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Segmentation and Quantification for Angle-Closure Glaucoma Assessment in Anterior Segment OCT

Huazhu Fu, Yanwu Xu, Stephen Lin, Xiaoqin Zhang, Damon Wing Kee Wong, Jiang Liu, Alejandro F. Frangi, Mani Baskaran, and Tin Aung

Abstract—Angle-closure glaucoma is a major cause of irreversible visual impairment and can be identified by measuring the anterior chamber angle (ACA) of the eye. The ACA can be viewed clearly through Anterior Segment Optical Coherence Tomography (AS-OCT), but the imaging characteristics and the shapes and locations of major ocular structures can vary significantly among different AS-OCT modalities, thus complicating image analysis. To address this problem, we propose a data-driven approach for automatic AS-OCT structure segmentation, measurement and screening. Our technique first estimates initial markers in the eye through label transfer from a hand-labeled exemplar dataset, whose images are collected over different patients and AS-OCT modalities. These initial markers are then refined by using a graph-based smoothing method that is guided by AS-OCT structural information. These markers facilitate segmentation of major clinical structures, which are used to recover standard clinical parameters. These parameters can be used not only to support clinicians in making anatomical assessments, but also to serve as features for detecting anterior angle closure in automatic glaucoma screening algorithms. Experiments on Visante AS-OCT and Cirrus HD-OCT datasets demonstrate the effectiveness of our approach.

Index Terms—Data-driven, segmentation, AS-OCT, anterior chamber angle, angle-closure glaucoma.

I. INTRODUCTION

Glaucoma is the second leading cause of blindness worldwide (only second to cataracts), as well as the foremost cause of irreversible blindness [1], [2]. Since vision loss from glaucoma cannot be reversed, improved screening and detection methods for glaucoma are essential to preserve vision and life

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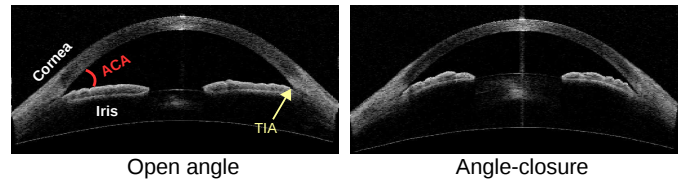


Fig. 1. The angle-closure glaucoma: open angle and angle-closure. The small anterior chamber angle (ACA) blocks drainage channels of aqueous fluid and results in optic nerve damage.

quality. The two main types of glaucoma are open angle and angle-closure, according to the configuration of the anterior chamber angle (ACA) within the eye, as shown in Fig. 1. Primary angle-closure glaucoma is a major form of glaucoma in Asia [3], in which a narrow ACA between the iris and cornea blocks the drainage channels of aqueous fluid, resulting in rising eye pressure that causes optic nerve damage [4], [5]. Imaging and assessment of the ACA is thus critical for diagnosis of angle-closure glaucoma [6], [7].

Optical Coherence Tomography (OCT) provides a clear view of intraretinal morphology and enables noninvasive depth-resolved functional imaging of the retina [8], [9], which can be widely employed to image macular edema [10], segment retinal layers [11], [12], and detect the optic disc/cup [13], [14]. Anterior Segment Optical Coherence Tomography (AS-OCT) is an effective imaging modality for visually identifying the anterior segment structure [15], [16], by obtaining high-resolution cross-sections of the entire anterior chamber in a single image [17], [18].

For wide-scale screening, automatic AS-OCT segmentation and assessment methods are. Recently, the Zhongshan Angle Assessment Program [19] provided a semi-automatic algorithm to calculate the various anterior segment parameters. But this semi-automatic method requires the observer to input the location of the two scleral spurs, which makes it unsuitable for automatic analysis of large-scale clinical datasets. Tian *et al.* provided a Schwalbe's line detection method for High-Definition OCT (HD-OCT) to compute ACA measurements [20]. HD-OCT imaging uses spectral domain technology to obtain higher resolution images in which the Schwalbe's line is well defined. But this method [20] is only valid for HD-OCT and cannot be implemented with other AS-OCT modalities with low resolution. Williams *et al.* employed level-set-based shape priors to segment the corneal anterior and posterior boundaries [22]. This method estimates the cornea location, and then utilizes the level-set-based model

TABLE I
SUMMARY OF THE EXISTING AS-OCT ASSESSMENT METHODS.

Method	Year	Automatic	Cornea Segmentation	Iris Segmentation	Clinical Measurement	Glaucoma Screening	Multiple Modalities
Zhongshan [19]	2008	Semi	✓	✓	✓	✓	Visante OCT
Tian <i>et al.</i> [20]	2011	✓	✓	×	✓	✓	HD-OCT
Xu <i>et al.</i> [21]	2012	✓	×	×	×	✓	✓
Williams <i>et al.</i> [22]	2013	✓	✓	×	×	×	✓
Xu <i>et al.</i> [23]	2013	✓	×	×	×	✓	✓
Ni Ni <i>et al.</i> [24]	2014	✓	✓	✓	✓	✓	HD-OCT
Williams <i>et al.</i> [25]	2015	✓	✓	×	×	×	✓
Niwas <i>et al.</i> [26]	2015	×	×	×	×	×	Visante OCT
Fu <i>et al.</i> [27]	2016	✓	✓	✓	✓	×	✓
Proposed method	2017	✓	✓	✓	✓	✓	✓

to segment the corneal boundary. However, this method only produces a corneal boundary segmentation without the other ACA structures. Xu *et al.* localized the ACA region, and then extracted visual features directly to classify the glaucoma subtype [21], [23]. However, that method can only report classification results and cannot provide clinical measurements needed by doctors. A comparison of the existing methods is given in Table I. In summary, common drawbacks among existing AS-OCT assessment methods include the following:

