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1 **Designing biopolymer-coated Pickering emulsions to**
2 **modulate in vitro gastric digestion: A static model**
3 **study**

4
5 **Andrea Araiza-Calahorra and Anwesha Sarkar***

6
7 Food Colloids and Bioprocessing Group, School of Food Science and Nutrition, University of
8 Leeds, Leeds, LS2 9JT, UK

9
10 *Corresponding author:

11 Dr. Anwesha Sarkar

12 Food Colloids and Bioprocessing Group,

13 School of Food Science and Nutrition, University of Leeds, Leeds LS2 9JT, UK.

14 E-mail address: A.Sarkar@leeds.ac.uk (A. Sarkar).

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26 **Abstract**

27 The aim of this study was to restrict the degree of gastric destabilization of Pickering emulsions
28 by using electrostatic deposition of a biopolymeric layer at the proteinaceous particle-laden oil-
29 water interface. Pickering emulsions (20 wt% oil) were prepared using whey protein nanogel
30 particles (WPN, $D_h \sim 91.5$ nm) (1 wt%) and the emulsions were coated by a layer of anionic
31 polysaccharide, dextran sulphate (DxS) of molecular weight (MW) of 40 or 500 kDa,
32 respectively. The hypothesis was that DxS coating on the protein nanogel particle-laden
33 interface would act as a steric barrier against interfacial proteolysis of WPN by pepsin. During
34 static in vitro gastric digestion, the droplet size, ζ -potential, microstructure (confocal
35 microscopy with fluorescently labelled dextran) and protein hydrolysis were monitored. The ζ -
36 potential measurements confirmed that 0.2 wt% DxS was sufficient to coat the WPN-stabilized
37 emulsion droplets with clear charge reversal from +35.9 mV to -28.8 (40 kDa) and -46.2 mV
38 (500 kDa). Protein hydrolysis results showed a significantly lower level of free amino groups
39 upon addition of 0.2 wt% DxS of either 40 or 500 kDa MW to the WPN ($p \leq 0.05$). Emulsions
40 coated with DxS-500 kDa presented stable droplets with lower degree of pepsin hydrolysis of
41 the adsorbed layer as compared to those coated with DxS-40 kDa or uncoated protein nanogel-
42 stabilized interface after 120 min of digestion, highlighting the importance of charge density
43 and molecular weight of the polymer coating. Insights from this study could enable designing
44 gastric-stable emulsions for encapsulation of lipophilic compounds that require delivery to the
45 intestine.

46

47

48 Keywords

49 Pickering emulsion; nanogel; whey protein; dextran sulfate, electrostatic; in vitro gastric
50 digestion

51 Abbreviations:

52 WPN: Whey protein nanogel particles; DxS: Dextran sulfate; E_{WPN}: Pickering emulsions
53 stabilized by WPN, DxS-E_{WPN}-40: Pickering emulsions stabilized by WPN and coated with
54 dextran sulfate of molecular weight (MW) 40 kDa; DxS-E_{WPN}-500: Pickering emulsions
55 stabilized by WPN and coated with dextran sulfate of MW 500 kDa.

56

57 **1. Introduction**

58 The global prevalence of obesity has nearly tripled in the last 40 years¹. Currently, one
59 of the proposed strategies to attenuate this global epidemic is food structuring to increase
60 satiety. Such strategies include designing food structures that delay the digestion of calorie-
61 dense lipids to provoke generation of satiety hormones and enhance post-meal satiation via an
62 ‘ileal brake’ mechanism²⁻⁴. Although significant attempts have been made to delay the
63 digestion of lipid-based food structures i.e. via designing model oil-in-water emulsions through
64 interfacial engineering, many if not most of these interfacial layers, are competitively displaced
65 by bio-surfactants i.e. bile salts, consequently preventing such delay⁵⁻⁷. The key conclusion
66 from these colloidal studies is that a more structurally complex and/or thicker interfacial
67 structure is needed that is resistant to this competitive displacement and at the same time not
68 readily digested by human proteolytic enzymes⁸⁻¹¹.

69 Recently, colloidal particles have been used for the interfacial design of either oil-in-
70 water or water-in-oil interfaces and these are referred to as Pickering emulsions^{12, 13}. An
71 important reason why Pickering emulsions have gained significant interest is that as opposed
72 to conventional emulsions stabilized by proteins or surfactants, Pickering emulsions are highly

73 resilient to coalescence and Oswald ripening ¹³. Such ultra-stability is given by the high
74 desorption energies (thousands of kT/particle), which makes it practically impossible to desorb
75 these particles once they are adsorbed at the interface. Thus, Pickering stabilizers are promising
76 candidates for delaying lipid digestion as there is negligible possibilities of these particles to
77 be displaced by bile salts once they have been adsorbed at the oil-water interface ^{11, 14}. For
78 example, protein microgel particles have been recently used as Pickering stabilizers for oil-in-
79 water emulsions ¹⁵. Such protein microgel particle-stabilized interfaces have been shown to
80 delay lipolysis to a certain extent by providing a transient barrier to the access of bile salts and
81 lipase ¹⁶. However, such behaviour was only observed when the gastric phase of these
82 Pickering emulsions was completely bypassed in a highly unrealistic condition and
83 consequently the effect of digestion of the protein microgel particles by pepsin was not taken
84 into account. In other words, the main drawback of these protein particle-stabilized emulsions
85 is that there is hydrolysis of the particle-laden interface by pepsin ¹⁶ under simulated gastric
86 digestion conditions ¹⁷. Peptic hydrolysis of the adsorbed protein particle layer at the interface
87 may lead to changes in emulsion microstructure and stability and thus might not be able to
88 delay lipid digestion in the later phases. Thus, the unresolved challenge is to develop particle-
89 stabilized emulsions that are protected against pepsin-induced hydrolysis in the gastric phase.

