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1 **In-exercise vascular shear rate during acute continuous and interval exercise: impact upon**
2 **endothelial function and MiR-21**

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8 **Running Head:** In-exercise vascular shear rate

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16 **Abstract**

17 **Background:** Endothelial cell phenotype and endothelial function are regulated by hemodynamic
18 forces, particularly wall shear stress (WSS). During a single bout of exercise, the specific exercise
19 protocol can affect in-exercise WSS patterns, and consequently endothelial function. MicroRNAs
20 might provide a biomarker of in-exercise WSS pattern, to indicate whether a specific exercise bout
21 will have a positive effect on endothelial function. We evaluated the effect of acute interval (IT) and
22 continuous (CON) in-exercise WSS patterns upon post-exercise endothelial function and circulating
23 miR-21 expression. **Methods and Results:** 13 participants performed CON and 3 different IT exercise
24 protocols matched for duration and intensity, on separate days. Oxygen uptake, heart rate and
25 brachial artery blood flow were recorded throughout exercise. Brachial artery flow mediated dilation
26 (FMD) was performed pre and 15 min post exercise. Plasma samples were acquired pre and 6 hours
27 post exercise to determine miR-21 expression. In-exercise shear-rate (SR) patterns (a surrogate of
28 WSS) differed according to the CON or IT work rate profile. In-exercise anterograde SR was greater in
29 CON than IT ($P<0.05$), retrograde SR was equivalent between exercise protocols ($P>0.05$). Oscillatory
30 shear index was higher during IT versus CON ($P<0.05$). Post-exercise FMD increased (pre 7.08 ± 2.95 ,
31 post $10.54\pm 4.24\%$, $P<0.05$), whilst miR-21 expression was unchanged (pre 12.0 ± 20.7 %cel-miR-39,
32 post 11.1 ± 19.3 %cel-miR-39, $P>0.05$); with no effect of exercise protocol ($P>0.05$). **Conclusions:** CON
33 and IT exercise induced different SR patterns, but equivalent improvements in acute endothelial
34 function. The absence of change in miR-21 expression suggests miR-21 is not a suitable biomarker of
35 exercise-induced SR.

36 **New & Noteworthy**

37 Interval exercise has the potential to negatively impact vascular adaptations due to repeated
38 oscillations in vascular shear. We are the first to continuously assess exercise-induced shear
39 throughout different acute exercise protocols and examine its relationship with acute endothelial

40 function and a circulating biomarker of shear (miR-21). These experiments provide clear data
41 indicating enhancement of the acute vascular response from differing interval exercise protocols,
42 with the study also providing detailed vascular and shear responses for future reference.

43 **Keywords:** interval exercise; endothelial function; FMD; microRNA; shear rate

44 **Introduction**

45 Atherosclerosis is the underpinning pathology of cardiovascular disease (CVD). Endothelial
46 dysfunction is the earliest stage in the silent development of atherosclerosis (24, 38) and has been
47 established as an independent risk factor for CVD (5, 19). Assessment of endothelial function thus
48 provides independent prognostic information beyond traditional CVD risk factors in both healthy
49 and patient populations (29, 40). Additionally, as the asymptomatic nature of atherosclerosis can last
50 many years, blood biomarkers as complementary indices of endothelial function are highly sought
51 after; however currently there is no such circulating biomarker.

52 Endothelial cell (EC) phenotype and thus endothelial function is regulated by hemodynamic
53 forces generated by blood flow in the lumen (6); in particular, endothelial wall shear stress (WSS)
54 (10). The relative impact of endothelial WSS upon endothelial function is highly dependent upon
55 blood flow velocity and flow profiles. High velocity, laminar WSS promotes an anti-atherogenic EC
56 phenotype, partially mediated through increased production of nitric oxide (NO) (51). Conversely,
57 low velocity and/or oscillatory WSS is associated with altered cell signaling pathways and a pro-
58 atherogenic EC phenotype through upregulation of inflammatory factors, oxidative enzymes and
59 vasoconstrictors (6).

60 Recently, mechano-sensitive microRNAs (miRs), small, non-coding RNAs which negatively
61 regulate gene expression (7), expressed by ECs have been found to be responsive to both laminar
62 and oscillatory WSS and contribute to the regulation of EC phenotype (27). MiR-21 in particular has
63 been identified as an important epigenetic regulator of EC apoptosis and NO production, with its
64 expression regulated by WSS (48). Overexpression of miR-21 in response to differing shear profiles
65 has been shown in previous studies, for example 24 hours of sustained oscillatory shear resulted in
66 miR-21 overexpression and a subsequent proinflammatory endothelial response (50). On the other
67 hand, 24 hours of unidirectional/laminar shear increased miR-21 expression creating an anti-

68 inflammatory endothelial environment (48). It thus appears that overexpression of miR-21 can
69 regulate endothelial phenotype, positively or negatively, via multiple downstream targets, of which
70 nuclear receptor PPAR α and PTEN are examples (48, 50), and that these downstream targets are
71 influenced by differing shear signaling pathways. Importantly, unlike most miRs which are only
72 detectable within cells, miR-21 is highly expressed in the circulation (2). Determining circulating miR-
73 21 expression in conjunction with assessment of endothelial function may provide an insight into the
74 endothelial environment in response to differing shear stimuli, thus offering miR-21 as a potential
75 systemic blood borne biomarker.