- 1) **Global Segmentation:** An AS-OCT image includes the corneal boundary and iris region, but many existing methods provide only single region segmentation (e.g., Schwalbe’s line [20] or corneal boundary [22], [25]), rather than the global structure segmentation needed for ACA measurement.
- 2) **Clinical Measurement:** In the field of medical image analysis, visual features have been shown to obtain good performance on glaucoma screening [21], [23]. However, clinical parameters defined by anatomic structure are more valuable for medical assessment and clinician validation.
- 3) **Multiple Modalities:** The imaging characteristics, as well as the location and shape of the iris and cornea, can vary significantly among different AS-OCT modalities, as shown in Fig. 2. Many existing methods are limited to only a particular type of AS-OCT image (e.g., HD-OCT [20], [24], or Visante OCT [19]), and cannot be applied directly with other types of AS-OCT imagery.

To address these issues, we propose a data-driven approach for AS-OCT structure segmentation and measurement. Our key idea is to introduce an exemplar set containing manually labeled markers on the iris and corneal boundaries, and use it to estimate initial marker locations by transferring from the exemplars most similar to the input. These exemplars include images taken from different patients and AS-OCT modalities. The initially placed markers are then refined using a graph-based smoothing model that accounts for structural information within the AS-OCT image. These refined markers are employed to guide the segmentation of major AS-OCT structures – namely the corneal boundary, iris region, and

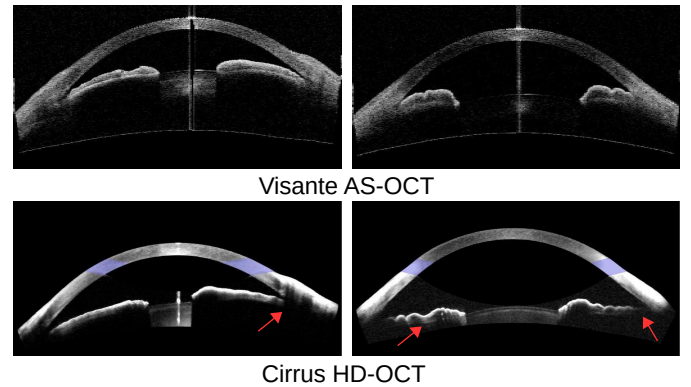


Fig. 2. Different subjects and AS-OCT modalities (e.g., Visante AS-OCT and Cirrus HD-OCT). It is observed that the iris positions and shapes are varied among different patients for the same AS-OCT modality. For different AS-OCT modalities, Cirrus HD-OCT has a clearer corneal boundary and slight noise, but the iris posterior and trabecular-iris contact (TIC) are missed, as indicated by the red arrows.

trabecular-iris contact¹ – which are used to calculate clinical parameters based on ocular anatomy. These clinical parameters are finally used for clinician assessment and angle-closure glaucoma screening.

An approach related to our method is multi-atlas segmentation [29]–[31], where an atlas dataset is built and pairwise registration is used between the input image and each atlas image. After that, these registration results are used to propagate the atlas labels to the input image coordinates. Our method has the following differences to multi-atlas segmentation: 1) our method employs labeled raw images to generate the exemplar dataset, allowing for easy addition of new images into the dataset; 2) our method uses K -nearest neighbor retrieval to replace pairwise registration, providing higher computational efficiency; 3) to our knowledge, our work is the first application of a data-driven scheme for AS-OCT image analysis.

The proposed approach is fully automatic and encompasses AS-OCT segmentation, measurement and screening. A major advantage is that its data-driven scheme provides robust performance over the imaging variations among different AS-OCT modalities as well as over various iris shapes among different

¹Note that due to low resolution, it has been found that the scleral spur is not identifiable in 20-30% of Visante AS-OCT images [28]. Thus we employ the trabecular-iris contact as an alternative biomarker that is located very close to the scleral spur.