90 One approach to protect these emulsions from gastric destabilization might be
91 biopolymer coatings through the layer-by-layer (LbL) deposition methodology. The LbL
92 technique has been conventionally used to increase the stability of protein-stabilized emulsions
93 against environmental stresses, such as changes in pH, ionic strength, temperature and spray-
94 drying ¹⁸⁻²³. This technique consists of electrostatic deposition of an ionic polysaccharide onto
95 the surface of a mutually oppositely charged protein-stabilized emulsion droplet ²⁴. In addition,
96 there has also been significant progress into the use of biopolymer coatings to improve the
97 chemical stability of encapsulated components, such as digestion, release and absorption rates

98 of lipid droplets within the gastrointestinal tract (GIT) ²⁵⁻²⁸. In the domain of Pickering
99 emulsions, one study reported a particle-particle interface, where negatively-charged inulin
100 particles were electrostatically deposited on Pickering emulsions stabilized by positively-
101 charged lactoferrin nanogel particles. In this study, it was shown that the electrostatic
102 deposition of inulin particles decreased the rate and degree of hydrolysis of the lactoferrin
103 nanogel particles at the oil-water interface during gastric digestion ²⁹. Electrostatic adsorption
104 of lactoferrin-based nanoparticles or nanogel particles with polysaccharides such as pectin,
105 carrageenan and inulin nanoparticles has been previously reported ²⁹⁻³¹. Nevertheless, use of
106 biopolymer coating at particle-laden interfaces is a simple tool to delay the gastric
107 destabilization in simulated gastric condition, which has not attracted much attention in
108 literature ³⁰.

109 In our previous study, we have comprehensively characterised the use of whey protein
110 nanogel particle (WPN) as Pickering stabilizers for oil-in-water emulsions (E_{WPN}) ³². In this
111 study we aimed to understand the influence of biopolymer coating on the gastric fate of whey
112 protein nanogel-stabilized Pickering oil-in-water emulsions using the INFOGEST in vitro
113 static gastric model ³³. Whey protein isolate (WPI) was used to produce the soft solid particles
114 i.e. whey protein nanogel particles (WPN), acting as the Pickering stabilizer. To coat the
115 emulsion stabilized by WPN, dextran sulphate (DxS), which is a branched-chain
116 polysaccharide with 1–6 and 1–4 glycosidic linkage with approximately 2.3 sulphate groups
117 per glucosyl unit, of two molecular weights i.e. 40 and 500 kDa, was used. The DxS was
118 selected due to the abundance of highly negatively charged sulphate groups that will allow
119 electrostatic deposition to cationic WPN-stabilized droplets at gastric pH i.e. below the
120 isoelectric point (pI ~5.2) of whey protein. We hypothesize that DxS coating on the protein
121 nanogel particle-laden interface would act as a steric barrier against interfacial proteolysis by
122 pepsin and the barrier properties will depend on the molecular weight of the DxS used. A

123 combination of complementary techniques, such as light scattering, zeta-potential, confocal
124 microscopy (with fluorescently-labelled DxS), protein hydrolysis using sodium dodecyl
125 sulphate polyacryl amide gel electrophoresis (SDS-PAGE) of the adsorbed layer and
126 standardized ortho-phthaldialdehyde (OPA) assay were used to test the above-stated
127 hypothesis.

128

129 **2. Materials and methods**

130 2.1. Materials

131 Whey protein isolate (WPI) with $\geq 90\%$ protein content was gifted from Fonterra Co-operative
132 Group Limited (Auckland, New Zealand). Porcine pepsin (P7000, measured enzyme activity:
133 371 U mg^{-1} using haemoglobin as substrate), dextran sulphate sodium salt (DxS) of molecular
134 weight (MW) 40 and 500 kDa containing 15–19% and 16–19% of sulphur content,
135 respectively, and fluorescein isothiocyanate (FITC)-labelled dextran sulphate (MW 40 and 500
136 kDa) were purchased from Sigma-Aldrich Company Ltd, Dorset, UK. Sodium chloride,
137 sodium hydroxide, sodium phosphate monobasic monohydrate, sodium phosphate dibasic
138 anhydrous and hydrogen chloride were purchased from Thermo Fisher Scientific,
139 Loughborough, UK. The lipid phase consisted of medium-chain triglyceride (MCT-oil)
140 Miglyol[®] 812 with a density of 945 kg m^3 at $20 \text{ }^\circ\text{C}$ (Cremer Oleo GmbH & Co, Germany).
141 Sodium dodecyl sulphate polyacrylamide gel electrophoresis (SDS-PAGE) reagents including
142 Mini-Protean Precast TGX gels (8–16%) and Precision Plus Protein All Blue Standards were
143 purchased from Bio-Rad (Bio-Rad Laboratories Ltd., Richmond, CA, USA). All reagents were
144 of analytical grade and used without further purification unless otherwise reported. All
145 solutions were prepared with Milli-Q water with a resistivity of $18.2 \text{ M}\Omega \text{ cm}$ at $25 \text{ }^\circ\text{C}$ (Milli-
146 Q apparatus, Millipore, Bedford, UK). Sodium azide (0.02 wt %) was added as a preservative.

147

148 2.2. Preparation of whey protein nanogel particles (WPN)

149 The whey protein nanogel particles (WPN) were produced based on modification of a
150 previously developed top-down technique^{16, 29}. The WPI powder (10 wt%) was dissolved in
151 10 mM phosphate buffer at pH 7.0 for 2 hours to ensure complete dispersion. The WPI solution
152 was heated in a temperature-controlled water bath at 90 °C for 30 min to form a heat-set gel
153 (quiescent), followed by cooling down for 15 min and storage at 4 °C overnight to form heat-
154 set hydrogels. Obtained WPI gels were pre-homogenized with phosphate buffer (5 wt%) using
155 a hand blender (HB724, Kenwood) for 1 minute and transferred to a vacuum box (John Fraser
156 and Sons Ltd, London, UK) for degassing. The resulting 5 wt% whey protein gel was passed
157 through a Leeds Jet homogenizer, a bespoke two-chamber homogenizer developed in the
158 School of Food Science and Nutrition (University of Leeds, Leeds, UK) at 300 bars for two
159 passes, respectively. Final whey protein nanogel particles (WPN) were diluted with buffer to
160 the desired protein concentration for the emulsion preparation.

161

162 2.3. Preparation of Pickering oil-in-water emulsions

163 **Whey protein nanogel-stabilized emulsions (E_{WPN})**. Pickering oil-in-water emulsions were
164 prepared using MCT-oil (20 wt%) and a protein content of 1 wt% in the final emulsion. Briefly,
165 coarse E_{WPN} (20:80 w/w) droplets were prepared using Ultra Turrax T25 homogenizer (IKA-
166 Werke GmbH & Co., Staufen Germany) at 13, 500 rpm for 1 min. Following this, the coarse
167 emulsions were homogenized using Leeds Jet homogenizer (School of Food Science and
168 Nutrition, University of Leeds, UK) at 300 bars using two passes to prepare fine E_{WPN} droplets.