76 Acute exercise offers the capacity to investigate the impact of different WSS patterns on both
77 endothelial function and possible biomarkers of WSS, such as miR-21. Both acute and chronic
78 continuous (CON) exercise improves endothelial function, assessed via flow mediated dilation (FMD)
79 in the brachial artery, in healthy and patient populations (9, 14, 22, 25, 36, 43). It is purported that
80 this improvement is driven by exercise-induced WSS mediated effects upon ECs, both in the active
81 limb and in other systemic vessels (20). WSS patterns during exercise have only previously been
82 examined for brief periods during acute continuous (CON) exercise (4, 15, 16, 21, 34, 44, 47). During
83 rhythmic lower limb exercise WSS in the brachial artery has been seen to vary according to the blood
84 flow response to exercise and the upstream thermoregulatory modification to systemic blood flow
85 distribution and haemodynamics (42). For example, at the onset of exercise there is an immediate
86 increase in retrograde WSS in the brachial artery which declines as exercise continues;, in contrast
87 anterograde WSS increases throughout the exercise bout (42).

88 The acute impact of alternative modes of exercise upon WSS patterns and subsequent
89 endothelial function is yet to be explored. For example, comparatively little is known regarding the
90 effect of high intensity interval (IT) exercise regimes upon WSS patterns and subsequent endothelial
91 function. As IT exercise consists of multiple transients between “work” and “recovery” throughout a
92 single session, and the length of the recovery periods govern the magnitude of physiological

93 recovery between each work bout, the pattern of WSS in the brachial artery may oscillate such that
94 repeated transitions result in greater volumes of retrograde shear stress than seen in CON.
95 Increased volumes of retrograde shear stress have been seen to be acutely detrimental to
96 endothelial function (45) and EC phenotype (51). As circulating miR-21 concentration has been seen
97 to be responsive to acute bouts of short duration exercise (2, 31, 32), potentially as a result of
98 increased WSS throughout the arterial tree (48), its relationship with endothelial function may
99 provide a biomarker to differentiate between these differing WSS patterns.

100 The aims of this study were thus twofold: (i) to characterize the acute in-exercise brachial artery WSS
101 pattern induced by intensity and duration matched IT and CON exercise, and (ii) to investigate the
102 effect of acute IT and CON in-exercise WSS patterns upon post-exercise endothelial function and
103 circulating miR-21 levels. It was hypothesized that acute CON exercise would induce a more laminar
104 WSS pattern increasing mir-21 expression, and because of the more anti-inflammatory (laminar
105 WSS) exercise environment, increase endothelial function. On the other hand, acute IT exercise
106 would induce a more oscillatory WSS pattern, increasing mir-21 expression, but because of the more
107 pro-inflammatory environment (oscillatory WSS) exercise environment, decrease endothelial
108 function.

109 **Methods**

110 **Participants**

111 Thirteen healthy participants volunteered for this study (9 male: 4 female, mean \pm standard
112 deviation (SD): age 22 ± 3 years, BMI 23.6 ± 2.1 kg/m²). All participants were free of current or
113 previous risk factors associated with cardiovascular and respiratory diseases and metabolic
114 disorders. Participants were non-smokers and were not taking prescription medications. Females
115 were tested during the same phase of their menstrual cycle and those taking hormonal

116 contraceptives were tested during the same phase of their oral contraceptive use. The University of
117 Leeds ethics committee approved the study protocols which adhered to the declaration of Helsinki.
118 Written informed consent was gained prior to data collection.

119 **Experimental Protocol**

120 Participants attended the laboratory on five separate occasions, each separated by >48 hours.
121 Protocols were completed in a quiet, darkened, temperature controlled laboratory (22-24°C). The
122 initial visit comprised a pre-exercise health screening followed by a standard ramp incremental
123 exercise test (RIT) on a semi-recumbent cycle ergometer. The RIT was used to characterize
124 participant's aerobic function and identify the appropriate work rates for the subsequent exercise
125 protocols, as described in detail below. Following this visit, participants completed four different
126 exercise protocols in a random order. These four visits were conducted following >8 hours of
127 overnight fasting and abstinence from caffeine, alcohol and exercise training for 24 hours. At each of
128 the four visits, participants provided a 10 ml venous blood sample from the antecubital fossa on the
129 arm not used for FMD assessment. Participants then rested supine for >10 min prior to ultrasound
130 recordings of brachial artery FMD. A >3 min warm up (unloaded cycling) and 24 min semi-recumbent
131 cycling exercise protocol was then completed. During each exercise protocol the right arm was
132 extended and supported at the level of the heart. Heart rate (HR), breath-by-breath pulmonary gas
133 exchange and Duplex ultrasound of the brachial artery were recorded throughout the exercise
134 period. Upon cessation of the exercise protocol, a cool down (>2 min unloaded cycling) was
135 completed. Following 15 min supine rest, a post-exercise FMD assessment was completed. Finally, a
136 second venous blood sample was obtained 6 hours post cessation of the exercise protocol. This
137 sampling time point was chosen to be consistent with previous literature assessing circulating
138 microRNA expression in-vivo following acute exercise (39).