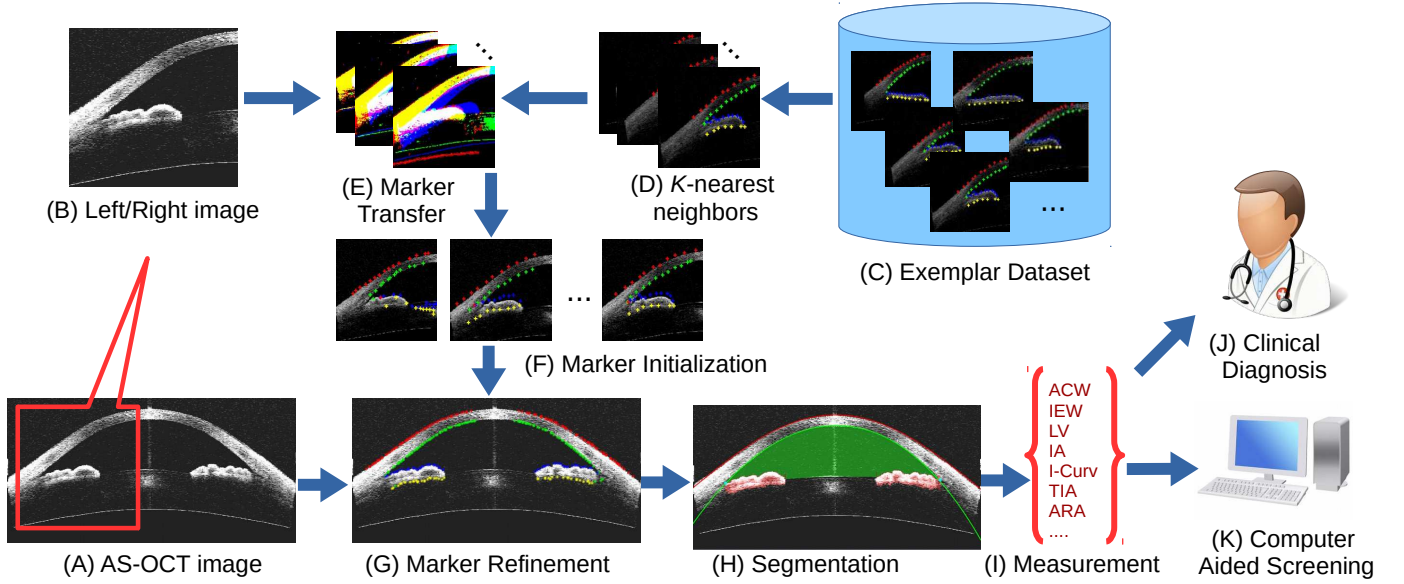


Fig. 3. Flowchart of our proposed method. (A) Given an AS-OCT image, we divide it into (B) left/right images, and retrieve (D) its K -nearest neighbors from (C) the exemplar dataset. Then (E) marker transfer is employed to obtain (F) the initial markers. After that, (G) these markers are refined and employed to (H) guide the segmentation of major structures. Finally, (I) clinical parameters are measured for (J) clinical diagnosis or (K) automatic angle-closure glaucoma screening.

subjects. Moreover, the measured clinical parameters can be used not only to support clinicians in making anatomical assessments, but also to serve as features for detecting anterior angle closure in automatic glaucoma screening algorithms. Our tests on two clinical AS-OCT datasets demonstrate encouraging performance of this method.

II. PROPOSED METHOD

As illustrated in Fig. 3, our method proceeds as follows. Given an AS-OCT image, we first retrieve the K -nearest neighbors from the labeled exemplar dataset, and transfer the labels to estimate initial marker locations in the input image. These markers are refined based on a graph-based model that utilizes prior structural information. The refined markers are then used to guide the segmentation of major structures. Finally, clinical parameters are calculated and used to support clinical assessment or automatically detect anterior angle closure for glaucoma screening.

A. Marker Transfer

Our marker transfer approach takes inspiration from the recent success of data-driven techniques that transfer label information from one image to another [32]–[35]. The AS-OCT image is first cropped into left/right images. Then the initial markers are obtained via transfer from the closest matching images in an exemplar dataset, which is composed of various AS-OCT images containing markers labeled manually by ophthalmologists. These images span various AS-OCT modalities and patients. In our method, the markers are placed along the ACA boundary, which is separated into four parts, namely the corneal epithelium/endothelium and the upper/lower iris layers, as shown in Fig. 3 (C). The use

of boundary markers for this transfer is motivated by the following: 1) Markers on boundaries are more stable to locate than those within the iris or cornea regions; 2) Boundary alignment is a priority for most registration methods; 3) Manual labeling of boundary markers is much more feasible than completely tracing the boundaries over a large exemplar set; and 4) A set of approximate boundary points provided by the transferred markers is sufficient to initialize the subsequent steps in our algorithm.

From this exemplar dataset, we retrieve the K -nearest neighbors for the left/right image ($K = 5$ in our implementation) based on the Edge Orientation Histogram (EOH) feature [36], [37]. EOH is calculated based on the Canny edge detector and Sobel masks. The Canny edge detector is used to generate an edge map for the input image, and Sobel masks are employed to calculate five orientation gradients. The input image is divided into 4×4 non-overlapping rectangular regions, and we calculate the EOH for each region, yielding a feature of $4 \times 4 \times 5 = 80$ dimensions. Then the Euclidean distance is used to calculate the similarity between the input image and the exemplars. Finally, we directly transfer all the retrieved exemplar markers to the input image to serve as the initial markers, as shown in Fig. 4 (A).

B. Marker Refinement

Due to inaccuracies in direct marker transfer, some refinement of the initial markers is needed. In our work, we employ a graph-based smoothing method, which generates a graph $\mathcal{G} = \langle \mathcal{V}, \mathcal{E} \rangle$ with a set of nodes \mathcal{V} and edges \mathcal{E} . Each node $n \in \mathcal{V}$ can take a state u_n in a discrete space and has an associated unary energy function $\Psi(u_n)$. In our work, each initial marker p is represented as one node, and a vertical pixel list \mathbf{L}_p of length l ($l = 20$ in this paper) centered on initial

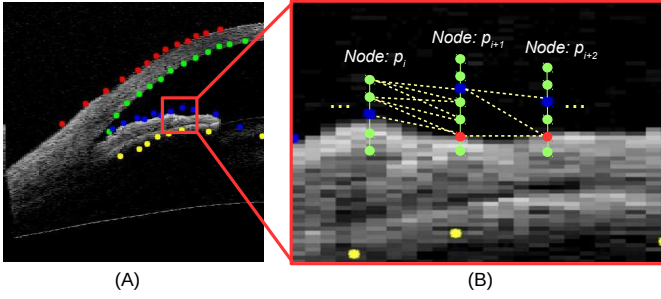


Fig. 4. (A): Initial markers of the AS-OCT image after marker transfer, where the red, green, blue, and yellow points denote the markers for the corneal epithelium/endothelium and the upper/lower iris, respectively. (B): A zoom-in region of the AS-OCT image, where each marker p_i is represented as a node in the graph, and the vertical pixel candidates centered on initial marker p_i (green points) are the states of corresponding node p_i . The refined markers (red points) are optimized by our graph-based processing.

