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Point of care creatinine testing for kidney function measurement prior to contrast-enhanced diagnostic imaging: Evaluation of the performance of three systems for clinical utility

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ABSTRACT

Background

Acute kidney injury (AKI) can occur rarely in patients exposed to iodinated contrast and result in contrast-induced AKI (CI-AKI). A key risk factor is the presence of pre-existing chronic kidney disease (CKD), therefore it is important to assess patient risk and obtain kidney function measurement prior to administration. Point of care (PoC) testing provides an alternative strategy but there remains uncertainty, with respect to diagnostic accuracy and clinical utility.

Methods

A device study compared three PoC analysers (Nova StatSensor, Abbott i-STAT, Radiometer ABL800 FLEX) with a reference laboratory standard (Roche Cobas 8000 series, enzymatic creatinine). Three hundred adult patients attending a UK hospital phlebotomy department were recruited to have additional blood samples for analysis on the PoC devices.

Results

The ABL800 FLEX had the strongest concordance with laboratory measured serum creatinine (mean bias=-0.86, 95% limits of agreement = -9.6 to 7.9) followed by the i-STAT (average bias=3.88, 95% limits of agreement = -8.8 to 16.6) and StatSensor (average bias=3.56, 95% limits of agreement = -27.7 to 34.8). In risk classification, the ABL800 FLEX and i-STAT identified all patients with an eGFR \leq 30, whereas the StatSensor resulted in a small number of missed high-risk cases (n=4/13) and also operated outside of the established performance goals.

Conclusions

The screening of patients at risk of CI-AKI may be feasible with PoC technology. However in this study it was identified that the analyser concordance with the laboratory reference varies. It is proposed that further research exploring PoC implementation in imaging department pathways is needed.

Trial registration

ISRCTN18805212

Point of care creatinine testing for kidney function measurement prior to contrast-enhanced diagnostic imaging: Evaluation of the performance of three systems for clinical utility

INTRODUCTION

The use of intravascular iodinated contrast agents is common in diagnostic imaging but the benefits of their use must be weighed against the potential risk [1]. Patients with pre-existing chronic kidney disease (CKD) and other factors, such as diabetes, may be at risk of developing acute kidney injury (AKI) following contrast administration. Contrast-induced AKI (CI-AKI) has been defined as AKI occurring 24-72 hours after the intravascular administration of iodinated contrast media that cannot be attributed to other causes [2]. Where the contrast may be one of a number of other additional attributable factors post intervention the term post contrast AKI (PC-AKI) may be more appropriate [3]. To minimise the risk of this potentially fatal complication, several international guidelines [1,4-9] recommend patient screening and kidney function testing. In the out-patient setting, the estimated glomerular filtration rate (eGFR), calculated from the serum creatinine (SCr) is used to risk stratify patients prior to contrast administration. Historically, most guidelines have traditionally advised that an eGFR below 60mL/min/1.73m² signifies an increased risk of CI-AKI triggering strategies aimed at optimising volume status with prophylactic oral hydration or intravenous (IV) volume expansion. The highest risk group is considered to be in patients with an eGFR below 30mL/min/1.73m² [1], which may, in some health systems result in restriction of iodinated contrast altogether. Despite variation in clinical practice internationally [10-13] regarding the best way to calculate a patients individual risk and which prevention strategies to

implement, testing of kidney function prior to administration of iodinated contrast is uniformly accepted as standard practice.

Point of care (PoC) testing for kidney function is an attractive method for providing a rapid result, particularly in the emergency department, acute medical unit or critical care setting where there is a need to make immediate decisions regarding treatment. With ever increasing demands on health services globally, it has been explored as a strategy to ensure patient safety before the administration of contrast media [14-25]. However, the literature reveals both disparity in clinical concordance with the central laboratory and the clinical utility of PoC in clinical practice and adoption has therefore been limited [10]. Importantly, even where they are available in diagnostic imaging departments, such devices have been widely integrated into the clinical pathway. There remains an important need to formally evaluate the role of PoC testing in terms of accuracy, clinical feasibility, and health economic benefits.