139 **Exercise Protocols**

140 Breath by breath pulmonary gas exchange (MedGraphics D-Series, Medical Graphics
141 Corporation, St Paul, MN, USA) was assessed during a standard RIT on a semi-recumbent ergometer
142 (Angio, Lode BV, Groningen, Netherlands) to measure peak oxygen uptake ($\dot{V}O_{2peak}$) and estimate
143 lactate threshold (LT). LT was calculated using the V-slope method and identified the target $\dot{V}O_2$,
144 which was used to select the work rates for each of the four exercise protocols. The four exercise
145 protocols were thus matched for exercise intensity ($\dot{V}O_2$ in the heavy intensity domain (49)) and
146 duration (24 min) but differed in pattern and work rate. The protocols are displayed in **Figure 1** and
147 were defined as (i) continuous exercise (CON), (ii) 4 x 180 s of work each interspersed with 180 s of
148 10 W active recovery (LONG IT), (iii) 12 x 60 s of work with 60 s 10 W active recovery (SHORT IT) and
149 (iv) 4 x 180 s work with 180 s recovery at work rate equivalent to 70% LT (LONG IT 70). The inclusion
150 of the Long IT 70 protocol was to maintain an increased $\dot{V}O_2$ during the recovery periods and
151 therefore elevate the mean $\dot{V}O_2$ and energy expenditure of the session to more closely match the
152 CON and Short IT exercise protocols.

153 **In-exercise assessment of blood flow**

154 The same site of the upper right arm as used in the FMD assessment was used for all in-exercise
155 recordings. The ultrasound (Vivid E9, GE Healthcare, Milwaukee, WI, USA) was operated in duplex
156 mode to obtain continuous second by second recordings of brachial diameter and blood flow
157 velocity during the exercise protocols. Recording, using a 10 MHz linear array probe, started during
158 the final 30 s of warm up and ended 1 min into cool down. Images were recorded directly onto the
159 ultrasound in consecutive 4 min loops and Vascular Imager (MIA, Coralville, IA, USA) utilized to
160 calculate anterograde and retrograde (decelerative) shear rate (SR). SR was used as a surrogate of
161 WSS and, as viscosity was not assessed in the current study, was used as an indicator of the frictional
162 force of blood flow (33). The term SR will thus be used hereafter. Intra-rater reliability CV for
163 anterograde and retrograde SR were 23.8% and 24.5% respectively.

164 **Assessment of endothelial function**

165 FMD procedures were conducted in accordance with previous guidelines (46) with an intra-rater
166 FMD reliability of 11.4%. Resting brachial artery diameter was recorded in duplex in the distal third
167 of the upper right arm for 20 s at 15 frames per second using the Vivid E9. Immediately following
168 this, a blood pressure cuff placed on the right forearm, distal to the ultrasound probe, was rapidly
169 inflated to >220 mmHg for 5 min. Recording of diameter and blood flow velocity began 30 s prior to
170 cuff deflation and continued for 150 s post cuff deflation. The sample volume was adjusted to
171 account for vessel diameter and the entirety of blood flow through the vessel. An insonation of 60°
172 was achieved for all measurements of blood flow velocity and did not vary between participants or
173 protocols.

174 **Plasma sampling and quantification of microRNA-21 expression**

175 Blood samples were collected in standard EDTA treated vacutainers, stored on ice and processed
176 within 2 hours of collection. Samples were centrifuged for 20 min at 1900xg at 4°C to obtain plasma.
177 The extracted plasma was centrifuged for 10 min at 16000xg at 4°C, producing platelet free plasma
178 which was aliquoted and immediately frozen at -80°C.

179 Total RNA was extracted from thawed platelet free plasma and cel-miR-39 spike-in control was
180 added using a miRNeasy serum/plasma kit (Qiagen, Maryland, USA). Extracted RNA was once again
181 stored at -80°C. To quantify circulating miR-21 levels within the extracted RNA, standard reverse
182 transcription-quantitative real time polymerase chain reaction (RT-qPCR) was used with TaqMan
183 probes and primer sets (TaqMan Small RNA assays transcription kit, Applied Biosciences, Foster City,
184 USA) for miR-21 (000397), with cel-miR-39 (000200) acting as a control. A 7500 Real-Time PCR
185 system (Applied Biosystems, Foster City, USA) assessed relative quantification of miR-21 compared
186 to cel-miR-39.

187 **Analysis of data**

188 All measures of vessel diameter and blood flow velocity were assessed offline using commercial
189 automated edge detection and wall tracking software (Brachial Analyzer for Research, MIA,
190 Coralville, IA, USA). Resting diameter was determined as a mean of the diameter across the 20 s
191 recording period, peak diameter as the greatest diameter recorded following cuff deflation and
192 relative FMD as:

$$193 \quad \text{Relative FMD (\%)} = (\text{peak diameter} - \text{baseline diameter}) / \text{baseline diameter} * 100.$$

194 Peak hyperemia as the stimulus for vasodilatation following occlusion was determined as the
195 highest blood flow velocity in the first 10 s following cuff deflation, whilst area under the shear rate
196 curve from cuff release to 60 s (AUC₆₀) and 90 s (AUC₉₀) post cuff release were also calculated. Peak
197 SR was calculated as:

$$198 \quad \text{Peak shear rate (s}^{-1}\text{)} = 8 * (\text{peak hyperemia} / \text{baseline diameter}).$$

199 During the exercise protocols anterograde and retrograde SR were calculated using:

$$200 \quad \text{Shear rate (s}^{-1}\text{)} = (\text{mean blood velocity} / \text{mean diameter}) * 8.$$

201 Oscillatory Shear Index (OSI) was utilized to indicate laminar (0-0.5 a.u.) or oscillatory (> 0.5 a.u.)
202 blood flow (32, 36):

$$203 \quad \text{OSI (a.u.)} = \text{retrograde SR} / (\text{retrograde SR} + \text{anterograde SR}).$$

204 **Statistical Analysis**

205 Statistical analysis was completed using SPSS Statistics 21 (IBM, Chicago, IL, USA). Data were
206 assessed for normality using the Shapiro-Wilk test and log transformed if not normally distributed.
207 Variables measured pre-exercise and during exercise (e.g. total SR, mean SR, mean $\dot{V}O_2$, mean HR
208 etc.) were compared between protocols via a repeated measures one-way ANOVA.