marker p is extracted as the candidate states of the node, as shown in Fig. 4 (A). The edge $(n, m) \in \mathcal{E}$ connecting nodes n and m has an associated pairwise energy function $\Phi(u_n, u_m)$. The overall objective function of our refinement is as follows:

$$E_g(\mathbf{u}) = \sum_{n \in \mathcal{V}} \Psi(\mathbf{u}_n) + \sum_{(n,m) \in \mathcal{E}} \Phi(\mathbf{u}_n, \mathbf{u}_m). \quad (1)$$

The configuration of states $\mathbf{u} = \{\mathbf{u}_1, \dots, \mathbf{u}_{|\mathcal{V}|}\}$ can be obtained by minimizing Eq. (1).

Unary term $\Psi(u_n)$ reflects the likelihood that a pixel candidate lies on a boundary, which is defined as

$$\Psi(u_n) = U_g(u_n) \cdot U_p(u_n), \quad (2)$$

where $U_g(u_n)$ is the vertical gradient magnitude of candidate u_n , encouraging the refined point to adhere to a boundary. $U_p(u_n)$ denotes structural prior information, where $U_p(u_n) = 1$ if the initial marker u_n is on the corneal epithelium or upper iris, and $U_p(u_n) = -1$ otherwise. This term is based on the observation that from top to bottom in an AS-OCT image, the upper boundaries of the cornea and iris go from dark to bright, and lower boundaries go from bright to dark.

Pairwise term $\Phi(u_n, u_m)$ provides a spatial smoothness constraint between neighboring markers, and we define this term as follows:

$$\Phi(u_n, u_m) = D_s(u_n, u_m) \cdot D_f(u_n, u_m), \quad (3)$$

where $D_s(u_n, u_m)$ represents a spatial penalty measured as the vertical coordinate difference between nodes u_n, u_m , which encourages markers to form a smooth layer. And $D_f(u_n, u_m)$ is the l_2 -norm similarity between the features of nodes u_n, u_m , which are taken simply as the intensity in a 5×5 region around the candidate.

Our refined markers are thus obtained based on a combination of boundary magnitude $U_g(\cdot)$, structural information $U_p(\cdot)$, spatial smoothness $D_s(\cdot, \cdot)$, and feature similarity $D_f(\cdot, \cdot)$ constraints. Eq. 1 can be optimized by using existing energy minimization methods (e.g., TRW-S [38], A*search [39]) to obtain a good approximate solution.

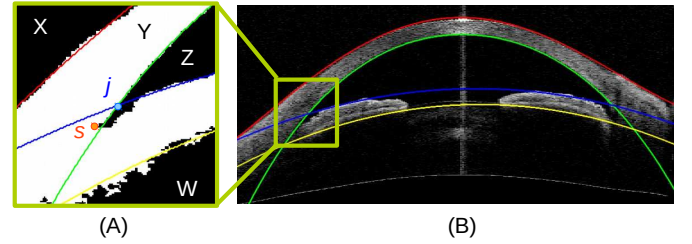


Fig. 5. (A): Regions in the binary image centered on junction j . The trabecular-iris contact s is located at the bottom-left corner of the top-right black region Z . (B): The AS-OCT image with fitted curves.

C. AS-OCT Structure Segmentation

Based on the localized markers, we segment three major structures of the AS-OCT image: the corneal boundary, iris region, and trabecular-iris contact.

Corneal boundary: The corneal boundary, including the corneal epithelium and endothelium, can be considered as a smooth curve. To the corresponding refined markers, a fourth order polynomial (also used in [20]) is fit to obtain the corneal boundary, as shown in Fig. 5 (B).

Iris region: The shape and location of the iris varies among different AS-OCT images, which makes it difficult to detect using a fixed pattern. With our transferred markers, we can detect the iris region reliably. We first fit two curves to the upper/lower boundary of the iris region based on the markers, as shown by the blue and yellow curves in Fig. 5 (B). Then we threshold the region between these two curves and obtain the iris areas by selecting the two maximum connecting regions, which determines one endpoint of the iris. The threshold value is set using Otsu's thresholding method. The other endpoint of the iris is determined by the trabecular-iris contact. In practice, we slightly expand the region between the two iris curves prior to thresholding, to account for iris morphologies such as plateau iris that do not closely fit a curve.

Trabecular-iris contact (TIC): The trabecular-iris contact is the key biomarker in the AS-OCT image, as it is used to localize the ACA position and iris endpoint. In our method, we first calculate the junction of the fitted corneal endothelium and upper iris curve, and crop a region of interest (ROI) of size 200×200 centered on the calculated junction. Then, we threshold this ROI using the same thresholding value as in the iris region segmentation, and perform morphological operations (dilation and erosion) to remove isolated noise pixels. After that, the ROI region can be divided into four major connecting regions as shown in Fig. 5 (A). The trabecular-iris contact s is located at the bottom-left corner of the top-right black region (region Z in Fig. 5 (A)).