169

170 **Whey protein nanogel-stabilized emulsion coated with dextran sulphate (DxS-E_{WPN})**. Two
171 types of emulsions of dextran sulphate (DxS)-coated Pickering emulsions (DxS-E_{WPN}) were
172 produced by mixing E_{WPN} at pH 3.0 (40 wt% MCT, 2.5 wt% WPN in aqueous phase) produced

173 using afore-mentioned method, with aqueous dispersions of DxS of 40 kDa or 500 kDa, while
174 maintaining the pH at pH 3.0. For confocal laser scanning microscopy, another set of samples
175 were prepared using Fluorescein isothiocyanate (FITC)-labelled DxS of 40 kDa or 500 kDa.
176 The biopolymer solutions were prepared by dissolving the powdered DxS of desired MW into
177 Milli-Q water (pH 3.0), and stirring overnight at 21 °C to ensure dissolution. The E_{WPN} and
178 aqueous dispersions of DxS were mixed in 1:1 w/w to produce DxS-E_{WPN} (20 wt% MCT, 1
179 wt% WPN) with different concentrations of DxS-40 kDa or DxS-500 kDa (0.05-1 wt%), pH
180 was readjusted to pH 3.0 using 1.0 M HCl and samples were stirred for 2 hours at 25 °C to
181 allow electrostatic deposition of DxS to the E_{WPN} droplets. Hereafter, the emulsions named as
182 DxS-E_{WPN}-40 and DxS-E_{WPN}-500 represent the polymer-coated emulsions containing DxS of
183 MW, 40 kDa or 500 kDa, respectively.

184

185 2.4 In vitro gastric digestion of particles and emulsions

186 The aqueous dispersions of WPN, WPN+DxS-40 kDa and WPN+DxS-500 kDa, respectively
187 and the corresponding emulsions i.e. E_{WPN}, DxS-E_{WPN}-40 and DxS-E_{WPN}-500 were digested
188 using slightly adapted digestion protocol³³, i.e. without the simulated oral phase considering
189 that neither WPN nor DxS are susceptible to α -amylase. Briefly, 10 mL of pre-incubated
190 sample (37 °C, 1 h) at pH 3.0 was mixed with 10 mL of simulated gastric fluid (SGF),
191 consisting of 0.257 g L⁻¹ of KCl, 0.061 g L⁻¹ of KH₂PO₄, 1.05 g L⁻¹ of NaHCO₃, 1.38 g L⁻¹ of
192 NaCl, 0.0122 g L⁻¹ of MgCl₂(H₂O)₆, 0.024 g L⁻¹ of (NH₄)₂CO₃ and 2000 U/mL pepsin at pH
193 3.0. The mixture was incubated for 2 h at 37 °C under agitation using a shaking water bath
194 (Grant Instruments Ltd, Cambridge, UK). As control, samples were also subjected to SGF
195 treatment without added pepsin i.e. SGF buffer. During the gastric phase, samples were
196 periodically withdrawn from the sample-SGF mixture at 5, 30, 60, 90, 120 and 150 min for
197 size, charge, microscopy and SDS-PAGE analysis. Proteolysis of the samples was terminated

198 by neutralizing to pH 7.0 using freshly prepared 1 M NH_4HCO_3 except for size and charge
199 measurements, in latter experiments, samples were characterized immediately after digestion.

200

201 2. 5 Particle size and droplet size distribution

202 The physicochemical properties and stability of aqueous dispersions of WPN+DxS-40 kDa and
203 WPN+DxS-500 kDa, respectively and their corresponding emulsions i.e. E_{WPN} , $\text{DxS-}E_{\text{WPN-40}}$
204 and $\text{DxS-}E_{\text{WPN-500}}$ before and after digestion were monitored using their particle size
205 distribution, ζ -potential and microstructural changes as a function of gastric digestion time.

206 Particle size of the aqueous dispersions of WPN, WPN+DxS-40 kDa and WPN+DxS-500 kDa,
207 respectively was determined using dynamic light scattering (DLS) at 25 °C using a Zetasizer
208 Nano-ZS (Malvern Instruments, Malvern UK) in a PMMA standard disposable cuvette.

209 Particle size of the samples before and after gastric digestion was measured after diluting the
210 samples in SGF buffer (pH 3.0). Droplet size distributions of the three Pickering emulsion
211 samples i.e. E_{WPN} , $\text{DxS-}E_{\text{WPN-40}}$ and $\text{DxS-}E_{\text{WPN-500}}$ were determined using static light
212 scattering at 25 °C using Malvern MasterSizer 3000 (Malvern Instruments Ltd, Malvern,
213 Worcestershire, UK). The refractive index of the MCT (Miglyol® 812 oil) and the dispersion
214 medium were set at 1.445 and 1.33, respectively. The absorbance value of the emulsion
215 droplets was 0.001. The mean particle size distribution of the emulsions was reported as
216 volume mean diameter (d_{43}) and surface mean diameter (d_{32}) based on five measurements on
217 triplicate samples.

218

219 2.9. ζ -potential

220 The ζ -potential of aqueous dispersions of WPN, WPN+DxS-40 kDa and WPN+DxS-500 kDa,
221 respectively and their corresponding emulsions i.e. E_{WPN} , $\text{DxS-}E_{\text{WPN-40}}$ and $\text{DxS-}E_{\text{WPN-500}}$
222 before and after digestion was determined using a particle electrophoresis instrument

223 (Zetasizer, Nano ZS series, Malvern Instruments, Worcestershire, UK). Samples were diluted
224 in SGF buffer (pH 3.0) (0.1 wt% particle or 0.002 wt% emulsion droplet concentration) and
225 added to a folded capillary cell (Model DTS 1070, Malvern Instruments Ltd., Worcestershire,
226 UK). Samples were equilibrated for 1 min and the data was processed using the Smoluchowski
227 model. The ζ -potential results were reported as mean result of at least five reported readings
228 made on triplicate samples.