209 To assess the impact of exercise protocol upon miR-21 expression and FMD and its associated
210 measures, a linear mixed model was conducted with time (pre vs. post) and protocol (CON vs. Long
211 IT vs. Short IT vs. Long IT 70) treated as fixed factors. Resting brachial artery caliber influences the
212 vasodilation of the brachial artery following FMD (1), therefore resting brachial artery diameter was
213 used as a covariate during analysis of FMD. Brachial artery diameter assessed second-by-second
214 throughout each exercise protocol did not change during exercise. Additionally, resting brachial
215 artery diameter did not differ pre- to post-exercise ($P=0.86$) or between exercise protocols ($P=0.99$;
216 *Table 1*). For assessment of miR-21 expression, pre-exercise miR-21 expression was used as the
217 covariate. Bonferroni post-hoc analysis was performed when significant effects were found. Pearson
218 correlations were used to identify relationships between normally distributed variables. All data are
219 presented as mean \pm standard deviation (SD). An *a priori* analysis using GLIMMPSE
220 (<https://glimmpse.samplesizeshop.org/#/>), revealed a sample size of 13 would be required to find a
221 difference in FMD following exercise of 3% between two of the four protocols, assuming a power of
222 0.8, alpha of 0.5 and a SD of 3.0.

223 Results

224 Shear rate patterns during exercise

225 Patterns of anterograde and retrograde SR mirrored the work rate profile of the exercise (**Figure**
226 **2A**) undertaken and were consistent with patterns of forward and decelerative blood flow, HR
227 (**Figure 3A**) and $\dot{V}O_2$ (**Figure 3B**). However, in contrast to $\dot{V}O_2$ and HR, both of which reached a
228 steady-state (CON) or pseudo-steady-state (IT) as expected during exercise in the heavy intensity
229 exercise domain (47) (**Figure 3**), anterograde SR continued to increase throughout each exercise
230 protocol (**Figure 2A I-IV**). Retrograde SR stabilized over time in each protocol following an initial
231 increase (**Figure 2A I-IV**).

232 Total, mean, maximum and minimum volume of retrograde SR did not differ between protocols
233 ($P>0.05$; **Figure 2B**). Whilst minimum anterograde SR did not differ between protocols ($P>0.05$;
234 **Figure 2B**), total, mean and maximum anterograde SR were greater in CON (total: $14 \times 10^5 \pm 4 \times 10^5 \text{ s}^{-1}$,
235 mean: $1044 \pm 297 \text{ s}^{-1}$, max: $1892 \pm 408 \text{ s}^{-1}$) than in Long IT (total: $10 \times 10^5 \pm 3 \times 10^5 \text{ s}^{-1}$, mean: 803 ± 251
236 s^{-1} , max: $1403 \pm 441 \text{ s}^{-1}$; $P<0.05$; **Figure 2B**), with mean and maximum anterograde SR in CON also
237 greater than Short IT (mean: $859 \pm 265 \text{ s}^{-1}$, max: $1584 \pm 430 \text{ s}^{-1}$; $P<0.05$; **Figure 2B**). Additionally,
238 mean and maximum anterograde SR was greater in Long IT 70 (mean: $963 \pm 224 \text{ s}^{-1}$, max: 1738 ± 435
239 s^{-1}) than in Long IT ($P<0.05$; **Figure 2B**). The pooled protocol mean HR was correlated with the pooled
240 protocol mean and total anterograde (mean: $r=0.61$, $P<0.001$; total: $r=0.57$, $P<0.001$) and retrograde
241 SR (mean: $r=-0.64$, $P<0.001$; total: $r=-0.68$, $P<0.001$).

242 **Oscillatory Shear Index**

243 Maximum and minimum OSI did not differ between the four exercise protocols ($P>0.05$; **Figure**
244 **4**). However, mean OSI was lower in CON ($0.22 \pm 0.06 \text{ a.u.}$) than in Long IT ($0.27 \pm 0.07 \text{ a.u.}$) and
245 Short IT ($0.27 \pm 0.07 \text{ a.u.}$; $P<0.05$; **Figure 4**). Importantly, a period of time with an OSI >0.5 (indicating
246 periods of purely oscillatory shear) occurred in each protocol (**Figure 4**). This time was not different
247 between protocols with a pooled protocol mean of $26.8 \pm 32.2 \text{ s}$ ($P>0.05$). An OSI >0.5 typically
248 occurred during the first 360 s of each protocol equating, to CON 69%, Long IT 61%, Short IT 49% and
249 Long IT 70 66% of the 360 s ($P>0.05$).

250 **Acute brachial artery endothelial function**

251 Following acute exercise, absolute and relative FMD were increased by $0.14 \pm 0.01 \text{ mm}$ (time
252 effect $P<0.05$; **Table 1**) and $3.36 \pm 0.48 \%$ (time effect $P<0.001$; **Table 1**), respectively, with no
253 difference between exercise protocols (time x protocol $P>0.05$). The vasodilatory stimuli recorded
254 during the FMD procedure differed pre to post exercise, with an increase in peak SR values (peak
255 hyperemia, peak SR, time to peak dilation; time effect $P<0.05$; **Table 1**) and a reduction in total
256 volume of SR (AUC_{60} ; time effect $P<0.05$; **Table 1**) although not SR AUC_{90} (time effect $P>0.05$; **Table**

257 1). These stimuli were not different between protocols (time x protocol $P>0.05$; **Table 1**). Adjusting
258 FMD for peak SR did not alter the result (data not shown).