Aims of this investigation

This Bias Estimation of Point of Care Creatinine (BEPoCC ISRCTN 18805212) sought to compare the performance of 3 CE-marked PoC analysers against a reference laboratory standard to confirm the accuracy of kidney function categorisation and assess their validity for clinical decision making in diagnostic imaging.

MATERIALS AND METHODS

Study participants

Over a six-week period in September and October 2016, consecutive adult outpatients (≥ 18 years) attending a UK hospital phlebotomy department for routine Urea and Electrolytes (U&E) blood tests were approached. No upper age limit was adopted, but pregnant individuals and those unable to consent were excluded.

Following consent, participants completed a screening questionnaire based on previous studies [22,26,27] to examine patients kidney risk status and stratify the sample into low and high risk groups based on their co-morbidities and medication. This stratification method ensured the study sample comprised patients with a range of kidney function levels to ensure applicability to a diagnostic imaging setting. The PoC results were not reported to the referring clinician and did not influence any clinical decisions. Demographics, including age, gender and race (Afro-Caribbean or not Afro-Caribbean) were collected for each participant.

Method agreement is a question of estimation, not hypothesis testing. In this scenario there is no 'minimum' sample size required. The confidence interval for 95% limits of agreement is $\pm 1.96 \sqrt{(3/n)}s$, where n is the sample size and s is the standard error [28]. Therefore, a sample size of 300 provides a 95% CI of approximately $\pm 0.2s$.

Ethics

The research complied with all the relevant regulations, institutional policies and in ran in accordance to the tenets of the Helsinki Declaration. Ethical approval for the

study was granted by South East Scotland Research Ethics Committee (IRAS:202240) and all participants gave written informed consent. The study was adopted onto the NIHR portfolio (CPMS ID: 31955).

Blood sampling

The standard U&E blood sample was collected by an experienced phlebotomist and processed following local operating procedures. To ensure minimal patient intervention, an additional sample of blood was immediately collected from the same venous puncture site. The whole blood research sample (S-Monovette Lithium Heparin 2.7mL tube, Ref 05.1553, Sarstedt, Numbrecht, Germany) was labelled with a unique study identifier and transferred to the on-site laboratory for analysis.

Capillary blood sampling was subsequently performed from the fingertip of each participant by two research radiographers (BS & MAH), as would be the case in routine practice. The skin was pierced with a spring-loaded lancet and the sample collected directly onto the analysis strip avoiding squeezing of the finger or milking of blood.

Phlebotomy and laboratory staff were unaware of the patients' eGFR, reference method results and other PoC results at the time of sample collection and analysis. Where there was incomplete data, i.e. results not available across all methods, the participants were excluded from the sample.

Test methods

The reference standard was Roche Modular IDMS calibrated enzymatic creatinine analysis, performed on serum samples on a Cobas8000 platform (Roche, Inc., Mannheim, Germany). During the study period, for the five creatinine analysers on the reference laboratory platform, the between-run imprecision was determined using independent commercially available QC materials, the standard practice in the laboratory. CVs ranged from 1.3-2.1% (median=1.8%) at a concentration of 81 $\mu\text{mol/L}$, 1.0-1.4% (median=1.4%) at concentration of 203 $\mu\text{mol/L}$ and 0.9-1.3% (median 1.2%) at a concentration of 615 $\mu\text{mol/L}$.

The CE-marked PoC analysers were the StatSensor (Nova Biomedical, Waltham, MA, USA) and i-STAT (Abbott Laboratories, Princeton, NJ, USA), both handheld devices in current use in UK imaging departments and the ABL800 FLEX (Radiometer, Brønshøj, Denmark), a benchtop analyser. Capillary blood samples were analysed on the StatSensor in the phlebotomy department. Due to the larger volume requirements, whole blood samples were analysed on the i-STAT and ABL800 FLEX devices which were situated in the laboratory due to space constraints. Each PoC analyser employs a creatinine method based on the amperometric detection of H_2O_2 generated by three enzyme cascade reactions and expresses plasma calibrated patient results. To avoid inter-device variation, a single analyser was used from each manufacturer for the duration of the study. Quality control (QC) was performed daily during the research using the manufacturers' quality control materials and limits of acceptability for imprecision.