229

230 2.6. Confocal scanning laser microscopy (CLSM)

231 The microstructure of the Pickering emulsions i.e. E_{WPN} , $DxS-E_{WPN-40}$ and $DxS-E_{WPN-500}$ was
232 observed before and after the gastric digestion experiments using a Zeiss LSM 880 inverted
233 confocal microscope (Carl Zeiss MicroImaging GmbH, Jena, Germany). A stock solution of
234 Nile Red (1 mg/ mL in dimethyl sulfoxide, Sigma-Aldrich) was used to stain the MCT-oil to a
235 final concentration of 0.02 mg mL⁻¹ and a stock solution of Fast Green (1 mg mL⁻¹ in Milli-
236 Q water) was used to stain the WPN to a final concentration of 0.1 mg mL⁻¹. Fluorescein
237 isothiocyanate (FITC)-labelled-DxS of 40 kDa or 500 kDa was used to image $DxS-E_{WPN-40}$
238 and $DxS-E_{WPN-500}$, respectively, where FITC-DxS was used during the emulsion preparation
239 process. The emulsion samples were placed on a concave confocal microscope slide, secured
240 with a glass coverslip and finally imaged using an oil immersion 40× lens. The pinhole
241 diameter was maintained at 1 Airy Unit to filter out majority of the light scattering. Nile Red
242 was excited at a wavelength of 488 nm, Fast Green at 633 nm and FITC-DxS at 495 nm. The
243 emission filters were set at 555 - 620 nm for Nile Red, 660 - 710 nm for Fast Green and 450 –
244 520 nm for FITC-DxS.

245

246 2.7 Quantification of protein hydrolysis

247 Protein hydrolysis was quantified using the standardized ortho-phthaldialdehyde (OPA)
248 method, as described by ³⁴ with minor modifications. Briefly, OPA reagent consisted of 3.81 g
249 sodium tetraborate, 0.088 g dithiothreitol and 0.1 g sodium docecyl sulphate. Exactly, 0.080 g
250 OPA was dissolved in 2 mL ethanol and added to the above-mentioned solution and made up
251 to 100 mL with Milli-Q water. The solution was kept in the dark. Absorbance at 340 nm was
252 measured, using a UV-VIS spectrophotometer (6715 UV/VIS Spectrophotometer, Jenway,
253 UK) blanked with OPA reagent and Milli-Q water. Quantification of protein hydrolysis was
254 performed by using a reference calibration curve of L-leucine solution (0 - 200 μ M). Exactly,
255 160 μ L of standard solutions were added to 1200 μ L OPA reagent in a PMMA cuvette, mixed
256 for 5 seconds and absorbance was measured after standing for 2 min. The same procedure was
257 applied to the samples. The protein hydrolysis was expressed as a μ M free amino groups per
258 mass of the total protein in sample.

259

260 2.8 Sodium dodecyl sulphate polyacrylamide gel electrophoresis (SDS-PAGE)

261 The protein composition of the aqueous dispersions of WPN, WPN+DxS-40 and WPN+DxS-
262 500, respectively and corresponding absorbed phases of the emulsion droplets (E_{WPN} , DxS-
263 $E_{\text{WPN-40}}$ and DxS- $E_{\text{WPN-500}}$) after gastric hydrolysis by pepsin was examined using SDS-
264 PAGE under reducing conditions. The WPN-SGF, WPN+DxS-40 kDa-SGF or WPN+DxS-
265 500 kDa-SGF mixtures (1.5 mL) after gastric digestion with pepsin were mixed with SDS
266 buffer (0.5 M Tris, 2.0% SDS, 0.05% β -mercaptoethanol, pH 6.8), at a 1:2 ratio (sample : SDS
267 buffer), heated at 95 °C for 5 min and 10 μ L was loaded into precast gels placed on a Mini-
268 PROTEAN II system (Bio-Rad Laboratories, Richmond, CA, USA). 5 μ L of protein molecular
269 weight marker was added in the first lane. After running the gel at 100 V for an hour, the gel
270 was stained for 120 min with a Coomassie Brilliant Blue R-250 solution in 20% isopropanol.

271 The gels were destained overnight in Milli-Q water and scanned using a ChemiDoc™ XRS +
272 System with image Lab™ Software (Bio-Rad Laboratories, Richmond, CA, USA).

273 For measuring the composition of adsorbed phase in case of E_{WPN}, DxS-E_{WPN}-40 or
274 DxS-E_{WPN}-500, the emulsion–SGF mixtures (1.5 mL) after digestion and termination of the
275 pepsin-induced hydrolysis were collected at specific time points and centrifuged for 40 min at
276 4,000 g at 20 °C using an Eppendorf centrifuge (Thermo Scientific, Waltham, MA). The cream
277 layer was collected carefully and a certain amount of cream was then mixed with SDS buffer
278 at a sample : SDS buffer ratio of 1:4, heated at 95 °C for 5 min with 10 µL of sample loaded
279 and the SDS-PAGE experiment was conducted. The intensities of the protein bands were
280 quantified using Image Lab Software Version 6.0. Bands within the lanes was selected
281 automatically by the software to cover the whole band. Background intensity was subtracted
282 after scanning an empty lane. The percentage composition of each sample was determined by
283 scanning the gradual reduction in peak volume intensity for each intact protein bands of WPI
284 (β -lactoglobulin (β -lg), α -lactalbumin (α -la) and bovine serum albumin (BSA)). The SDS
285 PAGE experiments were carried out in triplicates and band intensities was reported as an
286 average of three reported readings.

287

288 2.8. Statistical analysis

289 Mean and standard deviation were calculated from three individual measurements performed
290 on triplicate samples and analysed using the one-way analysis of variance (ANOVA) and
291 Student's t-test where significance was accepted at $p < 0.05$.

292

293 **3. Results and discussion**

294 3.1 Optimization of the biopolymer-coated Pickering emulsions

295 Firstly, the influence of pH on the ζ -potential of WPN, DxS-40 kDa and DxS-500 kDa was
296 examined (Supplementary Fig. S1). The ζ -potential of the WPN went from being highly
297 positive to highly negative as the pH was increased from 2.0 to 7.0 due to the protonation of
298 the ionisable groups as they move from above to below the isoelectric point, respectively
299 (Supplementary Fig. S1). On the other hand, the ζ -potential of the DxS was negative at all pH
300 values examined within the experimental window (supplementary Fig. S1). The magnitude of
301 the negative charge of the low MW DxS-40 Da was smaller as compared to that of the high
302 MW DxS-500 kDa ($p < 0.05$), which is expected owing to the charge densities of the sulphate
303 groups per unit of the dextran molecule being proportional to the MW of the biopolymer.