259 **MicroRNA – 21 expression**

260 Circulating plasma levels of miR-21 reported as a percentage of cel-miR-39 showed no pre-
261 exercise differences between exercise protocols ($P>0.05$). Circulating plasma levels of miR-21 (%cel-
262 miR-39) were unaffected by acute exercise, irrespective of exercise protocol (time effect $P>0.05$;
263 time x protocol $P>0.05$; **Table 1**).

264 **Discussion**

265 This study is, to our knowledge, the first to explore a potential relationship between exercise-
266 induced SR, acute endothelial function and circulating miR-21 expression. The key findings are: 1)
267 exercise protocols produced distinct anterograde and retrograde SR patterns; 2) acute brachial
268 artery endothelial function improved following all exercise protocols; 3) expression of circulating
269 miR-21 was unaffected by exercise, regardless of the exercise-induced SR pattern. In agreement with
270 the original hypothesis, the IT exercise protocols, when matched for the same metabolic intensity as
271 CON, produced differing SR patterns resulting in a greater OSI. Importantly, and in contrast to our
272 original hypothesis, these differences in SR pattern did not differentially affect endothelial function
273 or circulating miR-21 expression.

274 **Acute endothelial function**

275 Previous studies have shown acute bouts of exercise to illicit different post-exercise FMD
276 responses; either increases, decreases or no change, as previously reviewed in detail (11). Acute
277 exercise conducted at higher exercise intensity has been seen in a previous study to lead to an early
278 decrease in post-exercise FMD, when compared to moderate intensity (3). Notably, Birk et al. (3)
279 reported that the post-exercise decrease in FMD was greatest after 30 min of cycling at 85% HR_{max}

280 but still decreased, although to a lesser extent after cycling at 70% HR_{max}. The immediate impairment
281 in endothelial function following acute high intensity exercise has been hypothesized to be a result
282 of either increased oxidative stress, substrate depletion, retrograde SR, decreased SR stimulus
283 during FMD or a reduction in EC sensitivity to SR (11). In the present study, FMD increased 15 min
284 following acute high intensity exercise irrespective of protocol.

285 In this study, the SR stimulus during FMD assessment was maintained following acute exercise and
286 whilst retrograde SR was induced during exercise, it did not have a detrimental impact upon FMD.
287 The current study did not assess EC sensitivity, substrate depletion or oxidative stress and therefore
288 determining the potential causes of differences in acute endothelial response to high intensity
289 exercise between this and previous studies is difficult. It has been purported that high intensity
290 exercise is associated with greater oxidative stress resulting in attenuation of FMD via reductions in
291 the bioavailability and production of nitric oxide (37). Antioxidant supplementation prevents FMD
292 attenuation following high intensity exercise (41), and habitual exercise training improves
293 antioxidant defense (13). This was demonstrated by Hwang et al. (23) whereby trained individuals
294 did not show an immediate decrease in FMD following acute exercise, in contrast to untrained
295 individuals. Participants in the present study were moderately well trained (mean $\dot{V}O_{2peak}$ 46.4±5.5
296 ml/kg/min), suggesting potentially high antioxidant defense resulting in increased FMD response to
297 high intensity exercise, although this was not measured. Additionally, by interspersing high work
298 rates with brief recovery periods during interval exercise, allowing both $\dot{V}O_2$ and HR to fall in the
299 recovery periods, ensured that (despite the higher work rate during IT) the exercise remained
300 remains tolerable, such that oxidative stress may have not become a factor in reducing post-exercise
301 FMD.

302 **In-exercise characterization of shear rate during CON and IT exercise**

303 At the onset of exercise, across all exercise protocols, we observed small increases in
304 anterograde SR accompanied by large increases in retrograde SR in the inactive limb, consistent with

305 previous literature (15). This pattern of response relates to brief changes in upstream and
306 downstream blood pressure gradients impacting SR during each cardiac cycle (30, 35). Indeed,
307 increased vascular tone in downstream resistance vessels may also induce retrograde SR (17), whilst
308 blood pressure changes during exercise increase sympathetic outflow in inactive muscle which has
309 previously been seen to correlate with increased brachial artery retrograde and oscillatory SR
310 following sympatho-excitatory maneuvers (35).

311 Subsequently, continuation of exercise induces a thermoregulatory response whereby the
312 microcirculation dilates leading to a reduction in downstream total peripheral resistance, altering
313 upstream blood flow and SR patterns (18, 34, 42). This thermoregulatory response reduces volumes
314 of retrograde SR, whilst further increasing anterograde SR (34, 42) leading to the more laminar SR
315 demonstrated in the present study. CON produced the greatest mean anterograde SR compared to
316 the other protocols, except Long IT 70, and the greatest total volume of anterograde SR compared
317 only to Long IT. The Short IT protocol, comprising of a high number of repetitions alternating
318 between short durations of exercise at a higher work rate and active recovery, affected the pattern
319 of SR resulting in lower mean volume of anterograde SR compared to CON. Increasing the work rate
320 during active recovery in the Long IT 70 protocol, increased peak and mean anterograde SR,
321 compared to Long IT, and more closely matched the CON protocol. Indeed, when assessing the
322 cardiorespiratory responses to CON and Long IT 70 it is evident that the protocols are closely
323 matched in terms of mean VO_2 (CON 72 ± 8 vs. Long IT 70 72 ± 9 % $\text{VO}_{2\text{peak}}$), mean HR (CON 79 ± 7 vs.
324 Long IT 70 83 ± 7 % HR_{peak}) and energy expenditure (CON 193 ± 38 vs. Long IT 70 185 ± 37 KJ). This
325 suggests that when interval exercise is manipulated to produce similar cardiorespiratory responses
326 to CON exercise, volume of SR becomes equivalent irrespective of the variable mean and pattern,
327 thus producing similar FMD responses. Thus, as the increase in FMD following an acute bout of
328 intensity-matched exercise did not differ as a result of variations in (i) SR pattern or (ii) the
329 subsequent mean in exercise SR, the similar post exercise FMD response appears to be resultant of
330 matched total SR.