D. Clinical Parameter Measurement

With the AS-OCT segmentation, we calculate the anatomical parameters needed for clinical assessment and that have been shown to be discriminative features for automatic glaucoma classification. The major clinical parameters used in our work are listed as follows [5], [26], [40]:

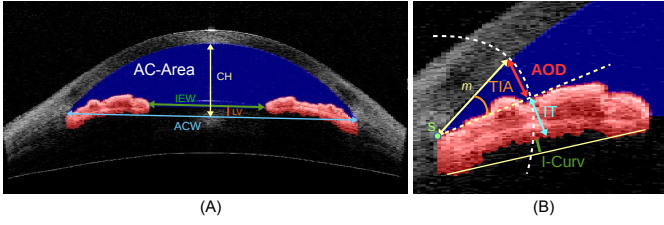


Fig. 6. The clinical parameters of AS-OCT. (A) Global AS-OCT parameters. AC-Area: Anterior Chamber Area. IEW: Iris Endpoint Width. LV: Lens-Vault. ACW: Anterior Chamber Width. CH: Chamber Height. (B) Local angle parameters, where point s denotes the Trabecular-iris contact, and m is the angle opening distances. TIA: Trabecular Iris Angle. AOD: Angle Opening Distance. IT: Iris Thickness. I-Curv: Iris Curvature.

- 1) **Anterior Chamber Width (ACW)**: distance between the two TIC points, along the blue line in Fig. 6 (A).
- 2) **Iris Endpoint Width (IEW)**: shortest distance between the two iris endpoints, along the green line in Fig. 6 (A).
- 3) **Lens-Vault (LV)**: perpendicular distance between the anterior pole of the lens and the horizontal line joining the two TIC points [41], along the red line in Fig. 6 (A).
- 4) **Chamber Height (CH)**: perpendicular distance between the anterior chamber and the horizontal line joining the two TIC points, as the yellow line in Fig. 6 (A).
- 5) **Chamber Height Ratio (CHR)**: the ratio of Chamber Height to Lens-Vault.
- 6) **Anterior Chamber Area (AC-Area)**: cross-sectional area of the anterior segment bounded by the endothelium, iris, and anterior surface of the lens, shown as the blue shaded region in Fig. 6 (A).
- 7) **Anterior Chamber Volume (AC-Vol)**: calculated by rotating the ACA 360° around its central vertical axis.
- 8) **Iris Area (IA)**: cumulative cross-sectional area along the full length of the iris, shown as the red shaded region in Fig. 6 (B).
- 9) **Iris Curvature (I-Curv)**: calculated by drawing a line from the most peripheral to the most central points of the iris pigment epithelium, extending a perpendicular line to the iris pigment epithelium at its point of greatest convexity, and taking the length of this line [5], indicated by the green line in Fig. 6 (B).
- 10) **Trabecular Iris Angle (TIA)**: angle at the apex of the iris recess defined between lines extending through a point on the trabecular meshwork at a distance m from the TIC point, shown as the orange angle in Fig. 6 (B).
- 11) **Angle Opening Distance (AOD)**: length of the line segment between the cornea and iris at distance m , along the red line in Fig. 6 (B).
- 12) **Angle Recess Area (ARA)**: area bounded by the AOD line, corneal endothelium and the iris.
- 13) **Iris Thickness (IT)**: thickness of the iris at a distance m from the TIC, along the blue line in Fig. 6 (B).

Parameters 1-7 are global AS-OCT parameters of dimension 1, and 8-9 are local angular parameters of dimension 1. Parameters 10-13 are also local angular parameters but with different angle opening distances ($m = \{750, 1000, 1200\} \mu\text{m}$), as shown in Fig. 6 (B), thus each of them has $|m|$ dimensions

TABLE II
ERROR SCORES (UNIT: PIXEL) IN PIXELS FOR DIFFERENT STEPS OF OUR METHOD. IE: IRIS ENDPOINT. 1 PIXEL \approx 0.016 MM

	TIC Err.	IE Err.	ACW Err.	IEW Err.
Baseline [20]	14.45	-	18.69	-
Transfer	21.26	24.91	23.26	37.38
Fitted curve	12.94	18.41	17.51	9.61
Final result	10.47	5.16	12.87	6.51

for each angle.

III. EXPERIMENTS

A. Segmentation Evaluation

The first experiment is for evaluating segmentation. In our experiments, the AS-OCT images (from a Carl Zeiss Visante AS-OCT) are centered on the pupil, and one cross-sectional horizontal scan (nasal-temporal angles at 0° - 180°) is evaluated for each subject. We collected 100 Visante AS-OCT images, where the TIC points and iris endpoints are labeled manually as the ground truth, and ACW and IEW are calculated from them. We evaluate our method on this dataset and measure the following four error scores: point distances for TIC and iris endpoint, and the absolute width for ACW and IEW.

We report the results of our method, including at two intermediate steps. The first result is determined after the marker transfer step, using the initial markers directly. The second result is from points computed by fitting a curve to the refined markers. The last is our final result with all refinement and segmentation steps. We additionally report results of the TIC detection method [20] as a baseline. The TIC method [20] is highly dependent on detecting the feature change along the lower boundary of the cornea in an HD-OCT image, which is hard to observe in a low resolution OCT (e.g., Visante OCT). Thus in our implementation we extract the HOG feature within small windows (50×50) along the corneal boundary to detect the feature change and localize the TIC point. Note that the TIC method [20] does not segment the iris region, thus only comparisons to TIC and ACW scores can be done. The performance scores are shown in Table II. Due to the low resolution of the Visante OCT image, the feature change is slight and the TIC is hard to detect by using [20]. Its performance is only better than the initial marker transfer of our method. In our method, the result of marker transfer is rough and has large error. The marker refinement step deals with outliers and improves performance by using fitted curves. Our final result obtains the best performance on all point localizations and measurements. Some visual results of our method are shown in Fig. 7. Our method segments the corneal boundary, iris region, and TIC accurately for different ACA shapes and positions in the AS-OCT images.

