treatment visual acuity.
 227
 228 Model performance using Hosmer-Lemeshow showed a strong correlation between observed and
 229 predicted risk of visual acuity deterioration for both logistic regression models. The model
 230 goodness-of-fits are illustrated in Appendix C for both visual acuity analyses.
 231

	Analysis 1: Visual acuity deterioration	Analysis 2: Loss of good pre-treatment visual acuity
Variables in logistic model	Odds ratio (95 % CI)	Odds ratio (95 % CI)
Tumour height	1.25 (1.14-1.38)	1.51 (1.29-1.79)
Optic disc-tumour distance	0.98 (0.93-1.03)	0.96 (0.90-1.02)
Optic disc D _{20%} ⁺	-	1.01 (0.58-1.81)
Optic disc D _{2%} ⁺	1.11 (1.01-1.22)	-
Optic disc V _{26Gy} *	-	1.10 (0.90-1.33)
Optic disc V _{5Gy} *	-	1.00 (0.78-1.27)
Macula D _{2%} ⁺	1.18 (1.09-1.28)	1.28 (1.15-1.44)
Retina D _{20%}	1.12 (0.98-1.29)	-
Globe V _{10Gy}	1.11 (0.76-1.61)	1.01 (0.98-1.04)
Globe V _{5Gy}	0.91 (0.63-1.31)	-
Follow-up (1 y increase)	1.08 (1.04-1.13)	-

232 **Table 2:** Odds ratios with 95 % confidence intervals (CI) from multivariable logistic regression
 233 analyses. ⁺=10 Gy increase, * = 10 %-point increase.



234

235 **Figure 3:** A) Dose response of visual acuity deterioration at 5 years as a function of near-maximum
 236 macula dose (macula $D_{2\%}$). The shaded area represents the 95% confidence interval. The model is
 237 adjusted for tumour height (4.9 mm), optic disc-tumour distance (4.0 mm), optic disc $D_{2\%}$ (4.0 Gy),
 238 retina $D_{20\%}$ (51.7 Gy), globe V_{10Gy} (36% of total eye volume), globe V_{5Gy} (38% of total eye volume)
 239 and follow-up (5.1 years). The values were set as the median value for the entire visual acuity
 240 group. B) Dose response of visual acuity deterioration at 5 years as a function of macula $D_{2\%}$ for
 241 three tumour heights (3.0, 6.0 and 9.0 mm). C) Dose response of pre-treatment visual acuity loss at
 242 5 years after a baseline visual acuity of ≤ 0.5 logMAR as a function of macula $D_{2\%}$. The model is

243 adjusted for tumour height, optic disc-tumour distance, optic disc V_{26Gy} (0%), optic disc V_{5Gy} (0%),
 244 optic disc D_{20%} (1.3 Gy) and globe V_{10Gy}. D) Dose response of pre-treatment visual acuity loss at 5
 245 years after a baseline visual acuity of ≤ 0.5 logMAR as a function of macula D_{2%} for the three
 246 tumour heights.

247
 248 **Group 2: Complications**

249 The hazard ratios (HRs) including 95% CI for complication data are listed in Table 3. No predictors
 250 were found for vasculopathy and no analysis was consequently made for this late complication.

251

Complication	Hazard ratio (95 % CI)
Maculopathy	
Retina D _{20%} ⁺	1.21 (1.07-1.36)
Optic neuropathy	
Optic disc-tumour distance	0.83 (0.72-0.95)
Optic disc D _{20%} ⁺	1.15 (0.94-1.41)
Optic disc V _{42Gy} [*]	1.04 (0.96-1.13)
Neovascular glaucoma	
Tumour height	1.31 (1.16-1.47)
Cornea D _{20%} ⁺	1.26 (1.12-1.41)
Globe D _{50%} [#]	1.00 (0.98-1.02)
Globe V _{52Gy}	0.99 (0.96-1.02)
Optic disc V _{52Gy} [*]	1.10 (1.05-1.15)
Ocular hypertension	
Tumour height	1.08 (0.96-1.20)