331 The differences in volumes of anterograde SR between the exercise protocols resulted in
332 differing mean OSI, with CON demonstrating the lowest OSI (**Figure 4**). Purely oscillatory SR occurred
333 during the first half of each exercise protocol, consistent with previous research where the greatest
334 OSI occurred within the first 5-10 min of a 60 min CON cycling protocol (34). This has been attributed
335 to constriction of resistance vasculature in the forearm via sympathetic neural mechanisms, or other
336 circulating vasoconstrictors at the onset of exercise (34). These short time periods above an OSI of
337 0.5 in our study were not sufficient to adversely affect endothelial function, as evidenced by the
338 increase in post-exercise FMD with all exercise protocols. However, chronic exposure to episodes of
339 purely oscillatory SR may promote endothelial dysfunction and atherosclerotic lesion development
340 (10), suggesting further investigation of these exercise protocols in an exercise training setting is
341 required.

342 **Circulating microRNA-21 expression**

343 MiR-21 was chosen as a potential biomarker as it is reportedly flow sensitive and has a role in
344 regulation of target genes involved in endothelial function. In previous studies by others, human
345 umbilical vein endothelial cells (HUVECs) exposed to unidirectional SR for 24 hours demonstrated a 5
346 fold increase in miR-21 expression (48). This was associated with decreased EC apoptosis and
347 increased eNOS phosphorylation and NO production, via a 83% reduction in PTEN gene expression (a
348 negative regulator of the PI3K/Akt/eNOS signaling pathway (48)). In another study, when HUVECs
349 were exposed to oscillatory SR for 24 hours there was a 3 fold upregulation in miR-21 expression,
350 with peak expression (10 fold increase) occurring following 6 hours of exposure, leading to the
351 promotion of a pro-atherogenic EC phenotype reportedly via inhibition of PPAR α (50). Short
352 duration (30 min) exposure of HUVECS to oscillatory and pulsatile SR resulted in no change or a
353 decrease in miR-21 expression, respectively (50). Studies using short duration exercise as a stimulus
354 have reported an approximately 2 fold upregulation in circulating miR-21 following a maximal
355 exercise test (<20 min duration)(2), reductions in circulating miR-21 expression 30 min following 4 x

356 4min interval exercise (26) and no effect immediately, 1 hour and 3 hours following a period of 60
357 min continuous aerobic exercise (32). The differing responses observed in these studies may be due
358 to different sites used for blood sampling, lack of standardized participant preparation i.e. fasted or
359 not, diverse intensities and/or differing shear patterns produced from the varying exercise regimes.
360 The present study attempted to establish the miR-21 response to acute exercise by controlling
361 exercise intensity and manipulating the shear rate patterns. However, despite evidence from
362 previous studies for divergent SR mediated effects upon cultured ECs, the differing patterns of
363 exercise-induced SR in our current study did not result in any changes in expression of circulating
364 miR-21, at least at the time point we selected based on these previous studies (39).

365 SR patterns in the brachial artery differed between the exercise protocols in the present study,
366 with much greater increases in anterograde SR observed compared to retrograde SR. We have
367 observed a similar SR response in the femoral artery during acute 125 % LT CON and 60:60s INT
368 exercise, where no time spent in pure oscillatory shear was seen (unpublished data). It may thus be
369 that for acute short duration exercise at submaximal intensity the magnitude of oscillatory shear is
370 not able to differentiate miR-21 expression. Furthermore, as miR-21 is not only a regulator of EC
371 phenotype but is also highly expressed in many other cardiovascular tissues (as reviewed in detail by
372 Cheng and Zhang (8)), for example vascular smooth muscle cells, cardiomyocytes and cardiac
373 fibroblasts (8), therefore in the present study we cannot determine the cell source of miR-21. It thus
374 appears that for varying acute exercise protocols circulating miR-21 is not a viable biomarker of
375 exercise-induced SR.

376 **Limitations**

377 Pressure influences EC growth and alignment via cyclic circumferential strain, which might be
378 further increased with increased blood pressure associated with exercise (18, 28). Blood pressure
379 was not continually assessed during exercise in the current study. This should be assessed

380 continuously during exercise in future work, to yield further understanding of the mechanisms
381 governing SR patterns.

382 The assessment of miR-21 only may oversimplify the complex regulation of EC phenotype and
383 NO production pathways, particularly when assessed in the circulation. In future, a broader screen of
384 additional miRs as known regulators of EC phenotype should be assessed as potential biomarkers, in
385 combination with potential gene targets which are known to be associated with endothelial
386 function. Additionally, further work on circulating miR expression and determination of the time-
387 course of detecting circulating miR at the point of greatest expression and relevance is required
388 before it can become a viable option as a circulating biomarker of SR and endothelial function.