304 Secondly, we examined the influence of MW and concentration of DxS on the droplet size
305 and charge of emulsions stabilized by WPN (Fig. 1). At pH 3.0, the ζ -potential of the E_{WPN} was
306 highly positive since WPN is below its isoelectric point (supplementary Fig. S1). As the
307 biopolymers were added, there was a significant reduction in net ζ -potential values. Upon
308 adding 0.1 wt% DxS-40 kDa or DxS-500 kDa, the net charge almost reduced to zero
309 particularly in case of DxS- E_{WPN} -40 (Fig. 1a1) whilst some positive charge remained in case
310 of DxS- E_{WPN} -500 (Fig. 1a2). This suggests that the coverage by DxS was incomplete at such
311 low concentration. When the DxS concentration was increased to 0.2 wt%, the ζ -potential
312 values of the DxS- E_{WPN} -40 or DxS- E_{WPN} -500 droplets showed a charge reversal from positive
313 to negative values, highlighting that electrostatic interaction was sufficient between WPN-
314 laden interface and DxS, irrespective of the MW. This result was attributed to the electrostatic
315 deposition of anionic groups of the biopolymers onto the cationic surface of the protein-
316 stabilized droplets³⁵⁻³⁸. The net charge reached a plateau at ≥ 0.2 wt% DxS, which suggests
317 that the anionic DxS had fully saturated the surface of cationic E_{WPN} droplets, with DxS-40
318 having lower magnitude of ζ -potential as compared to DxS-500, as discussed before.

319 Droplet size measurements indicated that addition of DxS increased the volume-
320 average mean diameter (d_{43}) of the DxS- E_{WPN-40} droplets, which ranged from 6.84 to 98.4 μm
321 (Fig. 1b1), whereas for DxS- $E_{WPN-500}$ droplets, the d_{43} ranged from 6.84 to 58.9 μm (Fig. 1b2).
322 These observations suggests droplet flocculation due to the formation of polymeric bridges
323 between anionic DxS adsorbed to WPN-laden interface and some cationic patches in the
324 surface of the neighbouring uncoated E_{WPN} droplets³¹. In addition, these flocculated droplets
325 were not easily disrupted by the dilution or shear effects within the static light scattering (SLS)
326 equipment. Interestingly, at an optimum concentration of 0.2 wt% DxS (Fig. 1c1 and 1c2), the
327 droplet size distribution became smaller with shrinkage in the more prominent peak in the size
328 range of 10-1000 μm to 1-100 μm . This suggests that on adding higher amounts of DxS, a
329 reduction in the droplet flocculation and electrostatic stabilization of the droplets was observed,
330 as corroborated by the charges on the electrical charge observed in Fig. 1a1 and 1a2. Since 0.2
331 wt% of anionic DxS was the minimum concentration needed to completely coat the cationic
332 E_{WPN} droplets at pH 3.0, irrespective of the MW of DxS, resulting in negatively charged DxS-
333 E_{WPN-40} or DxS- $E_{WPN-500}$ emulsion droplets (Fig. 1a1 and 1a2), this concentration was
334 selected for the preparation of the DxS- E_{WPN-40} or DxS- $E_{WPN-500}$ droplets.

335

336 3.2 In vitro gastric digestion of aqueous dispersions of WPN and DxS+ WPN

337 Firstly, we determined the behaviour of the aqueous dispersions of WPN in absence and
338 presence of 0.2 wt% DxS-40 kDa or DxS-500 kDa, respectively (Fig. 2, 3 and supplementary
339 Table S1 and supplementary Fig. S2 and S3). This sets the scene to understand how the particles
340 might behave when present in the continuous phase of the respective emulsions and compare
341 it when they are present at the adsorbed phase. To determine the behaviour of the aqueous
342 dispersion of WPN in presence or absence of DxS in the in vitro gastric digestion model,
343 changes in their physiochemical properties and protein composition were examined as a

344 function of digestion time. As controls, an aqueous dispersion of 1 wt% WPN and 1wt% WPN
345 in presence of 0.2 wt% DxS-40 kDa or DxS-500 kDa in SGF without pepsin were also analysed
346 (supplementary Table S2).

347 **WPN.** At pH 3.0, WPN had a hydrodynamic diameter of 91.5 nm and a ζ -potential of
348 +30.2 mV (supplementary Table S1). Formation of WPN during the heat treatment is the result
349 of the association of small aggregates via hydrophobic, electrostatic and disulphide bonds ³⁹.
350 After addition of SGF buffer (pH 3.0) without pepsin, changes in ζ -potential were not
351 significant ($p > 0.05$) (see time zero in Supplementary Fig. S2). Upon gastric incubation in
352 SGF containing pepsin, the size distribution of the particles became multi-modal and it was no
353 longer possible to measure the hydrodynamic diameter using DLS as the particle size was too
354 polydisperse to be considered for Rayleigh fitting (data not shown). This indicates that WPN
355 was hydrolysed by pepsin and created different sizes of particle aggregates. As can be
356 expected, a significant decrease in the ζ -potential value was also observed within the first 15
357 min of digestion, which remained fairly constant at $\sim +20$ mV even after 2 h (supplementary
358 Fig. S2).

359 The results are in agreement with the protein hydrolysis monitored using SDS-PAGE
360 (Fig. 2a1 and b1). It can be observed that, after just 5 min of incubation, the intensity of the
361 bands corresponding to the major whey proteins i.e. β -lactoglobulin (β -lg), α -lactalbumin (α -
362 la) as well as bovine serum albumin (BSA) bands was reduced considerably (remaining intact
363 proteins were 24%, 19.27% and 0%, respectively), with simultaneous appearance of a mixture
364 of peptides with molecular weights < 10 kDa after 2 h incubation (Fig. 2a1). These results can
365 be explained in terms of temperature-induced conformational changes in the whey protein
366 structure. In native state, β -lg (the major protein in whey protein isolate) has most of the
367 hydrophobic amino acids buried inside the β -barrel structure making them not easily accessible
368 to pepsin, which makes native β -lg resistant to pepsin hydrolysis ⁴⁰. Upon heating, unfolding

369 of the protein molecule exposes the hydrophobic amino acids, making it highly susceptible to
370 hydrolysis by pepsin⁴¹. From our results it is evident that the thermal treatment during WPN
371 preparation exposed the hydrophobic amino acids, which were not refolded during the particle
372 formation making them more accessible to pepsin hydrolysis during gastric incubation as
373 compared to native WPI.

374 **WPN+DxS.** At pH 3.0, aqueous dispersions of WPN containing either DxS-40 kDa or
375 DxS-500 kDa had highly negative ζ -potential values of -21.6 mV and -37.4 mV, respectively,
376 which suggest that the DxS saturated the surface of cationic WPN (Supplementary Table S1).
377 Addition of DxS caused particle aggregation irrespective of the MW, and it was not possible
378 to measure the hydrodynamic diameter using DLS (supplementary Fig. S3b and S3c).