Ciliary body D _{20%} ⁺	1.46 (1.10-1.95)
Ciliary body V _{26Gy} [*]	1.10 (0.74-1.64)
Cornea D _{20%} ⁺	1.06 (0.86-1.30)
Retina D _{50%}	1.01 (0.99-1.03)
Cataract	
Ciliary body V _{26Gy} [*]	1.31 (1.22-1.40)
Dry eye syndrome	
Optic disc-tumour distance	1.09 (1.05-1.12)
Retinal detachment	
	Odds ratio (95 % CI)
Age at treatment	0.98 (0.97-0.99)
Tumour height	1.15 (1.06-1.25)
Largest base dimension	1.07 (1.00-1.14)
Optic disc-tumour distance	0.88 (0.84-0.91)
Retina V _{52Gy}	1.06 (1.00-1.12)
Retina V _{42Gy}	0.98 (0.93-1.03)

252 **Table 3:** Hazard ratios (HR) and 95 % confidence intervals (CI) for each of the complications in
253 multivariable Cox regression analysis. ⁺=10 Gy increase, ^{*}=10 %-point increase, [#] percent of
254 volume relative to eye volume.

255

256 *Maculopathy*

257 Retina D_{20%} was the only variable chosen from the Lasso procedure to impact the risk of developing
258 maculopathy, although this relationship was relatively weak. The dose-response for this relationship
259 is illustrated in Figure 4A.

260 *Optic neuropathy*

261 The dose delivered to 20% of the optic disc (optic disc $D_{20\%}$) was the variable with the largest HR
262 for optic neuropathy, but this was also a relatively weak correlation. Figure 4B illustrates the dose-
263 response model for this relationship. Tumour-optic disc distance was the only clinical variable
264 associated with the risk of developing optic neuropathy.

265 *Neovascular glaucoma*

266 The dose delivered to 20% of the cornea (cornea $D_{20\%}$) demonstrated the strongest association with
267 neovascular glaucoma; see illustration in Figure 4C.

268 *Ocular hypertension*

269 Several dose metrics were chosen from the Lasso procedure for ocular hypertension and
270 demonstrated association with the risk of developing this late complication, but ciliary body $D_{20\%}$
271 was the variable with the strongest correlation (although this was still relatively weak). Figure 4D
272 illustrates this relationship.

273 *Cataract*

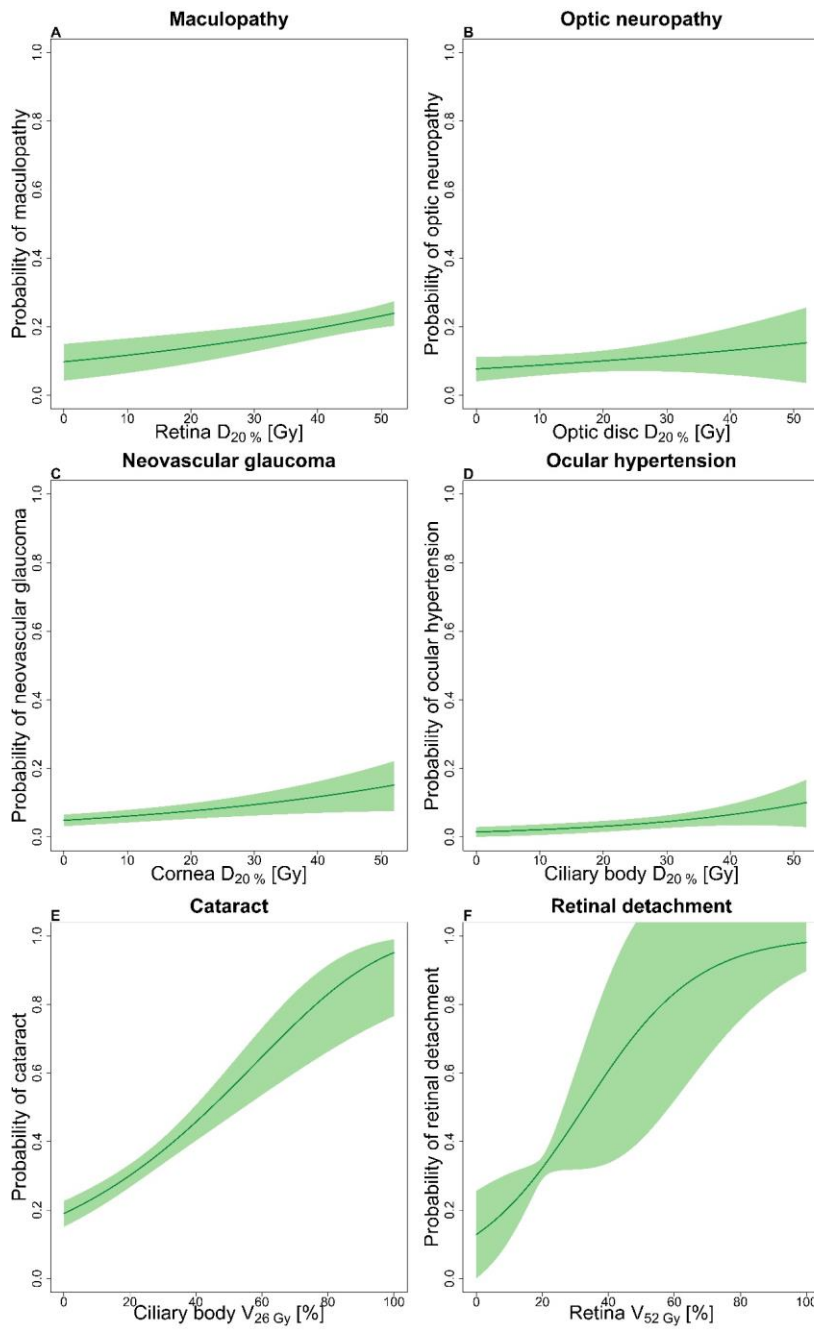
274 The volume of the ciliary body receiving 50% of the prescribed dose (ciliary body V_{26Gy}) was the
275 only variable associated with the risk of cataract and this strong relationship is illustrated in Figure
276 4E.