389 **Conclusion**

390 In conclusion, acute CON and different IT exercise protocols, matched for intensity and duration,
391 produced distinct protocol specific SR patterns. By manipulating the exercise protocols through
392 changes in work rate and the duration of the work and recovery periods, we were able to produce
393 high intensity IT exercise protocols which demonstrated acute improvements in endothelial
394 function, independent of any detectable change in circulating miR-21. This finding has implications
395 for chronic exercise training interventions, where a targeted approach to IT exercise could be used
396 for specific physiological adaptations, whilst not detrimentally impacting endothelial function. The
397 acute exercise and resultant SR patterns utilized in the present study did not affect circulating miR-
398 21 levels suggesting that in the current scenario, this miR is not a suitable biomarker of exercise
399 induced SR.

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402 **Disclosures**

403 **Author Contributions**

404 G.L. and K.B. designed these experiments. The article was written by G.L. with editorial input from
405 K.B., M.D., K.P. and C.F. Experimental research was carried out by G.L. and M.D. and analyzed by G.L.
406 and K.B. G.L. performed all of the ultrasound analysis. K.P. advised on all miR experiments.

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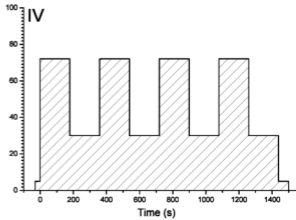
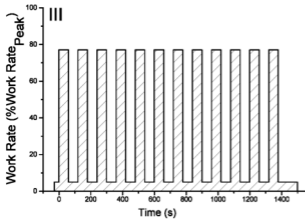
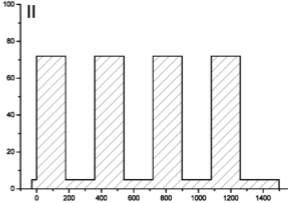
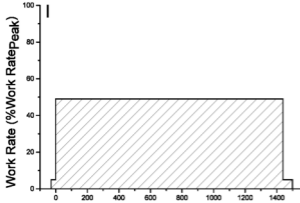
546 **Figure Legends**

547 **Figure 1:** The four exercise protocols utilized in the current study (I) CON (II) Long IT (III) Short IT and
548 (IV) Long IT 70, with relative mean work rates displayed as a percentage of the work rate peak
549 achieved during the initial ramp incremental test.

550 **Figure 2: Panel A)** Mean anterograde (black) and retrograde (grey) SR patterns for all participants
551 during the four exercise protocols (shaded area): (I) CON (II) Long IT (III) Short IT and (IV) Long IT 70.
552 **Panel B)** Mean retrograde SR (white columns) was not different between protocols ($P>0.05$).
553 However, mean (shaded columns) and maximum (▪) anterograde SR was greater in CON than in both
554 Long IT and Short IT ($P<0.05$), additionally Long IT 70 was greater than Long IT ($P<0.05$). Maximum
555 retrograde SR (=) and minimum anterograde (●) and retrograde (●) SR did not differ between
556 protocols. All data are presented as group mean \pm SD. * denotes a significant effect of exercise
557 protocol for mean and maximum anterograde SR ($P<0.05$; $n=13$).

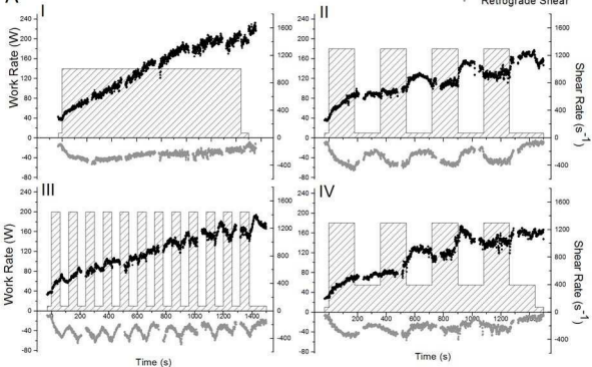
558 **Figure 3:** Panel A) Heart rate for a representative participant recorded throughout the four exercise
559 protocols. Panel B) $\dot{V}O_2$ data for the same representative participant recorded during the four
560 exercise protocols demonstrating that the exercise was within the heavy intensity exercise domain
561 (47). Heart rate peak (HR_{peak}), lactate threshold (LT) and $\dot{V}O_{2peak}$ were determined from the initial
562 ramp incremental test.

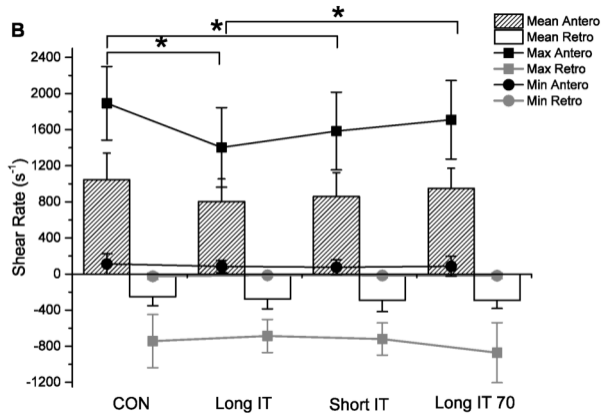
563 **Figure 4:** Mean OSI (grey columns) was lower in CON compared to both Long IT and Short IT
564 ($P<0.05$). Maximum (▪) and minimum (●) OSI were not different between protocols ($P>0.05$). In all
565 protocols periods of purely oscillatory shear were achieved as indicated by maximum OSI > 0.5 but
566 did not differ between exercise protocols ($P>0.05$). All data are presented as group mean \pm SD. *
567 denotes a significant effect of exercise protocol for mean OSI ($P<0.05$; $n=13$).