379 Presence of SGF without pepsin did not showed significant ($p < 0.05$) changes in the
380 ζ -potential for both 40 and 500 kDa DxS (-37.7 and -40.5 mV, respectively) (see time zero in
381 supplementary Fig. S2). During gastric incubation with pepsin, the magnitude of ζ -potential of
382 the particles was reduced from -37.7 mV to a constant value ranging between -4.4 and +2.2
383 mV for 40 kDa DxS samples (Supplementary Fig. S2). The ζ -potential of the WPN+DxS-500
384 kDa particles was more negative than that of the WPN+DxS-40 kDa and was reduced from -
385 40.5 mV to a constant value ranging between -15.7 and -22.3 mV, during the 120 min of gastric
386 incubation (Supplementary Fig. S2). The most likely explanation for this effect is that there
387 was electrostatic screening of charge of the biopolymer-coated particles by the SGF buffer, as
388 can be corroborated by the control samples subjected to the SGF without pepsin
389 (supplementary Table S2).

390 The SDS-PAGE electrograms of WPN+DxS for both biopolymers are shown in Figs.
391 2a2 and 2a3. It can be seen that for both biopolymers i.e. DxS-40 kDa or DxS-500 kDa, the β -
392 Ig bands remained relatively resistant to pepsin hydrolysis as compared to that of WPN alone
393 (Fig. 2a1). Particularly, it can be observed that the band corresponding to α -la protein remained

394 resistant to pepsin hydrolysis for DxS-500 kDa, with a clear band still present after up to 2.5 h
395 incubation in SGF (Fig. 2a3). Quantification of the SDS-PAGE gel bands (Figs. 2b2 and 2b3)
396 suggests that in presence of DxS-40 kDa, the proportion of β -lg and α -la decreased to 11.47%
397 and 0.25%, respectively after 2 h of incubation (Fig. 2b2). As for DxS-500 kDa, the proportion
398 of intact protein bands were much higher, with 27.70% of β -lg and 14.88% of α -la remaining
399 after 2 h of incubation (Fig. 2b3).

400 In addition, the free amino group (NH_2) content was determined by OPA method for
401 the WPN and WPN after addition of 0.2 wt% DxS of 40 and 500 kDa before and after gastric
402 digestion with added pepsin and shown in Fig. 3. The concentration of free NH_2 increased
403 generally with digestion time for all samples. Results indicated that for WPN, there was an
404 increase in the proteolysis profile in the first 30 min gastric digestion from 989.97 mM NH_2/g
405 to 3,747 mM NH_2/g , after which it levelled off to values between 3,747–4088.66 mM NH_2/g
406 during the 120 min gastric digestion. These values are in agreement with previously
407 reported hydrolysis of different whey proteins^{42, 43}. Levels of proteolysis were
408 significantly ($p < 0.05$) lower after addition of DxS. For lower molecular weight DxS (40 kDa),
409 after 30 min gastric digestion, the free NH_2/g concentration was 3,105.88 mM NH_2/g (as
410 compared to 3,747 mM NH_2/g in WPN) with a relatively constant value between 3,105.88 –
411 3,808.97 mM NH_2/g during the 120 min (Fig. 3). The proteolysis profile for DxS of higher
412 molecular weight of 500 kDa was 771.01 mM NH_2/g in the first 30 min with values between
413 771.01 – 2,752.21 mM NH_2/g after the 120 min gastric digestion, clearly indicating the barrier
414 effect of DxS-500 kDa on proteolysis of WPN.

415 A possible explanation from the increased protection to WPN upon DxS addition might
416 be related to the aggregation state of the particles, i.e. DxS was aggregating the WPN particles
417 limiting the access of pepsin to the peptic cleave sites of WPN. In addition, the higher extent
418 of protection to WPN against proteolysis by DxS-500 kDa as compared to that of DxS-40 kDa

419 may arise from a combination of high ζ -potential values, and/or the MW (degree of branching)
420 that somehow physically inhibited the enzyme to reach the hydrophobic moieties of the protein
421 nanogel particles. These results are in agreement with a previous study that have reported
422 increased resistance to gastric proteolysis during first 10 min of simulated gastric conditions of
423 lactoferrin nanoparticles, when coating these particles with low methoxyl pectins as compared
424 to that of high methoxyl pectins. The increased gastric resistance was largely associated with
425 the increased electro-kinetic charge of the former ³⁰. Overall, these results suggest that the
426 extent of the protective effect of DxS-500 kDa was markedly higher than that of DxS-40 kDa
427 in the bulk phase and it would be interesting to see whether such effects exist when DxS coats
428 the WPN-stabilized droplets at the surface.

429

430 3.3 Physicochemical and microstructural characterization of E_{WPN} , DxS- E_{WPN} -40 and DxS-
431 E_{WPN} -500 during in vitro gastric digestion

432 Pickering emulsion samples with or without the biopolymer coating of 0.2 wt% DxS were
433 prepared at pH 3.0, subjected to in vitro gastric model (SGF, pH 3.0) at 37 °C and then the
434 droplet size, charge, and microstructure were measured as a function of digestion time (Figs. 4
435 and 5). In addition, as controls, E_{WPN} , DxS- E_{WPN} -40 and DxS- E_{WPN} -500 in SGF without pepsin
436 were also analysed (Supplementary Fig. S3).

437 E_{WPN} . Freshly prepared E_{WPN} at pH 7.0 presented a bimodal droplet size distribution
438 with the droplet population in the peak area of 0.1-1.0 μm corresponding to the unadsorbed
439 WPN and the population in the peak area of 10-100 μm corresponding to the emulsion droplets
440 (Fig. 4a1). The mean droplet diameter (d_{43}) was 9.61 μm and the droplets presented a highly
441 negative charge of -26.70 mV, because the adsorbed layer of WPN was above its pI (data not
442 shown). Confocal images of the E_{WPN} shows the WPN particles (stained green by Fast Green)
443 clearly adsorbed on the surface of the oil droplets (stained by Nile Red) (Fig. 4a1). Upon

444 decreasing the pH to gastric pH 3.0, the droplet size distribution and the volume average mean
445 diameter (d_{43}) were not significantly changed ($p > 0.05$) (Fig. 4a1 and Table 1), but the droplets
446 presented a charge reversal to a highly positive charge of +35.9 mV, as the pH was below the
447 pI as previously discussed with respect to Fig. 1a1 and 1a2.