The laboratory SCr result was confirmed from the hospital order communication system, as in routine practice. The PoC whole blood creatinine (WBCr) result was documented for each participant. No off-set adjustment was applied for PoC measurements. All results were transcribed into the EDGE research management system (University of Southampton, UK Version 2.0.28) and exported to Excel® (Microsoft Corporation) for initial analysis. For consistency, the eGFR for all PoC devices were derived using the Chronic Kidney Disease Epidemiology Collaboration (CKD-EPI) equation [29], taking account of race and gender. In addition, the Modification of Diet in Renal Disease (MDRD) study equation [30] was also used to calculate an alternative eGFR level for comparison.

Statistical Analysis

In the absence of repeated patient sample measurements from each PoC device, imprecision, expressed as coefficient of variation (CV), was calculated based on the daily analysis of quality control material. We report the mean, standard deviation (SD) and range across the patient samples for each device. We also report, and illustrate using Bland-Altman plots, the mean bias of the PoC devices relative to the laboratory reference standard along with the 95% limits of agreement for the differences. Passing-Bablok regression analyses explore the presence of proportional and constant error for each of the three devices (from the slope and intercept co-efficient, respectively). This approach does not assume that any measurement error in either the laboratory or PoC measurements is normally distributed.

Total analytical error was calculated in line with Clinical & Laboratory Standards Institute (CLSI) recommendations [31]:

$$T.A.E = \hat{x} \pm (t * s.d.)$$

Where \hat{x} is the average difference, *s. d.* is standard deviation of the differences, and *t* is a factor from a *t*-distribution (in this case, 1.65). Further to this, we assessed whether the derived eGFR measurements from each device meet the performance goal set by The Laboratory Working Group of the National Kidney Disease Education Program (NKDEP): that the average error in eGFR should not exceed 10% [32].

The eGFR results calculated using the CKD-EPI equation were categorised according to the associated risk of CI-AKI [1] using predefined categories (high risk= ≤ 30 ; moderate= $31-59$; low= ≥ 60). Overall clinical concordance was calculated as the number (%) of samples falling into the same CI-AKI risk category as that derived from the laboratory method. To evaluate clinical utility, eGFR values calculated from PoC devices were also compared to the laboratory derived eGFR values through error grid analysis [33], which visually demonstrates a scatter plot of both methods into clinically relevant areas.

The analyses and plots were generated using the Analyse-It add-in (Analyse-it Software Ltd, Leeds, UK) for Excel® (Microsoft Corporation, USA) and the statistical software package R (The R Foundation, <https://www.r-project.org/>).

RESULTS

Quality control/Device imprecision

The daily QC confirmed that all measurements were within the ranges given by the manufacturer for each device prior to analysis of participant samples (Table 1). Variation in the number of QC samples analysed relates to automatic daily QC with

the ABL800 FLEX and manual QC for the handheld analysers on recruitment days only.

Table 1. Summary of PoC quality control replication data

QC sample	i-STAT		StatSensor		ABL800 FLEX		
	Level 1	Level 3	Level 1	Level 3	Level 1	Level 2	High
Reference mean (range)*	380 (309-451)	44 (09-80)	(44-124)	(398-663)	(211-291)	(21-37)	1500
Mean $\mu\text{mol/L}$	384.9	47.6	80.9	496.5	243.8	29	1547.8
SD $\mu\text{mol/L}$	9.3	2.4	6.4	35.8	3.6	0.6	27.7
CV %	2.3	5	7.9	7.2	1.5	2.1	1.8
N	26	26	25	25	53	54	60

Key: QC=quality control; CV=coefficient of variation; N=number of samples; *values supplied by individual manufacturers for their QC materials.