277 *Retinal detachment*

278 The volume of the retina receiving 100% of the prescribed dose (retina V_{52Gy}) proved to have a
279 considerable impact on the risk of developing retinal detachment after the treatment. Figure 4F
280 illustrates this relationship.

281

282 Model performance using concordance index (c-index) and Brier score showed acceptable 5-year
283 accuracy, with the best calibration being for the ocular hypertension and neovascular glaucoma
284 models. The model goodness-of-fits are illustrated in Appendix C for all late complication analyses.



286 **Figure 4:** A) Dose response of maculopathy at 5 years as a function of retina $D_{20\%}$. The shaded area
287 represents the 95% confidence interval of the risk estimate. B) Dose response of optic neuropathy at
288 5 years as a function of optic disc $D_{20\%}$. The model adjusts for optic disc-tumour distance (3.7 mm)
289 and optic disc V_{42Gy} (0%) and optic disc V_{10Gy} (0%). C) Dose response of neovascular glaucoma at
290 5 years as a function of cornea $D_{20\%}$. The model adjusts for tumour height (4.9 mm), optic disc
291 V_{52Gy} (0%), globe $D_{50\%}$ (0 Gy) and globe V_{52Gy} (29.1%). D) Dose response of ocular hypertension
292 at 5 years as a function of ciliary body $D_{20\%}$. The model adjusts for tumour height, cornea $D_{20\%}$ (0
293 Gy), retina $D_{50\%}$ (0 Gy) and ciliary body V_{26Gy} (20%). E) Dose response of cataract at 5 years as a
294 function of ciliary body V_{26Gy} . F) Dose response of retinal detachment at 5 years as a function of
295 retina V_{52Gy} . The model adjusts for retina V_{42Gy} , age at treatment (65 years), tumour height, largest
296 base dimension (11 mm) and optic disc-tumour.

297

298 **Discussion**

299 In this retrospective study of a large single-institution cohort, we examined relationships between
300 dose delivered to healthy tissue and the occurrence of visual acuity deterioration and late radiation-
301 induced complications after proton therapy for choroidal melanoma. The novelty of this study is the
302 use of advanced statistics to identify risk factors with the strongest impact on each endpoint in
303 multivariable analysis. This was done to robustly explore the full scope of potential dose and
304 volume dependence. Normal tissue dose was important for visual acuity deterioration, and dose to
305 healthy structures was a considerable factor associated with the risk of developing most of the late
306 complications.

