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1 **Bone Density, Microstructure and Strength in Obese and Normal Weight Men and**
2 **Women in Younger and Older Adulthood**

3

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21

22 **Abstract**

23 Obesity is associated with greater areal BMD (aBMD) and considered protective against hip
24 and vertebral fracture. Despite this, there is a higher prevalence of lower leg and proximal
25 humerus fracture in obesity. We aimed to determine if there are site-specific differences in
26 BMD, bone structure or strength between obese and normal weight adults. We studied 100
27 individually-matched pairs of normal (BMI 18.5-24.9 kg/m²) and obese (BMI>30 kg/m²)
28 men and women, aged 25-40 or 55-75 years. We assessed aBMD at the whole body (WB),
29 hip (TH) and lumbar spine (LS) with DXA, LS Tb.vBMD by QCT and vBMD, and
30 microarchitecture and strength at the distal radius and tibia with HR-pQCT and micro-finite
31 element analysis. Serum PINP and β CTX were measured by automated ECLIA. Obese adults
32 had greater WB, LS and TH aBMD than normal adults. The effect of obesity on LS and WB
33 aBMD was greater in older than younger adults ($p<0.01$). Obese adults had greater vBMD
34 than normal adults at the tibia ($p<0.001$ both ages) and radius ($p<0.001$ older group), thicker
35 cortices, higher cortical BMD and tissue mineral density, lower cortical porosity, higher
36 trabecular BMD and greater trabecular number than normal adults. There was no difference
37 in bone size between obese and normal adults. Obese adults had greater estimated failure load
38 at the radius ($p<0.05$) and tibia ($p<0.01$). Differences in HR-pQCT measurements between
39 obese and normal adults were seen more consistently in the older than the younger group.
40 Bone turnover markers were lower in obese than normal adults. Greater BMD in obesity is
41 not an artefact of DXA measurement. Obese adults have higher BMD, thicker and denser
42 cortices and higher trabecular number than normal adults. Greater differences between obese
43 and normal adults in the older group suggest obesity may protect against age-related bone
44 loss, and also increase peak bone mass.

45

46 **Key words:** OBESITY, BONE MINERAL DENSITY, MICROARCHITECTURE, HR-

47 pQCT, BONE TURNOVER

48

49 **Introduction**

50 Most of the available evidence supports a lower overall risk of fracture and lower risk of
51 proximal femur and vertebral fracture in obese adults, compared to adults with a normal body
52 mass index (BMI) ⁽¹⁻⁸⁾. However, fracture risk in obesity is not lower at all skeletal sites; the
53 risk of some non-spine fractures including proximal humerus, upper leg and ankle fracture is
54 higher than in non-obese adults ^(3, 4, 7, 9). Protection against fracture in obesity may be partly
55 explained by the positive association between BMI and BMD ^(8, 10-12), while differences in fall
56 characteristics and soft tissue padding at the hip have also been proposed as mechanisms to
57 explain differences in fracture risk between normal BMI and obese adults ^(7, 8, 13). The greater
58 risk of lower limb fractures with obesity could result from differences in bone
59 microarchitecture, bone quality or factors unrelated to bone strength such as greater impact
60 during a fall.

61

62 The association of high BMD with obesity may be an artifact of the method used for
63 measuring BMD. Dual energy X-ray absorptiometry (DXA) is affected by soft tissue
64 overlying bone. Soft tissue thickness may cause a projection error affecting measurements of
65 bone area and thus BMC ⁽¹⁴⁻¹⁶⁾. The assumptions made about fat and lean tissue in a two-
66 compartment model may be inaccurate in obesity, introducing further error. BMD by DXA
67 may not be the best choice when comparing groups of different body weight. However, most
68 previous studies have assessed areal BMD in obesity by DXA.