Participant Demographics

A total of 363 individuals consented to complete the screening questionnaire. Of these, 63 were subsequently excluded prior to allocation to the relevant study arm, resulting in 300 participants proceeding to intervention (supplementary figure 1). The study sample comprised 158 males and 142 females, with 3 individuals (1.0%) defining their race as Afro-Caribbean. The age range was 18-92 years with a mean of 60 years (SD ± 18 years).

The participants were stratified into high (n=200) and low-risk (n=100) arms based on the result of the screening questions. A range of risk factors were identified, including previous abnormal kidney function or kidney disease, older age, hypertension, heart disease, gout, use of anti-inflammatories, chemotherapy or other nephrotoxic drugs and multiple myeloma.

Test failure

A total of 5 procedural failures were recorded during the study, 4 with the StatSensor and 1 with the ABL800 FLEX. No failures were recorded for the i-STAT. In relation to the StatSensor, 2 of the 4 failures were due to flow errors during sampling, one was due to the strip not being located correctly, and the other related to the machine timing out due to inactivity. In all cases, a second test was successful. The ABL800 FLEX failure was due to an incorrectly sited syringe during processing of the sample. The second attempt to analyse the same sample was completed successfully.

Participant samples

A summary of the creatinine concentrations for each participant sample measured by the laboratory reference standard and each of the 3 PoC devices is reported in Table 2.

Table 2 Descriptive and method comparison statistics for patient creatinine values (PoC devices compared with the laboratory reference standard)

	Mean (SD)	Range	<i>r</i>	Mean Bias (95% CI)	95% Limits of Agreement		Passing-Bablok	Passing-Bablok	Total Analytical Error
					Constant Error (95% CI)	Proportional Error (95% CI)	Lower (95% CI)	Upper (95% CI)	
Laboratory Reference Standard (μmol/L)	92 (34)	38-302	-	-	-	-	-	-	-
iSTAT (μmol/L)	96 (36)	35-323	0.985	3.88 (3.14 to 4.62)	-8.8 (-10.06 to -7.54)	16.6 (15.30 to 17.82)	-3.289 (-5.029 to -1.572)	1.079 (1.060 to 1.098)	-6.80 to 14.56
StatSensor (μmol/L)	95 (35)	44-330	0.891	3.56 (1.75 to 5.37)	-27.7 (-30.80 to -24.60)	34.8 (31.72-37.92)	0.778 (-6.103 to 6.217)	1.022 (0.957 to 1.103)	-22.75 to 29.87
ABL800 FLEX (μmol/L)	91 (33)	37-304	0.991	-0.86 (-1.37 to -0.35)	-9.6 (-10.52 to -8.78)	7.9 (7.06 to 8.81)	-0.046 (-1.000 to 1.538)	0.992 (0.975 to 1.000)	-8.26 to 6.54

All PoC devices demonstrated both positive and negative bias versus the laboratory results over the range of patient creatinine values measured (Table 2 and supplementary figures 2-4). The i-STAT and StatSensor both demonstrated a small positive average bias, although this was predominantly at higher creatinine with the i-STAT. Whereas, the ABL800 FLEX demonstrated a marginal negative average bias, but had the tightest 95% limits of agreement of the three devices.

The constant and proportional error for each PoC device compared to the laboratory reference standard is reported, estimated based on the Passing-Bablok regression models.

Clinical relevance

Calculation of eGFR

The average total error for eGFR calculated from the WBCr measurements for the i-STAT and ABL800 FLEX when compared to those from the laboratory reference standard were less than the desired 10% error goal (5.5% and 5.0%, respectively). The average total error for the StatSensor exceeded this goal (13.6%).