B. Screening Evaluation

The second experiment is on angle-closure glaucoma screening using clinical measurements obtained by our method. In this experiment, a total of 4135 Visante AS-OCT images from 2113 subjects are collected to generate the clinical dataset. Each AS-OCT image is split into two ACA

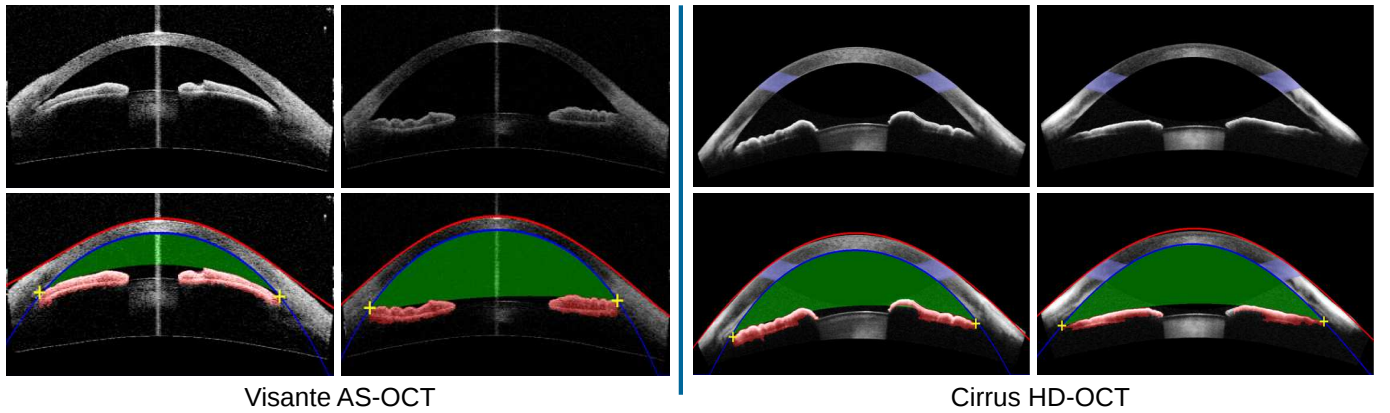


Fig. 7. Segmentation results of our proposed method on Visante AS-OCT and Cirrus HD-OCT images, where the corneal boundaries are marked by red and blue curves, and the iris and anterior chamber regions are indicated by red and green shading, respectively. (Note that the pale blue colors of Cirrus HD-OCT images, also seen in Fig. 2, are generated by the Cirrus machine, not by our method.)

sub-images (8270 ACA sub-images in total), since each image contains two ACA regions and the right ACA sub-image is flipped horizontally. For each ACA sub-image, the ground truth label of open-angle or angle-closure is determined by majority from three ophthalmologists. The data contains 7375 open-angle and 895 angle-closure cases. The dataset is divided equally and randomly into training and testing sets.

We repeat each algorithm 50 times and report the mean and standard deviations. We employ five evaluation criteria to measure the performance: Balanced Accuracy, Sensitivity, Specificity, Precision and F-measure. The Sensitivity (Sen), Specificity (Spe), and Precision (Pre) are defined as:

$$Sen = \frac{TP}{TP + FN}, Spe = \frac{TN}{TN + FP}, Pre = \frac{TP}{TP + FP},$$

where TP and TN denote the number of true positives and true negatives, respectively, and FP and FN denote the number of false positives and false negatives, respectively. The F-measure (F_m) and Balanced Accuracy (B_{Acc}) are as follows:

$$F_m = \frac{2TP}{2TP + FP + FN}, B_{Acc} = \frac{1}{2}(Sen + Spe).$$

We additionally report the ROC curves and area under ROC curve (AUC).

Our evaluation utilizes five classification algorithms for the detection of gonioscopic angle closure, including k-Nearest Neighbor, Naive Bayes, Random Forest, AdaBoost, and Linear SVM. The performances are reported in Table III and Fig. 8(a). k-Nearest Neighbor (kNN) is a non-parametric method based on the k closest training examples in the feature space, with the prediction set to the most common label among the k nearest neighbors ($k = 5$ in our experiment). Naive Bayes classification estimates the probability based on applying Bayes' theorem under the assumption that the covariates are independent and conditional on class membership. From the results, we observe that k-Nearest Neighbor and Naive Bayes do not perform well on our Visante AS-OCT dataset. Random Forests and AdaBoost are both ensemble learning methods, where Random Forests is bagging algorithm and AdaBoost is

a boosting algorithm. We set the tree numbers to 50 in our experiment. These two classifiers obtain similar performance on the AS-OCT classification task. The last classifier is Linear SVM, which constructs a hyperplane or a set of hyperplanes in a higher dimensional space to separate feature points. Linear SVM achieves the best scores in this experiment.