69

70 Quantitative computed tomography (QCT) allows the study of cortical bone and trabecular
71 bone separately. Such technology allows us to understand whether higher bone density in
72 obesity is a result of alterations in cortical bone and/or trabecular bone. Measurements of

73 bone density by QCT are less affected by overlying soft tissue than measurements by DXA
74 ⁽¹⁴⁾.

75

76 Bone density is not the sole determinant of bone strength. Additional factors include bone
77 geometry and bone microarchitecture. High resolution peripheral quantitative computed
78 tomography (HR-pQCT) allows study of architectural properties of bone such as cortical
79 thickness and trabecular number, and these measurements are less likely to suffer artefact due
80 to variation in body composition. The composite effects of bone size, geometry, density and
81 microarchitecture on bone strength can be evaluated by finite element models generated from
82 HR-pQCT images. Few studies have investigated associations between obesity and measures
83 of vBMD. Whether adiposity affects BMD and bone microstructure in men and women in
84 younger and older adulthood in a consistent manner is unclear.

85

86 So far only one study has been designed to look at bone microarchitecture in obese
87 individuals and that was restricted to older women ⁽¹²⁾. It is not known whether associations
88 between obesity and bone microarchitecture were the same in men and women, or whether
89 differences between obese and normal weight groups are present in younger adults at peak
90 bone mass. The results of a population-based study comprising men and women of a wide
91 age span, suggested that there may indeed be differences in the associations between
92 adiposity and bone density and microstructure by age, gender and menopausal status ⁽¹⁷⁾.

93

94 The aims of this study were to evaluate using DXA, QCT and HR-pQCT the effect of obesity
95 on 1) cortical and trabecular bone density of the spine, distal radius and distal tibia and 2)
96 bone structure and strength of the distal radius and distal tibia, in healthy younger and older

97 men and women. We also sought to characterise bone turnover in obese adults compared to
98 adults with a normal BMI.

99

100 **Materials and Methods**

101 **Study design and participants:** We conducted a cross-sectional case-control study of 200
102 community-dwelling men and women from South Yorkshire, UK, aged 25 to 40 years (n=80)
103 or 55 to 75 years (n=120). Participants were recruited through general practitioners,
104 university and hospital staff and students, and poster advertisements. Cases were obese
105 individuals (BMI \geq 30 kg/m²) and controls were normal weight individuals (BMI 18.5 to 24.9
106 kg/m²) based on the WHO BMI classifications. Controls were recruited to be individually
107 matched to an obese participant by sex, age (\pm 3years), height (\pm 5 cm), smoking status
108 (current smoker or non-smoker) and postcode.

109

110 All women aged 25 to 40 years were pre-menopausal, and those aged 55 to 75 years were at
111 least five years post-menopausal. Participants were excluded if they had pre-diagnosed
112 conditions (including diabetes) or were taking medications known to affect bone metabolism
113 (including hormonal contraceptives and hormone replacement therapy), had fractured or
114 undergone orthopaedic surgery within the last 12 months, were highly physically active (\geq 7
115 hours per week), consumed above 21 units of alcohol per week or were actively trying to lose
116 weight. All participants provided written informed consent. Ethical approval was obtained
117 from Sheffield Research Ethics Committee.

118

119 Height (cm) and weight (kg) were measured using a wall mounted stadiometer (Seca 242,
120 Seca, Birmingham, UK) and electronic balance scale (Seca, Birmingham, UK). BMI was

121 calculated using Quetelet's index ((weight kg/(height m)²). Dietary calcium was determined
122 from weekly milk, cheese and yoghurt intake reported in a questionnaire.

123

124 **DXA**

125 Bone density (g/cm²) at the whole body, lumbar spine (LS) and total hip (TH) was measured
126 by DXA (Hologic Discovery A, Bedford, MA, USA). Whole body fat mass (FM) was
127 determined by DXA.