448 Incubation of E_{WPN} with SGF without pepsin did not significantly influence the droplet
449 size distribution (Fig. 4a1), mean droplet size (d_{43} 16.93 μm) and ζ -potential of the droplets
450 (see time zero in Fig. 4b1), indicating that E_{WPN} was stable to any aggregation under the ionic
451 environment of the gastric conditions. From the confocal images, it can be seen that the
452 emulsion droplets did not show significant aggregation (Fig. 5b1) as compared to initial
453 emulsions (Fig. 5a1). When E_{WPN} was incubated in SGF with pepsin, the mean droplet size
454 decreased from 16.93 μm to 9.72 μm within the first 5 min of gastric digestion and remained
455 fairly constant obtained over time (Fig. 4b1). The droplet size distribution, shows the
456 appearance of a population of smaller droplet size (Fig. 4a1), which was not observed in the
457 control samples (Supplementary Fig. S3). Interestingly, the ζ -potential of the droplets remained
458 fairly constant at +37.6 mV by the end of the gastric incubation (Fig. 4b1) indicating the
459 presence of enough WPN at the interface. Therefore, it can be suggested that the decrease in
460 size of the E_{WPN} with smaller sized population might have been caused by pepsin hydrolysis
461 either hydrolysing the protein at the surface of the emulsion droplets, or the particles bridging
462 different droplets. This result is in agreement with previous studies that have reported decrease
463 of d_{43} values after gastric digestion of whey protein microgel-stabilized Pickering emulsions
464 ¹⁶.

465 Looking at the confocal images, after 30 minutes incubation, the microstructure of the
466 emulsion (Fig. 4c1) changed dramatically showing very limited population of droplets. One
467 might argue it is due to the dilution effect with SGF, however that can be negated by looking
468 at the image at 0 min which had equivalent droplet concentration due to dilution with SGF

469 buffer without any added pepsin. This suggests that pepsin was hydrolysing the bridges
 470 between the WPN-coated droplets as well as was rupturing the particle-layer at the interface to
 471 a certain extent resulting in some degree of droplet coalescence. Such coalesced droplets were
 472 most likely rising to the top and thus were not visualized by the confocal microscopy resulting
 473 in reduction in droplet volume (Figs. 5c1). Confocal micrographs of the emulsion after
 474 120 min of gastric digestion provided further evidence of the appearance of individual droplets
 475 that appeared to be less aggregated emulsion droplets (Fig. 5d1) than the ones in 0 min (Fig.
 476 4b1). A thin interfacial layer around the oil droplets even after 120 min was observed in the
 477 microscopic image (Fig. 5d1) suggesting that either WPN or peptide network of WPN were
 478 still present in the emulsion droplets after the gastric digestion that were somehow protecting
 479 the droplets against coalescence.

480

481 Table 1. Droplet size and ζ -potential values for E_{WPN} , DxS- E_{WPN} -40 and DxS- E_{WPN} - at pH
 482 3.0, respectively.

	E_{WPN}		DxS- E_{WPN} -40		DxS- E_{WPN} -500	
	$d_{43} / \mu\text{m}$	ζ -potential / mV	$d_{43} / \mu\text{m}$	ζ -potential / mV	$d_{43} / \mu\text{m}$	ζ -potential / mV
pH 3.0	11.50 ± 1.20	$+35.9 \pm 0.80$	22.2 ± 0.98	-28.8 ± 1.30	38.8 ± 0.07	-46.2 ± 2.42

483

484 **DxS- E_{WPN} -40 and DxS- E_{WPN} -500.** Before digestion, biopolymer-coated emulsions
 485 containing either of the two anionic DxS (40 or 500 kDa MW) had high negative charges (-
 486 28.8 and -46.2 mV for 40 kDa and 500 kDa, respectively) at pH 3.0 (Table 1), suggesting that
 487 the biopolymer had substantially adsorbed onto the cationic WPN-stabilized oil droplets at pH
 488 3.0. Both 40 and 500 kDa DxS- E_{WPN} presented a bimodal particle size distributions (Fig. 4a2
 489 and 4a3) with a mean droplet size (d_{43}) of 22.2 and 38.8 μm , respectively (Table 1). The
 490 increase of the droplet size might result from the aggregation of the E_{WPN} droplets after addition
 491 of DxS, as reflected by the confocal images (Figs. 5 a2 and 5a3). In addition, it can also be

492 observed in Figs. 5a2 and 5a3 that FITC-labelled DxS (stained in blue) is electrostatically
493 adsorbed to the WPN particles (stained in green). At this point, it is worth mentioning that,
494 Nile Red was not used to stain the oil droplets, since both Nile Red and FITC-labelled DxS
495 possessed similar excitation wavelengths. For this reason, images were only acquired using
496 Fast green (for WPN) and FITC-DxS for visualizing the biopolymer coating. Supplementary
497 Fig. S4 shows a control image indicating that the presence of FITC-labelled DxS only records
498 the DxS and not the WPN.

499 Incubation in SGF without pepsin showed no significant ($p < 0.05$) changes in the ζ -
500 potential values and d_{43} (see time zero for Figs. 4b2 and 4b3) for DxS of both MW, confirming
501 there was no SGF-induced effects on aggregation of the droplets. The confocal images (Figs.
502 5b2 and 5b3) further confirms that the FITC-labelled DxS remained adsorbed to the WPN and
503 that the emulsion droplets sizes are in agreement with the light scattering data. After addition
504 of pepsin, there was a pronounced decrease in the magnitude of their negative charge within
505 the first 5 min of digestion, reaching a fairly constant value at longer digestion time scales
506 (Figs. 4b2 and 4b3). This negative charge is in line with the anionic DxS being bound to the
507 DxS-E_{WPN} droplets under SGF, as evidenced by the bright blue ring surrounding the emulsion
508 droplets and indicating the presence of the FITC-labelled DxS (Figs. 5c2-c3 and 5d2-d3).
509 Emulsions were stable to the gastric conditions, since there was no increase in the mean particle
510 diameter (d_{43}) (Figs. 4b2 and 4b3), and there was no evidence of coalescence in the microscopy
511 images (Fig. 5c2-c3 and 5d2- d3). Irrespective of digestion times, DxS appeared to be in the
512 same region as the WPN highlighting that the electrostatic complexation at the interface
513 remained almost unaffected in presence of pepsin. These results clearly indicate that DxS-
514 E_{WPN-40} and DxS-E_{WPN-500} emulsion droplets at gastric conditions exhibited resistance to any
515 pepsin-induced microstructural changes.