307 Broad, composite endpoints showed correlation with a relatively wide range of normal tissue doses,
308 corresponding to a complex underlying pathophysiology. As such, dose metrics for several normal
309 structures appeared to have an impact on visual acuity deterioration. The maximum dose to the

310 macula, $D_{2\%}$, was, however, associated with the largest effect. In the group with good pre-treatment
311 visual acuity, where a change was more likely to be caused by the treatment, rather than other
312 factors, we also found the steepest dose-response relationship (Figure 3C). Interestingly, tumour
313 height was directly associated with risk of visual acuity deterioration and the correlation was
314 stronger than the maximum dose to the macula. This confirms similar findings reported previously,
315 where tumour height was the most important factor for visual loss and risk of enucleation [16–18].

316 Specific complication endpoints were to a larger extent related to dose metrics from specific
317 healthy structures, potentially representing a more direct link between structures, pathophysiology
318 of radiation damage, and the resulting clinical complications.

319 Remarkably, radiation dose had little importance on the risk of optic neuropathy (Table 3) even
320 though the Lasso analysis selected multiple closely correlated optic disc dose metrics. This was
321 reflected in the developed dose-response models for optic neuropathy, which had poor prognostic
322 value as the model contained no obvious threshold. Our data indicated that the most important
323 predictor for the risk of developing optic neuropathy was the proximity of the tumour to the optic
324 disc.

325 For maculopathy, we found no effect of radiation to the macula – in contrast to Gragoudas et al.,
326 where macular exposure to radiation was main risk factor [19]; this study was, however, based on a
327 selected group of patients and the prescribed tumour dose was higher than in our study (70 CGE vs
328 ~57 CGE) [18]. We found that dose delivered to 20% of the retina (retina $D_{20\%}$) was the only
329 variable with impact on the risk of maculopathy. We speculated that retina $D_{20\%}$ potentially
330 represented a surrogate for tumour extension or for macula $D_{2\%}$ and consequently for visual acuity
331 deterioration.

332 Post-treatment retinal detachment was not defined as a risk factor but as an endpoint in our analysis,
333 because retinal detachment involving the macula can cause visual impairment. It was the most
334 frequent side-effect in this cohort. Egger et al. found that only 29.3% of patients experienced no
335 retinal detachment [20]. However, the rate essentially depends on how it is diagnosed. We speculate
336 that some of the retinal detachments included in our data might have been present already before the
337 treatment was initiated even if the retina normalised after the treatment. It could not be determined
338 whether the retinal detachments were caused by tumour decay or direct radiation damage. We did
339 find that tumour height, posterior located tumours, and volume of the retina receiving full
340 prescription dose (retina V_{52Gy}) increased the risk.

341 Dose metrics for several normal tissue structures were identified from the Lasso analysis to increase
342 the risk of ocular hypertension. Dose to 20% of the ciliary body (ciliary body $D_{20\%}$) was found to
343 have the strongest impact; possibly an indirect effect from radiation-induced damage of the
344 trabecular meshwork preventing drainage of produced aqueous [21].

345 In addition to ocular hypertension, neovascular glaucoma involve new vessel formation in the
346 anterior segment, indicating a component of ischemia and release of angiogenic factors. Therefore,
347 neovascular glaucoma is a more complex endpoint that is likely to be caused from multiple various
348 factors, but it remains unknown which specific variables are main risk factors. We found that
349 tumour height was the variable with the strongest impact on the risk of neovascular glaucoma, while
350 the dose delivered to 20% of the cornea surface (cornea $D_{20\%}$) and the volume of the optic disc
351 receiving maximum dose (optic disc S/V_{52Gy}) increased the risk. This is in line with previous
352 findings by Mishra et al. that also reported increased tumour height, dose to anterior critical
353 structures (lens or ciliary body), and dose to the optic disc as main risk factors [22]. Daftari et al.
354 advocated sparing of radiation to the anterior segment to prevent neovascular glaucoma [23].
355 Sparing of dose to the anterior structures during treatment is, however, difficult since tumour

356 coverage and sparing of the macula and the optic disc are prioritized. This could explain why the
357 Lasso analysis selects globe $D_{50\%}$ and globe V_{52Gy} as risk factors (Table 3).