128

129 **QCT (55 to 75 age group only)**

130 QCT of the lumbar spine (L1-3) was obtained using the LightSpeed VCT XT device (GE
131 Healthcare, Milwaukee, WI, USA). We obtained data for L1, L2 and L3 and then the total
132 region L1-L3. Scans were performed in the axial plane, with a helical rotation and rotation
133 time of 0.8 seconds and a table height of 155. The scan pitch was 0.969 for each scan. All
134 scans had a noise index of 30 and a slice thickness of 0.625mm. The modulated Ma was at a
135 maximum 140, minimum 80, with a mean assumed tube current of 120mA and a tube voltage
136 of 80 kilovolt peak. Scans were attained from 5mm above the superior end plate of L1
137 (inclusive of the T12-L1 joint space) to 5mm below the end plate of L3 (inclusive of the L3-4
138 joint space). QCT scans were analysed using the QCTPro software (Version 5.0.3, Mindways
139 Software Inc. Austin, TX, USA).

140

141 **HR-pQCT**

142 HR-pQCT images of the distal radius and distal tibia (non-dominant, non-fractured limb)
143 were obtained using the XtremeCT device (Scanco Medical AG, Zurich, Switzerland) with
144 standard protocols. HR-pQCT images were analysed with standard software and extended
145 cortical measures software provided by Scanco Medical AG (version 6) ^(9,10). This software

146 identifies the periosteal and endosteal boundaries, enabling assessment of cortical micro-
147 structural bone properties, including apparent cortical thickness (Ct.Th, mm), cortical tissue
148 mineral density (TMD, mgHA/cm³) and cortical porosity (Ct.Po, %).

149

150 Radial images from one pair of women were excluded from analysis due to movement.

151 Extended cortical measures outcomes from one pair of men were excluded due the obese

152 participant exhibiting outlying results (Ct.Po = 0.737, Ct.Po.Dm = 2.388µm). Tibial images

153 from two pairs of women were excluded from analysis due to subject movement and data

154 loss.

155

156 Micro-finite element analysis (version 1.13, Scanco Medical AG, Zurich, Switzerland) was

157 applied to the HR-pQCT images to obtain measures of stiffness and ultimate failure load. The

158 model parameters were set as: material properties isotropic and elastic, cortical bone Young's

159 modulus 20 GPa, trabecular bone Young's modulus 17 GPa, Poisson's ratio 0.3. The

160 proximal end of the section was fixed and a compression strain of 1% was applied to the

161 distal surface of the section.

162

163 **Bone Turnover Markers**

164 Blood samples were collected from all participants between 08:00 and 10:00, following an

165 overnight fast. Serum was stored frozen at -80°C. Bone turnover markers (BTMs) serum

166 collagen type 1 C-telopeptide (CTX) and type 1 procollagen N-terminal peptide (PINP) were

167 measured using the Cobas e411 automated electrochemiluminescence immunoassay (Roche

168 Diagnostics, Germany). The inter-assay coefficients of variation (CVs) were <5%.

169

170 **Statistical Analysis:**

171 Power calculation: We used data sets from a previous study of healthy women in Sheffield to
172 estimate the difference and variability of the difference in hip BMD between normal weight
173 and obese pairs. The standardised difference was 1.125 g/cm² and the standard deviation of
174 the paired differences was 0.16. We set the effect size at 0.09 g/cm² as this is likely to
175 represent a clinically significant difference. A sample size of 200 has 80% power to detect a
176 0.09 g/cm² difference at p <0.05 based on a paired sample t-test.

177 As frequency distributions of CTX and PINP were non-normal, a log transformation was
178 applied prior to analysis. Standard deviation scores for PINP and CTX were calculated by
179 subtracting the mean of the normal BMI, age and gender matched group from each individual
180 result and dividing by the standard deviation of the normal BMI age and gender matched
181 group. Uncoupling index was calculated to assess the relative balance of bone formation and
182 resorption, as described by Eastell et al. ⁽¹⁸⁾ as the difference in the standard deviation scores
183 for PINP and CTX ($Z_{PINP} - Z_{CTX}$), where $Z_{PINP} = (\text{observed PINP} - \text{mean PINP})/SD$ and Z_{CTX}
184 $= (\text{observed CTX} - \text{mean CTX})/SD$. Uncoupling index has previously been shown to be
185 correlated with postmenopausal BMD bone loss ⁽¹⁹⁾.