516

517 3.4 Protein composition of adsorbed phase of EWP_N, DxS-EWP_N-40 and DxS-EWP_N-500

518 during in vitro gastric digestion

519 The SDS-PAGE of the adsorbed phases of all emulsion systems, i.e. EWP_N, DxS-EWP_N-40
520 and DxS-EWP_N-500 were compared (Fig. 6). The SDS-PAGE electrograms revealed that in
521 EWP_N, the major protein constituents, β -lg and α -la, as well as BSA were identified in the initial
522 undigested emulsion (Fig. 6a1). However, upon incubation in SGF containing pepsin, within
523 the first 5 min the BSA fraction almost completely disappeared, and the proportion of the β -lg
524 and α -la fractions decreased to 55.39% and 36.19%, respectively (Fig. 6b1). These results
525 suggest that the emulsification of the WPN slightly decreased the accessibility of pepsin as
526 compared to that when WPN was freely available in aqueous dispersion (Fig. 2a1). These
527 results can be explained in terms of wetting of WPN by the oil phase that consequently reduced
528 its accessibility to pepsin. However, after 120 min of gastric incubation, both β -lg and α -la
529 bands completely disappeared, indicating complete hydrolysis of these proteins. At the end of
530 the gastric phase (2.5 h), a fuzzy thick band representing a mixture of peptides with molecular
531 weights < 10 kDa was observed in the gels (Fig. 6a1). This supports the thin particle-laden
532 interface observed in the micrographs even after 2 hours of digestion, which might be the
533 peptide remnants of nanogel particles or peptides (Fig. 5d1).

534 In contrast, the digestion pattern of the DxS-EWP_N emulsion during gastric proteolysis
535 was very different from that EWP_N (Figs. 6a1 and 6a3). In addition, it should be noted that some
536 interfacial material remained in the stacking gel. It is possible that the protein aggregates of the
537 absorbed phase were too large (>250 kDa) to enter the resolving gel. The hydrolysis pattern for
538 DxS-EWP_N-40 emulsions after 5 minutes of gastric incubation revealed that the proportion of
539 BSA decreased to 17.4%, whereas significant proportion of β -lg and α -la fractions remained
540 with intact fractions of about 48.4% and 40.3%, respectively (Fig. 6b2). After 120 min, the
541 quantity of BSA, β -lg and α -la remaining undigested was 0.12%, 11.62% and 11.88%,

542 respectively (Fig. 6b2). Confocal fluorescent microscopy images of the emulsions after 120
543 min digestion indicated the aggregated microstructure arrangement of the droplets, which may
544 also contribute to the slowed pepsin hydrolysis, since pepsin would have to diffuse through the
545 outer parts of these aggregates before it could reach the protein sites underneath these DxS
546 coating (Figs. 5c2-d2). These results suggested that the polysaccharide coating decreased the
547 digestibility of the WPN located at the interface of E_{WPN} .

548 In the case of 500 kDa DxS- E_{WPN} , a considerable amount of interfacial material was
549 also observed to remain in the stacking gel (Fig. 6a3). However, within the first 5 min of gastric
550 incubation, the BSA fraction was reduced to 95.27%, whereas the proportion of the β -lg and
551 α -lg fractions decreased to 89.70% and 94.518%, respectively (Figs. 6b3). At the end of the
552 2.5 h gastric digestion, around 83.42%, 67.50% and 73.75% of the BSA, β -lg and α -la fractions
553 remained still intact. These result are in agreement with previous studies that have reported that
554 the presence of a polysaccharide coating reduced the activity of pepsin for protein-stabilized
555 emulsions after 2 h gastric incubation^{30 44}.

556 A possible explanation for this effect could be that the formation of a more complex
557 structure increased the barrier properties of DxS+WPN and reduced the pepsin diffusion to the
558 underneath WPN-stabilized interface. Previous proteolytic studies on casein-stabilized
559 emulsions with an absorbed dextran sulphate layer have suggested that there may be an
560 associative interaction of the enzyme (trypsin) with the absorbed DxS layer, as a large increase
561 in the interfacial shear viscosity was observed⁴⁵. Thus, it seems reasonable to suppose that,
562 pepsin may be trapped or co-adsorbed within the DxS coatings, reducing the availability of
563 pepsin in the close vicinity of hydrophobic groups of WPN for potential proteolysis.
564 Consequently, we can reasonably infer that, a bigger molecular structure may impart a greater
565 barrier effects to WPN substrate against pepsin attack, which is consistent with the differences
566 in extent of hydrolysis between the two different MW of DxS used. A schematic diagram to

567 illustrate the physical state of the DxS-E_{WPN} when it is exposed to in vitro gastric conditions is
568 presented in Fig. 7. The E_{WPN} is stable in presence of SGF in absence of enzymes, but when
569 pepsin is added to the system, hydrolysis of the interfacial protein layer occurs producing
570 remnants of nanogel particle or peptides. On the contrary, hydrolysis of the interfacial protein
571 layer on the DxS-E_{WPN} is delayed by the presence of a physical barrier provided by a
572 biopolymer either by providing an electrostatically repelling layer or simply providing a steric
573 hindrance to pepsin, thus preventing gastric destabilization of the emulsion droplets.

574

575 **4. Conclusions**

576 In this study, we have studied the influence of coating of anionic dextran sulphate on the
577 physicochemical properties and digestibility of whey protein nanogel particle-coated droplets
578 under in vitro gastric conditions. Findings from this study report that the stability and degree
579 of pepsin hydrolysis of the whey protein nanogel particles at the interface is restricted in
580 presence of a secondary coating of dextran sulphate, latter could provide a steric and
581 electrostatic barrier. In addition, the molecular weight of the coating had an appreciable effect
582 on the degree of pepsin hydrolysis, with dextran sulphate of a molecular weight of 500 kDa
583 presenting a better barrier to pepsin-hydrolysis of the underlying protein nanogel particle-laden
584 interface as compared to that of the 40 kDa molecular weight within the simulated gastric
585 phase. Such results are mainly attributed to the higher negative charge density associated with
586 higher degree of sulphate groups in the higher molecular weight system or the higher order
587 molecular structure that trapped pepsin protecting the protein-laden interface against complete
588 enzymatic hydrolysis. Insights from this study could enable creating future gastric-stable
589 emulsions for food and pharmaceutical applications targeting altered lipid digestion profile in
590 the intestinal phase or encapsulation of lipophilic bioactive compounds that need to be
591 delivered to intestines without any gastric destabilization.

592

593 **5. Conflict of interest**

594 The authors declare no conflicts of interests.

595

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601

602 **7. References**

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