358 Cataract was a common side-effect in our cohort; occurring in one third of patients. The lens has
359 been reported to be the most radiosensitive ocular structure [24]. However, we found the volume of
360 ciliary body that received 50% of the dose (ciliary body V_{26Gy}) as the most important variable for
361 the development of cataract, most likely since development of cataract is a multifactorial event with
362 various risk factors. Additionally, we speculate that the finding of ciliary body dose might reflect an
363 indirect effect of the dose to the lens. To explore this further, we performed an explorative analysis
364 including solely the lens DVH along with clinical factors. We found that the maximum dose to the
365 lens (lens $D_{2\%}$) was important for the risk of cataract when no other dose metrics were included in
366 the selection process (results not shown). This has been reported in previous studies [25,26].
367 Phacoemulsification can, however, be carried out safely even after proton therapy, and visual acuity
368 can be recovered after surgery.

369 For dry eye syndrome, the only variable associated with increased risk was the optic disc-tumour
370 distance; the longer the distance the higher the risk. This lack of dependence could possibly be
371 explained by the lack of lachrymal gland contouring in the treatment planning system;
372 consequently, it was not possible to explore all relevant dose relationships [27].

373 We used advanced statistical methodology for selecting appropriate variables to include in the
374 analyses. In this way, we included the predictors associated with risk of each specific endpoint,
375 while excluding variables with no clear impact. The use of Lasso for variable selection is a well-
376 established and robust method to handle many variables. It is, however, recognised that the method
377 has problems when the included variables are highly correlated. Additionally, the cross-validation
378 performed to select the optimal shrinkage parameter has previously been described to select too

379 many non-informative variables. This may explain the selection of competing dose metrics for some
380 of the toxicities in this study [28].

381 It is important to recognize that this was a retrospective analysis. It is a considerable strength of the
382 study, however, that complications were recorded during follow-up and extracted from the database
383 for the purpose of this study. Unfortunately, the time-to-event information for visual acuity
384 deterioration and retinal detachment were not available. We did, however, include total follow-up
385 time in the model to adjust for any time-effect. Furthermore, the effect of tumour volume was not
386 explored. Since tumours often have complex shapes (e.g. mushroom shape) the volumes are
387 difficult to measure, making tumour height a much more precise measure. Additionally, tumour
388 height has been the standard variable to include in analyses in the literature. As such, the knowledge
389 gained from including tumour height in the model is valuable and can be comparable to the
390 literature.

391 We report relatively low prevalence of some of the radiation-induced toxicities compared to
392 previous works [29], which might be a result of using a personalized treatment plan and a dedicated
393 eyeline for all treatments. However, another reason for the low prevalence could be that mild
394 toxicities were underreported. Toxicity reporting is most likely heterogeneous among centres;
395 indicating lack of standardization in terms of diagnosing radiation-induced ocular toxicities. Finger
396 et al. have established guidelines for the diagnosis of retinopathy but an expansion to the remaining
397 complications are needed [30].

398 Limited data currently exist on the tolerance of various eye structures to radiation dose for external
399 beam photon treatment. It has solely been described by the QUANTEC review for the optic nerve
400 and the chiasm [31]. The maximum dose (D_{\max}) to the optic nerve was related to the risk of late
401 radiation-induced optic neuropathy, with maximum tolerable dose for normo-fractionated (1.8-2

402 Gy/fraction) external beam photon treatment at around 60 Gy. Importantly, these data cannot be
403 compared directly to the hypo-fractionated physical doses used for choroidal melanomas. Similarly,
404 the current results will not be applicable to brachytherapy (Ru-106) [32] due to different dose-
405 fractionation/dose-rate effects and different underlying radiobiology of the radiation modalities.

406 The dose-response models established in this study can ultimately help guide the radiation
407 oncologists' decisions on optimal treatment and gaze direction during the treatment planning. The
408 established models could additionally guide future treatment planning to maintain a low level of
409 radiation-induced toxicities. Individualized toxicity risk estimates may also help treatment modality
410 selection – keeping in mind that besides filter and margins, there are no further optimization options
411 during proton planning in most currently available treatment planning systems. Further dedicated
412 studies are needed for each treatment modality, especially if individualised treatment modality
413 selection and optimisation is to be realised.

414

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