186
187 Paired samples t-tests were used to determine significant differences between normal BMI
188 and obese adults. Paired samples t-tests were performed for men and women combined, as
189 after considering the results both by gender and in combination, the direction and categorised
190 degree of significance remained the same for all outcomes. Standard deviation scores were
191 calculated by standardising the mean difference between normal BMI and obese groups for
192 each variable against the standard deviation of the normal weight, gender and age matched
193 group. Univariate general linear models (GLM) were used to identify whether age group,
194 gender and BMI had an effect on bone outcomes and GLM interaction terms were used to
195 determine any interaction of age or gender with the relationship between obesity and bone

196 outcomes. Analysis was performed using IBM SPSS Statistics for Windows (Version 21.0.
197 Armonk, NY: IBM Corp.). Significance was accepted when $p < 0.05$.

198

199 **Results**

200 The total sample consisted of 200 individuals. The 25 to 40 years group consisted of 18 male
201 and 22 female pairs and the 55 to 75 years group of 30 male and 30 female pairs.
202 Characteristics of the study population are shown in Table 1. Obese and normal BMI
203 individuals were well matched for age and height (Table 1). The obese group had
204 significantly greater whole body fat mass than the normal group (Table 1).

205

206 **Areal bone density by DXA:**

207 Obese individuals had significantly greater mean aBMD than normal BMI individuals at the
208 total hip ($p < 0.001$ both age groups) and lumbar spine ($p = 0.019$ younger, $p < 0.001$ older).
209 Whole body aBMD was also significantly greater in the obese older adults ($p < 0.001$), but not
210 in the obese younger adults ($p = 0.158$).

211

212 There was an interaction between age group and the effect of obesity on aBMD at the lumbar
213 spine ($p = 0.001$) and whole body ($p = 0.008$), but not at the total hip ($p = 0.071$), with a greater
214 effect of obesity on aBMD in the older adults than the younger adults. In the younger adults,
215 aBMD was 0 to 1 SD scores greater in the obese group than in the normal weight group
216 (Figure 1). In the older adults, aBMD was 1 to 2 SD scores greater in the obese group than in
217 the normal weight group (Figure 1).

218

219 There was no interaction between gender and the effect of obesity on aBMD at the total hip,
220 lumbar spine or whole body, in either age group.

221

222 **HR-pQCT:**

223 Volumetric bone density (vBMD) was significantly greater in obese adults compared to
224 adults with a normal BMI at the distal tibia in both age groups ($p < 0.001$) (Figure 2) and at the
225 distal radius in the older adults ($p < 0.001$) (Figure 3). There was an interaction between age
226 group and the effect of obesity on vBMD at the distal radius ($p = 0.005$) with a greater effect
227 of obesity on vBMD in the older adults. There was no interaction between age group and the
228 effect of obesity on vBMD at the distal tibia ($p = 0.222$). There was no interaction between
229 gender and the effect of obesity on vBMD at the distal radius or distal tibia in either age
230 group.

231

232 Microstructure measurements showed that the higher vBMD in obesity was due to greater
233 trabecular density in younger adults ($p = 0.021$ radius, $p < 0.001$ tibia) and greater trabecular
234 and cortical density in older adults (all $p < 0.001$) (Figure 2, Figure 3). The higher trabecular
235 density in the obese adults was due to greater trabecular number (Tb.N) ($p < 0.001$ all ages, all
236 sites) and lower trabecular separation (Tb.Sp) ($p < 0.001$ all ages, all sites) with no difference
237 in trabecular thickness (Tb.Th) at the radius ($p = 0.696$ younger, $p = 0.056$ older) and tibia
238 ($p = 0.357$ younger, $p = 0.205$ older) (Figure 2, Figure 3).