When eGFR results, derived from the reference standard laboratory SCr, were categorised according to the potential risk of CI-AKI and a subsequent need for the initiation of preventative measures, there was variation between the outcomes when using the CKD-EPI and MDRD calculations (Table 3). When risk stratifying into high and moderate vs. low risk, CKD-EPI and MDRD agreed for 94.2% of individuals. In 5% of cases, the MDRD calculations overestimated the risk and therefore would have resulted in unnecessary preventative measures being applied. In the remaining 3 cases the risk was underestimated, although the results were close to the cut-off values.

Table 3 Comparison of the eGFR result from laboratory reference standard serum creatinine using the CKD-EPI and MDRD equations

		MDRD			Total
		High	Moderate	Low	
CKD-EPI	High	12	1	-	13
	Moderate	1	59	2	62
	Low	-	14	211	225
	Total	13	74	213	300

Key: High=eGFR≤30; Moderate=eGFR31-59; Low=≥60

Error grid analysis

When identifying patients with an abnormal kidney function (eGFR<60), i-STAT WBCr results and ABL800 FLEX WBCr results showed 98.6% (n=74/75) and 97.3% (n=73/75) concordance respectively with the laboratory SCr results, whilst StatSensor WBCr results showed 89.3% (n=67/75) concordance.

In relation to those at highest clinical risk where contrast may be withheld (eGFR≤30), clinical concordance with the laboratory reference standard the results were similar (i-STAT n=13/13; 100%; ABL800 FLEX n=13/13; 100.0%; StatSensor n= 9/13; 69.2%).

When the CKD-EPI eGFR values were grouped according to the risk of CI-AKI all PoC devices resulted in the risk of CI-AKI being over- or under-estimated in a small number of patients in comparison to the laboratory reference standard (table 4). Error grids (Figure 1a-c) demonstrate performance zones for risk categorisation based on the CKD-EPI eGFR calculations. The number of participants placed in each zone and the patient management repercussions of risk misclassifications are summarised in Table 4.

Figure 1: Error grid analysis of concordance between eGFR risk stratification derived from laboratory measured serum creatinine and 3 POC devices (1a= i-STAT, 1b= StatSensor, 1c= ABL800 FLEX). Zones relating to patient management repercussions are highlighted and related data is summarised in Table 4.

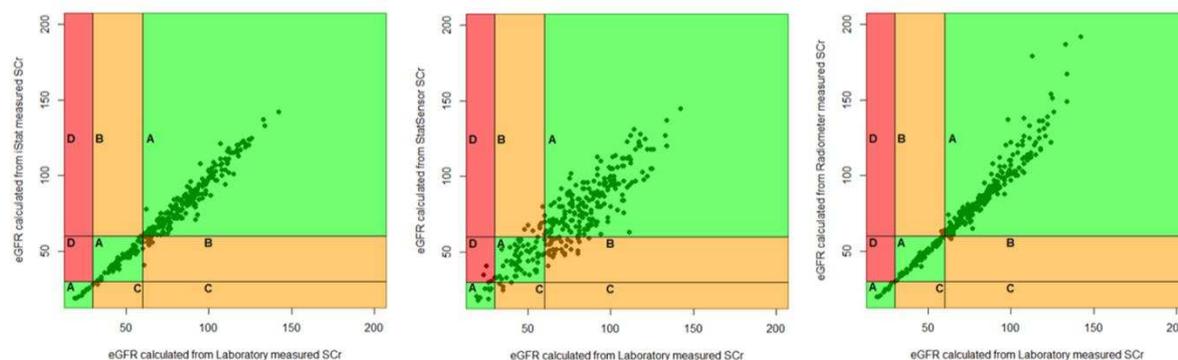


Table 4: Patient management implications of concordance between eGFR risk stratification based on UK guidelines during data collection [1]