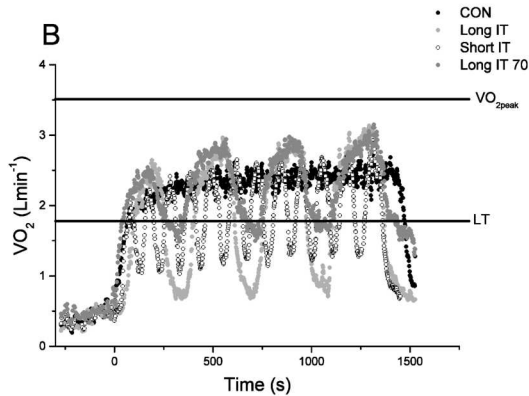
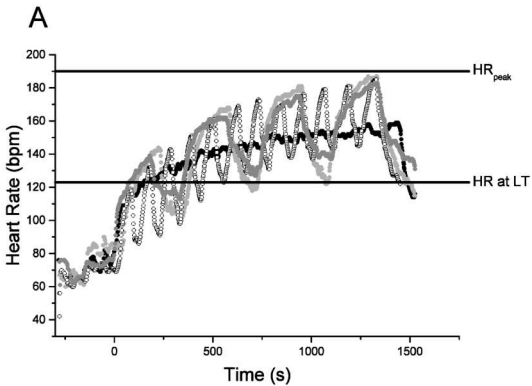


A

- Anterograde Shear
- Retrograde Shear



B



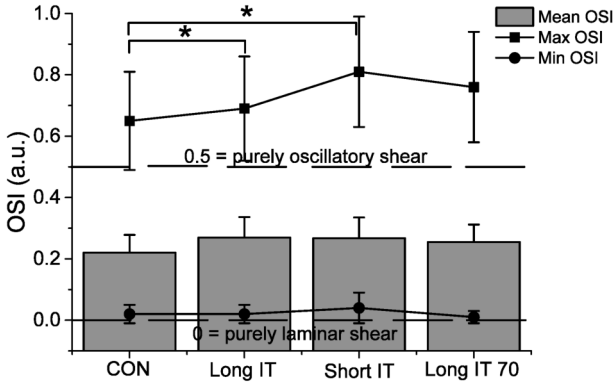


Table 1. Variables assessed during the FMD protocol at pre- and 15 min post each acute exercise bout are reported in the table. miR-21 was also assessed pre- and 6 hours post each acute exercise bout. Data reported as mean \pm SD.

	CON		Long IT		Short IT		Long IT 70		P - Values
	Pre	Post	Pre	Post	Pre	Post	Pre	Post	
Baseline diameter, mm	3.98 \pm 0.53	3.97 \pm 0.54	3.98 \pm 0.57	3.97 \pm 0.54	3.96 \pm 0.54	3.97 \pm 0.51	3.98 \pm 0.50	3.97 \pm 0.54	Time P=0.80 Interaction P=0.97
Peak diameter, mm	4.24 \pm 0.55	4.36 \pm 0.56	4.26 \pm 0.62	4.40 \pm 0.53	4.24 \pm 0.57	4.38 \pm 0.57	4.23 \pm 0.51	4.30 \pm 0.58	Time P=0.001* Interaction P=0.83
Time to Peak Diameter, s	45 \pm 22	74 \pm 33	55 \pm 27	68 \pm 40	53 \pm 24	68 \pm 31	48 \pm 14	69 \pm 31	Time P=0.001* Interaction P=0.52
Absolute FMD, mm	0.25 \pm 0.12	0.40 \pm 0.21	0.29 \pm 0.11	0.43 \pm 0.16	0.28 \pm 0.14	0.42 \pm 0.17	0.26 \pm 0.15	0.36 \pm 0.16	Time P=0.001* Interaction P=0.99
Relative FMD, %	6.40 \pm 3.02	10.24 \pm 5.33	7.27 \pm 2.46	10.98 \pm 4.84	7.23 \pm 3.55	10.54 \pm 3.97	6.63 \pm 3.05	9.24 \pm 3.87	Time P=0.001* Interaction P=0.99
Peak Hyperemia, cm/s	93.1 \pm 28.8	104.2 \pm 14.7	88.5 \pm 16.5	96.4 \pm 19.8	89.2 \pm 17.7	100.1 \pm 21.3	95.0 \pm 24.9	100.0 \pm 17.7	Time P=0.002* Interaction P=0.88
Peak Shear Rate, s⁻¹	1910 \pm 700	2124 \pm 489	1842 \pm 397	1982 \pm 560	1864 \pm 446	2049 \pm 388	1914 \pm 551	2054 \pm 482	Time P=0.002* Interaction P=0.88
AUC₆₀, a.u.	41206 \pm 11671	41353 \pm 10824	42130 \pm 8439	36899 \pm 10367	44371 \pm 8760	38431 \pm 8016	41758 \pm 13173	37081 \pm 8566	Time P=0.01* Interaction P=0.48
AUC₉₀, a.u.	58894 \pm 20133	61263 \pm 17507	61937 \pm 15001	53889 \pm 15771	62840 \pm 13783	56530 \pm 12061	60752 \pm 23066	57023 \pm 12833	Time P=0.12 Interaction P=0.28
miR-21 expression (%cel-miR-39)	16.80 \pm 24.14	7.88 \pm 7.96	11.84 \pm 23.12	11.02 \pm 23.53	6.66 \pm 23.06	18.16 \pm 26.98	8.75 \pm 3.75	6.16 \pm 2.48	Time P=0.21 Interaction P=0.32

**denotes significant time effect at P<0.05. There were no significant time by protocol interactions.*