239

240 Cortical thickness was significantly greater in obese groups at the tibia ($p = 0.001$ younger,
241 $p < 0.001$ older) (Figure 2) and at the radius in the older adults ($p < 0.001$) (Figure 3). The
242 higher cortical density in the older obese adults was due to higher cortical tissue mineral
243 density (Ct.TMD) ($p = 0.027$ radius, $p < 0.001$ tibia) and lower cortical porosity ($p = 0.017$
244 tibia). No differences between normal BMI and obese groups were observed in these cortical
245 parameters in the younger adults (Figure 2, Figure 3).

246

247 The difference between normal BMI and obese adults in Ct.vBMD ($p=0.048$ radius, $p=0.008$
248 tibia) and Ct.TMD ($p=0.040$ radius, $p=0.003$ tibia) was greater in women than in men. At the
249 tibia, the difference in Ct.Th ($p=0.017$) and cortical area ($p=0.012$) was also greater in older
250 women than older men. In the younger adults, differences in cortical or trabecular properties
251 between normal BMI and obese adults were similar in men and women.

252

253 No difference was observed in bone size between normal BMI and obese adults, as assessed
254 by total area or cortical perimeter (Figure 2, Figure 3).

255

256 Whilst patterns of bone microarchitecture were consistent between the distal radius and distal
257 tibia in the older population, the differences between obese and normal BMI adults in the
258 younger group were seen at the tibia, but less consistently at the radius.

259

260 **QCT:**

261 Lumbar spine Tb.vBMD was significantly greater in obese women compared to women with
262 normal BMI ($p=0.003$). There was no difference in lumbar spine Tb.vBMD between normal
263 BMI and obese groups in men ($p=0.166$). There was an interaction between gender and the
264 effect of obesity on Tb.vBMD at the lumbar spine, with a greater effect of obesity on
265 Tb.vBMD in women than in men ($p=0.001$).

266

267 **Bone Strength:**

268 Bone stiffness was greater in obese adults at the distal tibia in both age groups ($p=0.001$
269 younger, $p<0.001$ older) (Figure 2) and at the distal radius in the older adults ($p<0.001$)
270 (Figure 2). In both age groups, obesity was associated with greater estimated failure load at

271 the distal radius ($p=0.048$ younger, $p<0.001$ older) and distal tibia ($p=0.001$ younger, $p<0.001$
272 older) (Figure 2, Figure 3).

273

274 Therefore, although in the younger group the differences in bone density and
275 microarchitectural outcomes between obese and normal BMI adults were less pronounced,
276 the differences appear to contribute to an overall increase in bone strength. There was no
277 interaction between age group and the effect of obesity on stiffness or failure load at either
278 site.

279

280 There was no interaction between gender and the effect of obesity on bone stiffness or
281 estimated failure load at the distal radius or distal tibia, in either age group.

282

283 **Bone Turnover Markers:**

284 CTX was lower in the obese adults in both age groups ($p=0.024$ younger, $p<0.001$ older) and
285 PINP was lower in obese older adults ($p=0.084$ younger, $p=0.008$ older) (Figure 4). GLM
286 revealed no interaction between gender or age group and the effect of obesity on CTX or
287 PINP. CTX and PINP were highly correlated ($r=0.779$, $p<0.001$). Obese adults had an
288 uncoupling index on average 0.24 SD scores greater than normal BMI adults ($p=0.009$). The
289 ratio of PINP to CTX was higher in young adults than older adults ($p=0.022$). Young obese
290 adults had an uncoupling index on average 0.16 SD scores greater than normal BMI young
291 adults ($p=0.342$). Older obese adults had an uncoupling index on average 0.29 SD scores
292 higher than normal BMI older adults ($p=0.007$).