Zone	Implication on Management Decision	i-STAT No (%)	StatSensor No (%)	ABL800 FLEX No (%)
A	Correct risk classification – appropriate management	282 (94.0)	250 (83.3)	297 (99.0)
B	Incorrectly classified, but no implication for clinical management	16 (5.3)	42 (14.0)	3 (1.0)
C	Incorrect classification, potential for unnecessary prophylaxis or with-holding of contrast	2 (1.0)	4 (1.3)	0
D	Incorrect classification and potential for increased risk of CI-AKI due to insufficient prophylaxis	0	4 (1.3)	0

DISCUSSION

Clinical practice guidelines recommend targeted screening of kidney function based on individual risk [7,8]. However, due to the silent nature of many forms of kidney disease and complex workflows within diagnostic imaging, it is usual practice for all patients receiving iodinated contrast-enhanced imaging to have had a SCr and

eGFR checked prior to the examination [10-13]. This result establishes whether it is safe for a patient to receive iodinated contrast media and identify if any preventative measures are required or whether contrast media is withheld. It is therefore very important that the kidney function result is available and that this is accurate and reliable. In practice, problems with availability of a kidney function result can lead to significant implications for patients in terms of delay in diagnosis and reduction in service efficiency [10,15]. These issues may be addressed by the introduction of PoC technology.

The i-STAT and the StatSensor have been evaluated most frequently in the diagnostic imaging literature [14-25] and are available in a small number of clinical departments across the UK [10]. The sampling techniques used in this study mirror how they are being used in practice. The results confirm that kidney function testing is feasible on a PoC device but variation in clinical concordance between the devices tested and the laboratory reference standard was evident similar to previous research [14]. The ABL800 FLEX analyser was the most precise of the three with the lowest total analytical error, closely followed by the i-STAT. The StatSensor fared worst in both categories and failed to identify a small proportion of high-risk patients. The capillary samples were taken by fingerprick, which may have contributed to the analytical error during participant testing. Crucially this study evaluated clinical performance which establishes whether the test can identify individuals with pre-defined criteria or conditions within a particular clinical context [34]. In line with other recent studies [14,17,22,24,35] the ABL800 FLEX or i-STAT may be appropriate for use in this context, whereas the StatSensor results were outside the recommended performance goals for eGFR [32].

The CKD-EPI creatinine equation has been recommended to estimate GFR, using creatinine assays with calibration traceable to the standardised reference material [36]. Our study confirmed previous evidence of variation in eGFR calculation when using the two different equations [37], with over-estimation of CI-AKI risk with MDRD in some patients [38, 39]. Although, only the laboratory differences are reported, this pattern would be seen across methods. In clinical practice for PoC devices with an inbuilt eGFR calculator this confirms the importance of ensuring that the equation used (CKD-EPI or MDRD) is aligned to the local laboratory. Importantly, this also identifies the relevance of cross-laboratory standards where patient results are shared but different calculation standards are used.

This study, which is the first to utilise error grid analysis for eGFR based clinical outcomes, demonstrated that PoC analysers aligned the majority of participant samples to the correct CI-AKI risk category and reassuringly no high-risk cases would have been missed with two of the 3 PoC devices.

The need for efficient workflow and rapid turn-around of contrast-enhanced diagnostic imaging studies supports the introduction of PoC creatinine testing [15, 22]. However, due to previous concerns around the accuracy of PoC creatinine technology, it is yet to make its way into mainstream use. Further evidence is required of the feasibility and practicality of embedding this technology into clinical practice.

Robustness of findings

This study was conducted in a phlebotomy setting and the patients may not wholly represent those referred for contrast-enhanced imaging. Despite the stratification of participants, only one quarter of samples in the present study demonstrated an abnormal kidney function (eGFR<60), however this is comparable with other studies [14,25] and considered a sufficient spread to review the appropriateness of PoC for clinical practice in the diagnostic imaging context.