C. Performance with Visual Features

In this experiment, we examine the use of visual features instead of clinical parameters for glaucoma classification. In [21], the ACA region is localized based on geometric structure, and then visual features (e.g., HOG [42]) are extracted to classify the glaucoma subtype. In our implementation, we use the TIC obtained by our method as the center of the ACA region, and follow [21] by using HOG features to classify the glaucoma subtype on the Visante AS-OCT dataset. The results are shown in Table IV and Fig. 8(b). Our visual feature classification (VF) outperforms the original method in [21], which reports a 0.835 AUC and a 0.758 Balanced Accuracy for ACA images. We also found that classification with visual features (VF) is better than with just clinical parameters (CP). The more fundamental reason is that clinical parameter have already a prior on what information clinicians currently use, while visual features identify a wider set of image properties some of which are unrelated with what clinicians seem to recognize as relevant. Hence, visual feature have more image information, and more discriminative capacity than clinical parameters. Clinical parameters are nevertheless important to recover for clinical assessment. Combining the two types of features (CP + VF) produces the best performance on the Visante AS-OCT dataset. Moreover, our results are comparable to those of Niwas *et al.* [26], which achieves 0.866 Accuracy by using a Laplacian score feature selection method. Note that the ACA measurements used in [26] are measured manually, so it is not an automatic method.

D. Multiple Modality Evaluation

A major advantage of our system is its ability to deal with different AS-OCT imaging modalities. In this experiment, we

TABLE III
PERFORMANCES (*Mean ± Std*) OF DIFFERENT CLASSIFIERS USING CLINICAL MEASUREMENTS ON THE VISANTE AS-OCT DATASET.

	Balanced Accuracy	Sensitivity	Specificity	Precision	F-measure
k-Nearest Neighbor	0.770 ± 0.019	0.740 ± 0.071	0.800 ± 0.037	0.462 ± 0.073	0.528 ± 0.031
Naive Bayes	0.786 ± 0.013	0.722 ± 0.031	0.850 ± 0.019	0.377 ± 0.033	0.494 ± 0.027
Random Forest	0.814 ± 0.014	0.774 ± 0.034	0.855 ± 0.012	0.401 ± 0.016	0.526 ± 0.022
AdaBoost	0.812 ± 0.014	0.773 ± 0.033	0.850 ± 0.014	0.392 ± 0.027	0.519 ± 0.024
Linear SVM	0.828 ± 0.010	0.807 ± 0.024	0.851 ± 0.013	0.402 ± 0.028	0.536 ± 0.023

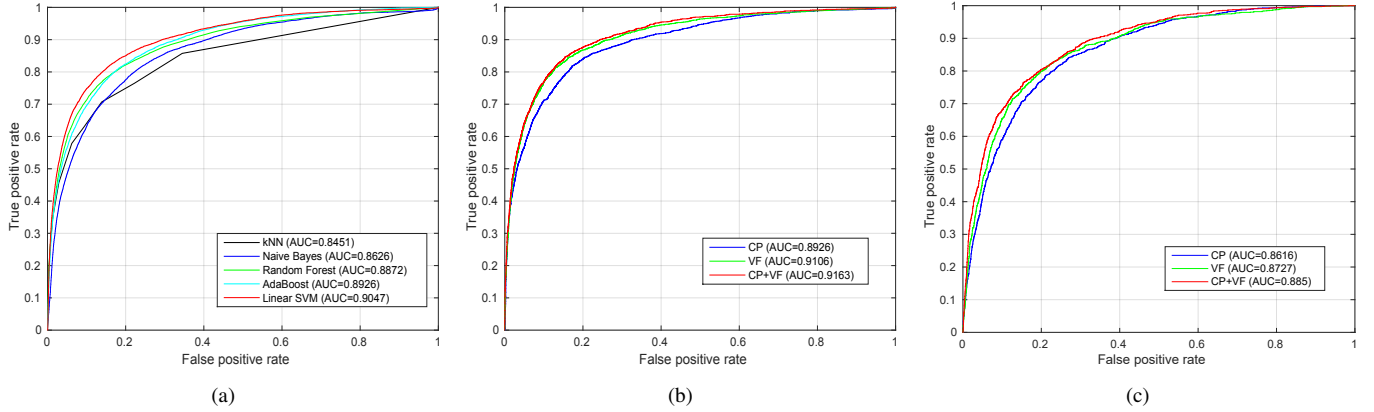


Fig. 8. (A) Performances of different classifiers on the Visante AS-OCT dataset. (B) Performances of Clinical Parameter (CP) and Visual Feature (VF) on the Visante AS-OCT dataset. (C) Performances of CP and VF on the Cirrus HD-OCT dataset.

TABLE IV
PERFORMANCES (*Mean ± Std*) OF DIFFERENT FEATURES WITH LINEAR SVM ON VISANTE AS-OCT DATASET.

	Balanced Accuracy	Sensitivity	Specificity	Precision	F-measure
Clinical Parameter	0.830 ± 0.011	0.810 ± 0.024	0.850 ± 0.012	0.410 ± 0.024	0.553 ± 0.020
Visual Feature	0.860 ± 0.011	0.869 ± 0.032	0.851 ± 0.017	0.423 ± 0.030	0.581 ± 0.022
Combination	0.872 ± 0.018	0.886 ± 0.037	0.862 ± 0.019	0.438 ± 0.032	0.610 ± 0.024

test our method on another modality, Zeiss Cirrus HD-OCT. Some visual segmentation results are shown in Fig. 7. It can be seen from the figure that the image structure for Cirrus HD-OCT is different from that of Visante AS-OCT. In Cirrus HD-OCT, post-processing is done during AS-OCT imaging, which makes the corneal boundary clearer. However, the iris posterior and the contact point of iris and cornea are not obvious, as shown in Fig. 2. Because of the data-driven marker localization, our method performs well and is robust for Cirrus HD-OCT.