293

294 There was no effect of gender on uncoupling index.

295

296 Multiple linear regression adjusting for age and gender showed that CTX was a significant
297 negative predictor of aBMD and vBMD (whole body aBMD p=0.002, TH aBMD p<0.001,
298 LS aBMD p=0.002, radius vBMD p=0.010, tibia vBMD p=0.038, LS Tb.vBMD p=0.157).
299 PINP was not a significant predictor of aBMD or vBMD.

300

301 **Discussion**

302 Obese adults had greater BMD at all sites measured and favourable bone microarchitecture
303 and greater bone strength at the distal radius and distal tibia, compared to normal adults.
304 Greater differences in BMD and HR-pQCT measurements between obese and normal adults
305 were observed in the older adults than the younger adults and suggest that obesity may
306 protect against age-related bone loss, and also increase peak bone mass.

307

308 Our results are consistent with the existing literature that shows greater aBMD in obesity.
309 High BMI has previously been positively associated with bone mass in adults ^(8, 11, 12, 20-28)
310 and older adults ^(29, 30) of both sexes. Body weight and BMI have been positively associated
311 with aBMD of the lumbar spine ^(12, 22, 23, 25, 28), femoral neck ^(22, 23, 28), distal radius ⁽¹²⁾,
312 proximal femur and leg ^(8, 22, 25, 26, 28, 30). Low body weight is associated with osteoporosis at
313 the lumbar spine, proximal femur, total hip, femoral neck and trochanter ⁽²²⁾.

314

315 This is the first study to address relationships between obesity, bone microarchitecture and
316 micro finite element derived bone strength in an individually-matched case control study of
317 younger and older men and women.

318

319 Sornay-Rendu et al. (2013) previously reported an assessment of bone microarchitecture in
320 obese postmenopausal women, compared with a non-obese control group ⁽¹²⁾. In agreement

321 with our findings, the authors reported greater vBMD at the distal radius and distal tibia in
322 obesity. This greater vBMD resulted from greater cortical thickness, greater Tb.BMD (due to
323 greater Tb.N and lower Tb.Sp), and greater Ct.BMD (due to lower Ct.Po). Also in agreement
324 with our results, the authors reported no difference in total area or trabecular area in obesity
325 ⁽¹²⁾. Greater percentage differences in microarchitectural parameters were observed at the
326 distal tibia compared to the distal radius in the obese group versus the non-obese group ⁽¹²⁾.

327

328 Similarly, in a study of young obese men, BMI was positively associated with Tb.N and
329 inversely associated with Tb.Sp ⁽³¹⁾. Using pQCT, BMI was also positively associated with
330 tibial Tb.BMD in both pre- and postmenopausal women ⁽²⁸⁾.

331

332 A recent study examined the effect of fat mass and lean mass on HR-pQCT derived bone
333 microarchitecture in obese individuals with metabolic syndrome ⁽³²⁾. The study reported
334 positive associations between lean mass and Tb.N and Tb.Sp at the radius, and vBMD,
335 Tb.vBMD, BV/TV, Tb.N, Tb.Sp and Ct.Th at the distal tibia ⁽³²⁾. No significant associations
336 between fat mass and microarchitectural outcomes were observed ⁽³²⁾. However, because
337 there was no control group, and metabolic syndrome may have effects on bone metabolism, it
338 is difficult to compare these findings directly with our results.

339

340 It was perhaps surprising that there was no difference in bone size between normal and obese
341 adults. We speculate that this indicates a minimal effect of habitual loading on bone structure
342 in obesity, and that the differences observed reflect alterations in the hormonal milieu
343 associated with greater adiposity. The observation of no difference in bone size might be the
344 result of inhibition of periosteal apposition due to greater circulating oestrogen in obesity,
345 associated with increased aromatisation of androgens ⁽³³⁾.