This was not a formal method evaluation study, as required for introduction into routine practice but focussed on exploring the clinical impact of using POCT compared to use of the laboratory. The study was limited to the assessment of bias, total error and clinical performance of the devices in relation to creatinine and eGFR. Precision, interference, cross-reactivity, linearity and quantitation limits of PoC analysers have not been investigated and are outside the scope of this study. The analytical goal for total allowable error in creatinine measurements is derived from repeated measurements, which was not possible in this study. The analysis is therefore limited to reporting the total analytical error and the performance goal for eGFR was defined as the key outcome.

Comparisons were made using the recommended CKD-EPI creatinine equation and an IDMS calibrated enzymatic creatinine assay, however both the MDRD equation and creatinine assays based on the Jaffe reaction are still being used in a number of laboratories [10]. Concordance between PoC and eGFR determined in these laboratories may differ from our findings.

Procedure failure rates have been reported but other practical factors, such as ease of device maintenance and pros and cons of bedside capillary vs venous whole blood sampling, were not explored further. The cost of PoC implementation has not been investigated in this study, however variations in the initial and ongoing costs of devices will vary depending on type (hand held vs benchtop) and volume of samples analysed [40].

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AUTHOR CONTRIBUTIONS

I can confirm that all authors listed have contributed to study design and the final version of the manuscript. They have accepted responsibility for the content and have approved submission.

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HONORARIUM

None declared

COMPETING INTERESTS

The funding organisations played no role in the study design; in the collection, analysis, and interpretation of the data; in the writing of the report; or in the decision to submit the report for publication.

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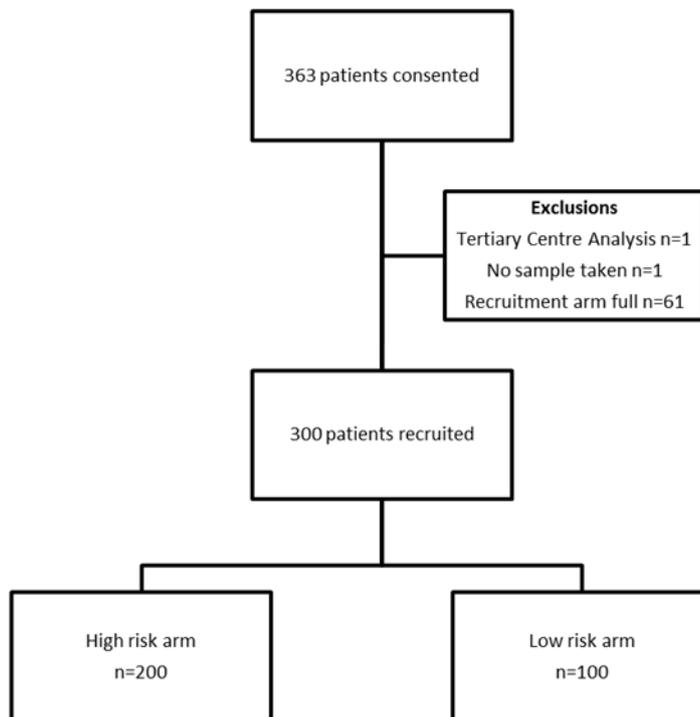
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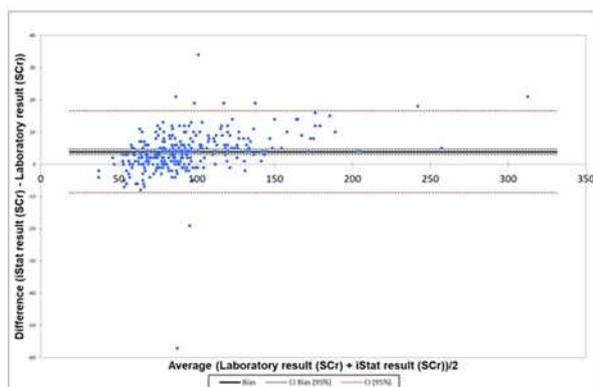
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Supplementary figures