For quantitative evaluation, we collected a Cirrus HD-OCT dataset, with 1402 ACA images in total (1102 open-angle and 300 angle-closure). The performances are shown in Table V and Fig. 8(c). Results using the feature combination (CP + VF) were found to be best. Note that due to the missing iris posterior and contact point of the iris and cornea, the scores for Cirrus HD-OCT are lower than those for Visante AS-OCT.

E. Discussion

1) *Exemplar Dataset*: In our method, we utilize the same exemplar dataset directly for different OCT machines. This is based on the observation that the relative positions of the cornea and iris are roughly consistent in different AS-OCT images after image normalization. For dividing the image into left/right images, we crop the image by tightening the ACA

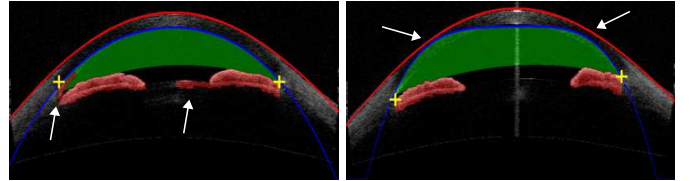


Fig. 9. Challenging cases for our segmentation method.

region to remove the excess margin and resize the cropped image to the same size as the exemplar. In this paper, we collect more than 20000 ACA images from Visante AS-OCT and use K-means to cluster them into 50 groups. The image of each cluster center is selected as an exemplar in the exemplar dataset. This exemplar data is utilized in both the Visante and Cirrus AS-OCT experiments.

2) *Running Time*: We run our method using a workstation with a Xeon 2.7GHz CPU and 64GB RAM. The code is implemented without optimizations in MATLAB 2014 (Natick, MA). Typically, our method takes less than 10 s for segmenting and measuring one AS-OCT image.

3) *Limitation*: Our method segments the corneal boundary, iris region, and trabecular-iris contact accurately for different iris shapes and positions in the AS-OCT images. One limitation of our method is that shadows within an AS-OCT image

TABLE V
PERFORMANCES (*Mean ± Std*) OF DIFFERENT FEATURES WITH LINEAR SVM ON THE CIRRUS HD-OCT DATASET.

	Balanced Accuracy	Specificity	Sensitivity	Precision	F-measure
Clinical Parameter	0.779 ± 0.029	0.850 ± 0.039	0.708 ± 0.063	0.527 ± 0.074	0.599 ± 0.048
Visual Feature	0.796 ± 0.031	0.851 ± 0.032	0.742 ± 0.053	0.536 ± 0.067	0.620 ± 0.053
Combination	0.802 ± 0.026	0.850 ± 0.032	0.753 ± 0.044	0.541 ± 0.063	0.627 ± 0.045

may lead to distortions of the iris shape, as shown in the first image of Fig. 9. This is a failure case for our method that is also a challenge for other segmentation methods and even ophthalmologists. Another challenging case is low contrast, which may lead to mis-segmentation as shown for the corneal boundary in the second image of Fig. 9.

4) *Comparison:* We compare the existing AS-OCT assessment methods with our method in Table VI. The work in [20] only deals with segmentation and detection, without providing glaucoma screening results. The method in [24] obtains outstanding performance with fuzzy kNN classification, but works only on the Casia SS-1000 OCT modality, which is a high-definition (HD) mode of SS-OCT imaging, and has been evaluated on just a small data size. Xu's methods in [21], [23] employ different visual features to classify angle-closure glaucoma, but they cannot produce clinical measurements. Our work is evaluated on two AS-OCT modalities, Visante AS-OCT and Cirrus HD-OCT, and the data sizes are the largest in each AS-OCT modality. Our method also achieves satisfactory performance.

IV. CONCLUSION

In this paper, we proposed an automatic anterior chamber angle segmentation and measurement method for AS-OCT imagery. The key contributions of this work are the introduction of marker transfer from labeled exemplars to generate initial markers, and segmentation of the corneal boundary and iris regions to obtain clinical ACA measurements. The experiments on both the Visante AS-OCT and Cirrus HD-OCT datasets demonstrate the effectiveness and robustness of our method. Potential applications of our proposed method include clinical anatomical assessment, automatic angle-closure glaucoma screening, and statistical analysis of large clinical datasets.

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TABLE VI

A COMPARISON OF THE EXISTING AS-OCT ASSESSMENT METHODS. CP: CLINICAL PARAMETER, VF: VISUAL FEATURE. DATA SIZE: THE NUMBER OF ACA SUB-IMAGES.

Method	Image Modality	Data Size	Feature	Classifier	Performance
Tian <i>et al.</i> [20]	Cirrus HD-OCT	40	CP	-	-
Xu <i>et al.</i> [21]	Visante AS-OCT	4096	VF (HOG)	Linear SVM	AUC= 0.835, BAcc= 0.758
Xu <i>et al.</i> [23]	Visante AS-OCT	4096	VF (HEP)	Linear SVM	AUC= 0.921, BAcc= 0.840
Ni Ni <i>et al.</i> [24]	Casia SS-1000 OCT	264	CP + VF (Shape)	fuzzy kNN	AUC = 0.98, BAcc = 0.99
Our method	Visante AS-OCT	8270	CP + VF (HOG)	Linear SVM	AUC = 0.916, BAcc = 0.872
Our method	Cirrus HD-OCT	1406	CP + VF (HOG)	Linear SVM	AUC = 0.885, BAcc = 0.802

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