346
347 Obese adults have lower bone turnover than individuals with a normal BMI, with lower CTX
348 and PINP. By calculating an uncoupling index, as described by Eastell et al. ⁽¹⁸⁾, we were able
349 to demonstrate a positive balance of bone formation to bone resorption in obese adults. These
350 findings are consistent with the existing literature which shows lower markers of resorption
351 and formation with high BMI in premenopausal women ⁽³⁴⁾, through the menopausal
352 transition ⁽³⁵⁾ and in postmenopausal women ^(12, 34, 36-38). Studies in obese men are lacking,
353 although a recent study of young men and women by Viljakainen et al. showed lower PINP,
354 CTX, TRAP, total OC and carboxylated OC in obese adults compared to non-obese age and
355 gender matched controls ⁽³⁹⁾. In further agreement with our results Viljakainen et al. found no
356 difference in uncoupling index between young obese and non-obese men and women ⁽³⁹⁾.
357 Despite bone turnover typically increasing with age, we found no effect of age on bone
358 resorption in the present study. This may be explained by the age stratification of our young
359 adults, as bone turnover markers remain elevated until age 35 years ⁽⁴⁰⁾. Younger adults had
360 higher bone formation than older adults, possibly associated with the period of consolidation
361 in early adulthood.

362
363 Fat distribution may affect associations between adiposity and bone microarchitecture ^{(17, 31,}
364 ^{41, 42)}. Premenopausal women with greater central adiposity have been shown to have lower
365 trabecular bone volume, bone stiffness and bone formation on bone biopsy ⁽⁴¹⁾. The inverse
366 relationship between trunk fat and trabecular bone volume remained significant after
367 controlling for age and BMI ⁽⁴¹⁾. Ng et al. reported differences in the association between
368 subcutaneous and visceral adipose compartments and bone density and microstructural
369 parameters, differences which were also age and gender dependent ⁽¹⁷⁾. A key limitation of
370 the present study is the lack of assessment of body fat compartments, which should be
371 addressed in future work.

372

373 Sornay-Rendu et al suggested that the greater BMD observed in obesity does not appear to be
374 proportional to the greater body weight, so that adaptation of bone in obesity may not be
375 sufficient to withstand the greater falls force ⁽¹²⁾. Fractures often occur in obese individuals
376 despite normal or high aBMD ^(9, 10). In particular, tibial vBMD and estimated failure load are
377 greater in obese people, so lower bone density is not the cause of the increased risk of lower
378 limb or ankle fracture observed in obesity ^(2, 6, 8, 43). Simple linear scaling may not be
379 sophisticated enough to fully determine appropriate bone strength for body size. Further
380 development of finite element models that account for body weight in the forces acting may
381 provide a better understanding of fracture risk in obesity. Bone is more likely to adapt to
382 daily forces and loads, which differ from forces acting in a fall impact. Therefore it may not
383 be surprising that obese individuals continue to fracture at some sites despite greater BMD
384 than normal weight individuals.

385

386 Whilst the greater BMD at the hip and lumbar spine may explain obesity being protective
387 against hip and vertebral fracture, non-skeletal factors, such as greater soft tissue thickness at
388 the greater trochanter may also contribute to fracture risk in obesity ⁽⁴⁴⁾. Obese individuals
389 may be at greater risk of falls due to impaired muscular function, sarcopenic obesity, and/or
390 fat infiltration of skeletal muscle ⁽⁴⁵⁻⁴⁷⁾. Different fall direction and fall forces in obesity could
391 also contribute to the greater risk of lower limb and proximal humerus fractures.

392

393 The cross-sectional design of this study must be acknowledged as a limitation. BMI may be
394 considered too crude a measure of obesity, as body fat distribution could be a determinant of
395 bone density and microarchitecture, but our obese group did have significantly higher fat
396 mass than the normal weight group. Whilst the most likely confounding differences between

397 obese and normal weight individuals (age, body size, smoking, exercise and socioeconomic
398 status) were controlled for as much as possible, any remaining differences may have affected
399 the results.