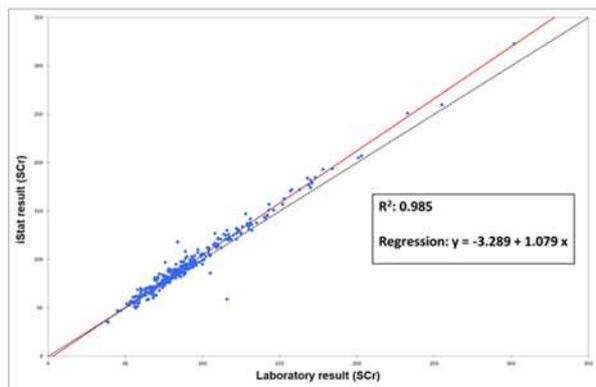
Supplementary figure 1: Recruitment flow chart



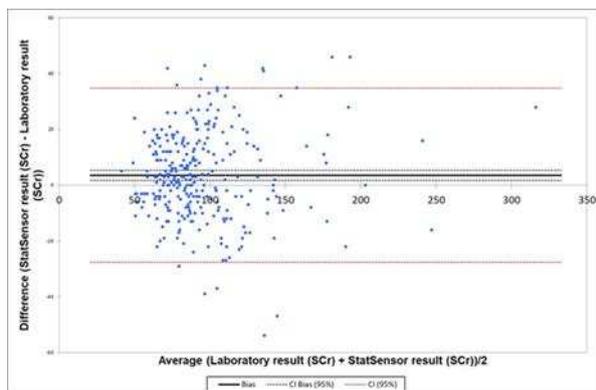
Supplementary figure 2(A) Scatter diagram of the difference versus the means of paired creatinine results analysed with the i-STAT and reference method creatinine.



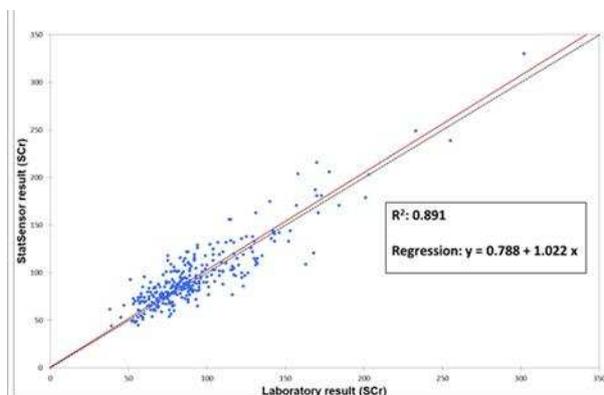
Supplementary figure 2(B) Scatter diagram mapping the creatinine results from the i-STAT to the laboratory measurements, with Passing-Bablok line and equation



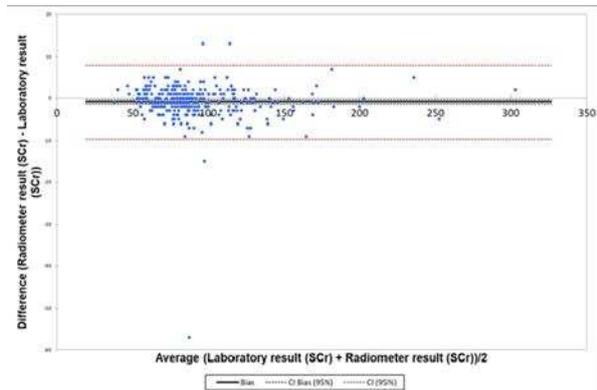
Supplementary figure 3(A) Scatter diagram of the difference versus the means of paired creatinine results analysed with the StatSensor and reference method creatinine.



Supplementary figure 3(B) Scatter diagram mapping the creatinine results from the StatSensor to the laboratory measurements, with Passing-Bablok line and equation



Supplementary figure 4(A) Scatter diagram of the difference versus the means of paired creatinine results analysed with the ABL800 FLEX and reference method creatinine.



Supplementary figure 4(B) Scatter diagram mapping the creatinine results from the ABL800 FLEX to the laboratory measurements, with Passing-Bablok line and equation