400

401 CT density measurements may be affected by the soft tissue thickness effects of increasing
402 BMI measures, for example beam hardening due to greater adiposity. While bone density
403 measurements might be affected in obesity, it is less likely that microarchitectural outcomes
404 would be affected.

405

406 Our finding of greater bone strength in young obese adults despite less pronounced
407 differences in bone density and microarchitecture between normal and obese groups could be
408 due to unmeasured factors rather than the cumulative effect of non-significant differences in
409 bone structure. It is possible that the absence of an interaction between age and the effect of
410 obesity on failure load could exist when there is no effect in young adults, a small effect in
411 older adults, and insufficient power to detect a difference.

412

413 The HR-pQCT finite element analysis model used in this study does not take into account
414 individual loads upon falling and this approach would increase the sophistication of the
415 model. The current model simulates a direct compression force on the distal tibia which may
416 not be the most suitable strength test for the prediction of ankle fracture which is affected by
417 torsion forces and contribution of ligaments.

418

419 In conclusion, obese individuals had greater bone density than their normal weight
420 counterparts, at all sites measured. The greater density in trabecular bone was due to greater
421 trabecular number, but trabecular thickness did not differ between obese and normal weight

422 people. Cortical thickness and cortical tissue mineral density were also higher in obese
423 people, and cortical porosity was lower. Bone size at the radius and tibia did not differ
424 between obese and normal weight people. The magnitude of the difference in bone density
425 observed between obese and normal weight individuals using DXA was comparable to that
426 observed using HR-pQCT suggesting that greater bone density in obesity is not solely an
427 artefact resulting from greater soft tissue thickness.

428

429 The differences in bone turnover and BMD between obese and normal weight groups
430 manifest by young adulthood, suggesting that obesity has positive effects on peak bone mass
431 acquisition. The greater differences between obese and normal groups in the older adults
432 suggest obesity may also be protective against age-related bone loss.

433

434 The identification of mechanisms responsible for greater bone density in obesity will improve
435 our understanding of the pathophysiology of osteoporosis and could lead to new therapeutic
436 targets. Understanding why some fractures are increased in obesity may require more
437 sophisticated models for the assessment of bone strength, which may lead to further insights
438 into the site-specific mechanisms of fractures.

439

440 **Disclosures**

441 The authors state that they have no conflicts of interest.

442

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452

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587

588

589 **Table Legend:**

590 Table 1: Study population characteristics by age and gender group (Mean (SD)).

591

592 **Figure Legends:**

593 Figure 1: Mean standard deviation score (95% CI) of obese groups calculated against normal
594 weight groups for aBMD at the total hip, lumbar spine and whole body, by age and
595 gender.

596 Zero line indicates the mean of the age and gender matched normal group.
597 Y=Younger adults, O=Older adults. The p-value refers to the comparison between
598 obese and normal BMI groups, where * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$

599

600 Figure 2: Mean standard deviation score (95% CI) of obese groups calculated against normal
601 groups for total and cortical parameters at the distal tibia, by age and gender. Zero
602 line indicates the mean of the age and gender matched normal group. Y= Younger
603 adults, O= Older adults. The p-value refers to the comparison between obese and
604 normal BMI groups, where * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$.

605

606 Figure 3: Mean standard deviation score (95% CI) of obese groups calculated against normal
607 groups for microarchitectural parameters at the distal radius, by age and gender.
608 Zero line indicates the mean of the age and gender matched normal group. Y=
609 Younger adults, O=Older adults. The p-value refers to the comparison between
610 obese and normal BMI groups, where * $p < 0.05$, ** $p < 0.01$, *** $p < 0.001$

611

612 Figure 4: Box and whisker plots for serum CTX and PINP in obese and normal, younger and
613 older adults.